



(51) International Patent Classification:

A61B 17/56 (2006.01) A61B 17/80 (2006.01)
A61B 17/60 (2006.01)

(21) International Application Number:

PCT/US2015/052373

(22) International Filing Date:

25 September 2015 (25.09.2015)

(25) Filing Language:

English

(26) Publication Language:

English

(30) Priority Data:

62/056,276	26 September 2014 (26.09.2014)	US
62/108,503	27 January 2015 (27.01.2015)	US
14/666,095	23 March 2015 (23.03.2015)	US

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(81) Designated States (unless otherwise indicated, for every
kind of national protection available): AE, AG, AL, AM,

AO, AT, AU, AZ, BA, BB, BG, BH, BN, BR, BW, BY,
BZ, CA, CH, CL, CN, CO, CR, CU, CZ, DE, DK, DM,
DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT,
HN, HR, HU, ID, IL, IN, IR, IS, JP, KE, KG, KN, KP, KR,
KZ, LA, LC, LK, LR, LS, LU, LY, MA, MD, ME, MG,
MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM,
PA, PE, PG, PH, PL, PT, QA, RO, RS, RU, RW, SA, SC,
SD, SE, SG, SK, SL, SM, ST, SV, SY, TH, TJ, TM, TN,
TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA, ZM, ZW.

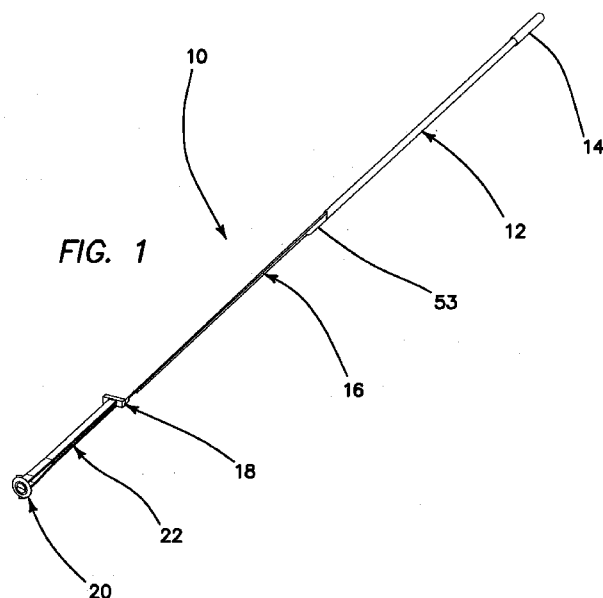
(84) Designated States (unless otherwise indicated, for every
kind of regional protection available): ARIPO (BW, GH,
GM, KE, LR, LS, MW, MZ, NA, RW, SD, SL, ST, SZ,
TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, RU,
TJ, TM), European (AL, AT, BE, BG, CH, CY, CZ, DE,
DK, EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU,
LV, MC, MK, MT, NL, NO, PL, PT, RO, RS, SE, SI, SK,
SM, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ,
GW, KM, ML, MR, NE, SN, TD, TG).

Published:

- with international search report (Art. 21(3))
- before the expiration of the time limit for amending the
claims and to be republished in the event of receipt of
amendments (Rule 48.2(h))

(54) Title: IMPLANT DEVICES AND SYSTEMS FOR STABILIZED FIXATION OF BONE AND SOFT TISSUE

FIG. 1



(57) Abstract: An implant system for providing stabilized fixation of tissue includes a button having a slot, a band threaded through the slot, and a lock including a member having a slot for receiving an end of the band and a movable member for clamping the band in place. The movable member is movable between an open position and a locking position. The lock is a plug assembly which includes a flange. The slot is disposed in the flange. The movable member is a cap which is movable between clamping and non-clamping orientations relative to the flange. The plug assembly further comprises a screw for moving the cap between its clamping and non-clamping orientations relative to the flange. The flange is a portion of a plug, which plug further includes a boss extending from one side of the flange.

IMPLANT DEVICES AND SYSTEMS FOR STABILIZED FIXATION OF BONE AND SOFT TISSUE

Background of the Invention

5 A syndesmosis is a slightly movable articulation where the contiguous bony surfaces are united by an interosseous ligament. If the syndesmosis is separated because of bone fracture, surgeons will sometimes fix the relevant bones together with a syndesmotic screw. The screw inhibits normal movement of the bones and, thereby, the corresponding joint or joints. When the natural articulation is healed, the screw may be removed.

10 Syndesmosis screws have significant problems, including loosening, breakage, the need for removal, and late diastasis. The present invention has been developed to address these problems, by providing a low profile implant device intended to facilitate stabilized fixation of tissues, including bone and soft tissue to bone, for syndesmosis repair, as well as other applications.

Summary of the Invention

15 The inventive implant system comprises a low profile implant device intended to provide stabilized fixation of tissue to facilitate syndesmosis repair. These tissues include bone and soft tissue to bone. The inventive system can provide stabilized fixation for bone fractures, osteotomies, and arthrodesis, plus soft
20 tissue to bone attachment. The system design applies a restorative fixation force across the tissue segments to stabilize them. The rigidity and compliant nature of the inventive implant provides rigid and consistent fixation during the healing phase.

The implant is delivered through a pre-drilled hole through the tibia and fibula by means of a guide needle delivery, exiting the skin opposite the initial insertion site. The flat band is secured to the bone by pulling the narrow button through both the tibia and fibula bones and then toggled into position to create tension across the two segments. Once the button is secure against the bone, the suture attached to the needle can be cut and removed from the operative site. Pulling the flat suture tails against the lock at the initial insertion site will tension the band and bone segments into place. The inventive implant system offers syndesmosis repair with a knotless closure.

10 The inventive implant is supplied as a one-size-fits-all single-use sterile implant. A kit containing one or more inventive implants, packaged for use in a single procedure, also contains a band of the type described in prior U.S. Application Serial No. 14/449,878, already expressly incorporated herein by reference, in its entirety.

15 The inventive implant system and method are intended for use as an adjunct in fracture repair involving metaphyseal and periarticular small bone fragments where screws are not indicated, and as an adjunct in external and intramedullary fixation systems involving plates and rods, with fracture braces and casting. Specifically, the inventive implant is intended to provide fixation during the healing process following a syndesmotic trauma, such as fixation of syndesmosis (syndesmosis disruptions) in connection with Weber B and C ankle fractures.

25 Although the inventive implant system is targeted to repair syndesmosis injuries of the ankle, it has application to other suitable types of repair as well, including, for example the shoulder.

In operation, the implant system is placed after pre-drilling by the practitioner. Standard drill, drill bits, and drill guides typically associated with orthopedic surgery are used to conduct the procedure. After appropriate reduction

of the tibia and fibula bones, the operative technique is to A) first pass the guide needle through and out of the medial skin, B) pull through the lead, "narrow" button that is attached to the cortical surface so that it slips across and engages onto the medial tibial cortex, and D) pull on the implant suture tails to tighten and lock
5 the proximal button.

After passing the distal button through the pre-drilled holes by means of the pass-through needle, reduction of the ankle joint is achieved by applying tension to the band and the metallic button. Fixation forces are activated by pulling on the suture tails after removing the pass-through needle and pass-through sutures and
10 using a screwdriver to tighten the screw. A hand-held stainless steel tensioner instrument is considered if higher tension levels are necessary to meet physiological requirements.

The inventive implant is a sterile device using common implant materials, such as stainless steel or titanium, or other suitable materials. Bio-absorbable
15 materials may also be considered for the implant system and the narrow button mechanism. The flat band is constructed of polyester suture material, or a suitable Ultra-High Molecular Weight Polyethylene (UHMWPE). Materials used in the deployment of the implant comprise suture material, a stainless steel guide needle, and a plastic protective cap.

20 Possible associated instrumentation, such as a stainless steel hand-held instrument tensioner or anti-rotation tool may be used if the mechanism requires higher levels of tensioning.

More particularly, in one aspect of the invention there is provided an implant system for stabilized fixation of tissue. The system comprises a button
25 having a slot, a band threaded through the slot, and a lock comprising a member having a slot for receiving an end of the band and a movable member for clamping the band in place. The movable member is movable between an open position and a locking position. The button comprises a pair of slots and the band is threaded

through each of the pair of slots in sequence, so that the band is wrapped around a portion of the button separating the two slots. The band, in present embodiments, is formed of suture material, such as a length of flat suture material, which can be threaded through the pair of slots of the button and through the slot of the lock so
5 that between the button and the lock the band comprises the length of suture doubled over itself.

The lock comprises a plug assembly which includes a flange. The slot is disposed in the flange. The movable member comprises a cap which is movable between clamping and non-clamping orientations relative to the flange. The plug
10 assembly further comprises a screw for moving the cap between its clamping and non-clamping orientations relative to the flange.

A second slot is provided in the flange, so that the band may be threaded through the first slot in the flange, cross a surface of the flange, and then extend through the second slot in the flange, thereby securing the band to the flange. The
15 flange comprises a portion of a plug, the plug further comprising a boss extending from one side of the flange.

When the band is threaded through the slots of the flange, each end of the band extends along a length of the boss. Accordingly, the boss may comprise flat surfaces disposed along its length for accommodating the band ends extending
20 therealong.

The implant system further comprises a suture tether attached to the button, and further comprises a guide needle attached to the suture tether, for assisting in positioning the implant as desired at a procedural site.

In another aspect of the invention, there is provided a lock for use in an
25 implant system for stabilized fixation of tissue. The lock comprises a member having a slot for receiving an end of a band and a movable member for clamping the band in place. The movable member is movable between an open position and a locking position. The lock comprises a plug assembly which includes a flange.

The slot is disposed in the flange. The movable member comprises a cap which is movable between clamping and non-clamping orientations relative to the flange. The plug assembly further comprises a screw for moving the cap between its clamping and non-clamping orientations relative to the flange.

5 A second slot is provided in the flange, so that a band may be threaded through the first slot in the flange, cross a surface of the flange, and then extend through the second slot in the flange, thereby securing the band to the flange. The flange comprises a portion of a plug, the plug further comprising a boss extending from one side of the flange.

10 When a band is threaded through the slots of the flange, each end of the band extends along a length of the boss. Accordingly, the boss may comprise flat surfaces disposed along its length for accommodating the band ends extending therealong.

In yet another aspect of the invention, there is disclosed a method for
15 effecting repair of tissue using a tissue fixation band apparatus comprising a lock, a button, and a suture band, under tension, extending between the lock and the button. The inventive method comprises a step of pulling the button through a hole extending through the tissue to be repaired, until it exits a distal surface of the tissue and engages the distal surface of the tissue. Then, the suture band is pulled
20 on each end to locate the lock in position on a proximal surface of the tissue. Additional steps include applying tension to free ends of the suture band exiting from the lock of the fixation band apparatus to tension the suture band to a desired level and causing a movable clamping member within the lock to move to a locking position, to thereby engage the lock and clamp the suture band in place at the
25 desired tension level.

More specifically, the causing step comprises tightening a screw to cause the movable clamping member to move to its locking position. The lock comprises a plug assembly and the movable clamping member comprises a cap.

In another aspect of the invention, there is disclosed a method for effecting repair of tissue using a tissue fixation band apparatus comprising a lock, button and a suture band, under tension, extending between the lock and the button. The inventive method in accordance with this aspect of the invention is similar to that
5 previously described. However, for procedures such as Lis franc or other procedures involving smaller bone and lower strength requirements, a smaller hole may be used. Therefore, a smaller suture and implant embodiment may be used.

In another aspect of the invention, there are disclosed embodiments that may be more suitable for use with some bone fracture repair plates.

10 The invention, together with additional features and advantages thereof, may best be understood by reference to the following description taken in conjunction with the accompanying illustrative drawings.

Brief Description of the Drawings

Fig. 1 is an isometric view of an implant system constructed in accordance
15 with the principles of the present invention;

Fig. 2A is a top isometric view of the assembly of Fig. 1, with suture tether, guide needle and cap excluded for clarity;

Fig. 2B is a bottom isometric view, similar to Fig. 2A, of the assembly of Fig. 1;

20 Fig. 3 is an isometric view of the inventive implant installed with a tibia and fibula, according to one particular method of the present invention;

Fig. 4A is a top exploded isometric view of the plug assembly, including

plug, screw, and cap components of the inventive system;

Fig. 4B is a top isometric view of the plug assembly shown in Fig. 4A;

Fig. 4C is a bottom isometric view of the plug assembly shown in Figs. 4A and 4B;

5 Fig. 5A is a top view of the cap component of the present invention;

Fig. 5B is a cross-sectional view taken along lines 5B-5B of Fig. 5A;

Fig. 5C is a top isometric view of the cap of Figs. 5A and 5B;

Fig. 5D is a bottom isometric view of the cap of Figs. 5A-5C;

Fig. 5E is a side view of the cap of Figs. 5A-5D;

10 Fig. 5F is a bottom view of the cap of Figs. 5A-5E;

Fig. 6A is a top isometric view of the plug component of the present invention;

Fig. 6B is a bottom isometric view of the plug component of Fig. 6A;

Fig. 6C is a top view of the plug component of Figs. 6A-6B;

15 Fig. 6D is a side view of the plug component of Figs. 6A-6C;

Fig. 6E is a bottom view of the plug component of Figs. 6A-6D;

Fig. 7A is a top exploded view of a modified embodiment of the plug assembly, including plug, screw, and cap components of the present invention;

Fig. 7B is a top isometric view of the plug assembly of Fig. 7A;

5 Fig. 7C is a bottom isometric view of the plug assembly of Figs. 7A-7B;

Fig. 8A is a top isometric view of the plug component of the assembly shown in Figs. 7A-7C;

Fig. 8B is a bottom isometric view of the plug component shown in Fig. 8A;

Fig. 8C is a top view of the plug component shown in Figs. 8A-8B;

10 Fig. 8D is a cross-sectional view taken along lines 8D-8D of Fig. 8C;

Fig. 8E is a side view of the plug component shown in Figs. 8A-8D;

Fig. 8F is a bottom view of the plug component shown in Figs. 8A-8E;

Fig. 9 is a top exploded isometric view of an alternative embodiment of the plug assembly, for use in procedures requiring a smaller drilled hole;

15 Fig. 10 is a top exploded isometric view illustrating a variation of Fig. 9 with a smaller diameter cap in relation to the plug;

Fig. 11 is a top exploded isometric view illustrating a variation of Fig. 9, with cap and plug configurations that are nested together; and

Fig. 12 is a top exploded isometric view of another alternative embodiment of the plug assembly, with a smaller diameter plug flange and cap.

5

Description of the Preferred Embodiment

Referring more particularly to the drawings, there is shown in Fig. 1 an implant system 10 for providing stabilized fixation of tissues. The system 10 includes a guide needle 12, a protective cap 14 on one end of the needle 12, to
10 protect the sharp tip of the needle and prevent needle sticks, a suture tether 16 attached at one end to an opposed second end of the guide needle 12, a button 18 attached to an opposed second end of the suture tether 16, a plug assembly 20, and a band 22 joined to and extending between the button 18 and plug assembly 20. Although the dimensions of these components may be varied considerably, within
15 the scope of the invention, in one particular embodiment, the total length of the system is approximately 14 inches, with the length of the band 22, plug 20, and button 18 portion of the system totaling about 3.0 inches, the length of the suture tether 16 being about 5.0 inches, and the length of the guide needle 12 and cap 14 being about 6.0 inches. By itself, in one embodiment, by way of example only, the
20 cap is about 0.77 inches in length.

Figs. 2A and 2B illustrate an implant assembly 23 of the implant system shown in Fig. 1. Notably, the button 18 may be manufactured from a surgical stainless steel or other suitable biocompatible material, such as 316 LVM stainless steel, titanium, or other suitable materials, such as bio-absorbables. Suture 24,
25 comprising the suture band 22, is laced through slots 26 in a frame 28 forming the button 18, prior to use. As noted above, the band 22 is comprised of suture 24,

which is, in particular embodiments, a woven polyester suture made from PET (polyethylene terephthalate), the same polyester as most commercially available sutures, or a suitable UHMWPE. The band may be poly-coated or uncoated. In one embodiment, the suture 24 is provided in an overall length of 36 inches. The
5 suture length between the narrow button 18 and the plug assembly 20 is nominally set to 3 inches, and is adjustable by the practitioner per the anatomical requirements of the patient.

It is noted that the narrow button 18 is small enough to pass through a hole 42 through the tibia and fibula (discussed below), with a suture band attached and a
10 tether suture and guide needle attached. The slots 26 in the button 18 are large enough to lace the suture band therethrough. The edges of the slots are smooth, with an internal radius to prevent band breakage during loading. The thickness of the narrow button is just enough to withstand ankle loads. The sides of the narrow button 18 are contoured in the shape of the hole 42 to provide maximum strength
15 and clearance through the holes in the tibia and fibula.

Now with reference more particularly to Figs. 4A-4C, the plug assembly 20 is shown in greater detail. The plug assembly 20 comprises three main components, namely, a plug 30, a cap 32, and a screw 34. The entire assembly 20 is preferably made of 316 LVM stainless steel or titanium or other suitable
20 biocompatible materials, such as bio-absorbables. The suture 24 is laced through slots 36 in a flange 37 of the plug 30 and the two ends of the suture 24 are tensioned. When the cap 32 is secured with the captive screw 34, as shown in Figs. 4B and 4C, the plug assembly 20 is in a locked orientation.

The screw is of sufficient strength to withstand the loads of tensioning the
25 implant assembly 23 and to endure subsequent stresses after implantation. It preferably has a flat head 35 to allow the fastener to lie flush with the cap 32, and additionally has a cross feature to allow for a standard matching driver. The length

of the screw threads 35a is sufficient to withstand the required loads and provide adjustment of the suture, plug, and cap during installation. The cap 32 has a countersink feature 33 for receiving the flat head 35 of the screw 34, as well as an undersized through hole 33a to keep the screw 34 captive. The cap 32 further has a
5 round body with smooth radii edges to aid in concealing the plug assembly 20 beneath the patient's skin. An internal counter bore 33b provides clearance for the plug flange 37, as well as a load bearing surface for the suture band 22. An internal edge radius assists in tensioning the suture and an additional contact surface traps the suture between the cap edge and the bone.

10 The plug flange 37 is thin, but of sufficient thickness to withstand the stresses of the ankle and thin enough to prevent excessive protrusion. The plug also comprises a boss 48, extending from the flange 37, which is long enough to allow for sufficient thread engagement. Flats 52 on the boss 48 act as clearance between the plug and bone to allow the suture to pass therebetween. A hole 54 in the plug
15 flange accommodates the screw 34.

Again referring to Fig. 1, the guide needle 12 may be made of 302 stainless steel, such as that used for most surgical needles, although other suitable biocompatible materials may be used as well. The needle, in the illustrated embodiment, is 6 inches in length and has a diameter of .078 inches. A 5 inch
20 polyester (PET) suture is used to attach the needle 12 and the narrow button 18, the suture being attached to the needle 12 via an eyelet 53. After placement of the narrow button 18, the suture and the straight needle are discarded.

In operation, the implant assembly 23 is delivered using similar techniques to other syndesmosis repair devices. In one such approach, a 3.6 mm hole 42 is
25 pre-drilled through the cortices of the tibia 38 and fibula 40 (Fig. 3) from the open lateral side 44, for the purpose of repairing a separated syndesmosis 46. After appropriate reduction of the tibial and fibula bones, the straight guide needle 12 of

the implant system 10 is passed through the drilled hole in the tibia and fibula and through the skin on the medial side, taking care to register the narrow button 18 into the pre-drilled hole 42. Tension is applied to the suture tether 16 to pull the narrow button 18 through both the fibula and tibia bones to the medial side, at which point
5 the button 18 is toggled into position, lying flat against the medial cortex of the tibial bone 38, as shown. This creates tension across the two bone segments. At this juncture, the suture tether 16 and needle 12 are removed and discarded. Pulling the suture band 22 lightly on each end brings the lateral plug 30 to rest, flat on the fibula 40, as shown. Using a driver, the screw 34 is rotated within the cap 32 until
10 the screw and cap are tight. The suture ends are then cut. The result is a syndesmosis repair with a knotless closure.

Figs. 7 and 8 illustrate an alternative embodiment of the plug assembly 20, which is particularly useful for providing stabilized fixation in an ACL repair, or other repairs where a separate anchor location is needed. The major difference
15 between the Fig. 7 embodiment and that shown in Figs. 1-6 is that the boss 48 of the Fig. 7 embodiment is substantially greater in length than the boss 48 of the Fig. 1-6 embodiment, and includes an aperture 50 extending laterally therethrough. In the ACL repair scenario, for example, a blind hole in the bone is drilled, the plug 30 is inserted into the hole, and, as the screw 34 is tightened, the plug body,
20 particularly the boss 48, expands and compresses against the bone defining the blind hole, thereby anchoring the plug in place.

It should be noted, however, that the Fig. 7 embodiment of the plug assembly 20 may be used in the procedure shown in Fig. 3, if desired.

Fig. 9 illustrates an alternative embodiment of the plug assembly 20, which
25 may be particularly useful in procedures requiring a smaller hole diameter or strength requirement, such as Lis franc or other procedures involving smaller bone and lower strength requirements. The primary difference of this embodiment with

respect to prior disclosed embodiments is the reduced size of the cap and plug. The plug flange diameter and lower boss is smaller and continuous and the slots are curved around the center mounting threads.

Fig. 10 illustrates an alternative embodiment of the plug assembly 20, which is similar to Fig. 9 with a cap that is reduced in diameter in relation to the top flange of the plug, and may provide advantages when used in conjunction with some bone plate configurations.

Fig. 11 illustrates an alternative embodiment of the plug assembly 20, which is similar to Fig. 9, with a cap that is reduced in diameter in relation to the top flange of the plug, and also has a stepped feature that nests into a matching counterbore in the plug.

Fig. 12 illustrates an alternative embodiment of the plug assembly 20, which uses a reduced diameter plug flange, and a cap that is reduced in diameter in relation to the plug flange. This embodiment may provide advantages when used in conjunction with some bone plate configurations.

Accordingly, although exemplary embodiments of the invention have been shown and described, it is to be understood that all the terms used herein are descriptive rather than limiting, and that many changes, modifications, and substitutions may be made by one having ordinary skill in the art without departing from the spirit and scope of the invention, which is to be limited only in accordance with the following claims.

What is claimed is:

1. An implant system for stabilized fixation of tissue, comprising:
a button having a slot;
a band threaded through the slot; and
a lock comprising a member having a slot for receiving an end of the band
5 and a movable member for clamping the band in place;
the movable member being movable between an open position and a locking position.
2. The implant system as recited in Claim 1, wherein the button comprises a pair of slots and the band is threaded through each of the pair of slots in sequence, so that the band is wrapped around a portion of the button separating the two slots.
3. The implant system as recited in Claim 1, wherein the band is formed of suture material.
4. The implant system as recited in Claim 2, wherein the band comprises a length of flat suture material threaded through the pair of slots of the button and through the slot of the lock so that between the button and the lock the band comprises the length of suture doubled over itself.
5. The implant system as recited in Claim 1, wherein the lock

comprises a plug assembly.

6. The implant system as recited in Claim 5, wherein the plug assembly comprises a flange, the slot being disposed in said flange.

7. The implant system as recited in Claim 6, wherein the movable member comprises a cap which is movable between clamping and non-clamping orientations relative to the flange.

8. The implant system as recited in Claim 7, wherein the plug assembly further comprises a screw for moving the cap between its clamping and non-clamping orientations relative to the flange.

9. The implant system as recited in Claim 8, and further comprising a second slot in the flange, so that the band may be threaded through the first slot in the flange, cross a surface of the flange, and then extend through the second slot in the flange, thereby securing the band to the flange.

10. The implant system as recited in Claim 9, wherein the flange comprises a portion of a plug, the plug further comprising a boss extending from one side of the flange.

11. The implant system as recited in Claim 10, wherein when the band is threaded through the slots of the flange, each end of the band extends along a length of the boss.

12. The implant system as recited in Claim 11, wherein the boss comprises flat surfaces disposed along its length for accommodating the band ends extending therealong.

13. The implant system as recited in Claim 1, and further comprising a suture tether attached to the button.

14. The implant system as recited in Claim 13, and further comprising a guide needle attached to the suture tether.

15. A lock for use in an implant system for stabilized fixation of tissue, the lock comprising:

a member having a slot for receiving an end of a band and a movable member for clamping the band in place;

5 the movable member being movable between an open position and a locking position.

16. The lock as recited in Claim 15, wherein the lock comprises a plug assembly.

17. The lock as recited in Claim 16, wherein the plug assembly comprises a flange, the slot being disposed in the flange.

18. The lock as recited in Claim 6, wherein the movable member

comprises a cap which is movable between clamping and non-clamping orientations relative to the flange.

19. The lock as recited in Claim 18, wherein the plug assembly further comprises a screw for moving the cap between its clamping and non-clamping orientations relative to the flange.

20. The lock as recited in Claim 19, and further comprising a second slot in the flange, so that a band may be threaded through the first slot in the flange, cross a surface of the flange, and then extend through the second slot in the flange, thereby securing the band to the flange.

21. The implant system as recited in Claim 20, wherein the flange comprises a portion of a plug, the plug further comprising a boss extending from one side of the flange.

22. The implant system as recited in Claim 21, wherein when a band is threaded through the slots of the flange, each end of the band extends along a length of the boss.

23. The implant system as recited in Claim 22, wherein the boss comprises flat surfaces disposed along its length for accommodating band ends extending therealong.

24. A method for effecting repair of tissue using a tissue fixation band

apparatus comprising a lock, a button, and a suture band, under tension, extending between the lock and the button, comprising:

pulling the button through a hole extending through the tissue to be repaired,
5 until it exits a distal surface of the tissue and engages the distal surface of the tissue;

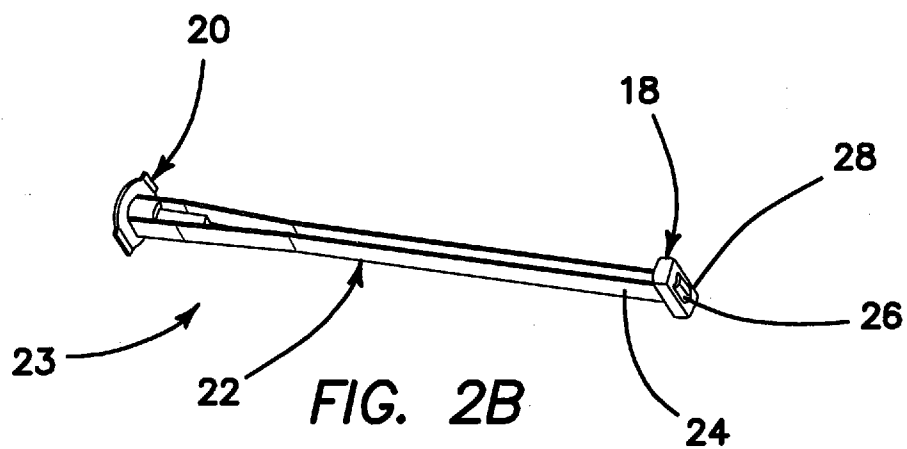
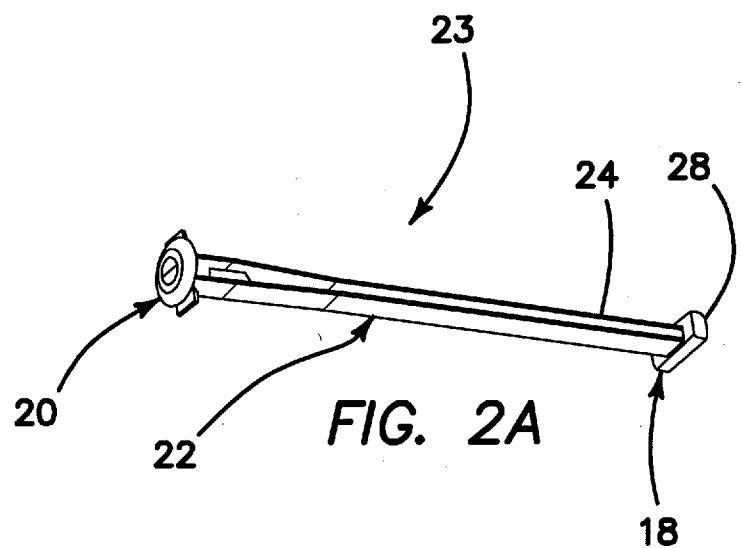
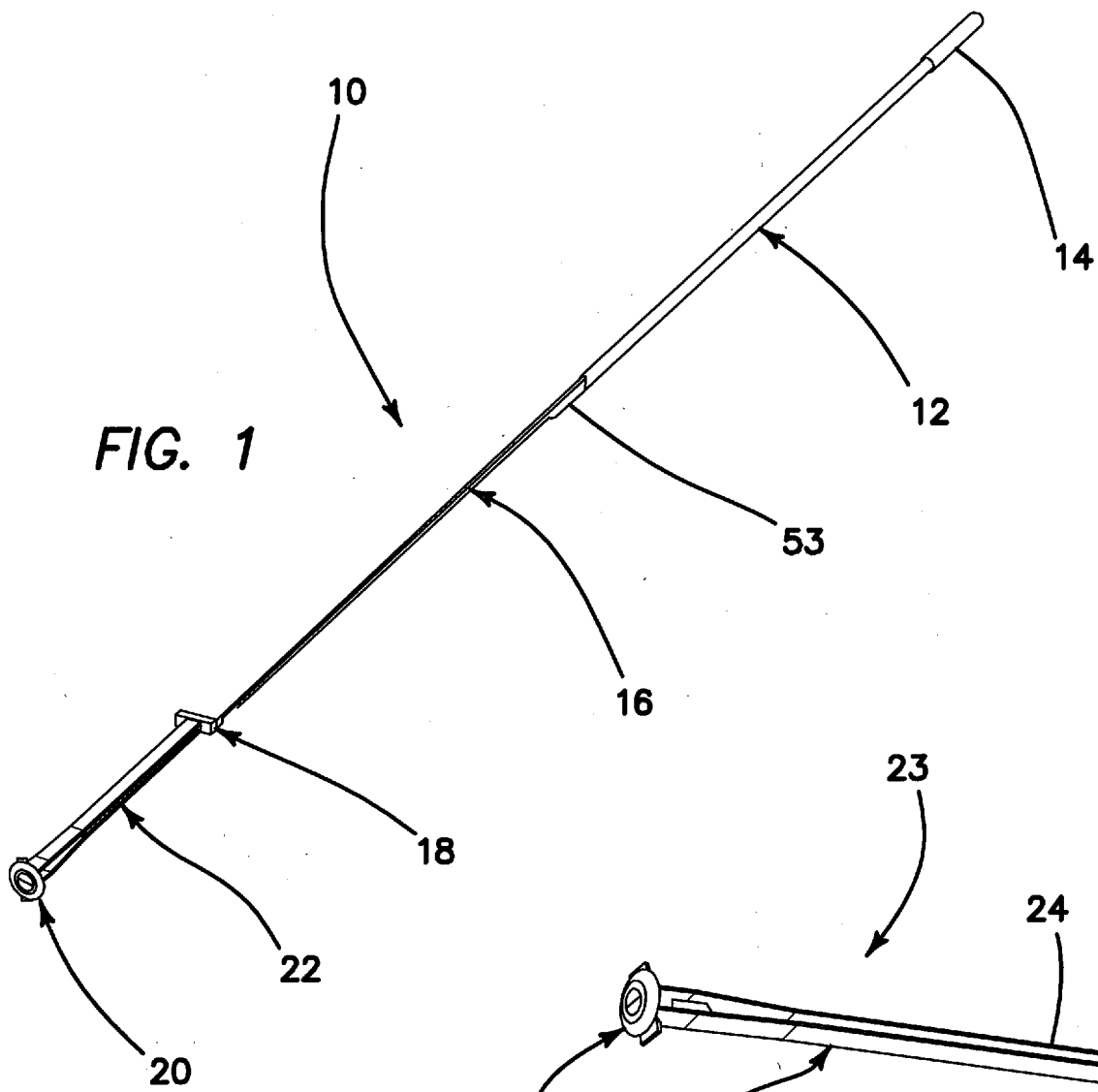
pulling the suture band on each end to locate the lock in position on a proximal surface of the tissue;

applying tension to free ends of the suture band exiting from the lock of the fixation band apparatus to tension the suture band to a desired level; and

10 causing a movable clamping member within the lock to move to a locking position, to thereby engage the lock and clamp the suture band in place at the desired tension level.

25. The method as recited in Claim 24, wherein the causing step comprises tightening a screw to cause the movable clamping member to move to its locking position.

26. The method as recited in Claim 25, wherein the lock comprises a plug assembly and the movable clamping member comprises a cap.



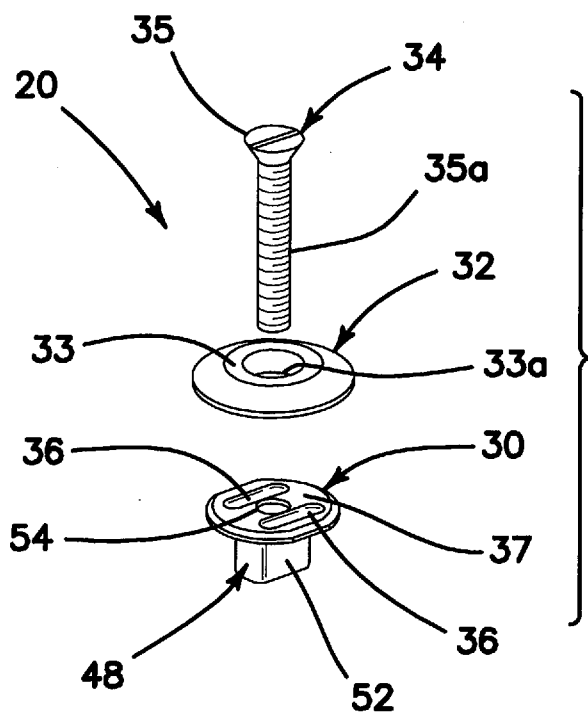
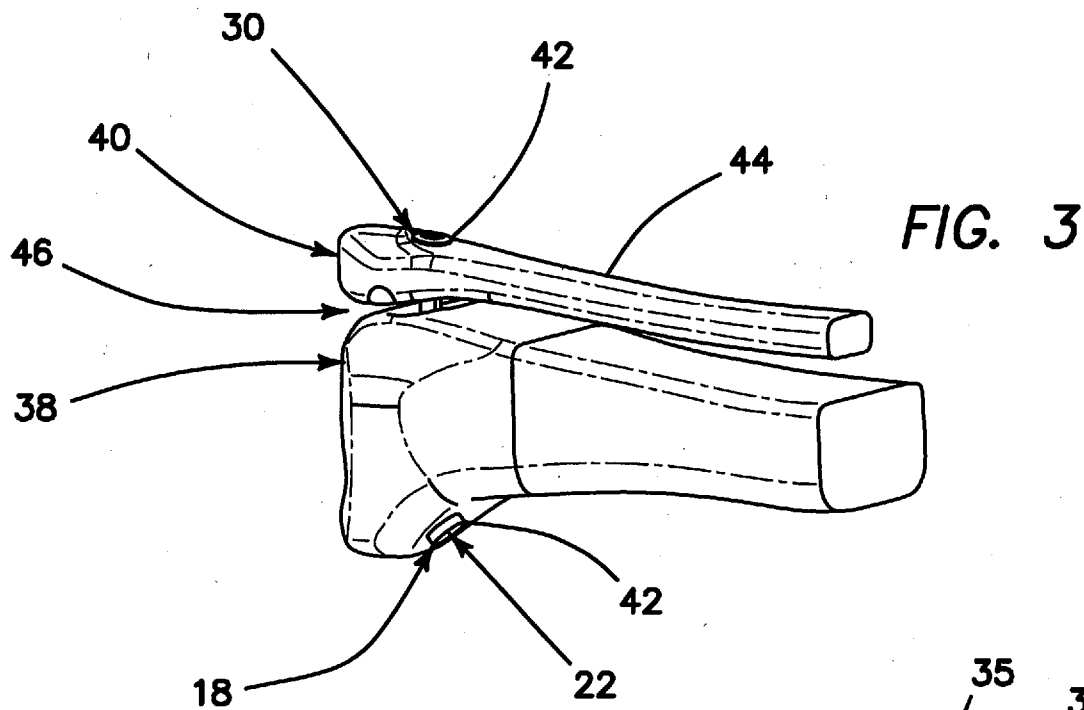


FIG. 4A

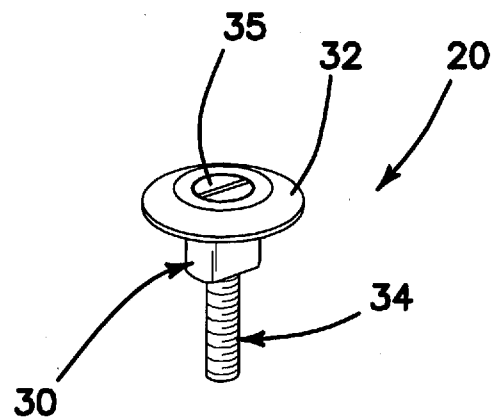


FIG. 4B

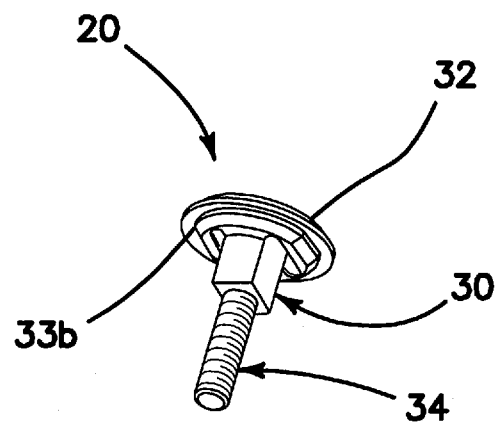


FIG. 4C

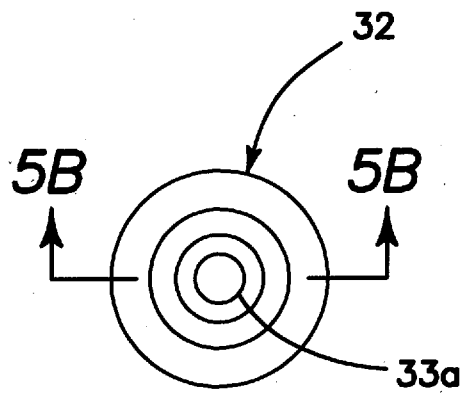


FIG. 5A

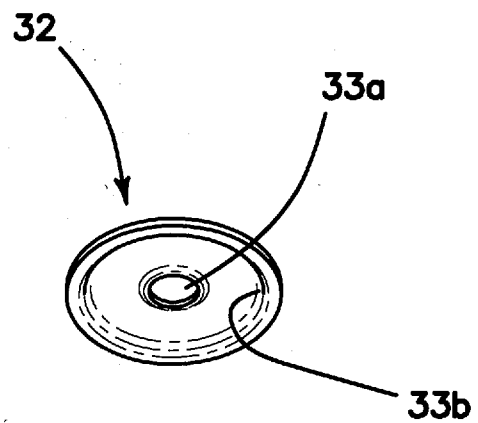


FIG. 5D

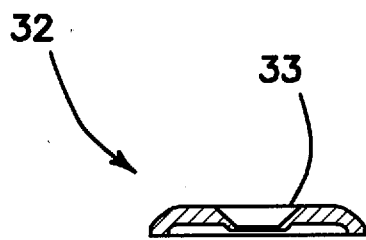


FIG. 5B

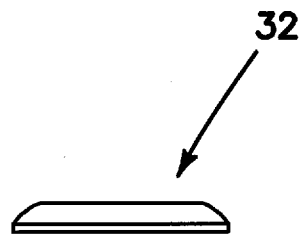


FIG. 5E

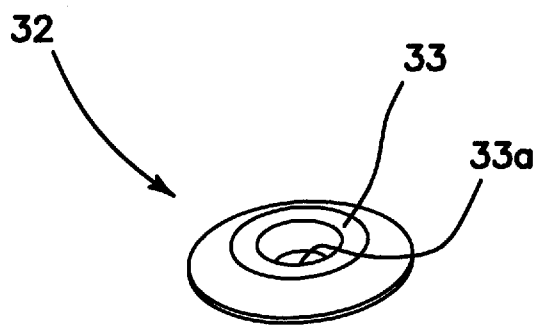


FIG. 5C

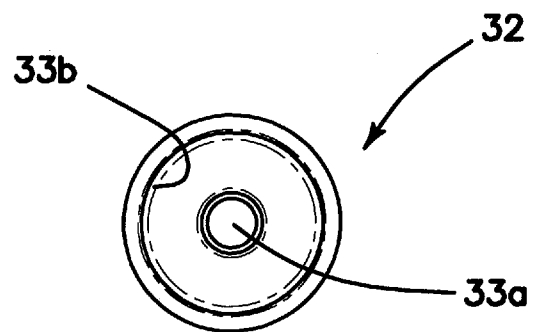
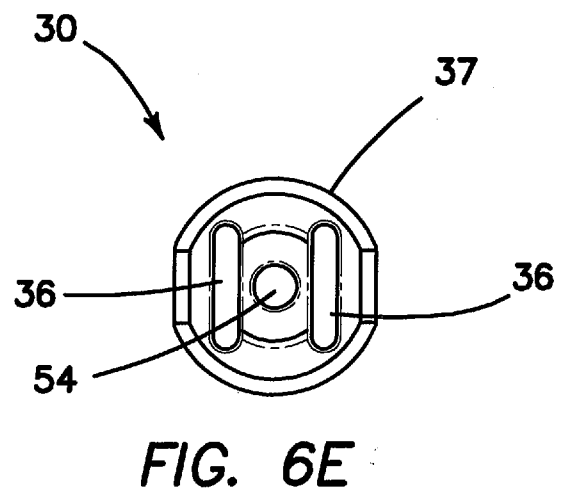
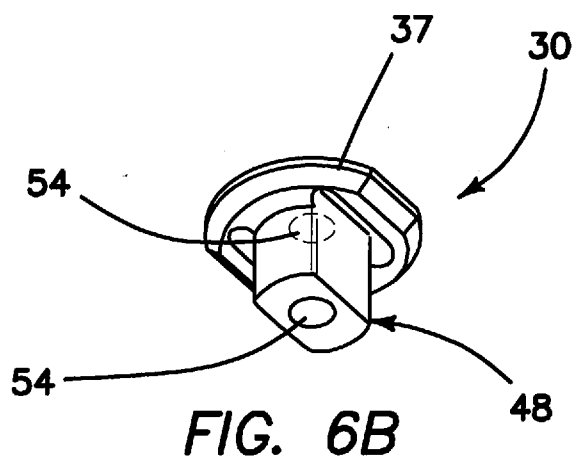
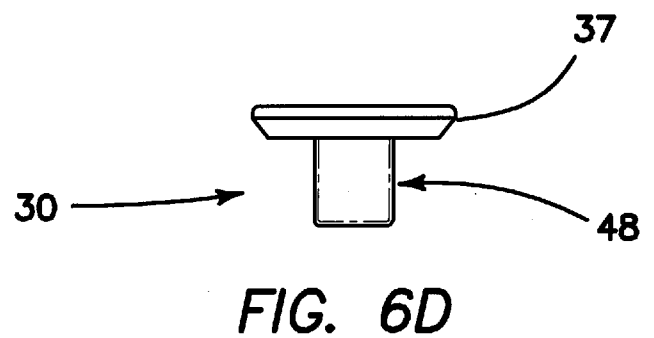
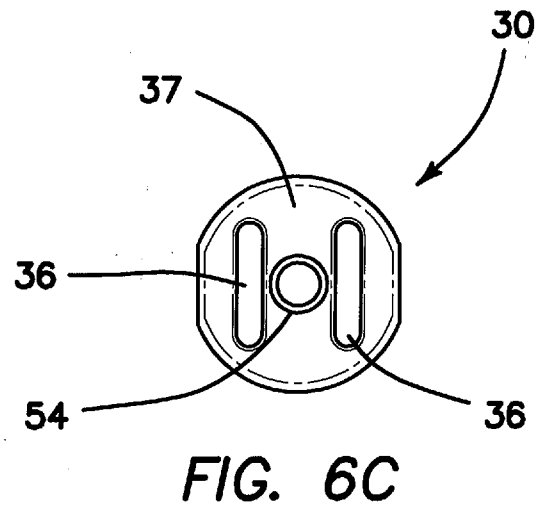
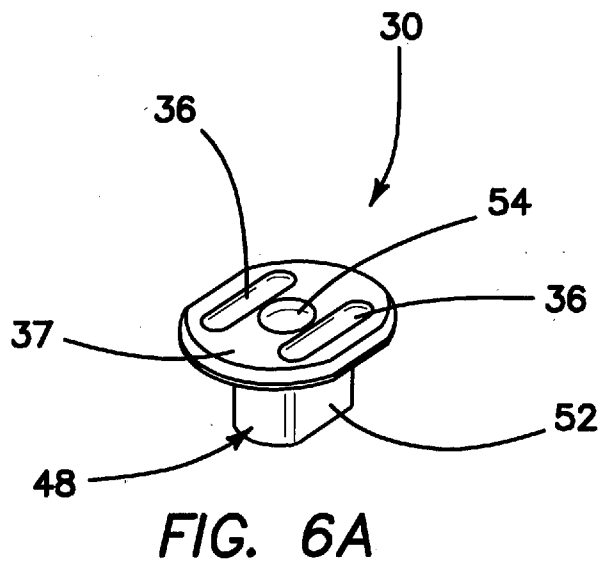


FIG. 5F



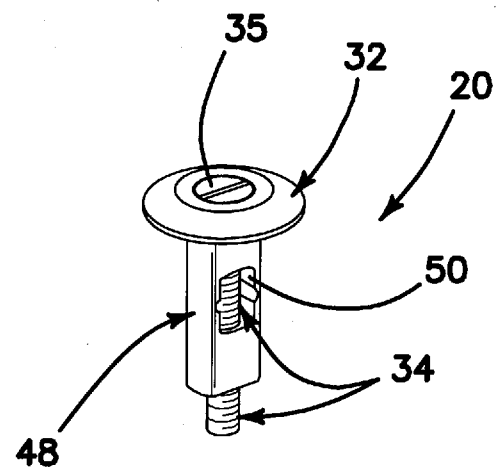
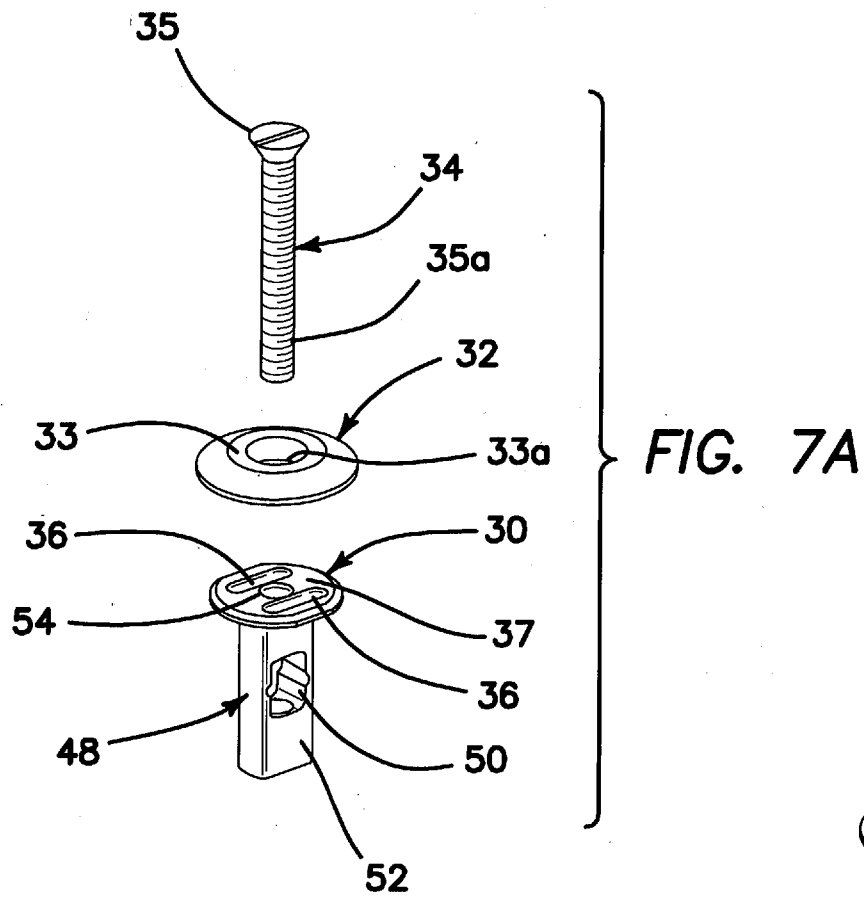
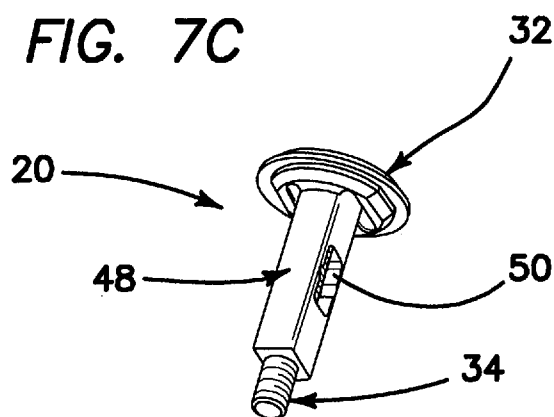


FIG. 7B



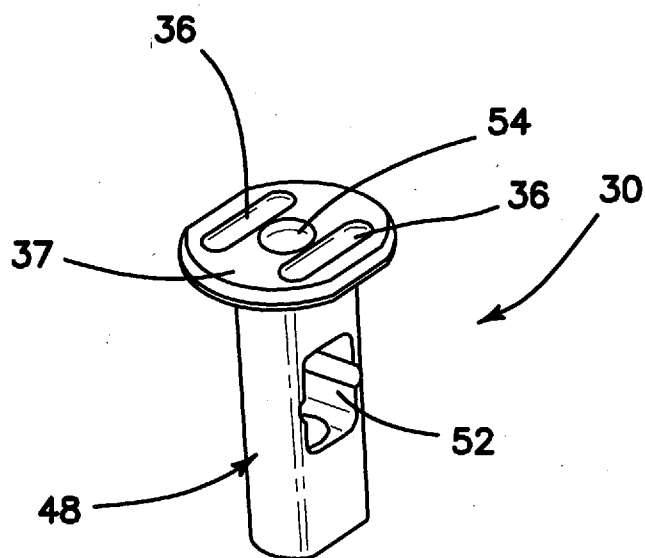


FIG. 8A

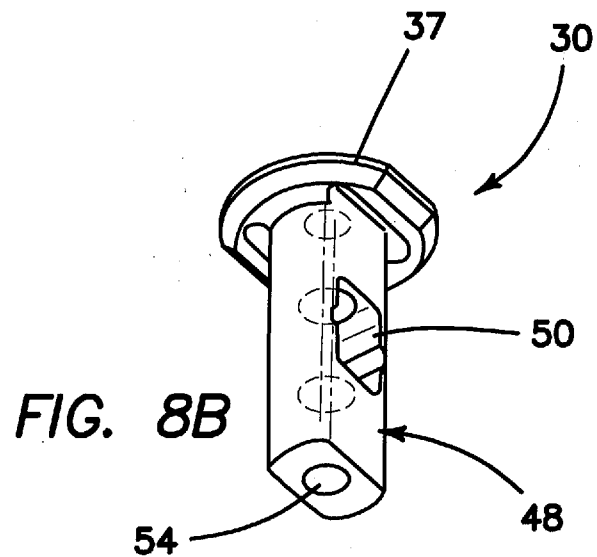


FIG. 8B

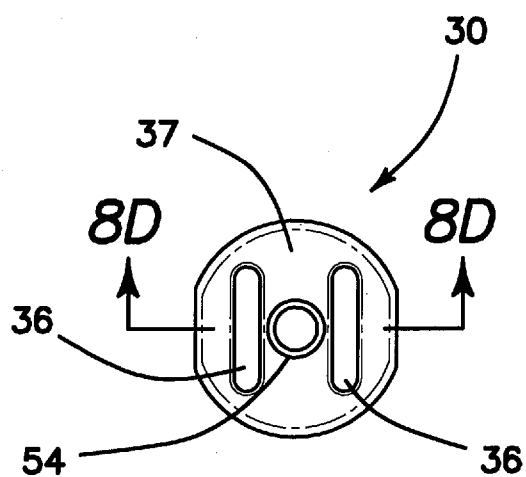


FIG. 8C

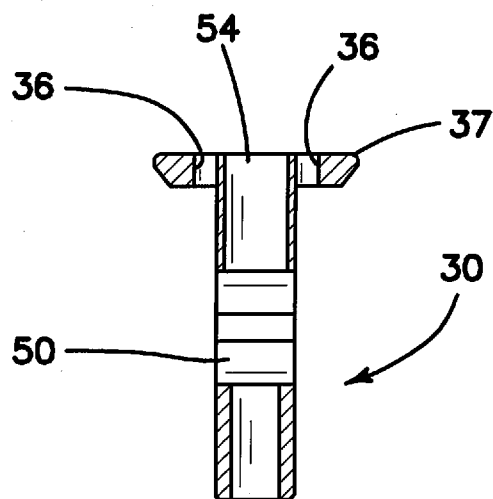


FIG. 8D

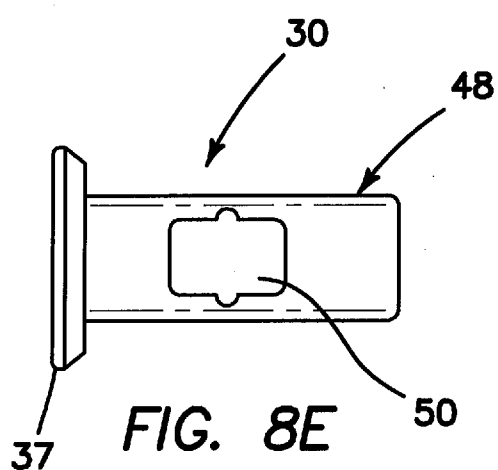


FIG. 8E

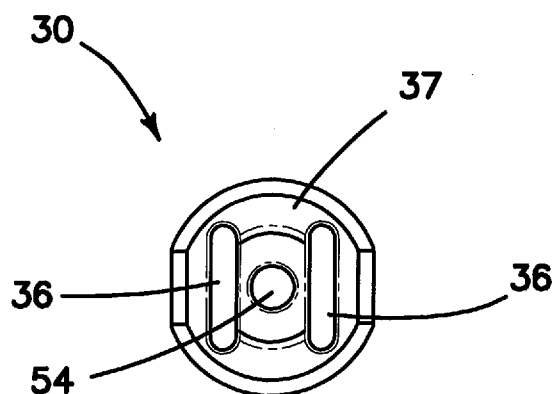


FIG. 8F

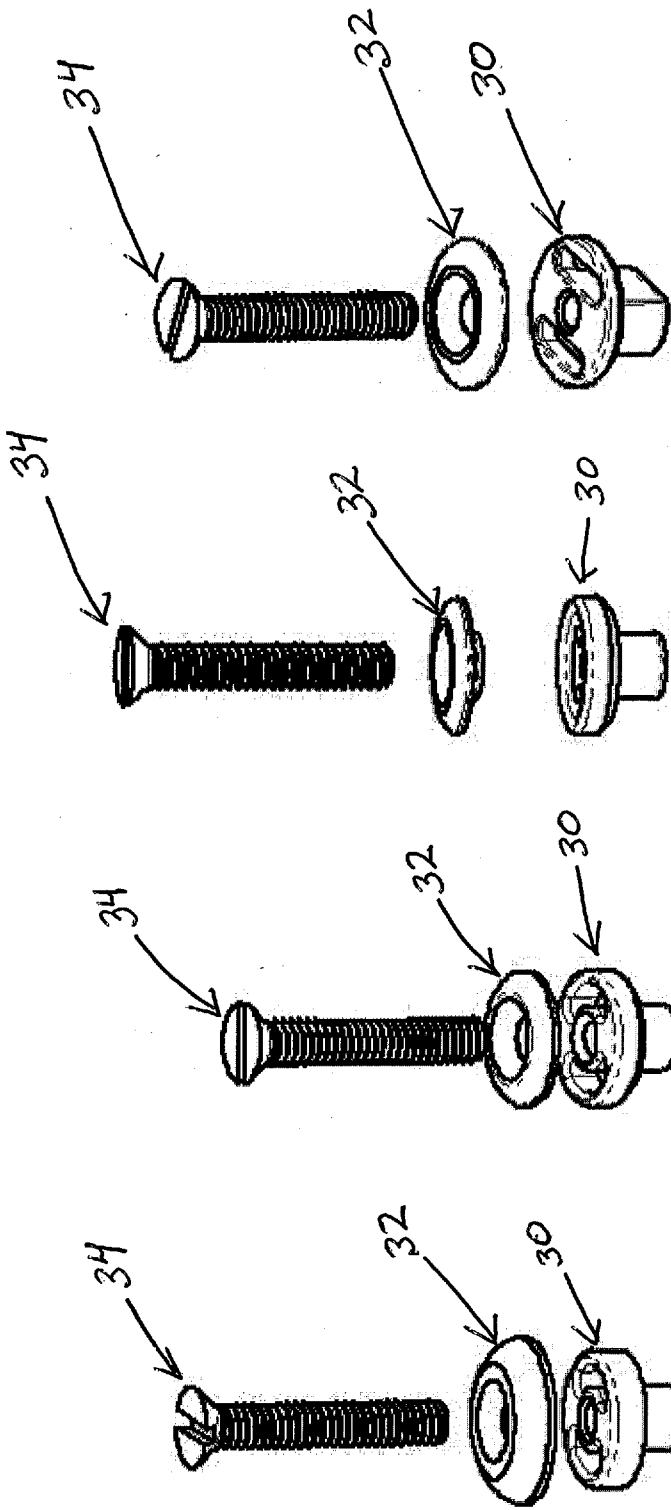


Fig. 9

Fig. 10

Fig. 11

Fig. 12

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US2015/052373**A. CLASSIFICATION OF SUBJECT MATTER****A61B 17/56(2006.01)i, A61B 17/60(2006.01)i, A61B 17/80(2006.01)i**

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61B 17/56; A61F 2/08; A61F 5/00; A61B 17/04; A61B 17/60; A61B 17/80

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Korean utility models and applications for utility models

Japanese utility models and applications for utility models

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

eKOMPASS(KIPO internal) & Keywords: syndesmosis, fixation, tibia, fibula, button, slot, band, suture, screw, cap, lock, flange, plug, boss, tether, guide needle

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 8512376 B2 (THORNES, BRIAN) 20 August 2013 See column 1, line 15 - column 9, line 26; claims 1-13; and figures 1-7f.	1-23
A	US 8771316 B2 (DENHAM, GREGORY J. et al.) 08 July 2014 See column 1, line 65 - column 9, line 19; claims 1-20; and figures 1-28.	1-23
A	US 7833244 B2 (CERUNDOLO, DANIEL) 16 November 2010 See column 1, line 38 - column 13, line 24; claims 1-20; and figures 1-17.	1-23
A	US 8591578 B2 (ALBERTORIO, RICARDO et al.) 26 November 2013 See column 1, line 46 - column 7, line 35; claims 1-6; and figures 1-52.	1-23
A	US 2012-0123474 A1 (ZAJAC, ERIC S. et al.) 17 May 2012 See paragraphs [0007]-[0080]; claims 1-22; and figures 1A-34.	1-23



Further documents are listed in the continuation of Box C.



See patent family annex.

* Special categories of cited documents:

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"E" earlier application or patent but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

18 January 2016 (18.01.2016)

Date of mailing of the international search report

19 January 2016 (19.01.2016)

Name and mailing address of the ISA/KR

International Application Division

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INTERNATIONAL SEARCH REPORTInternational application No.
PCT/US2015/052373**Box No. II Observations where certain claims were found unsearchable (Continuation of item 2 of first sheet)**

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.: 24-26
because they relate to subject matter not required to be searched by this Authority, namely:
Claims 24-26 pertain to a method for treatment/diagnosis of the human body by surgery and thus relate to a subject matter which this International Searching Authority is not required, under PCT Article 17(2)(a)(i) and PCT Rule 39.1(iv), to search.
2. ☐ Claims Nos.:
because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:
3. ☐ Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box No. III Observations where unity of invention is lacking (Continuation of item 3 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fees, this Authority did not invite payment of any additional fees.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest and, where applicable, the payment of a protest fee.
- ☐ The additional search fees were accompanied by the applicant's protest but the applicable protest fee was not paid within the time limit specified in the invitation.
- ☐ No protest accompanied the payment of additional search fees.

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No.

PCT/US2015/052373

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
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