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(54) **INSULIN ADAPTATION AND SAFETY MONITORING**

(57) Disclosed are a system, techniques and processes for monitoring and modifying a drug treatment regimen when a user partakes in a ketogenic diet. The disclosed system obtains ketone level measurements of a

user and indicates a user's adherence to the ketogenic diet as well as modifying a user's total daily dosage of a drug based on the user's following the ketogenic diet.

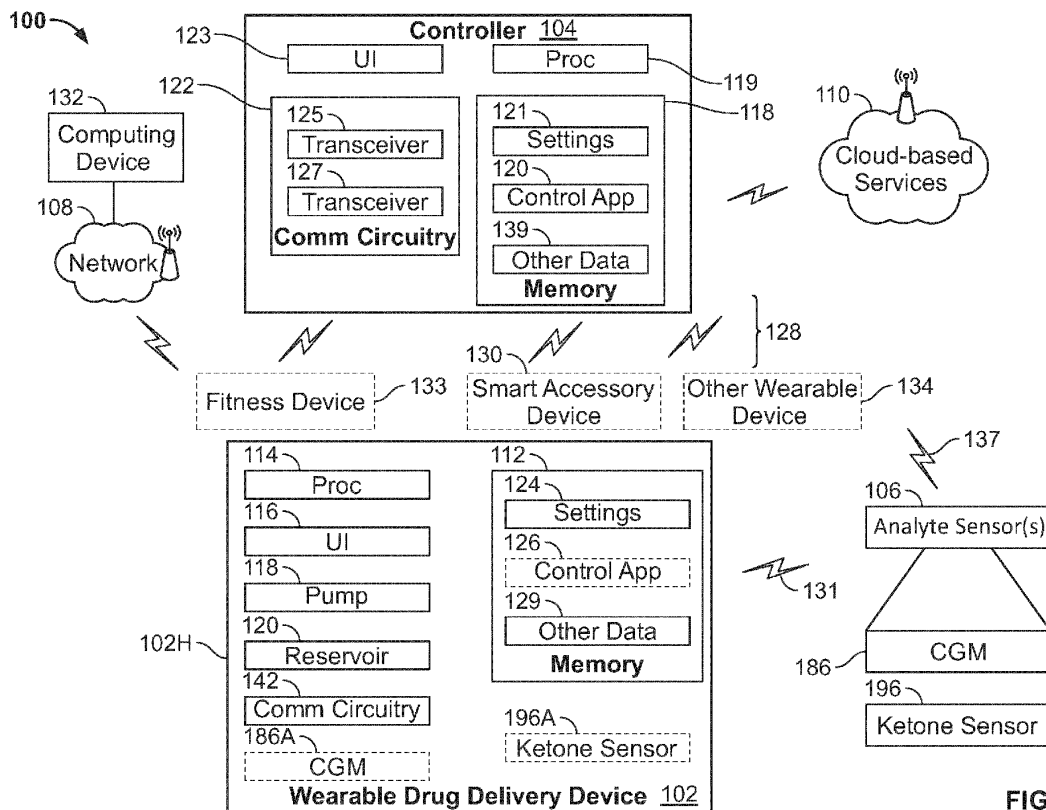


FIG. 1

Description

RELATED APPLICATIONS

[0001] This application claims the benefit of U.S. Provisional Patent Application No. 63/333,149, filed April 21, 2022, the entire contents of which are incorporated herein by reference in their entirety.

BACKGROUND

[0002] Assessment of the performance of a medication delivery algorithm, such as automated drug delivery (ADD) algorithms, are often executed in a stepwise process, where a significant amount of insulin delivery data and glucose measurement data is processed. Changes in the ADD algorithm that can result in improved glucose control outcomes are applied. However, the processing of significant amount of data may result in a significant delay in the time that it takes for each ADD algorithm to improve its behaviors.

[0003] Ketogenic diets are high in fat, moderate in protein and low in carbohydrate content. Type 1 diabetic users following ketogenic diets have shown improvement in hemoglobin A1c (HbA1c) levels and reduced glycemic variability and weight loss. As compared to the benefits, a ketogenic diet poses risks in diabetic ketoacidosis (DKA) as well as hypoglycemia. To successfully benefit from a ketogenic diet, the risks of DKA and hypoglycemia should be controlled.

[0004] With regard to another subject, sodium-glucose cotransporter-2 (SGLT2) inhibitors have been effective oral medications which can be added to treat users with Type 2 diabetes, which is a disease that is inadequately treated with insulin. SGLT2 inhibitors have beneficial renal and cardiovascular outcomes and are favored by physicians. Type 2 diabetics have benefitted from low carb diets with HbA1c drops up to 34%, lower triglyceride levels, increased HDL levels compared to high carb diets. SGLT2 inhibitors inhibit glucose reabsorption by proximal renal tubules and lead to a switch from glucose to lipid utilization, thereby increasing ketones and decreasing the insuloglucagon ratio. As a result, when taking SGLT2 inhibitors, a user's insulin needs and glucose levels behave differently on sick days. Risks of hypoglycemia, hyperglycemia as well as DKA (Diabetic Ketoacidosis) and euglycemic DKA (euDKA) increase. SGLT2 inhibitors might also be taken off label by Type 1 diabetics and presents risks of euDKA.

[0005] It would be beneficial if there was a system or a process by which the behavior of an ADD algorithm could be modified to account for the above issues with DKA and euDKA as well as addressing the challenges raised by use of SGLT2 inhibitors and diet changes resulting from fasting and food composition intake, such as a ketogenic diet.

BRIEF SUMMARY

[0006] This Summary is provided to introduce a selection of concepts in a simplified form that are further described below in the Detailed Description. This Summary is not intended to identify key features or essential features of the claimed subject matter, nor is it intended as an aid in determining the scope of the claimed subject matter.

[0007] Disclosed is an example of a drug delivery system that includes a processor, a user interface, a memory, and communication circuitry. The processor is operable to execute programming instructions. The user interface includes a touchscreen display and user input circuitry. The memory is operable to store the programming instructions; and the communication circuitry is coupled to the processor and is operable to receive and transmit communication signals. The processor is operable to receive an indication that a user is starting a ketogenic diet. The processor retrieves a baseline total daily insulin value. The processor calculates a keto total daily insulin value using the retrieved baseline total daily insulin value; and utilizing the keto total daily insulin value in the calculation of a keto basal dosage of insulin or a keto bolus dosage of insulin.

[0008] Disclosed is an example of another drug delivery system that includes a processor, a user interface, a memory, and communication circuitry. The processor is operable to execute programming instructions. The user interface may include a display and user input circuitry. The memory is operable to store the programming instructions. The communication circuitry is coupled to the processor and is operable to receive and transmit communication signals. The processor may be operable to receive ketone levels from a ketone sensor. The processor may generate a prompt on the user interface inquiring whether a user's diet for today or another time period is a keto diet or a non-keto diet. The processor may adjust parameter settings and insulin delivery based on input received from the user via the user interface. Further, the processor, based on the received ketone levels of the user, may generate an indication of whether the user is adhering to a keto diet.

[0009] Disclosed is an exemplary controller of a drug delivery system. The controller may include a processor, a memory, and a communication circuitry. The processor may be operable to execute programming instructions. The memory may be operable to store the programming instructions. The communication circuitry may be coupled to the processor and be operable to receive and transmit communication signals. The processor, when executing the programming instructions, is operable to obtain ketone levels of a user. The obtained ketone levels may be evaluated with reference to a plurality of ketone thresholds. Based on the result of the evaluation, the processor may select a further action to be performed. The selected further action is at least one of generating a notification to seek medical attention, generating a no-

tification to ingest food or drink such as carbohydrates, generating a notification to increase insulin, or a combination thereof. The processor may further cause performance of the selected further action.

BRIEF DESCRIPTION OF THE DRAWINGS

[0010]

FIG. 1 illustrates an example of a system that is suitable to implement the subject matter described herein.

FIG. 2 illustrates exemplary graphical user interface windows and a process for setting up a schedule for indicating to a medication delivery system a user transition to a ketogenic diet.

FIG. 3 illustrates an exemplary technique for modifying a drug delivery parameter of a drug delivery system when a user switches to a ketogenic diet.

FIG. 4 illustrates an exemplary process flow diagram for a user's transition from a ketogenic diet day to a non-ketogenic diet day.

FIG. 5 depicts an exemplary process flow diagram for a user's transition from a non-ketogenic diet day to ketogenic diet day.

FIG. 6 illustrates a flowchart of an exemplary process for monitoring a user's adherence to their diet.

FIG. 7 illustrates a flowchart of an exemplary process for monitoring and intervening steps for avoiding diabetic ketoacidosis.

FIG. 8 illustrates a flowchart of another exemplary process for monitoring a user using ketone sensing and activity sensing for DKA and euDKA.

FIG. 9 illustrates a flowchart of a process for monitoring a user for indications of hypoglycemia when the user is adhering to a ketogenic diet.

FIG. 10 illustrates a high-level example of a machine learning process for predicting a future glucose measurement value.

DETAILED DESCRIPTION

[0011] The following discussion provides a framework to assess the behavior of a medication delivery algorithm (MDA) system in real time based on near-term retrospective drug delivery history (such as insulin delivery history) and glucose control outcomes through advisory mode assessments and describes the incorporation of changes to the MDA algorithm that retrospectively shows improved performance in historical data, which also holds promise in improving future delivery precision and outcomes as well.

[0012] The MDA system may implement, as the MDA algorithm, an "artificial pancreas" algorithm-based system, or more generally, an artificial pancreas (AP) application. For ease of discussion, the computer programs and computer applications that implement the medication delivery algorithms or applications may be referred

to, interchangeably, herein as an "AP application," an "ADD algorithm," an "MDA algorithm," an "MDA application," or an MDA/ADD/AP application." An AP application may be configured to provide automated delivery of a drug, such as insulin, based on an analyte sensor(s) input, such as signals received from an analyte sensor(s), such as a continuous glucose monitor, or the like. The signals from the analyte sensor(s) may contain data indicative of glucose measurement values, timestamps, or the like.

[0013] Additionally, or alternatively, while the disclosed examples may have been described with reference to a closed loop algorithmic implementation, variations of the disclosed examples may be implemented to enable open loop use. The open loop implementations allow for use of different modalities of delivery of a drug(s) such as a smart pen, a syringe, or the like. For example, the disclosed AP application and algorithms may be operable to perform various functions related to open loop operations, such as the generation of prompts requesting the input of information such as diabetes type, weight, and/or age. Similarly, a dosage amount of a drug may be received by the AP application or algorithm from a user via a user interface. Other open-loop actions may also be implemented by adjusting user settings or the like in an AP application or algorithm.

[0014] Systems, devices, computer readable media and methods in accordance with the present disclosure are now described more fully hereinafter with reference to the accompanying drawings, where one or more examples are shown. The systems, devices, and methods described herein may be embodied in many different forms and are not to be construed as being limited to the examples set forth herein. Instead, these examples are provided so the disclosure is thorough and complete, and may fully convey the scope of the techniques and devices to those skilled in the art. Each of the systems, devices, media, and methods disclosed herein provides one or more advantages over conventional systems, components, and methods.

[0015] FIG. 1 illustrates a drug delivery system operable to implement the subject matter described herein. In some examples, the drug delivery system 100 is suitable for delivering insulin to a user in accordance with the disclosed embodiments utilizing the MDA/ADD/AP application as discussed above. The drug delivery system 100 may include a wearable drug delivery device 102, a controller 104 and an analyte sensor(s) 106, and other exemplary devices reflected in FIG. 1.

[0016] The wearable drug delivery device 102 may be a wearable device that is worn on the body of the user. The wearable drug delivery device 102 may be directly coupled to a user (e.g., directly attached to a body part and/or skin of the user via an adhesive, or the like). In an example, a surface of the wearable drug delivery device 102 may include an adhesive to facilitate attachment to the skin of a user.

[0017] The wearable drug delivery device 102 may in-

clude a processor 114. The processor 114 may be implemented in hardware, software, or any combination thereof. The processor 114 may, for example, be a microprocessor, a logic circuit, a field programmable gate array (FPGA), an application specific integrated circuit (ASIC) or a microprocessor coupled to a memory. The processor 114 may maintain a date and time as well as be operable to perform other functions (e.g., calculations or the like). The processor 114 may be operable to execute a control application 126 stored in the memory 112 that enables the processor 114 to direct operation of the wearable drug delivery device 102. The control application 126 may control drug delivery to the user per an ADD control approach as describe herein. For example, the control application 126 may be an ADD algorithm. The memory 112 may hold settings 124 for a user, such as specific factor settings, subjective insulin need parameter settings, ADD algorithm settings, such as maximum insulin delivery, insulin sensitivity settings, total daily insulin (TDI) settings and the like. The memory may also store other data 129, such as total daily insulin values, glucose measurement values from analyte sensor(s) 106 or controller 104, insulin dosage amounts (both basal and bolus) and the like from previous minutes, hours, days, weeks, or months. In an additional example, the analyte sensor(s) 106 may include multiple sensors, such as a continuous glucose monitor 186 and a ketone sensor 196. In an example of the multiple sensor arrangement, the analyte sensor(s) 106 may be operable to collect physiological condition data, such as ketone values (also referred to as "ketone level(s)"), ketone values with a time stamp, glucose measurement values (also referred to herein as "glucose values," or "glucose level(s)"), glucose measurement values and a timestamp, both ketone values and glucose values that may be shared with the wearable drug delivery device 102, the controller 104 or both. Alternatively, the ketone sensor 196 or CGM 186 may be separate sensors (and may be located separately on the user's body) and be configured to individually output measurement information (e.g., the above referenced ketone values, glucose measurement values and timestamp values or other data) to the controller 104 or wearable drug delivery device 102. The ketone sensor 196 may be configured to include hydrogel membranes that are used to improve ketone concentration and reduce electrode fouling. In a further example, the wearable drug delivery device 102 may optionally include a continuous glucose monitor 186A and/or a ketone sensor 196A, which may be removably incorporated in, on, or adjacent to, or fully integrated within the wearable drug delivery device 102. For example, the continuous glucose monitor 186A and/or the ketone sensor 196A may be incorporated in a housing 102H of the wearable drug delivery device 102. Note that ketones may also be detected using a breath sensor (which is not shown but may be incorporated in the controller 104) or urine content sensor (not shown); however, a subcutaneous ketone sensor as envisioned for ketone sensors 196 and 196A

gives more accurate information and is usually near continuous. As described herein, the MDA algorithm of the control application 120 or 126 and drug delivery system 100 is described with the understanding that the ketone values are based on measurements made subcutaneously. Use of a ketone breath sensor or a urine sensor as part of or in addition to the analyte sensor(s) 106 may delay receipt of the ketone values and modifications to account for the delay may be incorporated into control application 120 and 126 of the drug delivery system 100.

[0018] For example, the communication circuitry 142 of the wearable drug delivery device 102 may be operable to communicate with the analyte sensor(s) 106 and the controller 104 as well as devices 130, 133 and 134. The communication circuitry 142 may be operable to communicate via Bluetooth, cellular communication, and/or other wireless protocols. While not shown, the memory 112 may include both primary memory and secondary memory. The memory 112 may include random access memory (RAM), read only memory (ROM), optical storage, magnetic storage, removable storage media, solid state storage or the like.

[0019] The wearable drug delivery device 102 may include a reservoir 120. The reservoir 120 may be operable to store drugs, medications, or therapeutic agents suitable for automated delivery, such as insulin, morphine, methadone, hormones, glucagon, glucagon-like peptide, blood pressure medicines, chemotherapy drugs, fertility drugs, arthritis drugs, combinations of drugs, such as insulin and glucagon-like peptide, or the like. A fluid path to the user may be provided via tubing and a needle/cannula (not shown). The fluid path may, for example, include tubing coupling the wearable drug delivery device 102 to the user (e.g., via tubing coupling a needle or cannula to the reservoir 120). The wearable drug delivery device 102 may be operable based on control signals from the processor 114 to expel the drugs, medications, or therapeutic agents, such as insulin, from the reservoir 120 to deliver doses of the drugs, medications, or therapeutic agents, such as the insulin, to the user via the fluid path. The processor 114 may be operable to cause insulin to be expelled from the reservoir 120.

[0020] There may be one or more communications links 128 with one or more devices physically separated from the wearable drug delivery device 102 including, for example, a controller 104 of the user/caregiver and/or a sensor 106. The communication links 128 may include any wired or wireless communication link operating according to any known communications protocol or standard, such as Bluetooth®, Wi-Fi, a near-field communication standard, a cellular standard, or any other wireless protocol. The analyte sensor(s) 106 may communicate with the wearable drug delivery device 102 via a wireless communication link 131 and/or may communicate with the controller 104 via a wireless communication link 137.

[0021] The wearable drug delivery device 102 may also include a user interface 116, such as an integrated display device for displaying information to the user, and

in some embodiments, receiving information from the user. For example, the user interface 116 may include a touchscreen and/or one or more input devices, such as buttons, knob or a keyboard that enable a user to provide an input.

[0022] In addition, the processor 114 may be operable to receive data or information from the analyte sensor(s) 106 as well as other devices that may be operable to communicate with the wearable drug delivery device 102.

[0023] The wearable drug delivery device 102 may interface with a network 108. The network 108 may include a local area network (LAN), a wide area network (WAN) or a combination therein. A computing device 132 may be interfaced with the network, and the computing device may communicate with the insulin delivery device 102. The computing device 132 may be a healthcare provider device through which a user's controller 104 may interact to obtain information, store settings and the like. The ADD algorithm operating, as or in cooperation with, the control application 120 may present a graphical user interface on the computing device 132 enabling the input and presentation of information related to the ADD algorithm and the example techniques and processes described herein.

[0024] The drug delivery system 100 may include an analyte sensor(s) 106 for sensing the levels of one or more analytes of a user. The analyte levels may be used as physiological condition data and be sent to the controller 104 and/or the wearable drug delivery device 102. The sensor 106 may be coupled to the user by, for example, adhesive or the like and may provide information or data on one or more medical conditions and/or physical attributes of the user. The sensor 106 may be a continuous glucose monitor (CGM), such as 186, ketone sensor, such as 196, or another type of device or sensor that provides glucose measurements that is operable to provide glucose concentration measurements. The sensor 106 may be physically separate from the wearable drug delivery device 102 or may be an integrated component thereof. The sensor 106 may provide the processor 114 and/or processor 119 with physiological condition data indicative of measured or detected glucose levels of the user. The information or data provided by the sensor 106 may be used to modify an insulin delivery schedule and thereby cause the adjustment of drug delivery operations of the wearable drug delivery device 102.

[0025] The drug delivery system 100 may also include the controller 104. In the depicted example, the controller 104 may include a processor 119 and a memory 118. The controller 104 may be a special purpose device, such as a dedicated personal diabetes manager (PDM) device. The controller 104 may be a programmed general-purpose device that is a portable electronic device, such as any portable electronic device, smartphone, smartwatch, fitness device, tablet or the like including, for example, a dedicated processor, such as processor, a micro-processor or the like. The controller 104 may be used to program or adjust operation of the wearable drug de-

livery device 102 and/or the sensor 106. The processor 119 may execute processes to manage a user's glucose levels and for control the delivery of the drug or therapeutic agent to the user. The processor 119 may also be operable to execute programming code stored in the memory 118. For example, the memory 118 may be operable to store a control application 120, such as an ADD algorithm for execution by the processor 119. The control application 120 may be responsible for controlling the wearable drug delivery device 102, including the automated delivery of medicament, such as insulin, based on recommendations and instructions from the ADD algorithm, such as those recommendations and instructions described herein.

[0026] The memory 118 may store one or more applications, such as control application 120, and settings 121 for the insulin delivery device 102 like those described above. In addition, the memory 118 may be operable to store other data and/or computer programs 139, such as drug delivery history, glucose measurement values over a period of time, total daily insulin values, and the like. For example, the memory 118 is coupled to the processor 119 and operable to store programming instructions, such as the control application 120 and settings 121, and data, such as other data 139, related to a blood glucose of a user and/or data related to an amount of insulin expelled by the wearable drug delivery device 102.

[0027] The controller 104 may include a user interface (UI) 123 for communicating with the user. The user interface 123 may include a display, such as a touchscreen, for displaying information. The touchscreen may also be used to receive input when it is a touch screen. The user interface 123 may also include input elements, such as a keyboard, button, knob or the like. In an operational example, the user interface 123 may include a touchscreen display (including a display and user input circuitry, such as touch sensitive circuits and the like) controllable by the processor 119 and be operable to present a graphical user interface and receive inputs via the user input circuitry, the touchscreen display is operable to generate a signal indicative of the respective diet types, number of days, diet cycles, keto days, sick day mode, sickness symptoms, religious fasting mode, location information, calendar information, or the like. The touchscreen display, under control of the processor 119, may be operable to, in response to the received input, generate a response to a user's drug treatment regimen as well as cause the presentation of prompts on a graphical user interface as described with reference to the later examples described with reference to FIGs. 1-10. The graphical user interfaces discussed herein with respect to the later examples may be generated by the processor 119 of the controller 104 and be presented on the UI 123.

[0028] The controller 104 may interface via a wireless communication link of the wireless communication links 128 with a network, such as a LAN or WAN or combination of such networks that provides one or more servers or cloud-based services 110 via communication circuitry

122. The communication circuitry 122, which may include transceivers 127 and 125, may be coupled to the processor 119. The communication circuitry 122 may be operable to transmit communication signals (e.g., command and control signals) to and receive communication signals (e.g., via transceivers 127 or 125) from the wearable drug delivery device 102 and the analyte sensor(s) 106. In an example, the communication circuitry 122 may include a first transceiver, such as 125, that may be a Bluetooth transceiver, which is operable to communicate with the communication circuitry 122 of the wearable drug delivery device 102, and a second transceiver, such as 127, that may be a cellular or Wi-Fi transceiver operable to communicate via the network 108 with computing device 132 or with cloud-based services 110.

[0029] The cloud-based services 110 may be operable to store user history information, such as glucose measurement values over a set period of time (e.g., days, months, years), ketone levels over a set period of time (e.g., days, months, years), a drug delivery history that includes insulin delivery amounts (both basal and bolus dosages) and insulin delivery times, types of insulin delivered, indicated meal times, glucose measurement value trends or excursions or other user-related diabetes treatment information, specific factor settings including default settings, present settings and past settings, or the like.

[0030] Other devices, like smart accessory device 130 (e.g., a smartwatch or the like), fitness device 133 and other wearable device 134 may be part of the drug delivery system 100. These devices may communicate with the wearable drug delivery device 102 to receive information and/or issue commands to the wearable drug delivery device 102. These devices 130, 133 and 134 may execute computer programming instructions to perform some of the control functions otherwise performed by processor 114 or processor 119. These devices 130, 133 and 134 may include user interfaces, such as touch-screen displays for displaying information such as current glucose level, insulin on board, insulin deliver history, or other parameters or treatment-related information and/or receiving inputs, such as those described with reference to the examples of FIGs. 1-3. The display may, for example, be operable to present a graphical user interface for providing input, such as request a change in basal insulin dosage or delivery of a bolus of insulin. These devices 130, 133 and 134 may also have wireless communication connections with the sensor 106 to directly receive glucose level data or receive in parallel a presentation of the graphical user interface as shown in FIG. 1.

[0031] In another operational example, the controller 104 may be operable to execute programming code that causes the processor 119 of the controller 104 to perform the following functions. The processor 119 of the controller 104 may execute an ADD algorithm that is one of the control applications 120 stored in the memory or memory 118. The processor may be operable to present, on a

user interface that is at least one component of the user interface 123. The user interface 123 may be a touch-screen display controlled by the processor 119, and the user interface 123 is operable to present a graphical user interface that offers an input of a subjective insulin need parameter usable by the ADD algorithm. The processor 119 may cause presentation on a user interface of a user device, a graphical user interface offering an input device that enables input of a subjective insulin need parameter. The ADD algorithm may generate instructions for the pump 118 to deliver basal insulin to the user or the like.

[0032] The processor 119 is also operable to collect physiological condition data related to the user from sensors, such as the analyte sensor(s) 106 or heart rate data, for example, from the fitness device 133 or the smart accessory device 130. In an example, the processor 119 executing the ADD algorithm may determine a dosage of insulin to be delivered based on the collected physiological condition of the user and a specific factor determined based on the subjective insulin need parameter. The processor 119 may output a control signal via one of the transceivers 125 or 127 to the wearable drug delivery device 102. The outputted signal may cause the processor 114 to deliver command signals to the pump 118 to deliver an amount of related to the determined dosage of insulin in the reservoir 120 to the user based on an output of the ADD algorithm. The processor 119 may also be operable to perform calculations regarding settings of the ADD algorithm as discussed as herein. Modifications to the ADD algorithm settings may be stored in the memory 118, for example, as settings 121.

[0033] A wearable drug delivery device 102, typically, has a lifecycle that is based on the amount of liquid drug that is stored in a reservoir 120 of the wearable drug delivery device 102 and/or the amount of the liquid drug delivered to the user. An ADD application or algorithm may use a number of parameters, such as glucose measurement values, total daily insulin, insulin onboard, and the like, when making the determination of an amount of the liquid drug to have delivered. In an operational example, the processor 119 of the controller 104 may be operable to receive evaluate the effectiveness of the ADD algorithm's control of the drug delivery device 102. For example, the processor 119 may be operable to utilize historical data accessible by the processor in an evaluation of past performance of the ADD algorithm and generate recommendations for adjusting settings of the ADD algorithm accordingly as described in more detail with reference to the examples of FIGs. 2 and 3).

[0034] While the system 100 is described with reference to delivery of insulin and the use of an ADD algorithm, the system 100 may be operable to implement a drug delivery regimen via a medication delivery algorithm using a number of different liquid or therapeutic drugs or medicaments. A liquid medicament or drug may be or include any medicament or drug in liquid form capable of being administered by a drug delivery device via a subcutaneous cannula, including, for example, insulin,

glucagon-like peptide-1 (GLP-1) receptor agonist, pramlintide, glucosedependent insulinotropic polypeptide (GIP), glucagon, co-formulations of two or more of glucagon, GLP-1, pramlintide, and insulin; as well as pain relief drugs, such as opioids or narcotics (e.g., morphine, or the like), methadone, blood pressure medicines, chemotherapy drugs, fertility drugs, or the like.

Insulin Adaptation and Safety Monitoring for Ketogenic Diets for Drug Delivery Systems

[0035] In a common diet, a person intakes a moderate amount of carbohydrates, a moderate number of proteins, a moderate amount of fats, and a moderate amounts of other nutrients. In a person with diabetes, who is a user of a wearable drug delivery device, an ADD application monitors the user's glucose level and delivers medication that maintains the user's glucose level within a range of a glucose target set point.

[0036] When a user partakes in a ketogenic diet, the user intakes a higher amount of fat, a moderate amount of protein, and a low amount of carbohydrates. There are a number of benefits of a ketogenic diet, such as limited glucose spikes, weight loss, reduced need for medication insulin, and others. Anecdotally, a ketogenic diet has been shown to reduce the need for medication, such as, insulin, by up to 40%.

[0037] The discussion of FIG. 2 illustrates examples of graphical user interfaces that enable a process for indicating to the control application of the medication delivery system in which the user is transitioning to a ketogenic diet. The safe medicament delivery is framed in the context of a drug delivery system, such as the example of FIG. 1.

[0038] The controller 104 of FIG. 1 may be operable to present a graphical user interface on the user interface 123. FIG. 2 illustrates an example of windows of a graphical user interface 200 that may be configured to enable a user to enter a "Keto mode" setup. In an example, a ketone diet may be considered to be less than 30 g of carbohydrates, with higher portions of fat and protein to make up enough for caloric needs. When the ketone diet is followed, the user's metabolism makes greater use of glycogen stores initially, after which stored fats are broken down by the liver into ketones that are used as an alternate energy source by the body. Even a low carbohydrate diet does not lead to the production of ketones. When setting up the exemplary Keto mode of the drug delivery system implemented via the control application 120, the user may set up Keto mode to indicate switching to a ketogenic diet. Referring to FIG. 2, in window A, the user may indicate to the system that the user intends to begin starting the ketogenic diet. In window B of the user interface 200, the user may either select an option to enter timing for a ketogenic diet for the whole week (e.g., "All days") or indicate a diet cycle. A commonly favored diet cycle is the 5:2 cycle. In this option, the person follows the Ketogenic diet for 5 days and switches to a higher

carbohydrate diet on the other 2 days. Whatever the diet cycle selected by the user, it may have a constant pattern week to week or may change. An example of a change may be a user may select a 5:2 cycle for part of a month and switch to a different diet cycle for another part.

[0039] At window C of the user interface 200, the user may indicate to the control application 120, that the user intends to have fixed keto days by selection of the "Yes" or "No" buttons. The user interface (UI) 200 may transition from window C to window D, where the user is presented a graphical user interface that enables the user to input keto days that are days (represented by the first letter of the day starting at the left with S for "Sunday" and ending with at the right with S for "Saturday") the user intends to adhere to a keto diet. This enables the user to indicate to the control application the day the user intends to follow a variable diet cycle by selecting specific days as keto days. In a further example (not shown), a calendar may be presented the enables the user to indicate their diet cycle. Alternatively, the user may explicitly set the day as a specific keto day, for example at the beginning of the day (e.g., before breakfast) the user may indicate the day is a keto day. The control application may be operable to, according to a default or a user set notification schedule, present a graphical user interface so the control application can confirm with the user whether today is a Keto-Day first thing in the morning. Of course, the user has an option through the graphical user interface to end the ketogenic diet and return to a regular diet if desired at any time. With the keto day's indicated, the controller is operable to, based on the indication of the keto diet, the MDA algorithm may be operable to reduce the delivery of insulin to the user. This reduction in insulin delivery may be regardless of whether the user is a person with either type 1 diabetes or type 2 diabetes. The reduction in insulin delivery may be via a reduction in basal delivery, bolus dosages, or a combination of both as described below.

[0040] In an operational example, with reference to window A of FIG. 2, the processor may be operable to determine, based on an input received from a graphical user interface presenting on a touchscreen display, whether the user is starting a ketogenic diet. In response to the determination that the user is starting the ketogenic diet, the processor may present in window B of FIG. 2 a prompt to determine whether every day of the week is a ketogenic diet day or if the user is participating in a diet cycle (such as the 5 day: 2 day keto or the like). The processor, in response to the determination that the user is participating in the diet cycle, may be operable to generate, as shown in window C of FIG. 2, a prompt for an indication of whether the ketogenic diet is on fixed days of the week. In response to an indication that the ketogenic diet is on fixed days of the week, the processor as shown in window D of FIG. 2, may be operable to present an interactive calendar with days of the week for selection by a user.

[0041] Additionally, or alternatively, the control appli-

cation may be configured to respond to frequent changes between keto and non-keto diet on a meal-to-meal basis. For example, a user may turn off keto mode multiple times throughout the day but may, for example, be prompted to adjust the bolus number (e.g., a dosage and frequency of the bolus). If the user is switching their diet cycle mode on a meal-to-meal (i.e., keto to non-keto) basis, the algorithm may be operable to focus on adapting the bolus number (e.g., the number of boluses and/or the dosage amount per bolus). The GUI may include an indication of the meal mode, such as a Keto Diet banner on a main screen of the GUI when in either the Keto meal mode or a Non-Keto (or Regular) meal mode.

[0042] For example, when a user is cycling between a keto and non-keto diet either every day or several times a week or the like, the Drug delivery system may cause the presentation of the graphical user interface (GUI) on a controller. The user may select the diet cycle via an input to the UI 200, such as a ketogenic diet cycle. Other types of diets may also be presented, such as Paleo diet, vegan diet, or the like, and these may be referred to as a "diet mode" selectable by a user. The particular days or times or meals for which the user is following the particular diet may be referred to as a diet cycle. In a specific example, when the Ketogenic diet is selected as a diet mode in a diet cycle, the days which are non-keto days may utilize the baseline TDI values with the basal again calculated as $0.5 \cdot \text{TDI}/24$ units/hour and the bolus amounts being $x\%$ of TDI with x varying from 3% to 10% with larger ranges possible based on personalization. Of course, the value 0.5 may be modified based on the user's time in range (e.g., 110-150 mg/dL of glucose).

[0043] The described drug delivery system may be operable to provide ketone monitoring via, for example, by the ketone sensor 196 of FIG. 1. For example, under regular carbohydrate ingestion, glucose is the main substrate for glycolysis, which results in the production of adenosine triphosphate (ATP), the body's main energy source. However, under conditions of carbohydrate restriction (> 48-72 hours or the like) liver glycogen stores get depleted. Without glucose as a substrate for ATP production, the liver breaks down triglycerides to make ketone bodies to travel to target tissues (e.g., brain, muscles) and generate ATP. This process of ketogenesis may be regulated by insulin; the low carbohydrate levels leading to low insulin levels, which in turn promotes ketosis.

[0044] In some examples, a drug delivery system may be equipped with a continuous ketone sensor. For example, the continuous ketone sensor and the continuous glucose monitor (CGM) may be integrated within the insulin delivery system as one physical unit. The continuous ketone sensor may determine a concentration of the enzyme 3-hydroxybutyrate by detecting and measuring the 3-hydroxybutyrate dehydrogenase (3HBDH). Examples of ketone levels and their corresponding physiological status for nutritional ketosis are summarized in Table 1 below:

Physiological Status	Ketone Level
Nutritional Ketosis	0 - 1.4 mmol/L
Optimal Ketosis	1.5 - 3.0 mmol/L
Diminishing Returns	3 mmol/L
Danger	10 mmol/L

[0045] Where Ketosis = generation of ketones and nutritional ketosis is for users that on a keto diet, the body is changing and instead of using carbs, the liver is breaking down fat to produce energy, and as a result the user's ketone levels are low. Low ketone levels may be a new normal parameter for people who start a keto diet. If the person stays on the keto diet, it is presumed the user's ketone generation eventually elevates to "Optimal Ketosis" levels (1.5-3.0 mmol/L). When ketone levels rise over 3 mmol/L, the diet is providing diminished returns and the user may begin to experience progressive symptoms of nausea and diarrhea to vomiting and more extensive diarrhea as well as other physiological changes. As shown in the process examples herein, if a user's ketone levels go above 3 mmol/L, the control application may be configured to evaluate the amount of insulin delivered to the user (over a preset period of time) to determine whether additional insulin should be delivered, or provide a prompt via a graphical user interface on the user interface for the user to ingest additional carbohydrates. In one or more examples, the processor may be operable to detect automatically whether the user is adhering to a keto diet. In some examples, the processor by executing the algorithm may be able to use on the ketone sensor to determine the user's adherence to the keto diet. The algorithm may also be operable to determine adherence to the keto diet without a ketone sensor. For example, the algorithm may be operable to cause the processor to evaluate the BG pattern and total daily insulin (TDI) for a given period of time, such as 3 hour, 10 hours or the like. An alert may be generated to indicate that the user is not adhering to their keto diet, when the TDI increases upwards of approximately 67%.

[0046] The processor based on the disclosed algorithm, may be operable to adapt the basal and bolus insulin doses as the user transitions to a ketogenic diet by determining a reduction in TDI (e.g., approximately 60%). For example, TDI may initially be reduced by 40% on day 1 of the keto diet, then on day 2 and subsequent days of being on the keto diet, the basal and bolus insulin for the prior day is used to calculate TDI. The processor may be operable to predict basal and bolus insulin doses based on a different TDI input.

[0047] With regard to insulin adaptivity, as the user transitions from a regular diet to a ketogenic diet, both basal insulin and bolus insulin need to be reduced. Typical reductions in basal insulin on a ketogenic diet from baseline may be 10% to 20% or more. Total daily insulin

(TDI) requirements have been observed to drop by as much as 44% compared to baseline when on a ketogenic diet. Accordingly, the ketogenic diet TDI setting may be reduced by approximately 44%. In some embodiments, the processor may reduce the TDI by a lesser amount, say 15% to 20% initially, and gradually reduce TDI further up to approximately 40% - approximately 44%, or the like, from baseline as the Keto diet pattern is stabilized. The control application may monitor the user's ketone levels and glucose levels to ensure the user is staying within the optimal ketone range (e.g., 1.5-3.0 mmol/L). Based on the results of the monitoring, the control application may determine whether insulin (either basal and/or bolus) needs to be increased or further reduced. For example, the 15%-20% reduction in TDI may be modified based on levels of ketones and the user's glucose levels detected by a ketone sensor and a CGM. Frameworks for insulin adaptivity are discussed below and shown in FIGs. 3-6.

[0048] FIG. 3 illustrates an example technique that may be implemented by a control application of a drug delivery system when a user switches from a regular or non-ketogenic diet to a ketogenic diet. For example, after the user selects to enter "keto mode," for example, and/or indicates the respective days of a keto diet, the controller may adjust parameters or settings (e.g., 121, 124 or both of FIG. 1) of the control application.

[0049] As shown in FIG. 3, a user may switch to a ketogenic diet and enter a "keto mode" or "ketogenic diet mode." The technique 300 may be implemented when a user makes the switch to a ketogenic diet. In response to the indication that the user is following a ketogenic diet, the control application adjusts settings to correspond with the user's expected, reduced insulin needs. As the user's carbohydrate intake is reduced, the insulin delivered by the drug delivery system may be reduced a corresponding amount, or alternatively may be reduced by a reduction factor, to avoid the risk of hypoglycemia. As hypoglycemia is a primary risk in the transition to a ketogenic diet, the example technique 300 as executed by a processor may enable safe insulin delivery while monitoring the user's glucose and ketone levels.

[0050] The example technique 300 may include the interaction between a smartphone or a personal diabetes management device (PDM) 302, the MDA sensor sub-assembly 304 and MDA delivery system 306. The PDM 302 may be the same as or at least similar to the controller 104 of FIG. 1. For example, the PDM 302 may include a control application 303, a memory 305 and graphical user interface 307. The MDA delivery system 306 may be a wearable drug delivery system, such as wearable drug delivery system 102 of FIG. 1, or the like.

[0051] The control application 303 in response to the "start keto" indication 333 or entering "keto mode" (as described with reference to FIG. 2) via the GUI 307 may obtain a baseline total daily insulin (TDI) 331 from memory 305. The baseline TDI may be, for example, be the most recent TDI setting for the user regardless of whether

it is a TDI for a regular diet day or a Keto diet day. Baseline TDI may differ from one user to another user. Starting with the baseline TDI 331 and at the onset of a ketogenic day (e.g., Keto day), the Keto TDI may be set to approximately 60% of the baseline TDI. After 310, the Keto TDI may be provided to the MDA delivery system 306. The MDA delivery system 306 may be operable to use the Keto TDI to calculate basal and bolus dosages of insulin. For example, a keto-adjusted basal rate delivery may be set to $0.5 \times \text{Keto TDI} / 24$ units/hour. In the example, the MDA sensor subsystem 304 may include a processor that is operable to measure different physiological aspects of the user's blood. For example, the measurement of glucose following meals may be used to adjust bolus insulin delivery. A bolus dosage can be calculated as $x\%$ of TDI based on meal announcement. Typical values of x may range from 3% to 10% and may be personalized for larger ranges (e.g., 3% - 15%). Closed loop drug delivery systems may continue to deliver insulin based on glucose trends and MDA algorithm constraints. But with the Keto TDI that is reduced from the baseline TDI, the risk of hypoglycemia is significantly reduced. In some examples, ketone levels as well as glucose levels may be monitored continuously by the MDA sensor subsystem 304. The MDA sensor subsystem 304 may include a ketone sensor and a glucose sensor (such as those described with reference to FIG. 1) as well as other sensors, such as a blood oxygen sensor, a heart rate sensor, and the like, the outputs of which are provided to the control application 303 of the PDM 302.

[0052] In an example, the MDA sensor subsystem 304 may be operable to make measurements of nighttime glucose (e.g., 2:00 am or the like), via the measured nighttime glucose process 341, that may be used to further alter the Keto-adjusted basal rate. In the example, at 321, the processor may be operable to increase the Keto-adjusted basal rate by 5% or the like, if the measured nighttime glucose is elevated (e.g., + 10-20 mg/dL or greater) above the user's target set point (e.g., 110 mg/dL). This change at 321 indicates that basal insulin delivery was not sufficient.

[0053] Alternatively, at 322, if the measured nighttime glucose falls (e.g., - 15-25 mg/dL or more) below the user's target set point (e.g., 110 mg/dL), the processor may reduce the keto-adjusted basal dosage by 10% or the like. This change at 322 indicates that basal insulin delivery was greater than needed for the user.

[0054] The MDA sensor subsystem 304 when performing the process 300 may also be operable to measure a user's post prandial glucose via a measured post prandial glucose process 343. The control application 303, in response to receiving the measured post prandial glucose, the control application 303 may, at 323, increase the bolus dosage by 10%, if the post prandial glucose is elevated a predetermined amount, such as by 10-20 mg/dL or greater. Alternatively, the control application 303, in response to receiving the measured post prandial glucose, the control application 303 may, at 324, reduce the

bolus dosage by 10%, if the post prandial glucose falls a predetermined amount, such as by 10-20 mg/dL or more.

[0055] The MDA sensor subsystem 304 when performing the process 300 may also be operable to measure a user's post prandial ketone levels via a measure ketone level process 345. In response to the measured post prandial ketone levels, the control application 303 may be executed, at 325, a subprocess. In the subprocess at 325, if the post prandial ketone levels are low (e.g., 1 mmol/L), the control application 303 may reduce the bolus insulin to promote ketosis and safeguard against hypoglycemia. The output of whichever subprocess is executed at any of 321, 322, 323, 324 or 325 may be used by the control application 303 at 320 to calculate a new TDI. For example, the total insulin delivered via basal and bolus may be added to reestablish the new TDI. The new TDI may be used in calculations performed the next day. For example, the new TDI may be substituted for the baseline TDI 331 or may replace the baseline TDI 331 in the memory 305, where it would be used to set a Keto TDI in response to a start keto 333 indication.

[0056] FIG. 4 depicts an example diet cycle transition process from a ketogenic day diet back into a non-keto day of a diet cycle.

[0057] It is anticipated that users may alternate between consuming a ketogenic diet on some days (e.g., "Keto day(s)") and partaking in a non-ketogenic diet on other days (e.g., "Non-Keto day(s)"). To enable the MDA delivery system to accommodate this change in diet, an example diet cycle transition process 400 that utilizes the user interface of a controller, such as 104 of FIG. 1, to receive an indication of the change from a Keto day to a Non-Keto day, and this diet cycle transition process may be executed by a processor. In FIG. 4, the user is currently adhering to a keto day diet, but will be transitioning to a non-keto day diet. When the user is adhering to the keto day diet, the diet setting for the MDA delivery algorithm is a keto day 406 and the corresponding TDI setting is the keto day TDI setting 410. For example, the keto day 406 setting may include a keto day TDI 410 value that is determined based on historical data related to the user's glucose levels, meal-related data, such as carbohydrates, protein, and fat content of meals and the like, as well as other data (e.g., exercise history, ketone levels and the like). Recall that when a user is adhering to their keto diet, the keto day TDI 410 value is less than a non-keto day TDI value. In response to the keto day 406 setting, a processor, such as 119 or 114 of FIG. 1, may be operable to determine a keto day TDI value based on historical data related to the user's glucose levels, meal-related data, such as carbohydrates, protein and fat content of meals and the like, as well as other data (e.g., exercise history, ketone levels and the like).

[0058] In the diet transition example, the system setting for the user's total daily insulin (TDI) may be the keto day TDI setting 410. A user may indicate to the MDA delivery system that the present day is a non-keto day via a non-

keto day input 426 to the user interface (not shown in this example). In response, a processor executing the MDA delivery algorithm 432 may calculate a modified TDI as the non-keto day TDI using the keto day TDI. For example, the processor may calculate the non-keto day TDI as $1.67 \times \text{Keto TDI}$ as a modified TDI 420. The factor 1.67 may be tuned based on different user parameters and user adherence to the respective indicated diet day (i.e., keto day or non-keto day). Since the user was previously adhering to a keto diet in this example shown in FIG. 4, the baseline TDI is the determined Keto day TDI 410. At 430, the MDA algorithm 432 may utilize the modified TDI 420 and inputs from the MDA sensor subsystem 434 (e.g., ketone monitor, glucose monitor (including a CGM) and the like) to determine a modified treatment plan. For example, the MDA delivery algorithm 432, at 440, may determine adaptations to the user's non-keto day basal dosage and basal delivery rate as well as adaptations to the user's non-keto day bolus dosages, delivery rates and delivery schedules (i.e., basal and bolus insulin adaptation). At 450, the MDA delivery algorithm 432 executed by the processor may calculate a new non-keto day TDI based on the adaptations made to the non-keto day basal dosage and basal delivery rate and the user's keto day bolus dosages, delivery rates and delivery schedules at 440.

[0059] If a non-keto day continues the next day the new non-keto day TDI determined at 450 becomes (i.e., non-keto day TDI) will be the baseline TDI, such as 410, to be used for the next day as well, whether it is a repeat of the non-keto day or a start of a new keto day.

[0060] FIG. 5 depicts an example diet cycle transition from a non-ketogenic day diet back into a ketogenic day of the diet cycle. To enable the MDA delivery system to accommodate this change in diet, another example of a diet cycle transition process 500 that utilizes the user interface of a controller, such as 104 of FIG. 1, to receive an indication of a change in diet from a non-keto day to a Keto day may be executed by a processor. For example, when adhering to a non-keto day diet, the diet setting for the ADD delivery algorithm is a non-keto day 506 and the user's total daily insulin (TDI) may be the non-keto day TDI 510. Recall that when a user is adhering to their non-keto diet, the non-keto day TDI setting is typically greater than a keto day TDI setting. The non-keto day 506 setting may include the non-keto day TDI 510. A user may indicate via a keto day input 526 to the user interface (not shown in this example) to the MDA delivery system that today is "a non-keto day," which indicates the diet for the present day is a non-ketogenic diet. In response to the non-keto day 506 setting, a processor, such as 119 or 114 of FIG. 1, executing the MDA delivery algorithm 532 may calculate the modified TDI 520 based on historical data related to the user's glucose levels, meal-related data, such as carbohydrates, protein and fat content of meals and the like, as well as other data (e.g., exercise history, ketone levels, and the like). For example, the processor may calculate the modified TDI 520

as, for example, $0.6 * \text{Non_Keto_Day_TDI}$. The factor 0.6 may be tuned based on different user parameters and user adherence to the respective indicated diet day (i.e., keto day or non-keto day).

[0061] Since the user was previously adhering to a keto diet in this example shown in FIG. 5, the baseline TDI is the determined non-Keto TDI 510. At 530, the MDA algorithm 532 may utilize the modified TDI 520 and inputs from the ADD sensor subsystem 534 (e.g., ketone monitor, glucose monitor (including a CGM) and the like) to determine a modified treatment plan. For example, the MDA delivery algorithm 532 may determine, at 540, adaptations to the user's non-keto day basal dosage and basal delivery rate as well as adaptations to the user's non-keto day bolus dosages, delivery rates and delivery schedules (i.e., basal and bolus insulin adaptation). At 550, the MDA delivery algorithm 532 executed by the processor may calculate a new keto day TDI based on the adaptations made to the keto day basal dosage and basal delivery rate and the user's non-keto day bolus dosages, delivery rates and delivery schedules at 540.

[0062] In the example, if a keto day continues the next day, the new keto day TDI from 550 will be the baseline TDI to be used by the MDA delivery algorithm 532 for the next day. And the keto TDI or baseline TDI may be adjusted as explained above to account for the keto day continuing to the next day.

[0063] When implementing ketone monitoring, ketone levels are typically approximately < 0.5 mmol/L to approximately 1.0 mmol/L. Exercise may elevate ketone levels further by up to approximately 0.5 mmol/L for moderate exercise. Exercise may further elevate ketone levels with levels going up to approximately 3 mmol/L. Ketone levels are also increased under low carbohydrate diets. Under regular carbohydrate ingestion, glucose is the main substrate for glycolysis, resulting in the production of adenosine triphosphate (ATP), the body's main energy source. However, under conditions of carbohydrate restriction (> 48 - 72 hours) liver glycogen stores get depleted. Without glucose as a substrate for ATP production, the liver breaks down triglycerides to make ketone bodies to travel to target tissues (e.g., brain, muscles) and generate ATP. This process of ketogenesis is regulated by insulin; the low carbohydrate levels leads to low insulin levels, which in turn promotes ketosis. Starvation ketosis may elevate ketone levels up to a concentration of 5 mmol/L.

[0064] In either transition illustrated in FIG. 4 or FIG. 5, the monitoring of the ketone levels as well as the TDI trends may be used to determine how well the user is maintaining their time within range of their target glucose setpoints or another metric. If the ketone levels are between, for example, approximately 1.5 mmol/L to approximately 3 mmol/L for post meal periods, the MDA system may determine that the ketosis is optimal. However, if the user's TDI falls over a period of time, the MDA system may determine that the insulin requirements are reducing (which may be because of reduction in insulin resistance

as well as a user's weight loss).

[0065] FIG. 6 illustrates a flowchart of an example process for monitoring a user's adherence to their ketogenic diet. A control application executed by a processor of MDA system, such as the processor 119 of the controller 104 of FIG. 1, may be operable to monitor adherence of the users to the designated ketogenic diet by measuring and evaluating the user's ketone level. For example, the processor may prompt the user to indicate, at 610, whether the day's (or another time period) diet is a keto diet day (i.e., keto day). If, in response to the prompt, the processor receives an affirmative response, the process 600 may proceed to decision 620. Instead of the control application prompting the user, the control application may retrieve information obtained via the GUI 200 to determine whether today is a keto diet day. At 620, the processor may determine if the post meal ketone levels are between a preset range, such as, for example, approximately 1.5 mmol/L to approximately 3 mmol/L (which indicates optimal ketosis) or approximately 0.5 mmol/L to approximately 5 mmol/L. In response to the post meal ketone levels being determined to be between the preset range, the processor may determine that there is good adherence to the diet and return to the beginning of the process 600. Alternatively, if the post prandial ketone levels are not within the preset range at 620, the processor may determine the user is not adhering to the ketogenic diet and, at 625, sends a query or the like to a user device confirming with the user that today is a keto day.

[0066] Returning to step 610, if the user indicates to the processor that today is not a keto diet day, the processor may proceed to step 630. At 630, the processor may determine whether the post meal ketone levels are below a minimum value or lower boundary of the preset range, such as, for example, 0.5 mmol/L or the like. In response to a determination that the post meal (i.e., post prandial) ketone levels are less than the minimum value or the lower boundary, it is likely that the user is adhering to a non-ketogenic diet (i.e., a "YES" at 630). In response to such a determination, at 635, the process 600 may restart. Alternatively, at 630, if the post meal (i.e., post prandial) ketone levels are determined to be greater than the minimum value or lower boundary and the determination indicates that "NO" the user is not adhering to a non-ketogenic diet, the processor may send a notice confirming today is a non-keto diet day. For example, the process 600 may cause the generation of a pop-up menu to confirm with the user whether they are adhering to the expected diet plan.

[0067] Diabetic Ketoacidosis (DKA) Monitoring: The ketone levels and glucose levels may be monitored to detect incipient DKA, and if incipient DKA is detected, a prompt response may be carried out by the MDA system, for example, by delivering an insulin bolus and/or increasing the user's basal rate temporarily. Diabetic ketoacidosis, also known as DKA, is a buildup of acids in your blood. It can happen when your blood sugar is too high

for too long. DKA is a serious complication of diabetes and could be life-threatening.

[0068] FIG. 7 illustrates a flowchart of a process for monitoring and intervening steps for avoiding diabetic ketoacidosis (DKA). The monitoring of DKA includes a processor, an algorithm (such as 700 represented by programming code and stored in memory (not shown in this example)), and at least one or more inputs to a processor 710, such as recent glucose values 713, ketone levels 715 and auxiliary activity sensors 717, such as a smart watch, a heart rate monitor, a fitness device (e.g., wearable on the wrist), a global positioning system device, and the like. In the process 700, the processor may obtain ketone levels 715 from a memory or from a ketone sensor. At decision block 720, if the ketone levels 715 are, for example, greater than (>) 3 mmol/L, the processor may interpret this result as a sign that the ketone levels are elevated or on the higher side of an ideal range. In response to a determination that the ketone levels are less than (<) 3 mmol/L, the processor may return to 720 to continue to monitor the ketone levels 715. Alternatively, in response to an affirmative determination that ketone levels are greater than (>) 3 mmol/L, the processor may point to a need to increase insulin delivery and proceed to decision block 730.

[0069] Depending on the type of diabetes that a user has been diagnosed as having, the control application may implement different responses when the particular user is partaking in a ketogenic diet. For example, a user with Type 2 diabetes may have their bolus dosages reduced, and a user with Type 1 may have an overall reduction in the delivery of insulin. When the user is on a keto diet, the MDA algorithm implemented by the control application may, for example, be operable to reduce a user's TDI by separating out and independently adjusting basal delivery and bolus dosages to make sure that the respective basal deliveries and bolus dosages are delivered according to an appropriate schedule and within an acceptable range. The control application is operable to monitor ketones (via, for example, ketone sensor 196) simultaneously to ensure the user is adhering to the indicated keto diet and is not at risk of hypoglycemia.

[0070] For example, at 730, the processor may determine that one or more of the recent glucose (BG) values 713 are greater than 250 mg/dL. In response to a determination that the ketone levels are > 3 mmol/L and at least one of the BG values is greater than (>) 250 mg/dL, the processor may be operable, at 737, to cause delivery of a correction insulin dose of x% of TDI (where x is between 3% and 10%) (so as to increase insulin on board or IOB) and generate a prompt on a GUI for the user to increase hydration. Alternatively, at 730, in response to a determination that the ketone levels are > 3 mmol/L and none of the BG values is greater than (>) 250 mg/dL, the processor may proceed to 735. At 735, the processor may be operable to cause generation of a prompt for the user to increase hydration and ingest carbohydrates (carbs). After generation of the prompts and/or delivery

of the correction insulin dose, the process 700 returns to 720 to continue to monitor the ketone levels.

[0071] The examples of FIGs. 6 and 7 may be combined as a single embodiment to enable the system to determine adherence to a chosen diet (i.e., a ketogenic diet or a non-ketogenic diet) as well as provide assistance with the possibility of DKA.

[0072] Another process provides monitoring for diet adherence to the ketogenic diet. For example, the controller may confirm diet adherence by monitoring ketone levels and determining if nutritional ketosis has set in. Additionally, adherence to the ketogenic diet or the lack of adherence can be flagged and the appropriate feedback may be provided to the user. In an example, the control application may be operable to ensure compliance with a designated ketogenic diet (i.e., a diet plan set by the user according to the examples described above) based on ketone level measurements provided by the ketone sensor. The designated ketogenic diet from FIG. 2 may also include settings for how strict of a ketone diet the user intends to follow. For example, a strict ketogenic diet may involve consumption of less than 30 grams of carbohydrates a day (with an appropriate range of fat and protein levels to meet caloric needs), while a less strict ketogenic diet may involve consumption of 50 grams of carbohydrates a day with a different range of fat and protein levels to meet caloric needs. In an example, after a user indicates that they are following a ketogenic diet, the user's ketone levels are expected to rise. For example, a typical ketone level increase experienced by a user following (or on or partaking in) a ketogenic diet may be approximately 1.5-3 mmol/L.

Safety Monitoring in Type 2 Users on drug delivery systems and sodium-glucose cotransporter-2 (SGLT2) inhibitors

[0073] A system, such as MDA system 100 of FIG. 1, equipped with a continuous ketone sensor and a glucose sensor that implements the process 600 may feasibly provide a warning system for both diabetic ketoacidosis (DKA) and euglycemic diabetic ketoacidosis (euDKA). DKA is a combination of hyperglycemia (e.g., a glucose level greater than 250 mg/dL), acidosis and ketosis. Euglycemic Diabetic Keto Acidosis (euDKA) is a rare condition that may be experienced by Type 2 diabetic patients who use SGLT2 and when the patient partakes in a low carbohydrate diet, and/or alcohol ingestion, and/or after exercising. Other precipitating factors can also include sickness (vomiting, dehydration, viral or bacterial infection) and fasting. The near normal glucose levels seen in euDKA caused by SGLT2 inhibitors results from a balance between endogenous glucose production and renal glucose clearance. Type 1 diabetics may also take SGLT2 inhibitors off label and face euDKA risks as Type 2 diabetics.

[0074] In addition to the above steps, additional steps may be implemented based on the determined levels of

ketones. For example, ketone levels greater than 10 mmol/L are a sign of impending DKA. The processor, for example, may cause implementation of DKA protocols for prompting the user to seek medical attention or consume hydration and/or electrolytes as well as manage insulin delivery via the drug delivery system to address impending DKA. However, actions may be taken before ketone levels are greater than 10 mmol/L. For example, preventive action can be taken when the ketone levels exceed 5 mmol/L, such as generating prompts for the user to increase hydration, ingest carbohydrates, and adjustments to the MDA to increase the amount of insulin delivered via basal and bolus delivery.

[0075] The following is a discussion of example processes for monitoring for euglycemic Diabetic Keto Acidosis (euDKA) by using continuous monitoring of ketone levels with a subcutaneous ketone sensor, a continuous glucose monitor, and exercise monitoring with on board heart rate and accelerometer sensors.

[0076] The processes include another example of ketone monitoring and exercise monitoring. In the example, processes, ketone monitoring may be performed by a drug delivery system using an embedded/auxiliary ketone sensor that monitors ketone levels continuously subcutaneously. Exercise is monitored because, in some cases, exercise elevates ketone levels. Exercise monitoring may be performed by using an optional onboard heart rate monitor and accelerometer sensors. Exercise can in some cases elevate ketone levels. The described processes also include euDKA monitoring, in which the ketone levels and glucose levels of a user may be monitored for prompt response to incipient euDKA. Since the drug delivery system processor has access to BG measurement values, the processor may also check for classic DKA.

[0077] Drug delivery systems, such as those shown in FIG. 1, may be equipped with a continuous subcutaneous ketone sensor. A concentration of 3-hydroxybutyrate may be determined by a ketone sensor, which may be integrated with a CGM sensor, based on a measurement of the 3-hydroxybutyrate dehydrogenase (3HBDH) enzyme. In some examples, hydrogel membranes have been used to improve ketone concentration and reduce electrode fouling. Ketone levels for nutritional ketosis are summarized in Table 1 above. In other examples, the ketone sensor and the CGM sensor may be integrated within the insulin delivery system (e.g., wearable drug delivery device 102 of FIG. 1) as one physical unit or a combination of units that may be coupled together to form a singular unit.

[0078] FIG. 8 illustrates a flowchart of an example process for monitoring a user using ketone sensing and activity sensing for DKA. The process 800 of FIG. 8 shows the evaluation of different ketone levels with respect to glucose levels, low carbohydrate diet type, and exercise level with actions taken in response to different evaluation results. The inputs 810 to the processor may be provided by a glucose (BG) sensor, a ketone sensor, and

an activity sensor and may include, respectively, recent glucose values 812 (e.g., BG values within the last 15 minutes or the like), ketone levels 814 (e.g., ketone values within the last 30 minutes or the like), and auxiliary activity sensor values 816 (e.g., heart rate in last 5 minutes, blood oxygen level in last 10 minutes, and the like). When all of those sensors are communicatively coupled to a controller, such as 104 of FIG. 1, no input is needed from the user. However, different actions or interpretations by the processor may be confirmed with user inputs/questions via a GUI. For example, different evaluation paths may be followed based on an evaluation of the respective recent glucose values 812, ketone levels 814, and auxiliary activity sensor values 816. These respective values may be evaluated beginning at step 821.

[0079] At 821, the processor may determine whether the user's ketone levels are greater than a second ketone threshold, such as 3 mmol/L, or the like. If the determination is "Yes", the user's ketone levels are greater than the second ketone threshold, the process 800 may proceed to 831 at which the processor may determine whether the user's ketone levels are less than a third ketone threshold, such as 5 mmol/L or the like. The second ketone threshold is less than the third ketone level. If the determination is "Yes", the user's ketone levels are less than the third ketone threshold, the process 800 may proceed to 851 at which the processor may generate a prompt on a GUI inquiring whether the user is on a low carbohydrate (carb) diet. If the processor receives an input at 851 confirming the user is on the low carbohydrate diet, the process 800 may return to 810. Alternatively, at 851, if the processor receives an input at 851 indicating that the user is not on a low carbohydrate diet, the process 800 may proceed to 852. At 852, the processor may generate a prompt on a GUI inquiring whether the user just exercised. If the response to the GUI query at 852 is "Yes," the process 800 may return to 810. Alternatively, if the response to the GUI query at 852 is "No, have not exercised," the process 800 may proceed to 853. At 853, the processor may determine whether the user's BG levels are greater than a maximum BG level, such as 250 mg/dL or the like. In response to the determination that the user's BG levels are greater than a maximum BG level (i.e., a "Yes" at 853), the processor may generate a notification, such as a window on a GUI, recommending that the user increase their hydration as well as, either automatically or upon user confirmation, cause a wearable drug delivery device to deliver increased insulin. Conversely, in response to the determination that the user's BG levels are less than a maximum BG level (i.e., a "No" at 853), the processor may generate a notification, such as a window on a GUI, recommending that the user increase their hydration.

[0080] Returning to 831, in response to a determination that the user's ketone levels are not below the third ketone threshold, the process 800 may proceed to 832. At 832, the processor may determine whether the user's ketone levels are less than an extreme ketone threshold.

If the determination is "No" or "the user's ketone levels are greater than an extreme ketone threshold," the processor may cause an alert, including audio signals as well as a visual notification in addition to the GUI prompt for the user to seek medical attention. Additionally, in a smartphone implementation example, the processor may be operable to cause a calling application of the smartphone to call a healthcare provider or emergency service provider (e.g., by dialing "911" or the like). In the case of ketone levels greater than 10 mmol/L (which is an indication of diabetic ketoacidosis), a notification may be provided for the user to seek medical attention. In addition, should the user's BG levels be greater than, for example, 250 mg/dL (which is a maximum BG threshold), the processor may cause the delivery of insulin (to lower the BG levels) by a wearable drug delivery device (such as 102 in FIG. 1 and a recommendation for the user to ingest carbohydrates (to reduce the ketone levels). For example, a healthcare provider may administer electrolytes, glucagon, carbohydrates and provide hydration. Alternatively, if at 832, the determination is "Yes", the user's ketone levels are less than an extreme ketone threshold, the process 800 may proceed to 841.

[0081] At 841, the processor evaluates the user's glucose levels with reference to a maximum BG threshold, which may be dependent on each respective user. In the example of FIG. 8, the maximum BG threshold is 250 mg/dL. If a user's glucose value is greater than the maximum BG threshold (e.g., 250 mg/dL) (i.e., "YES", the BG level is greater than the maximum BG threshold), the processor may cause a notification to be generated on the GUI for the user to increase their hydration and the processor may send a signal to the wearable drug delivery device causing an increase in the delivery of insulin to the user (e.g., via a correction bolus or via a temporary increase to the user's basal rate). Alternatively, if the determination at 841 is "No, the BG level is not greater than the maximum BG threshold, the processor may cause a notification to be generated on the GUI for the user to increase their hydration and ingest carbohydrates.

[0082] Returning to 821, if the determination by the processor is "No," the ketone levels are not greater than the second ketone threshold, the process 800 proceeds to 822. At 822, the processor evaluates the ketone levels 814 measured by the ketone sensor with respect to a first ketone threshold. The first ketone threshold is less than the second ketone level.

[0083] If the result of the evaluation or the determination at 822 is "Yes," the ketone levels are greater than the first ketone threshold, the process 800 proceeds to 823. At 823, the processor evaluates the user's glucose levels with reference to the maximum BG threshold, and if the result of the evaluation is the user's glucose levels are less than the maximum BG threshold (i.e., "NO"), the processor generates a prompt 824 on the GUI for the user to increase hydration. Alternatively, if the result of the evaluation is the user's glucose levels are greater than the maximum BG threshold (i.e., "Yes"), the proc-

essor generates a prompt 825 on the GUI for the user to increase hydration and the processor may send a signal to the wearable drug delivery device causing an increase in the delivery of insulin to the user.

5 **[0084]** Returning to 822, if the result of the evaluation or the determination at 822 is "No," the ketone levels are not greater than the first ketone threshold, the process 800 proceeds to 833.

10 **[0085]** At 833, the processor still takes the precaution to evaluate the user's glucose values with respect to the maximum BG threshold. If, at 833, the result of the evaluation by the processor is the user's glucose levels are less than the maximum BG threshold (i.e., "NO"), the processor generates a prompt 834 on the GUI for the user to increase hydration. Alternatively, if the result of the evaluation is the user's glucose levels are greater than the maximum BG threshold (i.e., "Yes"), the processor generates a prompt 835 on the GUI for the user to increase hydration and the processor may send a signal to the wearable drug delivery device causing an increase in the delivery of insulin to the user.

15 **[0086]** Recommendations such as to increase hydration; ingest carbs; and/or seek medical attention may be output via the GUI. The processor may be further operable to adjust medicament delivery to the user automatically without alerting the user.

20 **[0087]** For example, in an operational example, the processor may obtain ketone levels of a user either from the inputs to the processor 810 or by accessing a memory device storing the ketone levels. The processor may be operable to evaluate the obtained ketone levels with reference to a plurality of ketone thresholds. Based on the result of the evaluation, the processor may provide an indication for a further action by the processor, such as the further actions of presenting a notification to seek medical attention at 836, noting in an MDA/ADD/AP application that the user is on a low carbohydrate diet 851, or the user exercised 852. For example, the processor may adjust settings in the MDA/ADD/AP application to indicate that the user is on a low carbohydrate diet or the user exercised and the adjusting settings may be operable to compensate for the low carbohydrate diet (e.g., reducing bolus dosage amounts and the like) or the user's participation in exercise (e.g., a setting to deal with increased ketones and decreased glucose levels).

25 **[0088]** The processor based on the evaluation of a user's ketone levels and an evaluation of the user's glucose level(s) may be further operable to generate additional indications in case the user is potentially experiencing euDKA. Based on the additional indications, the processor may be operable to present a notification to ingest carbohydrates, such as at 836 and 842, presenting a notification to increase hydration, such as at 824, 825, 835, 842, 844, 854, and 855, generating a signal to increase insulin delivery, such as 825, 835, 836, 844, and 854, or a combination thereof, such as 825, 835, 836, 842, 844, and 854.

30 **[0089]** In the example process 800, the processor may

determine that the user's BG levels may be in range of the target setpoint, but the user's ketone levels might be higher than normal for the particular user. This condition may be in response to the user's use of SGLT2. In addition, if the user is taking SGLT2 and insulin, the user may go into higher ketosis states (e.g., ketones greater than 3 mmol/L) and yet the user's BG is in a normal range, so there is a risk of eDKA for the user.

[0090] Another process provides monitoring for hypoglycemia. Hypoglycemia monitoring may include a control application implementing a reduction in insulin dosages to safeguard against hypoglycemia. In addition, the control application may monitor trends in a user's glucose levels and/or insulin on board levels and based on the monitored trends, take actions to prevent occurrences of hypoglycemia. For example, based on the monitored trends, the control application may suspend insulin or alerting the user to ingest fast acting carbohydrates. Onboard (e.g., wearable, and wireless communication-equipped) activity sensors, when available or when coupled to a controller, provide additional insights into projected glucose trends of the user. For example, exercise monitoring may be accomplished via auxiliary activity sensors, such as a heart rate monitor and/or accelerometer. The data from one or both of these sensors may provide data related to an activity level and type of exercise performed by the patient. For example, the analyte sensor(s) may be a snap fit sensor unit including heart rate and accelerometer sensors for exercise monitoring and type of exercise and intensity level. In other embodiments, activity data from fitness devices, such as a Fitbit® or the like, may be used.

[0091] FIG. 9 illustrates a flowchart of a process for monitoring for hypoglycemia. The processor of drug delivery system may be operable to monitor a user for hypoglycemia. For example, inputs to processor 910 may include at least one or more of recent glucose values 913, recent insulin delivered values 915, ketone levels 917 or auxiliary activity sensors 919. Trends in the glucose and the current insulin on board can be used to predict if the glucose is going to fall rapidly in the next half hour at 920 (e.g., below a minimum target setpoint, for example, 70 mg/dL). Utilizing a recurrent neural network (RNN) model that accepts the inputs 913, 915, 917 and 919, the processor evaluates the glucose prediction from 920 at 930. For example, the processor, for example, using a recurrent model may determine a trend of the predicted glucose values over time, such as a rate of change or the like, to determine a projected value of the predicted glucose values over a short term. The short term may be a number of hours, such as 3-6, or the like.

[0092] Returning to back to the discussion of FIG. 9 at 930, if the determination is YES, a fall to below a minimum target setpoint or a minimum glucose threshold value is projected, the processor may proceed to 940 at which the processor may generate a prompt on a GUI for the user to ingest carbs, elevate the minimum target setpoint or a minimum glucose threshold value, and the processor

may also reduce or suspend basal insulin. Conversely, if NO, a fall below the minimum target setpoint or a minimum glucose threshold value is not projected, the processor may return to 910 to receive inputs.

5 **[0093]** The ADD sensor subsystem may, for example, also be equipped with other auxiliary sensors for activity monitoring including heart rate, accelerometer, skin conductance. These sensors may detect exercise and respond by lowering basal insulin at the time of exercise, elevate glucose setpoint in the Drug delivery system, suggest hydration. Glucose levels may, for example, be predicted using a recurrent neural network to alter basal insulin. The process 900 of FIG. 9 depicts hypoglycemia prediction and alerts.

10 **[0094]** A brief discussion of an RNN implementation may be beneficial. FIG. 10 illustrates an example of a recurrent neural network (RNN) in the form of a long short-term memory being trained to estimate or predict future glucose measurement values based on past glucose measurement values. As an example of glucose prediction, we may have a sequence of values that span 30 minutes of data (7 data points spread at 5 minutes). The RNN can be used to predict the glucose measurement value after 30 minutes. For example, given a sequence of glucose measurement values BG1 through BG7, the RNN may be trained to predict a later glucose measurement value, such as BG8. In the example of FIG. 4D, the glucose measurement values: BG1, BG2, BG3, BG4, BG5, BG6, BG7 may cause the RNN to output BG8. The BG8 value may be used in subsequent training. For example, a typical training sequence may resemble:

BG1, BG2, BG3, BG4, BG5, BG6, BG7->output BG8;
 35 BG2, BG3, BG4, BG5, BG6, BG7, BG8->output BG9;
 BG3, BG4, BG5, BG6, BG7, BG8, BG9->output BG10; ...
 40 BG18, BG19, BG20, BG21, BG22, BG23, BG24->output BG25.

45 **[0095]** FIG. 10 shows an example LSTM type of recurrent neural network being trained with a sequence of 7 glucose measurement values (BG₁ to BG₇) to predict the 8th value (BG₈). The above training framework may be extended with an input of greater than 7 glucose measurement values and an output greater than one glucose measurement value, for example, 2-10 estimated glucose measurement values may be output from the RNN. Also, the sequence of predictions may include additional input variables other than glucose measurement values. For example, the additional input variables may include inputs such as a stress value, an insulin dose and carbohydrate values to predict the sequence of glucose measurement values. The LSTM implementation is effective to mitigate and even eliminate the vanishing gradient problem that may occur when gradient-based learning methods and backpropagation is utilized. In the ex-

ample illustrated in FIG. 10, the long short-term memory (LSTM) 1010, may predict a user's glucose value after, for example, 30 minutes, 40 minutes, 60 minutes, or the like. The LSTM may be trained with sequences of 7 contiguous values and the LSTM is operable to learn the 8th value (which may be 30 minutes in the future) and more values.

[0096] As shown above, the represented training framework may be extended with an input of greater than 7 values and an output greater than one measurement. Also, the sequence predictions can include other variables such as a stress value, an insulin dose and carbohydrate values to predict the glucose sequence.

[0097] Software related implementations of the techniques described herein, such as the processes examples described with reference to the above discussion and figures may include, but are not limited to, firmware, application specific software, or any other type of computer readable instructions that may be executed by one or more processors. The computer readable instructions may be provided via non-transitory computer-readable media. The various elements of the processes described with reference to the figures may be implemented in devices, apparatuses or systems that may include various hardware elements, software elements, or a combination of both. Examples of hardware elements may include structural members, logic devices, components, processors, microprocessors, circuits, processors, circuit elements (e.g., transistors, resistors, capacitors, inductors, and so forth), integrated circuits, application specific integrated circuits (ASIC), programmable logic devices (PLD), digital signal processors (DSP), field programmable gate array (FPGA), memory units, logic gates, registers, semiconductor device, chips, microchips, chip sets, and so forth. Examples of software elements may include software components, programs, applications, computer programs, application programs, system programs, software development programs, machine programs, operating system software, middleware, firmware, software modules, routines, subroutines, functions, processes, procedures, software interfaces, application program interfaces (API), instruction sets, computing code, computer code, code segments, computer code segments, words, values, symbols, or any combination thereof.

[0098] Some examples of the disclosed device or processes may be implemented, for example, using a storage medium, a computer-readable medium, or an article of manufacture which may store an instruction or a set of instructions that, if executed by a machine (i.e., processor or controller), may cause the machine to perform a method and/or operation in accordance with examples of the disclosure. Such a machine may include, for example, any suitable processing platform, computing platform, computing device, processing device, computing system, processing system, computer, processor, or the like, and may be implemented using any suitable combination of hardware and/or software. The computer-readable medium or article may include, for example, any suitable

type of memory unit, memory, memory article, memory medium, storage device, storage article, storage medium and/or storage unit, for example, memory (including non-transitory memory), removable or non-removable media, erasable or non-erasable media, writeable or re-writable media, digital or analog media, hard disk, floppy disk, Compact Disk Read Only Memory (CD-ROM), Compact Disk Recordable (CD-R), Compact Disk Rewritable (CD-RW), optical disk, magnetic media, magneto-optical media, removable memory cards or disks, various types of Digital Versatile Disk (DVD), a tape, a cassette, or the like. The instructions may include any suitable type of code, such as source code, compiled code, interpreted code, executable code, static code, dynamic code, encrypted code, programming code, and the like, implemented using any suitable high-level, low-level, object-oriented, visual, compiled and/or interpreted programming language. The non-transitory computer readable medium embodied programming code may cause a processor when executing the programming code to perform functions, such as those described herein.

[0099] Certain examples of the present disclosure were described above. It is, however, expressly noted that the present disclosure is not limited to those examples, but the intention is that additions and modifications to what was expressly described herein are also included within the scope of the disclosed examples. Moreover, it is to be understood that the features of the numerous examples described herein were not mutually exclusive and may exist in various combinations and permutations, even if such combinations or permutations were not made express herein, without departing from the spirit and scope of the disclosed examples. In fact, variations, modifications, and other implementations of what was described herein will occur to those of ordinary skill in the art without departing from the spirit and the scope of the disclosed examples. As such, the disclosed examples are not to be defined only by the preceding illustrative description.

[0100] Program aspects of the technology may be thought of as "products" or "articles of manufacture" typically in the form of executable code and/or associated data that is carried on or embodied in a type of non-transitory, machine readable medium. Storage type media include any or all of the tangible memory of the computers, processors or the like, or associated modules thereof, such as various semiconductor memories, tape drives, disk drives and the like, which may provide non-transitory storage at any time for the software programming. It is emphasized that the Abstract of the Disclosure is provided to allow a reader to quickly ascertain the nature of the technical disclosure. It is submitted with the understanding that it will not be used to interpret or limit the scope or meaning of the claims. In addition, in the foregoing Detailed Description, various features are grouped together in a single example for streamlining the disclosure. This method of disclosure is not to be interpreted as reflecting an intention that the claimed exam-

ples require more features than are expressly recited in each claim. Rather, as the following claims reflect, novel subject matter lies in less than all features of a single disclosed example. Thus, the following claims are hereby incorporated into the Detailed Description, with each claim standing on its own as a separate example. In the appended claims, the terms "including" and "in which" are used as the plain-English equivalents of the respective terms "comprising" and "wherein," respectively. Moreover, the terms "first," "second," "third," and so forth, are used merely as labels and are not intended to impose numerical requirements on their objects.

[0101] The foregoing description of examples has been presented for the purposes of illustration and description. It is not intended to be exhaustive or to limit the present disclosure to the precise forms disclosed. Many modifications and variations are possible considering this disclosure. It is intended that the scope of the present disclosure be limited not by this detailed description, but by the claims appended hereto. Future filed applications claiming priority to this application may claim the disclosed subject matter in a different manner and may include any set of one or more features as variously disclosed or otherwise demonstrated herein.

[0102] Although the present invention is defined in the attached claims, it should be understood that the present invention can also (alternatively) be defined in accordance with the following embodiments:

1. A drug delivery system, comprising:

- a processor operable to execute programming instructions;
- a user interface including a touchscreen display and user input circuitry;
- a memory operable to store the programming instructions; and
- a communication circuitry coupled to the processor and operable to receive and transmit communication signals, wherein the processor is operable to:

- receive an indication that a user is starting a ketogenic diet;
- retrieve a baseline total daily insulin value;
- calculate a keto total daily insulin value using the retrieved baseline total daily insulin value; and
- utilize the keto total daily insulin value in the calculation of a keto basal dosage of insulin or a keto bolus dosage of insulin.

2. The drug delivery system of embodiment 1, further comprising:

- a glucose sensor operable to transmit glucose measurement values during a period of time;
- a ketone sensor operable to transmit ketone lev-

els, wherein the communication circuitry is operable to receive transmissions of the glucose measurement values and the ketone values; and
the processor is operable to:

- receive a glucose measurement value during a post prandial portion of the period of time and during a nighttime portion of the period of time;
- receive a ketone level during the post prandial portion of the period of time;
- calculate a new total daily insulin value based on the received glucose measurement value and the received ketone level;
- and
- adapt the keto basal dosage and the keto bolus dosage based on the new total daily insulin.

3. The drug delivery system of embodiment 2, wherein the ketone sensor is operable to transmit ketone levels also during the period of time.

4. The drug delivery system of embodiment 1 or 3, wherein the processor is further operable to:

- receive a glucose measurement value during a post prandial portion of the period of time and during a nighttime portion of the period of time;
- receive a ketone level during the post prandial portion of the period of time;
- calculate a new total daily insulin value based on the received glucose measurement value and the received ketone level; and
- adapt the keto basal dosage and the keto bolus dosage based on the new total daily insulin.

5. The drug delivery system of any one of embodiments 1 to 4, wherein the processor is further operable to:

- determine, based on an input received from a graphical user interface presenting on the touchscreen display, whether the user is starting a ketogenic diet; and
- in response to the determination that the user is starting the ketogenic diet, determine a time period over which the user is expected to continue the ketogenic diet.

6. The drug delivery system of embodiment 5, wherein the processor is further operable to:

- in response to the determination that the user is starting a ketogenic diet, determining whether the user is participating in a diet cycle, and in response to the determination that user is par-

icipating in a diet cycle, generating a prompt in the graphical user interface presented on the touchscreen display, whether the ketogenic diet is on fixed days of the week; and in response to an indication that the ketogenic diet is on fixed days of the week, present an interactive calendar with days of the week for selection by a user.

7. The drug delivery system of any one of embodiments 1 to 6, wherein the processor, when calculating the keto total daily insulin value using the retrieved baseline total daily insulin value, is further operable to:
multiply the retrieved baseline total daily insulin value by a keto day factor, wherein the keto day factor is less than 1.

8. The drug delivery system of any one of embodiments 1 to 7, wherein the processor is further operable to:

receive an indication that a user is starting a non-ketogenic diet;
retrieve the new total daily insulin value, which is a keto day total daily insulin value;
calculate a non-keto total daily insulin value using the keto day total daily insulin value; and
utilize the non-keto total daily insulin value in the calculation of a non-keto basal dosage of insulin or a non-keto bolus dosage of insulin.

9. The drug delivery system of embodiment 8, wherein the processor, when calculating the non-keto total daily insulin value using the keto day total daily insulin value, is further operable to:
multiply the keto day total daily insulin value by a non-keto day factor, wherein the non-keto day factor is greater than 1.

10. A drug delivery system, comprising:

a processor operable to execute programming instructions;
a user interface including a display and user input circuitry;
a memory operable to store the programming instructions; and
communication circuitry coupled to the processor and is operable to receive and transmit communication signals, wherein the processor is operable to:

receive ketone levels from a ketone sensor;
generate a prompt on the user interface inquiring whether a user's diet for a time period is a keto diet or a non-keto diet; and
based on the received ketone levels of the

user, generate an indication of whether the user is adhering to a keto diet.

11. The drug delivery system of embodiment 10, wherein the processor is further operable to:

in response to a response to the prompt indicating the user's diet for the time period is a keto diet, determine whether a user's post prandial ketone levels received from a ketone sensor are greater than a first ketone value and less than a second ketone value; and
in response to the user's post ketone levels being within the first ketone value and the second ketone value, generate an adherence indication.

12. The drug delivery system of embodiment 10 or 11, wherein the processor is further operable to:

in response to a response to the prompt indicating the user's diet for the time period is not a keto diet, determine whether a user's post prandial ketone levels received from a ketone sensor are less than the first ketone value; and
in response to the user's post ketone levels being less than the first ketone value, generate an adherence indication.

13. The drug delivery system of embodiment 12, wherein the processor is further operable to:

in response to the user's post prandial ketone levels being greater than the first ketone value, send a notice to a user device with query confirming the time period is a keto time period.

14. The drug delivery system of any one of embodiments 10 to 13, wherein the processor is further operable to:

in response to the user's post prandial ketone levels being outside a range of the first ketone value and the second ketone value, send a notice to a user device with query confirming today is a keto time period.

15. The drug delivery system of any one of embodiments 10 to 14, wherein:

the first ketone value is approximately 0.5 mmol/L and the second ketone value is approximately 5 mmol/L.

16. The drug delivery system of embodiments 10 to 15, wherein the processor is further operable to:

receive a glucose value from a glucose sensor;
determine whether the received ketone levels are greater than a first ketone value;
in response to the received ketone levels being greater than the first ketone value, determine

whether the received glucose value exceeds a predetermined glucose value; and
 in response to the received glucose value exceeding the predetermined glucose value, increase a delivery of insulin and generate a prompt on the touchscreen display for the user to increase consumption of liquids, or
 in response to the received glucose value being less than the predetermined glucose value, generate a prompt on the touchscreen display for the user to increase consumption of liquids and to ingest carbohydrates.

17. A controller of a drug delivery system, comprising:

a processor operable to execute programming instructions;
 a memory operable to store the programming instructions; and
 communication circuitry coupled to the processor and be operable to receive and transmit communication signals, wherein the processor, when executing the programming instructions, is operable to:

obtain ketone levels of a user;
 evaluate the obtained ketone levels with reference to a plurality of ketone thresholds;
 based on the result of the evaluation, selecting a further action to be performed, wherein the further action is at least one of generating a notification to seek medical attention, generating a notification to ingest carbohydrates, generating a notification that the processor will increase drug delivery, or a combination thereof.

18. The controller of the drug delivery system of embodiment 17, wherein:

the plurality of ketone thresholds include a first ketone threshold, a second ketone threshold, a third ketone threshold and an extreme ketone threshold, and
 the processor, when evaluating the obtained ketone levels with reference to the plurality of ketone thresholds, is further operable to:

compare a latest ketone value of the obtained ketone levels to a second ketone threshold of the plurality of ketone thresholds;
 in response to the latest ketone value being greater than the first ketone threshold, compare the latest ketone value to a third ketone threshold;
 in response to the latest ketone value being

greater than the third ketone threshold, compare the latest ketone value to an extreme ketone threshold; and
 in response to the latest ketone value being greater than the extreme ketone threshold, selecting generating the notification the user is to seek medical attention as the selected further action.

19. The controller of the drug delivery system of embodiments 17 or 18, wherein the processor, when executing the programming instructions, is further operable to:

obtain glucose levels of the user;
 evaluate the glucose level to a maximum glucose threshold;
 based on the evaluation of the obtained ketone levels with reference to the plurality of ketone thresholds and the evaluation of the glucose level to the maximum glucose threshold, provide an indication for additional action by the processor.

20. The controller of the drug delivery system of any one of embodiments 17 to 19, wherein the processor is further operable to:

determine the user is experiencing ketoacidosis; and
 increase delivery of the drug, in particular increase the delivery of insulin.

21. The controller of the drug delivery system of any one of embodiments 17 to 20, wherein the processor is further operable to:

determine whether the user is experiencing diabetic ketoacidosis;
 in response to the determination indicating a drop below a minimum glucose threshold value, perform at least one of:

generate a prompt on the user interface for the user to ingest carbs,
 elevate a minimum target setpoint or the minimum glucose threshold value, or reduce a basal rate of drug delivery.

Claims

1. A drug delivery system, comprising:

a processor operable to execute programming instructions;
 a user interface including a touchscreen display and user input circuitry;

a memory operable to store the programming instructions; and
 a communication circuitry coupled to the processor and operable to receive and transmit communication signals, wherein the processor is operable to:

receive an indication that a user is starting a ketogenic diet;
 retrieve a baseline total daily insulin value;
 calculate a keto total daily insulin value using the retrieved baseline total daily insulin value; and
 utilize the keto total daily insulin value in the calculation of a keto basal dosage of insulin or a keto bolus dosage of insulin.

2. The drug delivery system of claim 1, further comprising:

a glucose sensor operable to transmit glucose measurement values during a period of time;
 a ketone sensor operable to transmit ketone levels, wherein the communication circuitry is operable to receive transmissions of the glucose measurement values and the ketone values.

3. The drug delivery system of claim 1 or 2, wherein the processor is further operable to:

receive a glucose measurement value during a post prandial portion of the period of time and during a nighttime portion of the period of time;
 receive a ketone level during the post prandial portion of the period of time;
 calculate a new total daily insulin value based on the received glucose measurement value and the received ketone level; and
 adapt the keto basal dosage and the keto bolus dosage based on the new total daily insulin.

4. The drug delivery system of any one of claims 1 to 3, wherein the processor is further operable to:

determine, based on an input received from a graphical user interface presenting on the touchscreen display, whether the user is starting a ketogenic diet; and
 in response to the determination that the user is starting the ketogenic diet, determine a time period over which the user is expected to continue the ketogenic diet.

5. The drug delivery system of claim 4, wherein the processor is further operable to:

in response to the determination that the user is starting a ketogenic diet, determining whether

the user is participating in a diet cycle, and in response to the determination that user is participating in a diet cycle, generating a prompt in the graphical user interface presented on the touchscreen display, whether the ketogenic diet is on fixed days of the week; and
 in response to an indication that the ketogenic diet is on fixed days of the week, present an interactive calendar with days of the week for selection by a user.

6. The drug delivery system of any one of claims 1 to 5, wherein the processor, when calculating the keto total daily insulin value using the retrieved baseline total daily insulin value, is further operable to:
 multiply the retrieved baseline total daily insulin value by a keto day factor, wherein the keto day factor is less than 1.

7. The drug delivery system of any one of claims 1 to 6, wherein the processor is further operable to:

receive an indication that a user is starting a non-ketogenic diet;
 retrieve the new total daily insulin value, which is a keto day total daily insulin value;
 calculate a non-keto total daily insulin value using the keto day total daily insulin value, in particular by multiply the keto day total daily insulin value by a non-keto day factor, wherein the non-keto day factor is greater than 1; and
 utilize the non-keto total daily insulin value in the calculation of a non-keto basal dosage of insulin or a non-keto bolus dosage of insulin.

8. A drug delivery system, comprising:

a processor operable to execute programming instructions;
 a user interface including a display and user input circuitry;
 a memory operable to store the programming instructions; and
 communication circuitry coupled to the processor and is operable to receive and transmit communication signals, wherein the processor is operable to:

receive ketone levels from a ketone sensor;
 generate a prompt on the user interface inquiring whether a user's diet for a time period is a keto diet or a non-keto diet; and
 based on the received ketone levels of the user, generate an indication of whether the user is adhering to a keto diet.

9. The drug delivery system of claim 8, wherein the processor is further operable to:

- in response to a response to the prompt indicating the user's diet for the time period is a keto diet, determine whether a user's post prandial ketone levels received from a ketone sensor are greater than a first ketone value and less than a second ketone value; and
 in response to the user's post ketone levels being within the first ketone value and the second ketone value, generate an adherence indication; and/or
 in response to a response to the prompt indicating the user's diet for the time period is not a keto diet, determine whether a user's post prandial ketone levels received from a ketone sensor are less than the first ketone value; and
 in response to the user's post ketone levels being less than the first ketone value, generate an adherence indication.
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10. The drug delivery system of claim 9, wherein the processor is further operable to:
- in response to the user's post prandial ketone levels being greater than the first ketone value, send a notice to a user device with query confirming the time period is a keto time period; and/or
 in response to the user's post prandial ketone levels being outside a range of the first ketone value and the second ketone value, send a notice to a user device with query confirming today is a keto time period.
11. The drug delivery system of any one of claims 8 to 10, wherein the processor is further operable to:
- receive a glucose value from a glucose sensor; determine whether the received ketone levels are greater than a first ketone value; in response to the received ketone levels being greater than the first ketone value, determine whether the received glucose value exceeds a predetermined glucose value; and in response to the received glucose value exceeding the predetermined glucose value, increase a delivery of insulin and generate a prompt on the touchscreen display for the user to increase consumption of liquids, or in response to the received glucose value being less than the predetermined glucose value, generate a prompt on the touchscreen display for the user to increase consumption of liquids and to ingest carbohydrates.
12. A controller of a drug delivery system, comprising:
- a processor operable to execute programming instructions;
- a memory operable to store the programming instructions; and
 communication circuitry coupled to the processor and be operable to receive and transmit communication signals, wherein the processor, when executing the programming instructions, is operable to:
- obtain ketone levels of a user;
 evaluate the obtained ketone levels with reference to a plurality of ketone thresholds; based on the result of the evaluation, selecting a further action to be performed, wherein the further action is at least one of generating a notification to seek medical attention, generating a notification to ingest carbohydrates, generating a notification that the processor will increase drug delivery, or a combination thereof.
13. The controller of the drug delivery system of claim 12, wherein:
- the plurality of ketone thresholds include a first ketone threshold, a second ketone threshold, a third ketone threshold and an extreme ketone threshold, and
 the processor, when evaluating the obtained ketone levels with reference to the plurality of ketone thresholds, is further operable to:
- compare a latest ketone value of the obtained ketone levels to a second ketone threshold of the plurality of ketone thresholds;
 in response to the latest ketone value being greater than the first ketone threshold, compare the latest ketone value to a third ketone threshold;
 in response to the latest ketone value being greater than the third ketone threshold, compare the latest ketone value to an extreme ketone threshold; and
 in response to the latest ketone value being greater than the extreme ketone threshold, selecting generating the notification the user is to seek medical attention as the selected further action.
14. The controller of the drug delivery system of any one of claims 12 or 13, wherein the processor, when executing the programming instructions, is further operable to:
- obtain glucose levels of the user;
 evaluate the glucose level to a maximum glucose threshold;
 based on the evaluation of the obtained ketone

levels with reference to the plurality of ketone thresholds and the evaluation of the glucose level to the maximum glucose threshold, provide an indication for additional action by the processor.

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- 15.** The controller of the drug delivery system of any one of claims 12 to 14, wherein the processor is further operable to:

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determine the user is experiencing ketoacidosis;
and
increase delivery of the drug, in particular increase the delivery of insulin.

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- 16.** The controller of the drug delivery system of claims 12 to 15, wherein the processor is further operable to:

determine whether the user is experiencing diabetic ketoacidosis;
in response to the determination indicating a drop below a minimum glucose threshold value, perform at least one of:

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generate a prompt on the user interface for the user to ingest carbs,
elevate a minimum target setpoint or the minimum glucose threshold value, or
reduce a basal rate of drug delivery.

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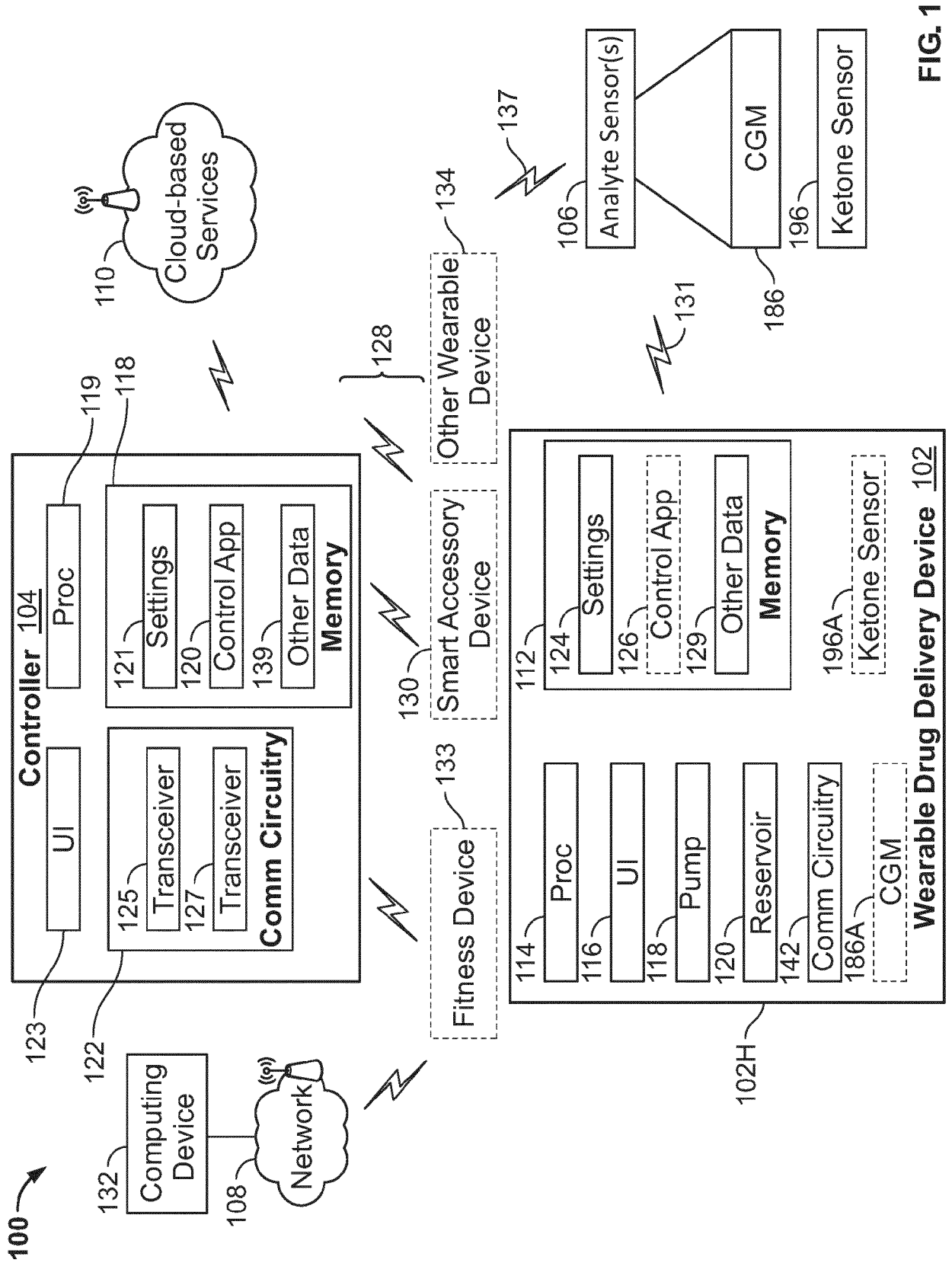


FIG. 1

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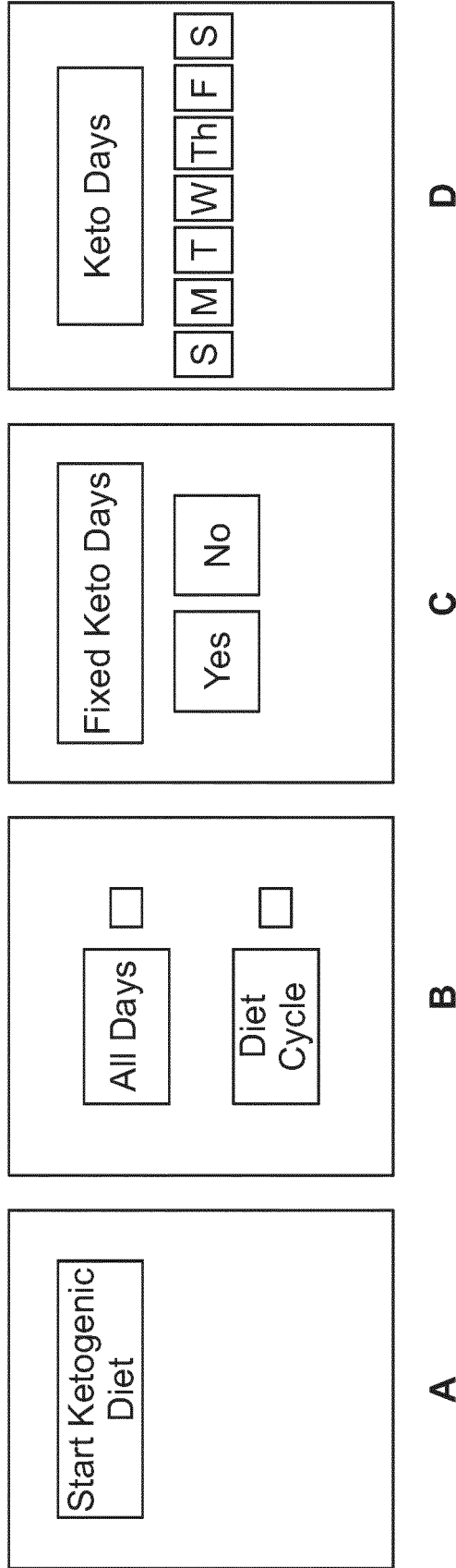


FIG. 2

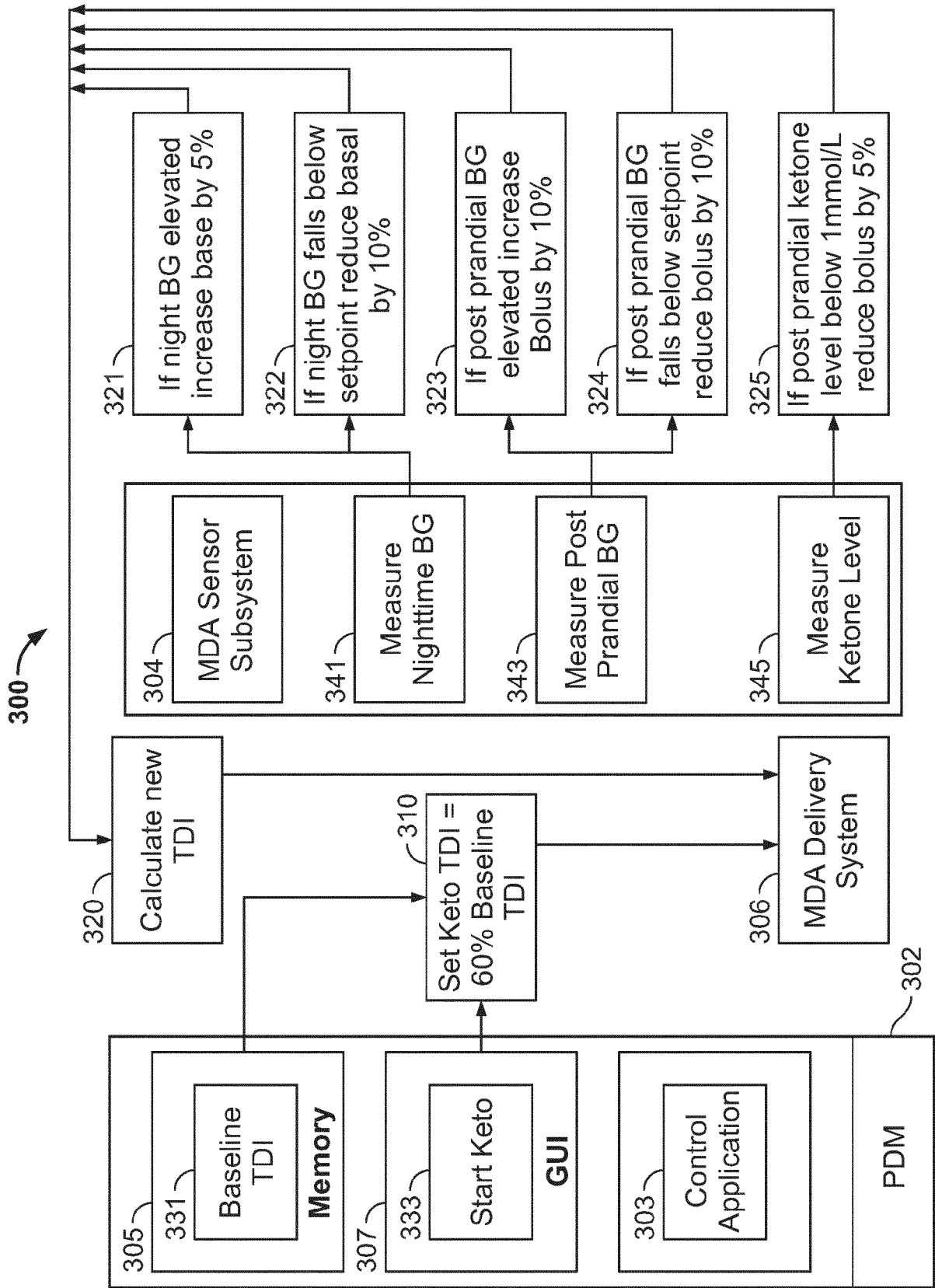


FIG. 3

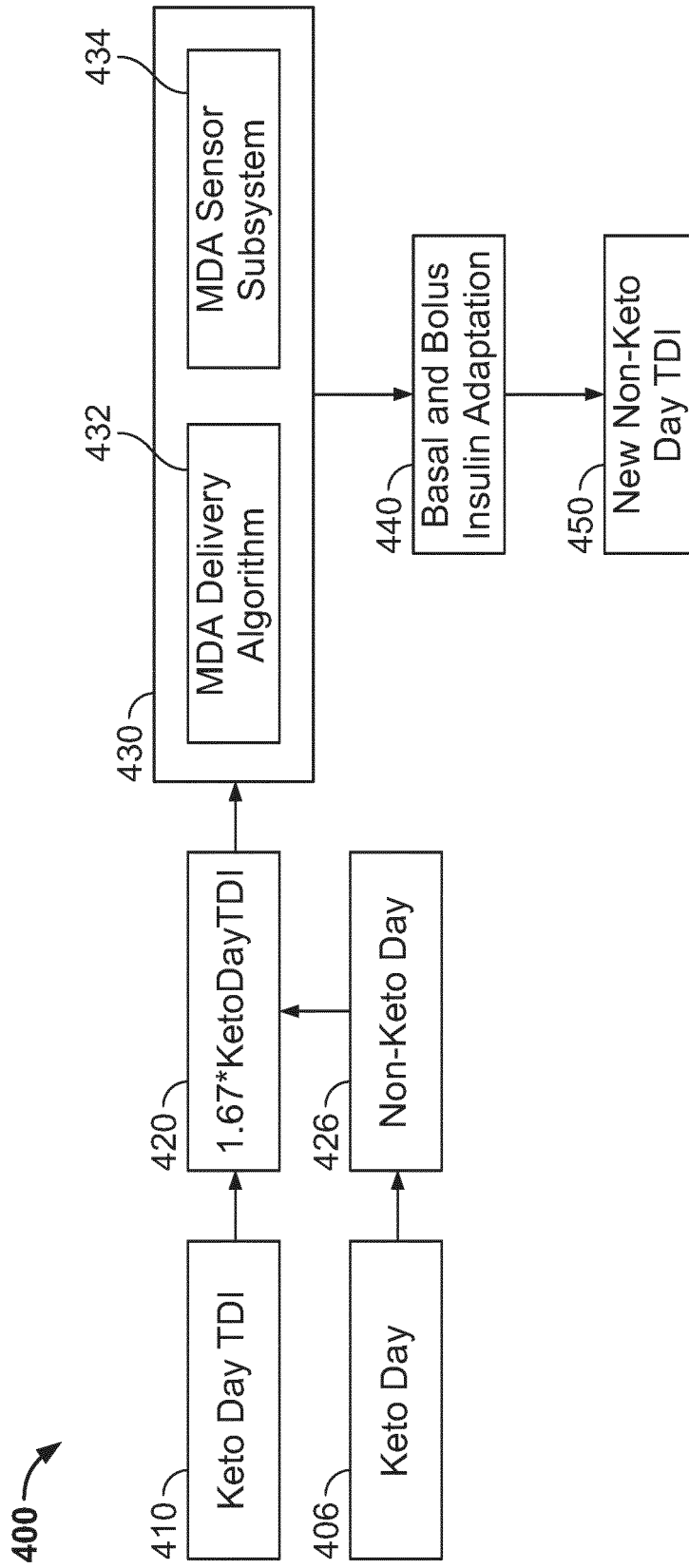


FIG. 4

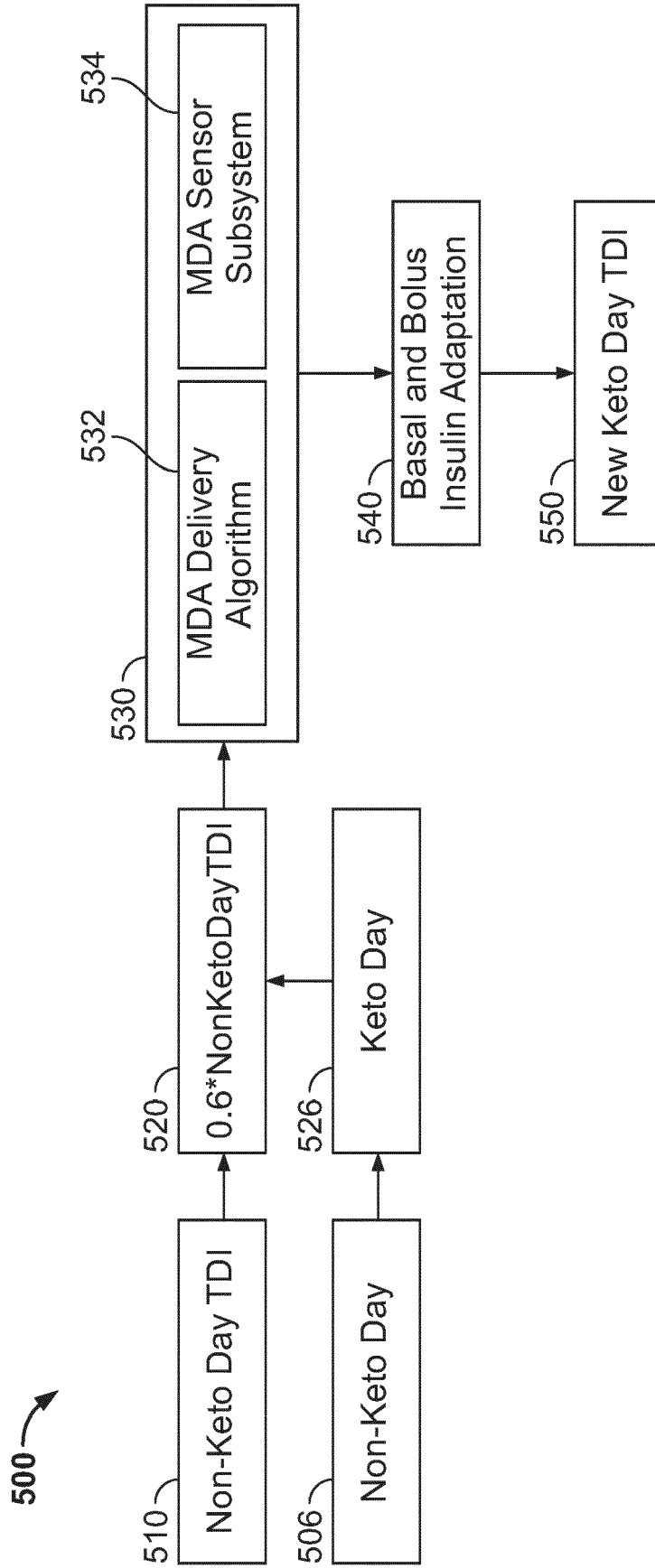


FIG. 5

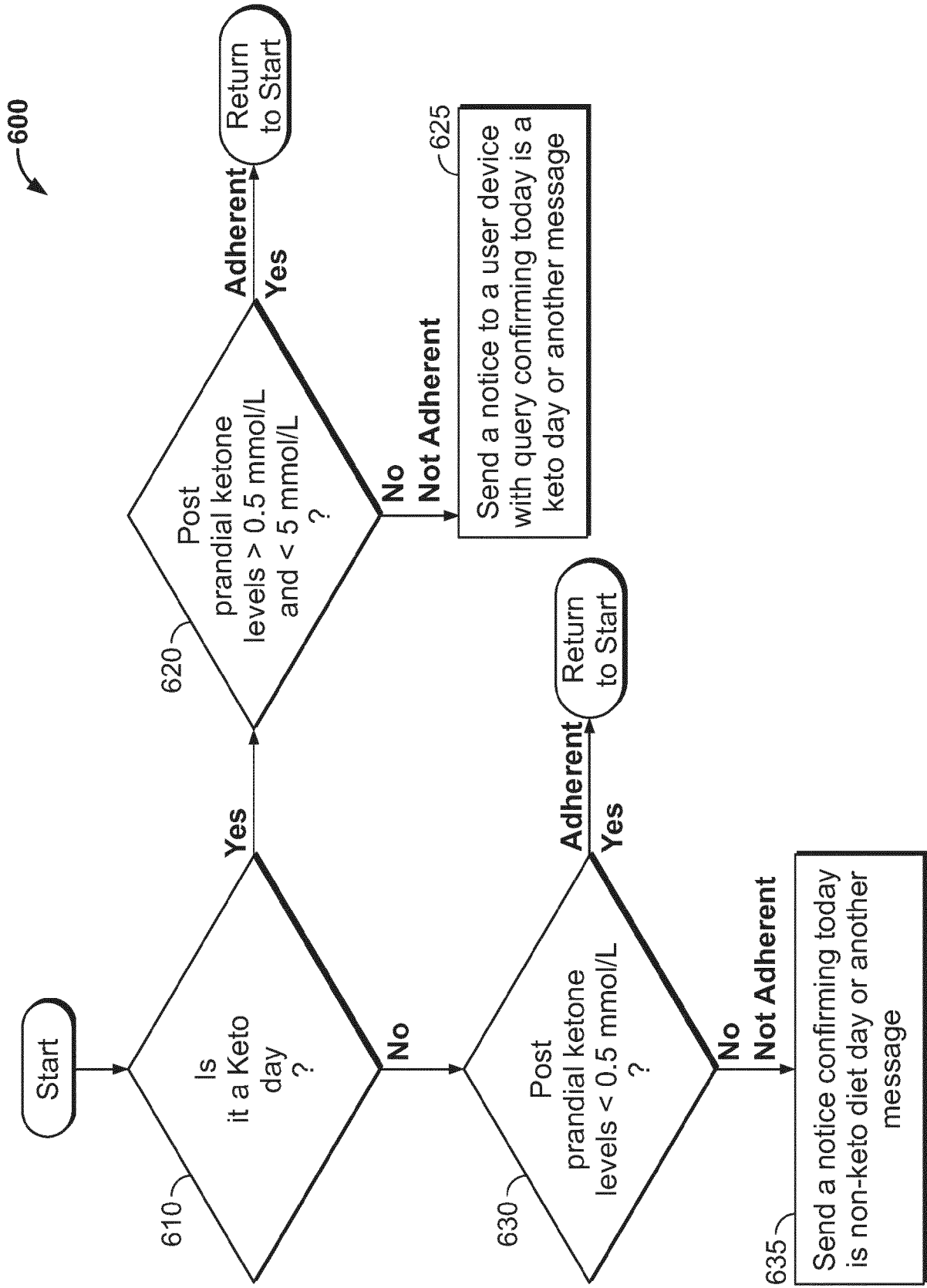


FIG. 6

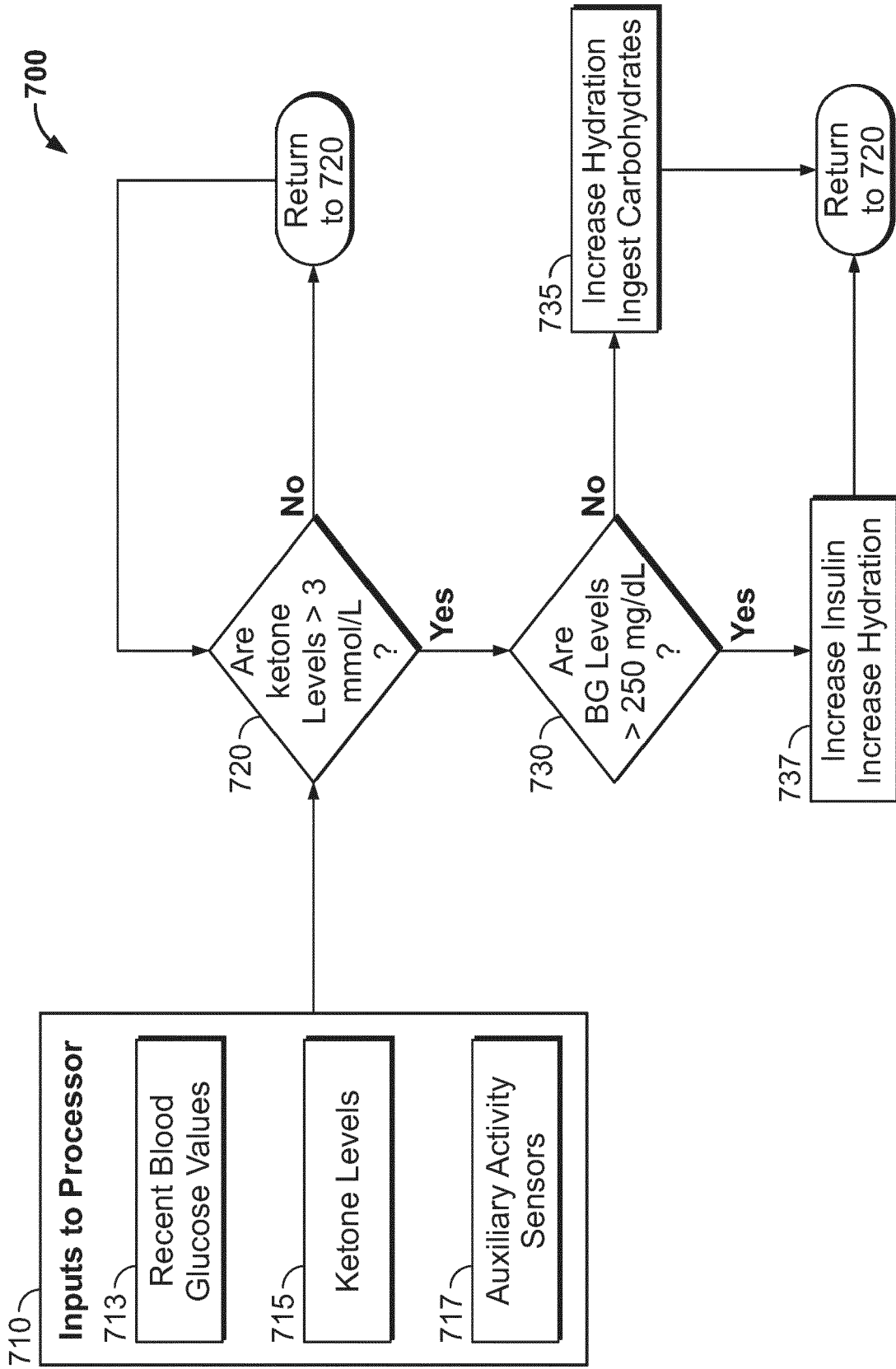


FIG. 7

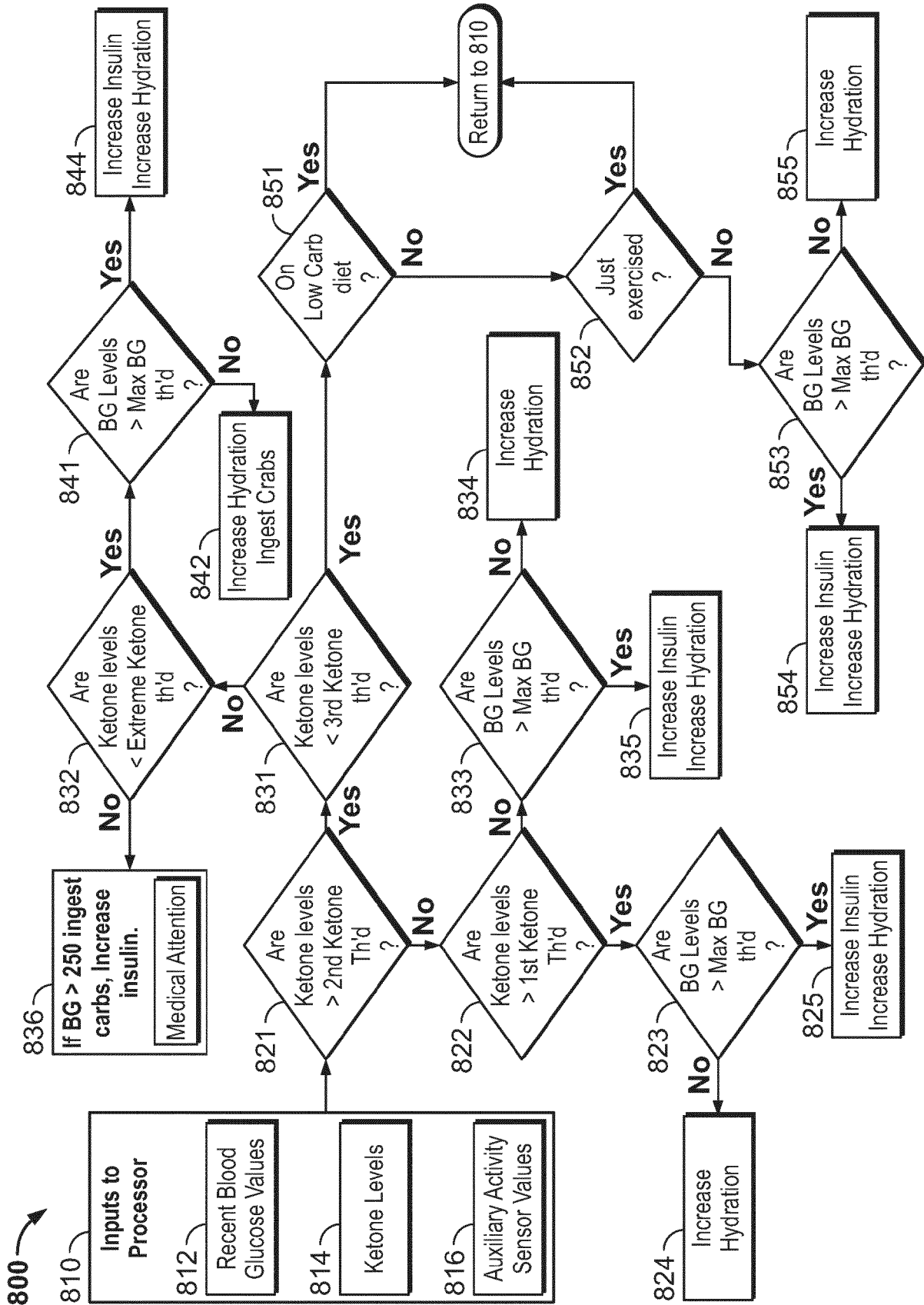


FIG. 8

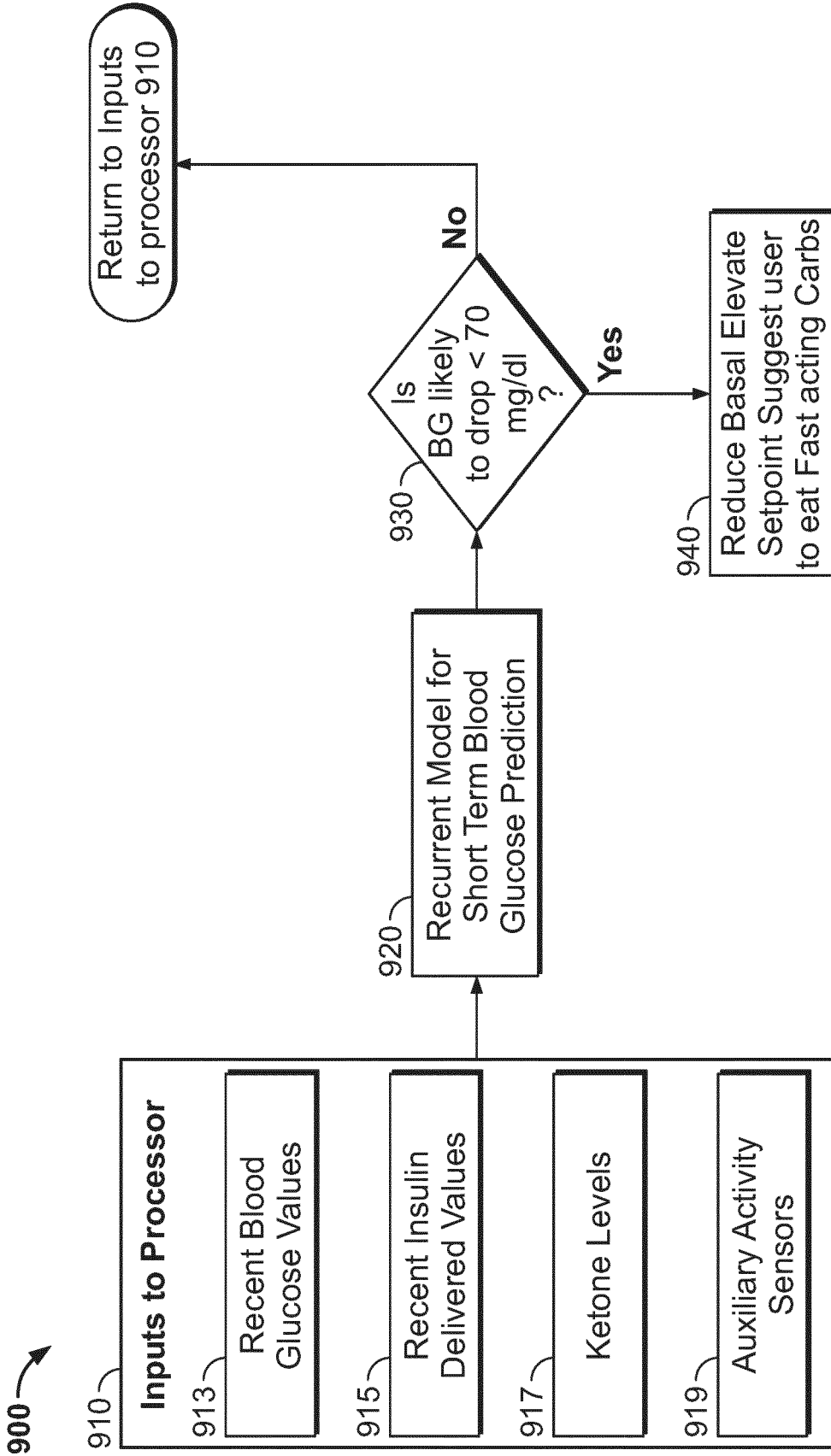


FIG. 9

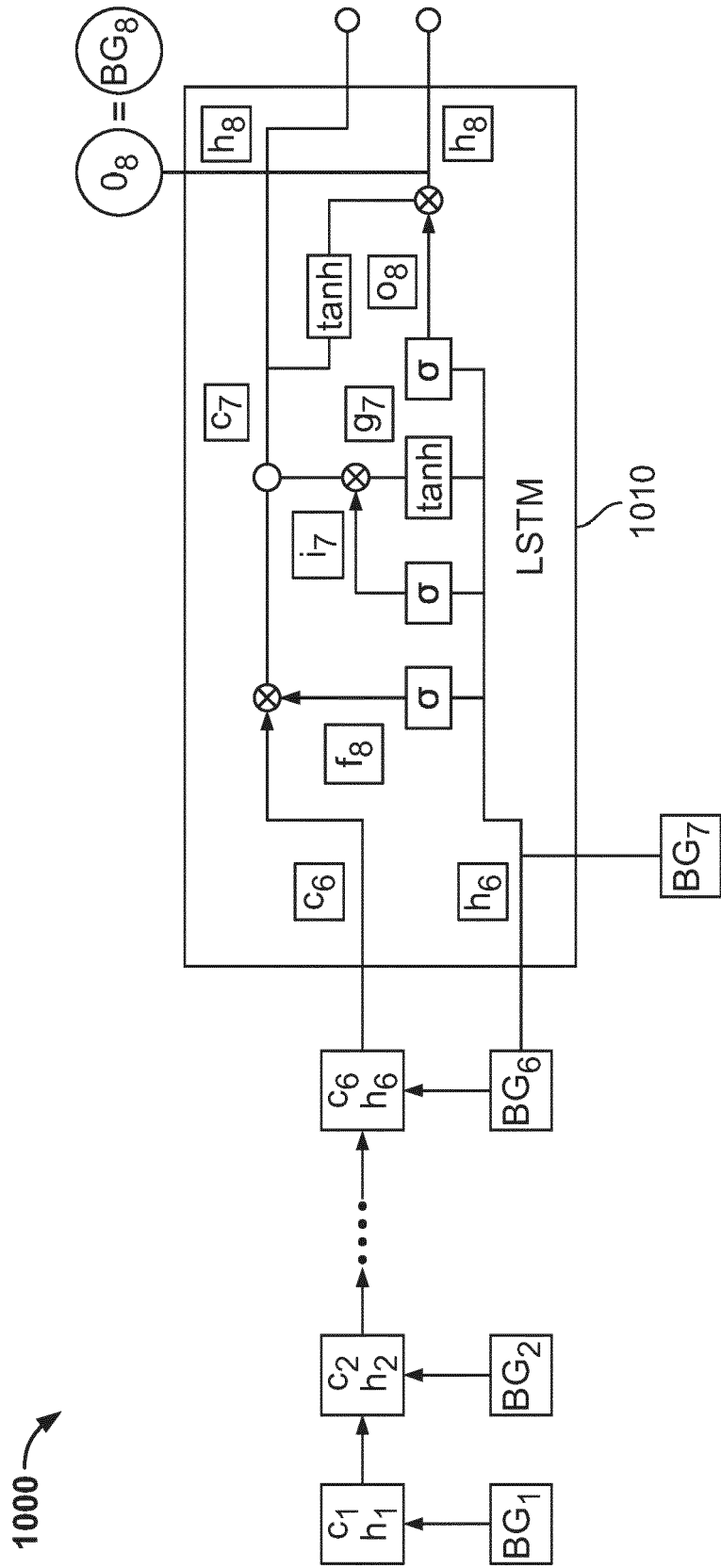


FIG. 10



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X	Lee Melissa H. ET AL: "The Clinical Case for the Integration of a Ketone Sensor as Part of a Closed Loop Insulin Pmp System", Journal of Diabetes Science and Technology Diabetes Technology Society, Vol. 13(5), 31 December 2019 (2019-12-31), pages 967-973, XP093059574, DOI: 10.1177/1932296818822986 Retrieved from the Internet: URL:https://journals.sagepub.com/doi/pdf/10.1177/1932296818822986 [retrieved on 2023-06-30]	11-16	
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The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 22 August 2023	Examiner Schechner-Resom, G
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			TECHNICAL FIELDS SEARCHED (IPC)
The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 22 August 2023	Examiner Schechner-Resom, G
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