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(54) **ACTIVE ALIGNMENT SYSTEM AND METHOD FOR LASER OPTICAL COUPLING**

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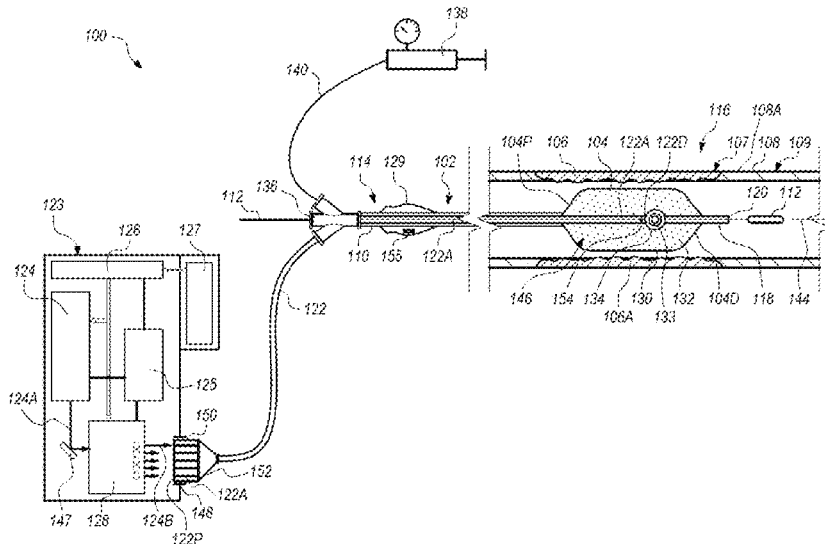
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(57) **ABSTRACT**

A catheter system for treating site within or adjacent to a vessel wall or a heart valve includes a light source, a first and second light guide, and an optical alignment system. The light source generates light energy. The first and second light guides receive the light energy from the light source and have respective guide proximal ends. A multiplexer directs the light energy toward the guide proximal ends of the first and second light guides. The optical alignment system determines an alignment of the light energy relative to at least one of the guide proximal ends and adjusts the positioning of the light energy relative to the at least one of the guide proximal ends based at least partially on the alignment of the light energy relative to the at least one of the guide proximal ends.

20 Claims, 6 Drawing Sheets



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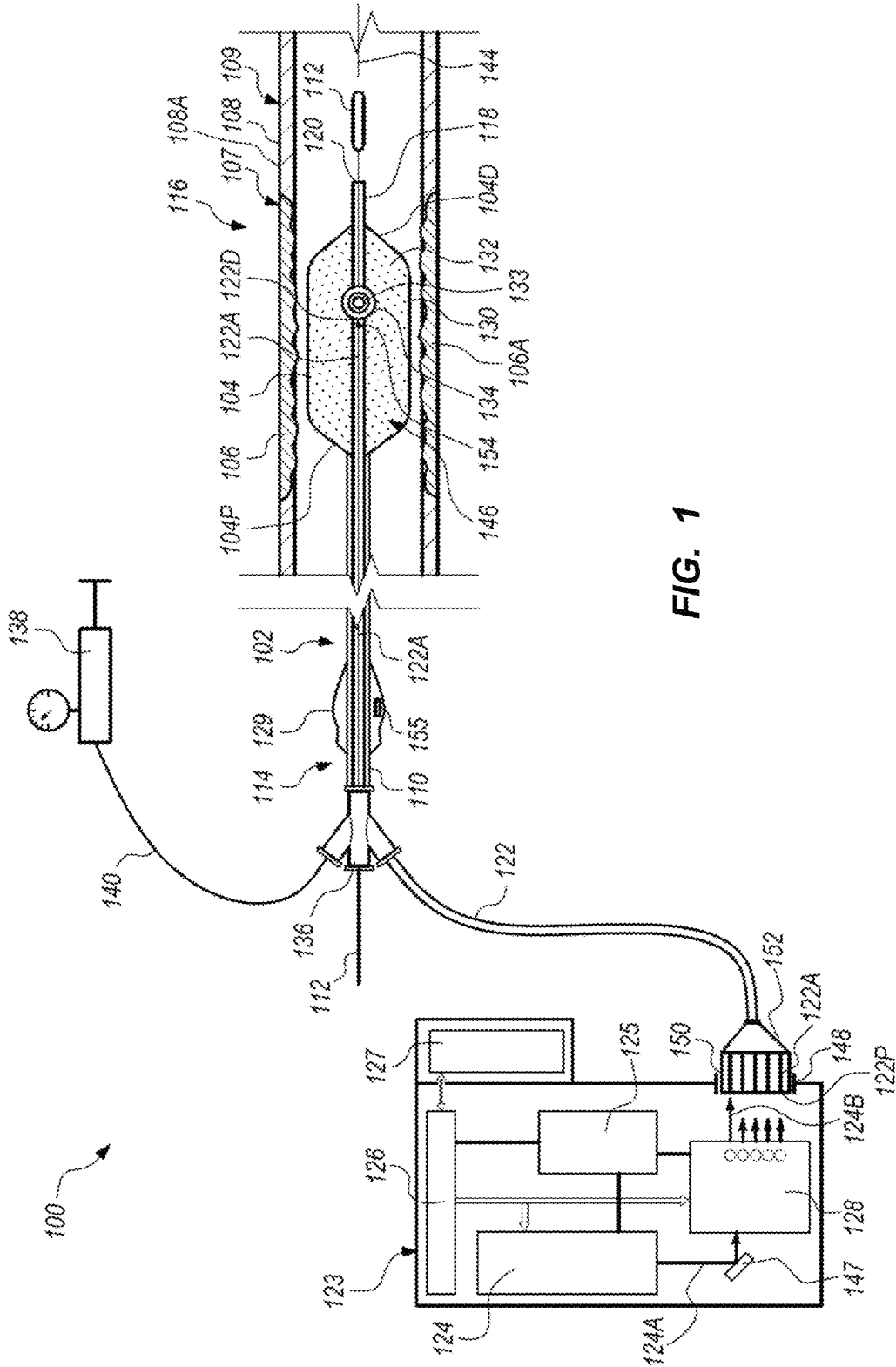


FIG. 1

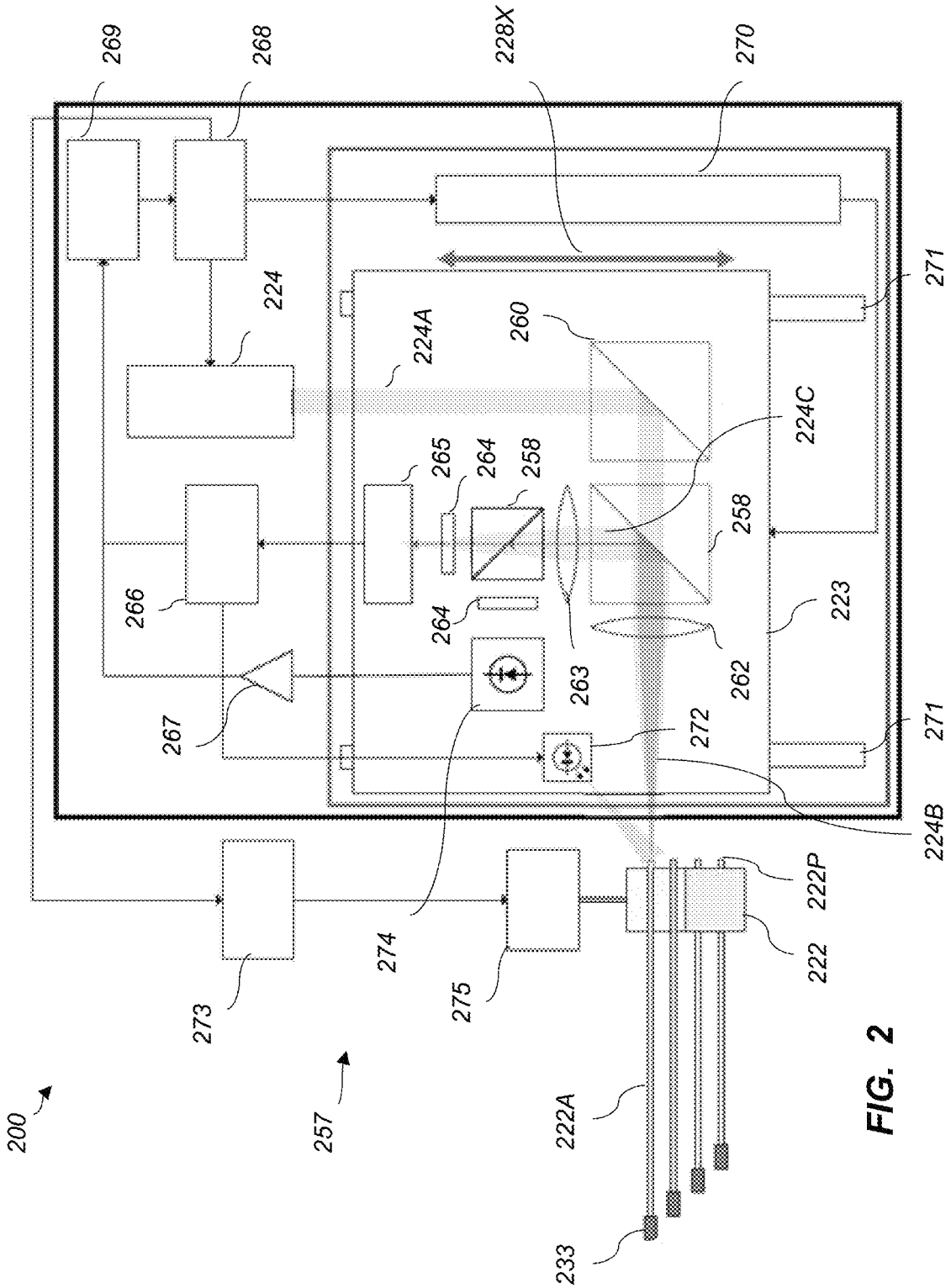


FIG. 2

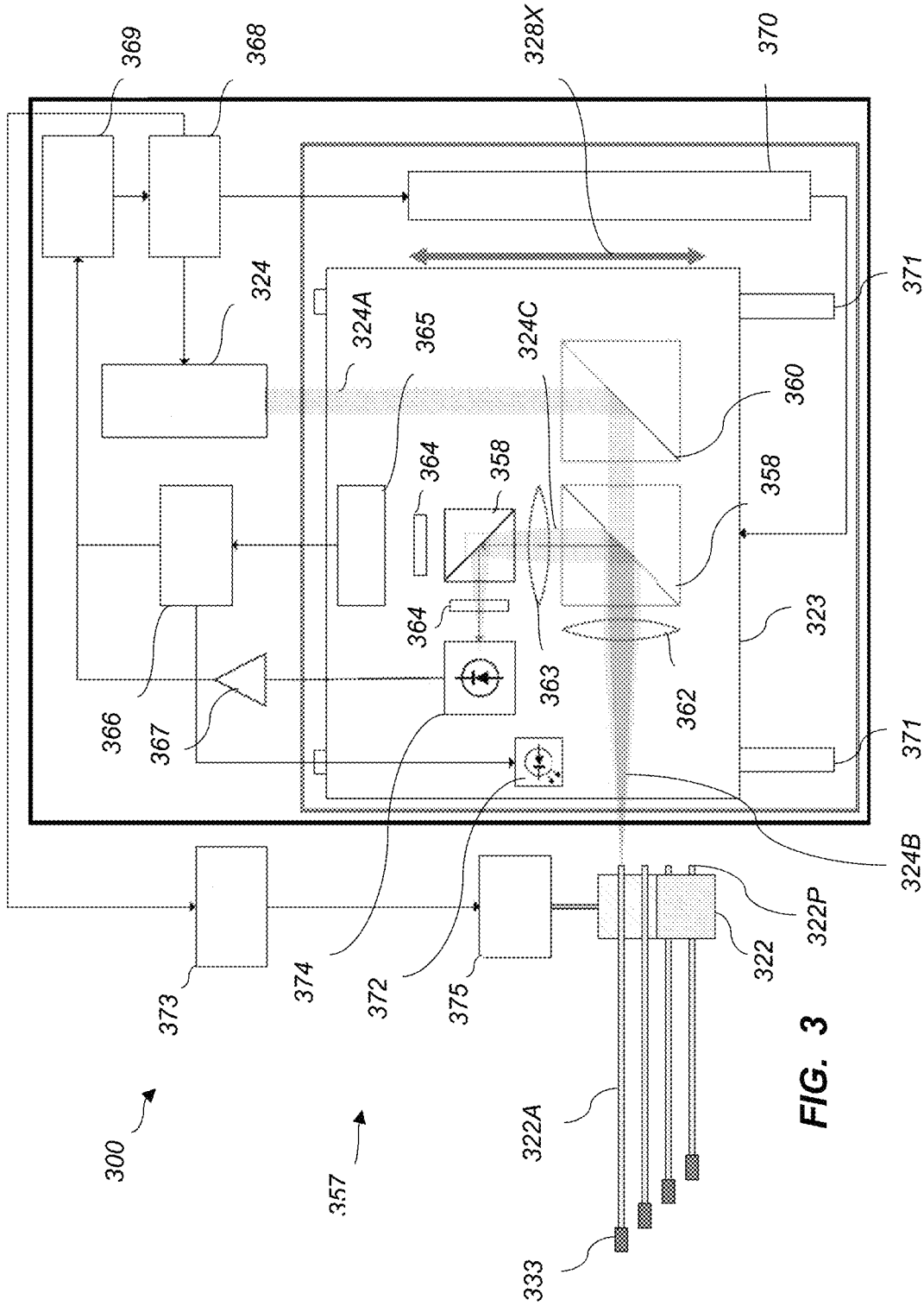
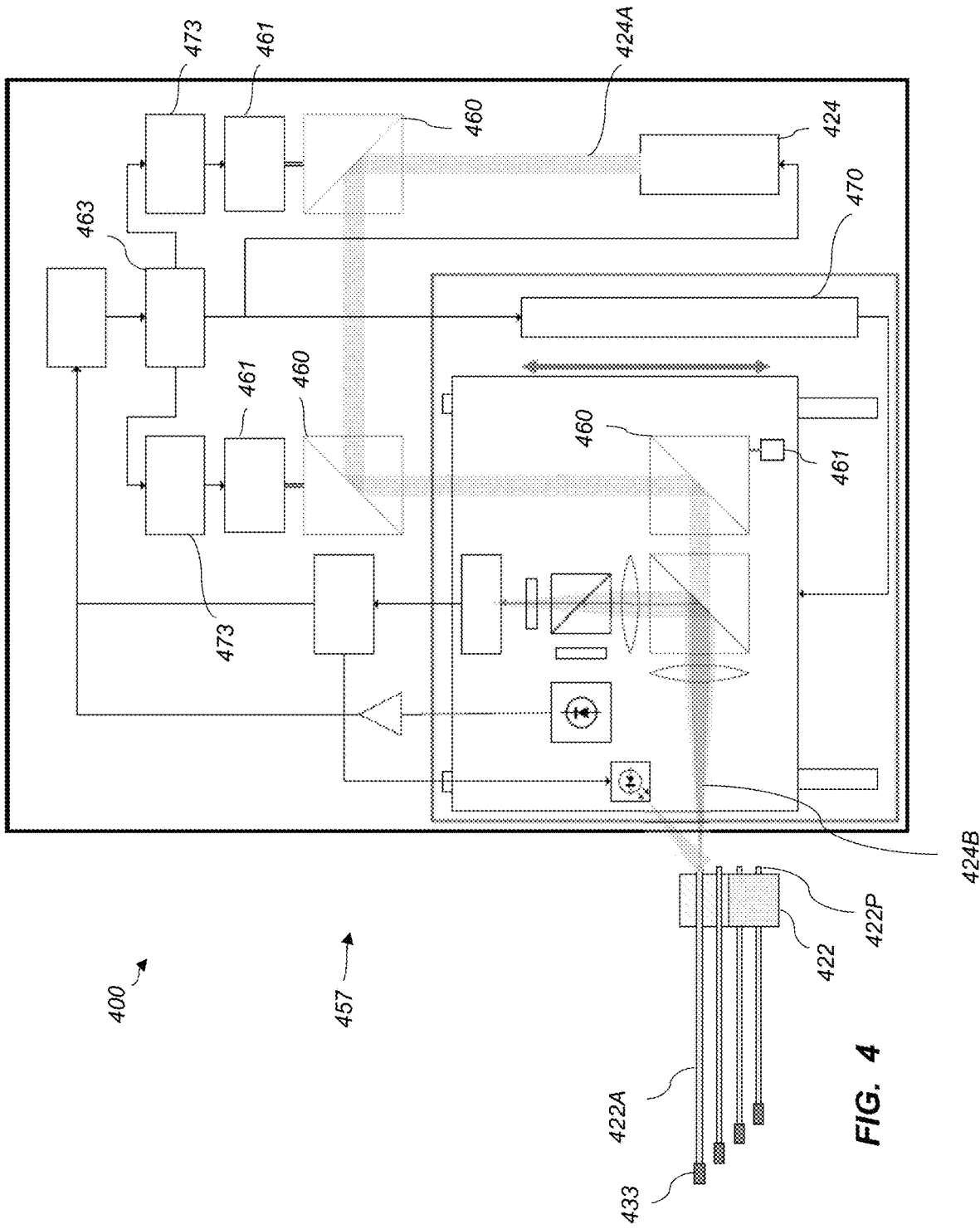


FIG. 3



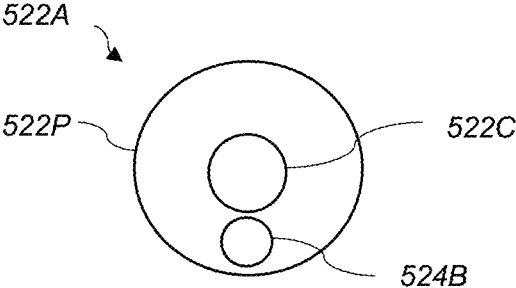


FIG. 5A

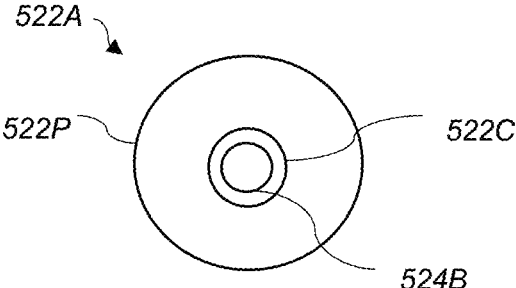


FIG. 5B

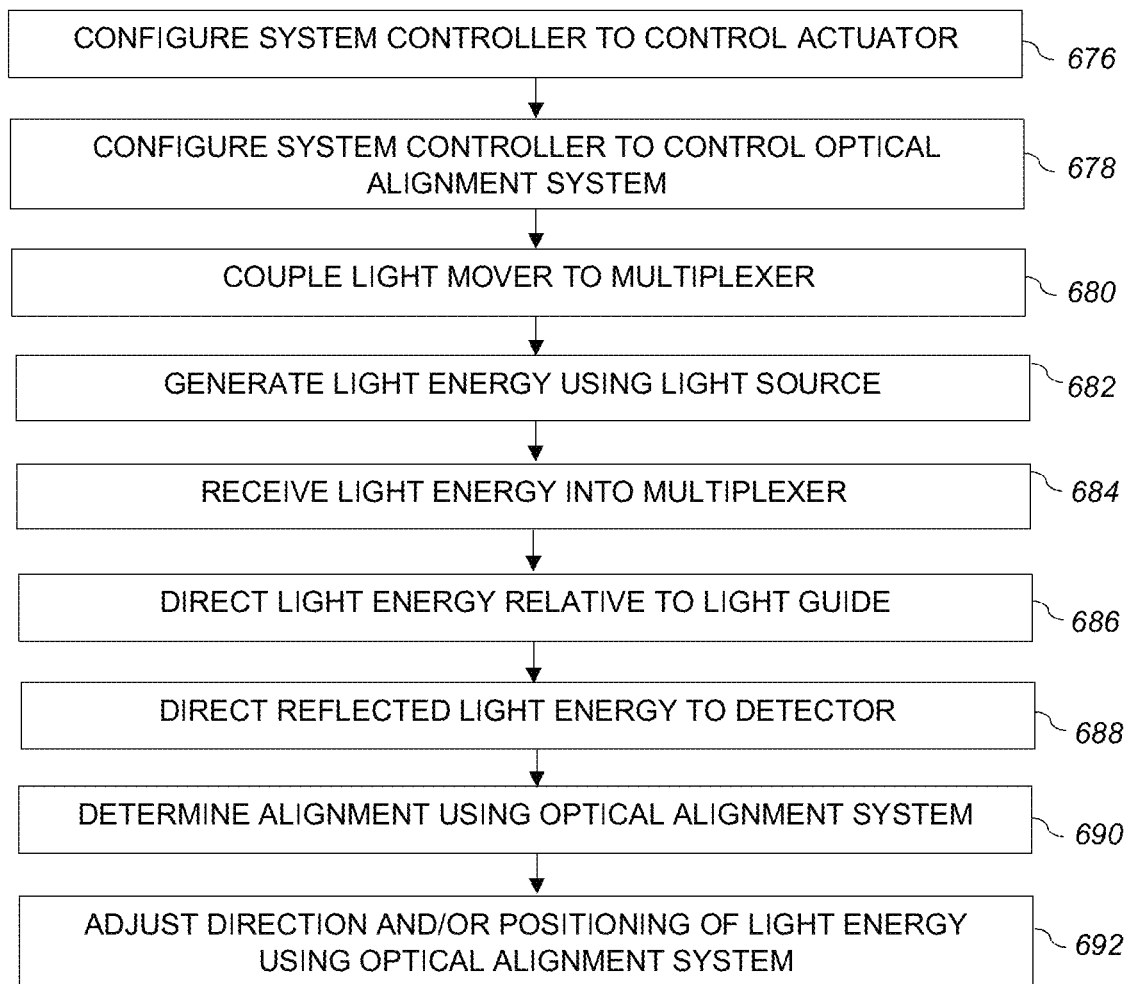


FIG. 6

ACTIVE ALIGNMENT SYSTEM AND METHOD FOR LASER OPTICAL COUPLING

RELATED APPLICATION

This Application is related to and claims priority on U.S. Provisional Patent Application Ser. No. 63/197,959 filed on Jun. 7, 2021, and entitled "ACTIVE ALIGNMENT SYSTEM AND METHOD FOR LASER OPTICAL COUPLING." To the extent permissible, the contents of U.S. Provisional Application Ser. No. 63/197,959 are incorporated in their entirety herein by reference.

BACKGROUND

Vascular lesions within vessels in the body can be associated with an increased risk for major adverse events, such as myocardial infarction, embolism, deep vein thrombosis, stroke, and the like. Severe vascular lesions can be difficult to treat and achieve patency for a physician in a clinical setting.

Vascular lesions may be treated using interventions such as drug therapy, balloon angioplasty, atherectomy, stent placement, and vascular graft bypass, to name a few. Such interventions may not always be ideal or may require subsequent treatment to address the lesion.

SUMMARY

The present invention is directed toward a catheter system for treating a treatment site within or adjacent to a vessel wall or a heart valve. In various embodiments, the catheter system includes a light source, a first light guide, a second light guide, and an optical alignment system. The light source generates light energy. The first light guide receives the light energy from the light source, the first light guide has a guide proximal end. The second light guide receives the light energy from the light source, the second light guide has a guide proximal end. A multiplexer directs the light energy toward the guide proximal end of the first light guide and the guide proximal end of the second light guide. An optical alignment system determines an alignment of the light energy relative to at least one of the guide proximal ends. The optical alignment system adjusts the positioning of the light energy relative to the at least one of the guide proximal ends based at least partially on the alignment of the light energy relative to the at least one of the guide proximal ends.

In some embodiments, the optical alignment system is configured to improve optical coupling between the light energy and at least one of the light guides.

In certain embodiments, the optical alignment system further includes an image sensor that senses the alignment of the light energy relative to at least one of the guide proximal ends, the image sensor being configured to provide a visualization of the alignment.

In various embodiments, the catheter system further includes a system controller that is configured to control the optical alignment system so that the light energy is substantially coupled to the at least one of the guide proximal ends.

In some embodiments, at least one of the light guides is an optical fiber.

In certain embodiments, the light source is a laser.

In various embodiments, the optical alignment system further includes an optical aligner that is configured to align the light energy with the at least one of the guide proximal ends.

In some embodiments, the optical aligner is controlled by the system controller.

In certain embodiments, the optical alignment system further includes an imaging system including an imaging sensor, the imaging system being configured to capture images of a focal point of the light source, and the at least one of the guide proximal ends.

In various embodiments, the imaging system is configured to simultaneously capture images of the focal point of the light source and a scattered energy beam scattered off the at least one of the guide proximal ends.

In some embodiments, the imaging system is configured to utilize an image reference frame that allows direct computation of distance offset from the center of the at least one of the guide proximal ends.

In certain embodiments, the imaging system is configured to determine the offset and compute compensation adjustment of the alignment of the light energy relative to the at least one of the guide proximal ends.

In various embodiments, the optical alignment system further includes an alignment positioner that positions the alignment of the light energy relative to the at least one of the guide proximal ends based on a computed compensation adjustment to substantially couple the light source and the at least one of the guide proximal ends.

In some embodiments, the catheter system further includes a system controller that is configured to control an optics mover that positions the multiplexer and aligns the light energy relative to the at least one of the guide proximal ends.

In certain embodiments, the catheter system further includes a light source mover coupled to the multiplexer, the light source mover being connected to the optics mover so that the optics mover can position the multiplexer along the light source mover.

In various embodiments, the system controller is configured to align the light source into one of (i) a third light guide that receives the light energy from the light source, the third light guide having a guide proximal end, and (ii) a third light guide that receives the light energy from the light source, the third light guide having a guide proximal end.

In some embodiments, the light source is a pulsed IR laser.

In certain embodiments, the multiplexer further includes optical elements including a dichroic beamsplitter that splits the light source into at least two light beams.

In various embodiments, the dichroic beamsplitter is configured to reflect a reflected light energy with a shorter wavelength than the light energy emitted by the light source.

In some embodiments, the dichroic beamsplitter includes a dichroic coating that is tuned to reflect a portion of the light energy emitted by the light source so that between 99% and 0.01% is reflected.

In certain embodiments, the dichroic beamsplitter is configured to reflect a portion of the light energy emitted by the light source as an imaging beam.

In various embodiments, the imaging beam is directed toward a detector for analysis of the light energy reflected from at least one of the light guides.

In some embodiments, the optical alignment system further includes an illuminator that illuminates the at least one of the guide proximal ends to provide improved image quality and brightness.

In certain embodiments, the system controller controls the illuminator and adjusts an image brightness and contrast.

In various embodiments, wherein the optical alignment system further includes one of a stepper motor and a piezo

actuator that is configured to adjust the yaw, pitch, and roll of at least one of the light guides.

In some embodiments, wherein the optical alignment system further includes optical compensators that are configured to adjust the positioning of the light source relative to the at least one of the guide proximal ends.

In certain embodiments, the optical compensators include a plurality of optical steering wedges positioned in the path of the light source, the plurality of optical steering wedges being configured to improve the coupling of the light source, and the at least one of the guide proximal ends.

The present invention is also directed toward a method for treating a vascular lesion within or adjacent to a vessel wall within a body of a patient using the catheter system of any of the embodiments described herein.

The present invention is further directed toward a method for manufacturing the catheter system of any of the embodiments described herein.

The present invention is also directed toward a method for treating a treatment site within or adjacent to a vessel wall or a heart valve using a catheter system. In various embodiments, the method can include the steps of generating light energy using a light source, directing the light energy toward at least one of a guide proximal end of a first light guide and a guide proximal end of a second light guide, determining an alignment of the light energy relative to at least one of the guide proximal ends of the light guides with an optical alignment system, and adjusting a positioning of the light energy relative to the at least one of the guide proximal ends of the light guides with the optical alignment system based on the alignment of the light energy.

In some embodiments, the optical alignment system is configured to improve optical coupling between the light energy and the at least one of the guide proximal ends of the light guides.

In certain embodiments, the optical alignment system further includes an image sensor that senses the alignment between the light energy and to the at least one of the guide proximal ends of the light guides, the image sensor being configured to provide a visualization of the alignment.

In various embodiments, the method can further include the step of configuring a system controller that is configured to control the optical alignment system so that the light energy is substantially coupled to the at least one of the guide proximal ends of the light guides.

In some embodiments, at least one of the light guides is an optical fiber.

In certain embodiments, the light source is a laser.

In various embodiments, the optical alignment system further includes an optical aligner that is configured to align the light energy with the at least one of the guide proximal ends of the light guides.

In some embodiments, the optical aligner is controlled by the system controller.

In certain embodiments, the optical alignment system further includes an imaging system including an imaging sensor, the imaging system being configured to capture images of a focal point of the light source.

In various embodiments, the imaging system is configured to simultaneously capture images of the focal point of the light source and a scattered energy beam scattered off the at least one of the guide proximal ends of the light guides.

In some embodiments, the imaging system is configured to utilize an image reference frame that allows direct computation of distance offset from the center of the at least one of the guide proximal ends of the light guides.

In certain embodiments, the imaging system is configured to determine the offset and compute compensation adjustment of the alignment of the light energy and the at least one of the guide proximal ends of the light guides.

In various embodiments, the method can further include the step of configuring a system controller that is configured to control an optics mover that positions the multiplexer and aligns the source and the at least one of the guide proximal ends of the light guides.

In some embodiments, the method can further include the step of coupling a light source mover to the multiplexer, the light source mover being connected to the optics mover so that the optics mover can position the multiplexer along the light source mover.

In certain embodiments, the system controller is configured to align the light source into one of (i) a third light guide that receives the light energy from the light source, the third light guide having a guide proximal end, and (ii) a third light guide that receives the light energy from the light source, the third light guide having a guide proximal end.

In various embodiments, the light source is a pulsed IR laser.

In some embodiments, the multiplexer further includes optical elements including a dichroic beamsplitter that splits the light source into at least two guide beams.

In certain embodiments, the dichroic beamsplitter is configured to reflect a reflected light energy with a shorter wavelength than the light energy emitted by the light source.

In various embodiments, the dichroic beamsplitter includes a dichroic coating that is tuned to reflect a portion of the light energy emitted by the light source so that between 99% and 0.01% is reflected.

In some embodiments, the dichroic beamsplitter is configured to reflect a portion of the light energy emitted the at least one of the guide proximal ends of the light guides as an imaging beam.

In certain embodiments, the method can further include the step of directing the light energy reflected from the at least one of the guide proximal ends of the light guides toward a detector for analysis.

In various embodiments, the optical alignment system further includes an illuminator that illuminates the at least one of the guide proximal ends of the light guides to provide improved image quality and brightness.

In some embodiments, the system controller controls the illuminator and adjusts an image brightness and contrast.

In certain embodiments, the optical alignment system further includes one of a stepper motor and a piezo actuator that is configured to adjust the yaw, pitch, and roll of at least one of the light guides.

In various embodiments, the optical alignment system further includes optical compensators that are configured to adjust the positioning of the individual guide beam relative to at least one of the light guides.

In some embodiments, the optical compensators include a plurality of optical steering wedges positioned in the path of the light source, the plurality of optical steering wedges being configured to improve the coupling of the light source, and the at least one of the guide proximal ends of the light guides.

In certain embodiments, the optical alignment system further includes a reflector and a reflector mover that moves the reflector.

The present invention is also directed toward a method for treating a treatment site within or adjacent to a vessel wall or a heart valve using a catheter system. In various embodiments, the method can include the steps of determining an

alignment of a light energy relative to at least one of a guide proximal ends of a first light guide and a guide proximal end of a second light guide with an optical alignment system, and adjusting a positioning of the light energy relative to the at least one of the guide proximal ends of the light guides with the optical alignment system based on the alignment of the light energy.

The present invention is directed toward a catheter system for treating a treatment site within or adjacent to a vessel wall or a heart valve. In various embodiments, the catheter system includes a light source, a first light guide, a second light guide, and a light source mover. The light source generates light energy. The first light guide receives the light energy from the light source, the first light guide having a guide proximal end. The second light guide that receives the light energy from the light source, the second light guide having a guide proximal end. An optical alignment system determines an alignment of the light energy relative to at least one of the guide proximal ends, the optical alignment system adjusting the positioning of the light energy relative to the at least one of the guide proximal ends based at least partially on the alignment of the light energy relative to the at least one of the guide proximal ends.

The present invention is also directed toward a method for treating a treatment site within or adjacent to a vessel wall or a heart valve using a catheter system. In various embodiments, the method can include the steps of generating light energy using a light source; receiving light energy into one of a first light guide and a second light guide; moving, using a light source mover, the light source so that the light energy is aligned within a guide proximal end of (i) the first light guide and (ii) the second light guide, and detecting, using the light source mover, the alignment of the light energy relative to the guide proximal end of at least one of the light guides.

This summary is an overview of some of the teachings of the present application and is not intended to be an exclusive or exhaustive treatment of the present subject matter. Further details are found in the detailed description and appended claims. Other aspects will be apparent to persons skilled in the art upon reading and understanding the following detailed description and viewing the drawings that form a part thereof, each of which is not to be taken in a limiting sense. The scope herein is defined by the appended claims and their legal equivalents.

BRIEF DESCRIPTION OF THE DRAWINGS

The novel features of this invention, as well as the invention itself, both as to its structure and its operation, will be best understood from the accompanying drawings, taken in conjunction with the accompanying description, in which in most cases, similar reference characters refer to similar parts, and in which:

FIG. 1 is a schematic cross-sectional view of an embodiment of a catheter system in accordance with various embodiments herein, the catheter system including a multiplexer having features of the present invention;

FIG. 2 is a simplified schematic view of a portion of an embodiment of the catheter system, including an embodiment of an optical alignment system, the optical alignment system being utilized in a first alignment configuration;

FIG. 3 is a simplified schematic view of a portion of an embodiment of the catheter system, including an embodiment of the optical alignment system, the optical alignment system being utilized in a second alignment configuration;

FIG. 4 is a simplified schematic view of a portion of an embodiment of the catheter system, including an embodi-

ment of the optical alignment system, the optical alignment system being utilized in a third alignment configuration;

FIG. 5A is a simplified view of a guide proximal end of a light guide, and a portion of the guide beam reflected off the guide proximal end of the light guide, the portion of the guide beam being shown in an unaligned state;

FIG. 5B is a simplified view of a guide proximal end of a light guide, and a portion of the guide beam reflected off the guide proximal end of the light guide, the portion of the guide beam being shown in an aligned state; and

FIG. 6 is a flow chart of one embodiment of a method for treating a treatment site within or adjacent to a vessel wall or a heart valve using a catheter system having features and/or steps of the present invention.

While embodiments of the present invention are susceptible to various modifications and alternative forms, specifics thereof have been shown by way of example and drawings, and are described in detail herein. It is understood, however, that the scope herein is not limited to the particular embodiments described. On the contrary, the intention is to cover modifications, equivalents, and alternatives falling within the spirit and scope herein.

DESCRIPTION

Treatment of vascular lesions (also sometimes referred to herein as “treatment sites”) can reduce major adverse events or death in affected subjects. As referred to herein, a major adverse event is one that can occur anywhere within the body due to the presence of a vascular lesion. Major adverse events can include but are not limited to, major adverse cardiac events, major adverse events in the peripheral or central vasculature, major adverse events in the brain, major adverse events in the musculature, or major adverse events in any of the internal organs.

As used herein, the terms “intravascular lesion,” “vascular lesion,” and “treatment site” are used interchangeably unless otherwise noted. The intravascular lesions and/or the vascular lesions are sometimes referred to herein simply as “lesions.” Also, as used herein, the terms “focused location” and “focused spot” can be used interchangeably unless otherwise noted and can refer to any location where the light energy is focused to a small diameter than the initial diameter of the light source.

Those of ordinary skill in the art will realize that the following detailed description of the present invention is illustrative only and is not intended to be in any way limiting. Other embodiments of the present invention will readily suggest themselves to such skilled persons having the benefit of this disclosure. Reference will now be made in detail to implementations of the present invention, as illustrated in the accompanying drawings.

In the interest of clarity, not all of the routine features of the implementations described herein are shown and described. It will, of course, be appreciated that in the development of any such actual implementation, numerous implementation-specific decisions must be made in order to achieve the developer’s specific goals, such as compliance with application-related and business-related constraints, and that these specific goals will vary from one implementation to another and from one developer to another. Moreover, it is appreciated that such a development effort might be complex and time-consuming, but would nevertheless be a routine undertaking of engineering for those of ordinary skill in the art having the benefit of this disclosure.

The catheter systems disclosed herein can include many different forms. Referring now to FIG. 1, a schematic

cross-sectional view is shown of a catheter system **100** in accordance with various embodiments. The catheter system **100** is suitable for imparting pressure waves to induce fractures in one or more treatment sites within or adjacent to a vessel wall of a blood vessel, or on or adjacent to a heart valve, within a body of a patient. In the embodiment illustrated in FIG. 1, the catheter system **100** can include one or more of a catheter **102**, a light guide bundle **122** including one or more light guides **122A**, a source manifold **136**, a fluid pump **138**, a multiplexer **123** including one or more of a light source **124**, a power source **125**, a system controller **126**, and a graphic user interface **127** (a "GUI"), a handle assembly **128**, and an optical analyzer assembly **142**. Alternatively, the catheter system **100** can include more components or fewer components than those specifically illustrated and described in relation to FIG. 1.

It is appreciated that while the catheter system **100** is generally described herein as including a light guide bundle **122** including one or more light guides **122A**, and a light source **124**, in some alternative embodiments, the catheter system **100** can include an energy guide bundle that includes different types of energy guides, and/or a different type of energy source.

In various embodiments, the catheter **102** is configured to move to a treatment site **106** within or adjacent to a vessel wall **108A** of a blood vessel **108** within a body **107** of a patient **109**. The treatment site **106** can include one or more vascular lesions **106A**, such as calcified vascular lesions, for example. Additionally, or in the alternative, the treatment site **106** can include vascular lesions **106A**, such as fibrous vascular lesions. Still alternatively, in some implementations, the catheter **102** can be used at a treatment site **106** within or adjacent to a heart valve within the body **107** of the patient **109**.

The catheter **102** can include an inflatable balloon **104** (sometimes referred to herein simply as a "balloon"), a catheter shaft **110**, and a guidewire **112**. The balloon **104** can be coupled to the catheter shaft **110**. The balloon **104** can include a balloon proximal end **104P** and a balloon distal end **104D**. The catheter shaft **110** can extend from a proximal portion **114** of the catheter system **100** to a distal portion **116** of the catheter system **100**. The catheter shaft **110** can include a longitudinal axis **144**. The catheter shaft **110** can also include a guidewire lumen **118**, which is configured to move over the guidewire **112**. As utilized herein, the guidewire lumen **118** defines a conduit through which the guidewire **112** extends. The catheter shaft **110** can further include an inflation lumen (not shown) and/or various other lumens for various other purposes. In some embodiments, the catheter **102** can have a distal end opening **120** and can accommodate and be tracked over the guidewire **112** as the catheter **102** is moved and positioned at or near the treatment site **106**. In some embodiments, the balloon proximal end **104P** can be coupled to the catheter shaft **110**, and the balloon distal end **104D** can be coupled to the guidewire lumen **118**.

The balloon **104** includes a balloon wall **130** that defines a balloon interior **146**. The balloon **104** can be selectively inflated with a balloon fluid **132** to expand from a deflated state suitable for advancing the catheter **102** through a patient's vasculature, to an inflated state (as shown in FIG. 1) suitable for anchoring the catheter **102** in position relative to the treatment site **106**. Stated in another manner, when the balloon **104** is in the inflated state, the balloon wall **130** of the balloon **104** is configured to be positioned substantially adjacent to the treatment sites **106**. It is appreciated that although FIG. 1 illustrates the balloon wall **130** of the

balloon **104** is shown spaced apart from the treatment site **106** of the blood vessel **108** when in the inflated state, this is done merely for ease of illustration. It is recognized that the balloon wall **130** of the balloon **104** will typically be substantially directly adjacent to and/or abutting the treatment site **106** when the balloon **104** is in the inflated state.

The balloon **104** suitable for use in the catheter system **100** includes those that can be passed through the vasculature of a patient **109** when in the deflated state. In some embodiments, the balloon **104** is made from silicone. In other embodiments, the balloon **104** can be made from polydimethylsiloxane (PDMS), polyurethane, polymers such as PEBAX™ material, nylon, or any other suitable material.

The balloon **104** can have any suitable diameter (in the inflated state). In various embodiments, the balloon **104** can have a diameter (in the inflated state) ranging from less than one millimeter (mm) up to 25 mm. In some embodiments, the balloon **104** can have a diameter (in the inflated state) ranging from at least 1.5 mm up to 14 mm. In some embodiments, the balloons **104** can have a diameter (in the inflated state) ranging from at least two mm up to five mm.

In some embodiments, the balloon **104** can have a length ranging from at least three mm to 300 mm. More particularly, in some embodiments, the balloon **104** can have a length ranging from at least eight mm to 200 mm. It is appreciated that a balloon **104** having a relatively longer length can be positioned adjacent to larger treatment sites **106**, and, thus, may be used for imparting pressure waves onto and inducing fractures in larger vascular lesions **106A** or multiple vascular lesions **106A** at precise locations within the treatment site **106**. It is further appreciated that a longer balloon **104** can also be positioned adjacent to multiple treatment sites **106** at any one given time.

The balloon **104** can be inflated to inflation pressures of between approximately one atmosphere (atm) and 70 atm. In some embodiments, the balloon **104** can be inflated to inflation pressures of from at least 20 atm to 60 atm. In other embodiments, the balloon **104** can be inflated to inflation pressures of from at least six atm to 20 atm. In still other embodiments, the balloon **104** can be inflated to inflation pressures of from at least three atm to 20 atm. In yet other embodiments, the balloon **104** can be inflated to inflation pressures of from at least two atm to ten atm.

The balloon **104** can have various shapes, including, but not to be limited to, a conical shape, a square shape, a rectangular shape, a spherical shape, a conical/square shape, a conical/spherical shape, an extended spherical shape, an oval shape, a tapered shape, a bone shape, a stepped diameter shape, an offset shape, or a conical offset shape. In some embodiments, the balloon **104** can include a drug-eluting coating or a drug-eluting stent structure. The drug-eluting coating or drug-eluting stent can include one or more therapeutic agents, including anti-inflammatory agents, anti-neoplastic agents, anti-angiogenic agents, and the like.

The balloon fluid **132** can be a liquid or a gas. Some examples of the balloon fluid **132** suitable for use can include, but are not limited to one or more of water, saline, contrast medium, fluorocarbons, perfluorocarbons, gases, such as carbon dioxide, or any other suitable balloon fluid **132**. In some embodiments, the balloon fluid **132** can be used as a base inflation fluid. In some embodiments, the balloon fluid **132** can include a mixture of saline to contrast medium in a volume ratio of approximately 50:50. In other embodiments, the balloon fluid **132** can include a mixture of saline to contrast medium in a volume ratio of approximately 25:75. In still other embodiments, the balloon fluid

132 can include a mixture of saline to contrast medium in a volume ratio of approximately 75:25. However, it is understood that any suitable ratio of saline to contrast medium can be used. The balloon fluid **132** can be tailored on the basis of composition, viscosity, and the like so that the rate of travel of the pressure waves are appropriately manipulated. In certain embodiments, the balloon fluid **132** suitable for use herein is biocompatible. A volume of balloon fluid **132** can be tailored by the chosen light source **124** and the type of balloon fluid **132** used.

In some embodiments, the contrast agents used in the contrast media can include, but are not to be limited to, iodine-based contrast agents, such as ionic or non-ionic iodine-based contrast agents. Some non-limiting examples of ionic iodine-based contrast agents include diatrizoate, metrizoate, iothalamate, and ioxaglate. Some non-limiting examples of non-ionic iodine-based contrast agents include iopamidol, iohexol, ioxilan, iopromide, iodixanol, and ioversol. In other embodiments, non-iodine based contrast agents can be used. Suitable non-iodine containing contrast agents can include gadolinium (III)-based contrast agents. Suitable fluorocarbon and perfluorocarbon agents can include, but are not to be limited to, agents such as perfluorocarbon dodecafluoropentane (DDFP, C5F12).

The balloon fluids **132** can include those that include absorptive agents that can selectively absorb light in the ultraviolet region (e.g., at least ten nanometers (nm) to 400 nm), the visible region (e.g., at least 400 nm to 780 nm), or the near-infrared region (e.g., at least 780 nm to 2.5 μm) of the electromagnetic spectrum. Suitable absorptive agents can include those with absorption maxima along the spectrum from at least ten nm to 2.5 μm . Alternatively, the balloon fluid **132** can include absorptive agents that can selectively absorb light in the mid-infrared region (e.g., at least 2.5 μm to 15 μm), or the far-infrared region (e.g., at least 15 μm to one mm) of the electromagnetic spectrum. In various embodiments, the absorptive agent can be those that have an absorption maximum matched with the emission maximum of the laser used in the catheter system **100**. By way of non-limiting examples, various lasers described herein can include neodymium:yttrium-aluminum-garnet (Nd:YAG—emission maximum=1064 nm) lasers, holmium:YAG (Ho:YAG—emission maximum=2.1 μm) lasers, or erbium:YAG (Er:YAG—emission maximum=2.94 μm) lasers. In some embodiments, the absorptive agents can be water-soluble. In other embodiments, the absorptive agents are not water-soluble. In some embodiments, the absorptive agents used in the balloon fluids **132** can be tailored to match the peak emission of the light source **124**. Various light sources **124** having emission wavelengths of at least ten nanometers to one millimeter are discussed elsewhere herein.

The catheter shaft **110** of the catheter **102** can be coupled to the one or more light guides **122A** of the light guide bundle **122** that are in optical communication with the light source **124**. The light guide(s) **122A** can be disposed along the catheter shaft **110** and within the balloon **104**. Each of the light guides **122A** can have a guide distal end **122D** that is at any suitable longitudinal position relative to a length of the balloon **104**. In some embodiments, each light guide **122A** can be an optical fiber, and the light source **124** can be a laser. The light source **124** can be in optical communication with the light guides **122A** at the proximal portion **114** of the catheter system **100**. More particularly, the light source **124** can selectively, simultaneously, sequentially, and/or alternatively be in optical communication with each

of the light guides **122A** in any desired combination, order, and/or pattern due to the presence and operation of the multiplexer **128**.

In some embodiments, the catheter shaft **110** can be coupled to multiple light guides **122A**, such as a first light guide, a second light guide, a third light guide, etc., which can be disposed at any suitable positions about the guidewire lumen **118** and/or the catheter shaft **110**. For example, in certain non-exclusive embodiments, two light guides **122A** can be spaced apart by approximately 180 degrees about the circumference of the guidewire lumen **118** and/or the catheter shaft **110**; three light guides **122A** can be spaced apart by approximately 120 degrees about the circumference of the guidewire lumen **118** and/or the catheter shaft **110**; or four light guides **122A** can be spaced apart by approximately 90 degrees about the circumference of the guidewire lumen **118** and/or the catheter shaft **110**. Still alternatively, multiple light guides **122A** need not be uniformly spaced apart from one another about the circumference of the guidewire lumen **118** and/or the catheter shaft **110**. More particularly, the light guides **122A** can be disposed either uniformly or non-uniformly about the guidewire lumen **118** and/or the catheter shaft **110** to achieve the desired effect in the desired locations.

The catheter system **100** and/or the light guide bundle **122** can include any number of light guides **122A** in optical communication with the light source **124** at the proximal portion **114**, and with the balloon fluid **132** within the balloon interior **146** of the balloon **104** at the distal portion **116**. For example, in some embodiments, the catheter system **100** and/or the light guide bundle **122** can include from one light guide **122A** to five light guides **122A**. In other embodiments, the catheter system **100** and/or the light guide bundle **122** can include from five light guides **122A** to fifteen light guides **122A**. In yet other embodiments, the catheter system **100** and/or the light guide bundle **122** can include from ten light guides **122A** to thirty light guides **122A**. Alternatively, in still other embodiments, the catheter system **100** and/or the light guide bundle **122** can include greater than 30 light guides **122A**.

The light guides **122A** can have any suitable design for purposes of generating plasma and/or pressure waves in the balloon fluid **132** within the balloon interior **146**. In certain embodiments, the light guides **122A** can include an optical fiber or flexible light pipe. The light guides **122A** can be thin and flexible and can allow light signals to be sent with very little loss of strength. The light guides **122A** can include a core surrounded by a cladding about its circumference. In some embodiments, the core can be a cylindrical core or a partially cylindrical core. The core and cladding of the light guides **122A** can be formed from one or more materials, including but not limited to one or more types of glass, silica, or one or more polymers. The light guides **122A** may also include a protective coating, such as a polymer. It is appreciated that the index of refraction of the core will be greater than the index of refraction of the cladding.

Each light guide **122A** can guide light energy along its length from a guide proximal end **122P** to the guide distal end **122D** having at least one optical window (not shown) that is positioned within the balloon interior **146**.

In various embodiments, the guide distal end **122D** can further include and/or incorporate a distal light receiver **122R** that enables light energy to be moved back into and through the light guide **122A** from the guide distal end **122D** to the guide proximal end **122P**. Stated another way, the light energy can move in a first direction **121F** along the light guide **122A** that is generally from the guide proximal end

122P toward the guide distal end 122D of the light guide 122A. At least a portion of the light energy can also move in a second direction 121S along the light guide 122A that is substantially opposite the first direction 121F, i.e., from the guide distal end 122D toward the guide proximal end 122P of the light guide 122A. Moreover, as described in greater detail herein below, the light energy emitted from the guide proximal end 122P after being moved back through the light guide 122A (in the second direction 121S) can be separated and then optically detected, interrogated, and/or analyzed through use of the optical analyzer assembly 142.

The light guides 122A can assume many configurations about and/or relative to the catheter shaft 110 of the catheter 102. In some embodiments, the light guides 122A can run parallel to the longitudinal axis 144 of the catheter shaft 110. In some embodiments, the light guides 122A can be physically coupled to the catheter shaft 110. In other embodiments, the light guides 122A can be disposed along a length of an outer diameter of the catheter shaft 110. In yet other embodiments, the light guides 122A can be disposed within one or more light guide lumens within the catheter shaft 110.

The light guides 122A can also be disposed at any suitable positions about the circumference of the guidewire lumen 118 and/or the catheter shaft 110, and the guide distal end 122D of each of the light guides 122A can be disposed at any suitable longitudinal position relative to the length of the balloon 104 and/or relative to the length of the guidewire lumen 118 to more effectively and precisely impart pressure waves for purposes of disrupting the vascular lesions 106A at the treatment site 106.

In certain embodiments, the light guides 122A can include one or more photoacoustic transducers 154, where each photoacoustic transducer 154 can be in optical communication with the light guide 122A within which it is disposed. In some embodiments, the photoacoustic transducers 154 can be in optical communication with the guide distal end 122D of the light guide 122A. Additionally, in such embodiments, the photoacoustic transducers 154 can have a shape that corresponds with and/or conforms to the guide distal end 122D of the light guide 122A.

The photoacoustic transducer 154 is configured to convert light energy into an acoustic wave at or near the guide distal end 122D of the light guide 122A. The direction of the acoustic wave can be tailored by changing an angle of the guide distal end 122D of the light guide 122A.

In certain embodiments, the photoacoustic transducers 154 disposed at the guide distal end 122D of the light guide 122A can assume the same shape as the guide distal end 122D of the light guide 122A. For example, in certain non-exclusive embodiments, the photoacoustic transducer 154 and/or the guide distal end 122D can have a conical shape, a convex shape, a concave shape, a bulbous shape, a square shape, a stepped shape, a half-circle shape, an ovoid shape, and the like. The light guide 122A can further include additional photoacoustic transducers 154 disposed along one or more side surfaces of the length of the light guide 122A.

In some embodiments, the light guides 122A can further include one or more diverting features or “diverters” (not shown in FIG. 1) within the light guide 122A that are configured to direct light to exit the light guide 122A toward a side surface which can be located at or near the guide distal end 122D of the light guide 122A, and toward the balloon wall 130. A diverting feature can include any feature of the system that diverts light energy from the light guide 122A away from its axial path toward a side surface of the light guide 122A. Additionally, the light guides 122A can each include one or more light windows disposed along the

longitudinal or circumferential surfaces of each light guide 122A and in optical communication with a diverting feature. Stated in another manner, the diverting features can be configured to direct light energy in the light guide 122A toward a side surface that is at or near the guide distal end 122D, where the side surface is in optical communication with a light window. The light windows can include a portion of the light guide 122A that allows light energy to exit the light guide 122A from within the light guide 122A, such as a portion of the light guide 122A lacking a cladding material on or about the light guide 122A.

Examples of the diverting features suitable for use include a reflecting element, a refracting element, and a fiber diffuser. The diverting features suitable for focusing light energy away from the tip of the light guides 122A can include, but are not to be limited to, those having a convex surface, a gradient-index (GRIN) lens, and a mirror focus lens. Upon contact with the diverting feature, the light energy is diverted within the light guide 122A to one or more of a plasma generator 133 and the photoacoustic transducer 154 that is in optical communication with a side surface of the light guide 122A. As noted, the photoacoustic transducer 154 then converts light energy into an acoustic wave that extends away from the side surface of the light guide 122A.

The source manifold 136 can be positioned at or near the proximal portion 114 of the catheter system 100. The source manifold 136 can include one or more proximal end openings that can receive the one or more light guides 122A of the light guide bundle 122, the guidewire 112, and/or an inflation conduit 140 that is coupled in fluid communication with the fluid pump 138. The catheter system 100 can also include the fluid pump 138 that is configured to inflate the balloon 104 with the balloon fluid 132 as needed.

As noted above, in the embodiment illustrated in FIG. 1, the multiplexer 123 includes one or more of the light source 124, the power source 125, the system controller 126, and the GUI 127. Alternatively, the multiplexer 123 can include more components or fewer components than those specifically illustrated in FIG. 1. For example, in certain non-exclusive alternative embodiments, the multiplexer 123 can be designed without the GUI 127. Still alternatively, one or more of the light source 124, the power source 125, the system controller 126, and the GUI 127 can be provided within the catheter system 100 without the specific need for the multiplexer 123.

In some embodiments, the multiplexer 123 can include a two-channel splitter design. The guide bundle 122 can include a manual positioning mechanism that is mounted on an optical breadboard and/or platen. This design enables linear positional adjustment and array tilting by rotating about a channel one light guide 122A axis (not shown in FIG. 1). The adjustment method, in other embodiments, can two adjustment steps, 1) aligning the planar positions of the source beam 124B at Channel 1, and 2) adjusting the light guide bundle 122 to achieve the best alignment at Channel 10.

As illustrated in FIG. 1, in certain embodiments, at least a portion of the optical analyzer assembly 142 can also be positioned substantially within the multiplexer 123. Alternatively, components of the optical analyzer assembly 142 can be positioned in a different manner than what is specifically shown in FIG. 1.

As shown, the multiplexer 123, and the components included therewith, is operatively coupled to the catheter 102, the light guide bundle 122, and the remainder of the catheter system 100. For example, in some embodiments, as illustrated in FIG. 1, the multiplexer 123 can include a

console connection aperture **148** (also sometimes referred to generally as a “socket”) by which the light guide bundle **122** is mechanically coupled to the multiplexer **123**. In such embodiments, the light guide bundle **122** can include a guide coupling housing **150** (also sometimes referred to generally as a “ferrule”) that houses a portion, e.g., the guide proximal end **122P**, of each of the light guides **122A**. The guide coupling housing **150** is configured to fit and be selectively retained within the console connection aperture **148** to provide the mechanical coupling between the light guide bundle **122** and the multiplexer **123**.

The light guide bundle **122** can also include a guide bundler **152** (or “shell”) that brings each of the individual light guides **122A** closer together so that the light guides **122A** and/or the light guide bundle **122** can be in a more compact form as it extends with the catheter **102** into the blood vessel **108** during use of the catheter system **100**. In some embodiments, the light guides **122A** leading to the plasma generator **133** can be organized into a light guide bundle **122**, including a linear block with an array of precision holes forming a multi-channel ferrule. In other embodiments, the light guide bundle **122** could include a mechanical connector array or block connector that organizes singular ferrule into a linear array.

The light source **124** can be selectively and/or alternatively coupled in optical communication with each of the light guides **122A**, i.e., to the guide proximal end **122P** of each of the light guides **122A**, in the light guide bundle **122**. In particular, the light source **124** is configured to generate light energy in the form of a source beam **124A**, such as a pulsed source beam, that can be selectively and/or alternatively directed to and received by each of the light guides **122A** in the light guide bundle **122** as an individual guide beam **124B**. Alternatively, the catheter system **100** can include more than one light source **124**. For example, in one non-exclusive alternative embodiment, the catheter system **100** can include a separate light source **124** for each of the light guides **122A** in the light guide bundle **122**. The light source **124** can be operated at low energies.

The light source **124** can have any suitable design. In certain embodiments, the light source **124** can be configured to provide sub-millisecond pulses of light energy from the light source **124** that are focused onto a small spot in order to couple it into the guide proximal end **122P** of the light guide **122A**. Such pulses of light energy are then directed and/or guided along the light guides **122A** to a location within the balloon interior **146** of the balloon **104**, thereby inducing plasma formation (also sometimes referred to herein as a “plasma flash”) in the balloon fluid **132** within the balloon interior **146** of the balloon **104**, such as via the plasma generator **133** that can be located at the guide distal end **122D** of the light guide **122A**. In particular, the light emitted at the guide distal end **122D** of the light guide **122A** energizes the plasma generator **133** to form the plasma within the balloon fluid **132** within the balloon interior **146**. The plasma formation causes rapid bubble formation and imparts pressure waves upon the treatment site **106**. An exemplary plasma-induced bubble **134** is illustrated in FIG. 1.

When the plasma initially forms in the balloon fluid **132** within the balloon interior **146**, it emits broad-spectrum electromagnetic radiation. This can be seen as a flash of broad-spectrum light detectable by the naked eye. A portion of the light emitted from the plasma bubble **134** can be coupled into the distal light receiver **122R** at the guide distal end **122D** of the light guide **122A** and travel back to the guide proximal end **122P**, where it can be separated,

detected, and analyzed through use of the optical analyzer assembly **142**. The intensity and timing of the visible light pulse relative to the plasma generating pulse provides an indication that the plasma generator **133** functioned, its energy output, and its functional condition. Visible light flashes may occur in other locations of the light guide **122A** if the light guide **122A** is damaged or broken. Such other visible light flashes will also be coupled into the light guide **122A** and carried back to the guide proximal end **122P**. The intensity and timing of these other light pulses provide an indication of damage to or failure of the light guide **122A** or the plasma generator **133**. In such situations, the optical analyzer assembly **142** can include a safety shutdown system **283** (illustrated in FIG. 2A) that can be selectively activated to shut down operation of the catheter system **100**.

The configuration of the plasma generator **133** and/or the distal light receiver **122R** further allows ambient light that originates outside of the catheter **102** to be coupled into the guide distal end **122D** of the light guide **122A**. In one implementation, the optical analyzer assembly **142** monitors for returned ambient light energy that traverses the light guide **122A** from the guide distal end **122D** to the guide proximal end **122P**. If any ambient light energy is present and detected by the optical analyzer assembly **142** in such situations, this is an indication that the catheter **102** is located outside of the body **107** of the patient **109**, and the optical analyzer assembly **142** can be configured to lock out the light source **124** accordingly. In particular, in such situations, the safety shutdown system **283** of the optical analyzer assembly **142** can be selectively activated to shut down operation of the catheter system **100**.

In various non-exclusive alternative embodiments, the sub-millisecond pulses of light energy from the light source **124** can be delivered to the treatment site **106** at a frequency of between approximately one hertz (Hz) and 5000 Hz, between approximately 30 Hz and 1000 Hz, between approximately ten Hz and 100 Hz, or between approximately one Hz and 30 Hz. Alternatively, the sub-millisecond pulses of light energy can be delivered to the treatment site **106** at a frequency that can be greater than 5000 Hz or less than one Hz, or any other suitable range of frequencies.

It is appreciated that although the light source **124** is typically utilized to provide pulses of light energy, the light source **124** can still be described as providing a single source beam **124A**, i.e., a single pulsed source beam.

The light sources **124** suitable for use can include various types of light sources, including lasers and lamps. For example, in certain non-exclusive embodiments, the light source **124** can be an infrared laser that emits light energy in the form of pulses of infrared light. Alternatively, as noted above, the light sources **124**, as referred to herein, can include any suitable type of energy source.

Suitable lasers can include short pulse lasers on the sub-millisecond timescale. In some embodiments, the light source **124** can include lasers on the nanosecond (ns) timescale. The lasers can also include short pulse lasers on the picosecond (ps), femtosecond (fs), and microsecond (us) timescales. It is appreciated that there are many combinations of laser wavelengths, pulse widths, and energy levels that can be employed to achieve plasma in the balloon fluid **132** of the catheter **102**. In various non-exclusive alternative embodiments, the pulse widths can include those falling within a range including from at least ten ns to 3000 ns, at least 20 ns to 100 ns, or at least one ns to 500 ns. Alternatively, any other suitable pulse width range can be used.

Exemplary nanosecond lasers can include those within the UV to IR spectrum, spanning wavelengths of about ten nanometers (nm) to one millimeter (mm). In some embodiments, the light sources **124** suitable for use in the catheter system **100** can include those capable of producing light at wavelengths of from at least 750 nm to 2000 nm. In other embodiments, the light sources **124** can include those capable of producing light at wavelengths of from at least 700 nm to 3000 nm. In still other embodiments, the light sources **124** can include those capable of producing light at wavelengths of from at least 100 nm to ten micrometers (μm). Nanosecond lasers can include those having repetition rates of up to 200 kHz. In some embodiments, the laser can include a Q-switched thulium:yttrium-aluminum-garnet (Tm:YAG) laser. In other embodiments, the laser can include a neodymium:yttrium-aluminum-garnet (Nd:YAG) laser, holmium:yttrium-aluminum-garnet (Ho:YAG) laser, erbium:yttrium-aluminum-garnet (Er:YAG) laser, excimer laser, helium-neon laser, carbon dioxide laser, as well as doped, pulsed, fiber lasers.

The catheter system **100** can generate pressure waves having maximum pressures in the range of at least one megapascal (MPa) to 100 MPa. The maximum pressure generated by a particular catheter system **100** will depend on the light source **124**, the absorbing material, the bubble expansion, the propagation medium, the balloon material, and other factors. In various non-exclusive alternative embodiments, the catheter system **100** can generate pressure waves having maximum pressures in the range of at least approximately two MPa to 50 MPa, at least approximately two MPa to 30 MPa, or at least approximately 15 MPa to 25 MPa.

The pressure waves can be imparted upon the treatment site **106** from a distance within a range from at least approximately 0.1 millimeters (mm) to greater than approximately 25 mm, extending radially from the light guides **122A** when the catheter **102** is placed at the treatment site **106**. In various non-exclusive alternative embodiments, the pressure waves can be imparted upon the treatment site **106** from a distance within a range from at least approximately ten mm to 20 mm, at least approximately one mm to ten mm, at least approximately 1.5 mm to four mm, or at least approximately 0.1 mm to ten mm extending radially from the light guides **122A** when the catheter **102** is placed at the treatment site **106**. In other embodiments, the pressure waves can be imparted upon the treatment site **106** from another suitable distance that is different than the foregoing ranges. In some embodiments, the pressure waves can be imparted upon the treatment site **106** within a range of at least approximately two MPa to 30 MPa at a distance from at least approximately 0.1 mm to ten mm. In some embodiments, the pressure waves can be imparted upon the treatment site **106** from a range of at least approximately two MPa to 25 MPa at a distance from at least approximately 0.1 mm to ten mm. Still alternatively, other suitable pressure ranges and distances can be used.

The power source **125** is electrically coupled to and is configured to provide the necessary power to each of the light source **124**, the system controller **126**, the GUI **127**, the handle assembly **128**, and the optical analyzer assembly **142**. The power source **125** can have any suitable design for such purposes.

The system controller **126** is electrically coupled to and receives power from the power source **125**. Additionally, the system controller **126** is coupled to and is configured to control operation of each of the light source **124**, the GUI **127**, and the optical analyzer assembly **142**. The system

controller **126** can include one or more processors or circuits for purposes of controlling the operation of at least the light source **124**, the GUI **127**, and the optical analyzer assembly **142**. For example, the system controller **126** can control the light source **124** for generating pulses of light energy as desired and/or at any desired firing rate. Additionally, the system controller **126** can control and/or operate in conjunction with the optical analyzer assembly **142** to effectively provide continuous real-time monitoring of the performance, reliability, safety, and proper usage of the catheter system **100**.

The system controller **126** can further be configured to control operation of other components of the catheter system **100** such as the positioning of the catheter **102** adjacent to the treatment site **106**, the inflation of the balloon **104** with the balloon fluid **132**, etc. Further, or in the alternative, the catheter system **100** can include one or more additional controllers that can be positioned in any suitable manner for purposes of controlling the various operations of the catheter system **100**. For example, in certain embodiments, an additional controller and/or a portion of the system controller **126** can be positioned and/or incorporated within the handle assembly **128**.

The GUI **127** is accessible by the user or operator of the catheter system **100**. Additionally, the GUI **127** is electrically connected to the system controller **126**. With such design, the GUI **127** can be used by the user or operator to ensure that the catheter system **100** is effectively utilized to impart pressure onto and induce fractures at the treatment site(s) **106**. The GUI **127** can provide the user or operator with information that can be used before, during, and after use of the catheter system **100**. In one embodiment, the GUI **127** can provide static visual data and/or information to the user or operator. In addition, or in the alternative, the GUI **127** can provide dynamic visual data and/or information to the user or operator, such as video data or any other data that changes over time during use of the catheter system **100**. In various embodiments, the GUI **127** can include one or more colors, different sizes, varying brightness, etc., that may act as alerts to the user or operator. Additionally, or in the alternative, the GUI **127** can provide audio data or information to the user or operator. The specifics of the GUI **127** can vary depending upon the design requirements of the catheter system **100**, or the specific needs, specifications, and/or desires of the user or operator.

As shown in FIG. 1, the handle assembly **128** can be positioned at or near the proximal portion **114** of the catheter system **100**, and/or near the source manifold **136**. In this embodiment, the handle assembly **128** is coupled to the balloon **104** and is positioned spaced apart from the balloon **104**. Alternatively, the handle assembly **128** can be positioned at another suitable location.

The handle assembly **128** is handled and used by the user or operator to operate, position, and control the catheter **102**. The design and specific features of the handle assembly **128** can vary to suit the design requirements of the catheter system **100**. In the embodiment illustrated in FIG. 1, the handle assembly **128** is separate from, but in electrical and/or fluid communication with one or more of the system controller **126**, the light source **124**, the fluid pump **138**, the GUI **127**, and the optical analyzer assembly **142**. In some embodiments, the handle assembly **128** can integrate and/or include at least a portion of the system controller **126** within an interior of the handle assembly **128**. For example, as shown, in certain such embodiments, the handle assembly **128** can include circuitry **156** that can form at least a portion of the system controller **126**. In some embodiments, the

circuitry 156 can receive electrical signals or data from the optical analyzer assembly 142. Further, or in the alternative, the circuitry 156 can transmit such electrical signals or otherwise provide data to the system controller 126.

In one embodiment, the circuitry 156 can include a printed circuit board having one or more integrated circuits, or any other suitable circuitry. In an alternative embodiment, the circuitry 156 can be omitted, or can be included within the system controller 126, which in various embodiments can be positioned outside of the handle assembly 128, e.g., within the multiplexer 123. It is understood that the handle assembly 128 can include fewer or additional components than those specifically illustrated and described herein.

FIG. 2 is a simplified schematic view of a portion of an embodiment of the catheter system 200, including an embodiment of the optical alignment system 257, the optical alignment system 257 being utilized in a first alignment configuration.

The design of the catheter system 200 is substantially similar to the embodiments illustrated and described herein. It is appreciated that various components of the catheter system 200, such as are shown in FIG. 1, are not illustrated in FIG. 2 for purposes of clarity and ease of illustration. However, it is appreciated that the catheter system 200 can include most, if not all, of such components. Additionally, in some embodiments, the components of the catheter system 200 can be mounted and/or fixed on platens.

As shown in FIG. 2, the catheter system 200 again includes a light source 224 that is configured to generate light energy in the form of a source beam 224A, e.g., a pulsed source beam, that can be selectively and/or alternatively directed to and received by each light guide 222A (within the light guide bundle 222) as an individual guide beam 224B (illustrated in FIG. 2A). In one non-exclusive embodiment, the light source 224 is an infrared laser source, and the light guide 222A is a small diameter, multimode optical fiber.

In certain embodiments, as shown in FIG. 2, the source beam 224A from the light source 224 passes through at least one optical element, including but not limited to one or more beamsplitters 258 (two beamsplitters 258 are illustrated in FIG. 2), one or more reflectors 260 (one reflector 260 is illustrated in FIG. 2), one or more coupling lenses 262 (one coupling lens 262 is illustrated in FIG. 2), one or more imaging lenses 263 (one imaging lens 263 is illustrated in FIG. 2), and/or one or more filters 264 (two filters 264 are illustrated in FIG. 2). Each optical element can be configured to focus, reflect, and/or filter the source beam 224A as the individual guide beam 224B down onto a guide proximal end 222P of the light guide 222A, thereby coupling the individual guide beam 224B in the form of the pulse of infrared energy into the light guide 222A. The individual guide beam 224B, when aligned with the light guide 222A, travels toward the plasma generator 233. In some embodiments, each optical element can be configured to focus, reflect, and/or filter an imaging beam 224C toward a camera 265.

The light energy of the individual guide beam 224B is guided along the light guide 222A from the guide proximal end 222P to the guide distal end 222D and energizes the plasma generator 233 that is positioned and/or incorporated at or near a guide distal end 222D of the light guide 222A. The plasma generator 233 utilizes the pulse of infrared energy to create a localized plasma in the balloon fluid 132 within the balloon interior 146 of the balloon 104.

The optical alignment system 257 can include any and/or all of the components shown in the embodiment illustrated

in FIG. 2, FIG. 3, and FIG. 4. The optical alignment system 257 aligns the light energy in the form of the source beam 224A and/or the individual guide beam 224B so that the light energy is coupled with one or more light guides 222A.

The optical alignment system 257 can vary depending on the design requirements of the catheter system 200, the light guides 222A, and/or the energy source 224. It is understood that the optical alignment system 257 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein. Additionally, or alternatively, the optical alignment system 257 can omit one or more of the systems, subsystems, and elements that are specifically shown and/or described herein.

In various embodiments, the optical alignment system 257 can include a multiplexer 223. The optical elements described herein can be included within a multiplexer 223 (such as the multiplexer 128 described in relation to FIG. 1). As displayed in the embodiment shown in FIG. 2, the multiplexer 223 can be movable about a multiplexer axis 223X. In some embodiments, the multiplexer 223 can be fixed or mounted to a multiplexer platen.

In some embodiments, the optical alignment system 257 can include one or more of the beamsplitter(s) 258, the reflector(s) 260, the coupling lens(es) 262, the imaging lens(es) 263, the filter(s) 264, a camera 265, a camera controller 266, an amplifier 267, a system controller 268, a signal processor 269, an optics mover 270, a light source mover 271, an illuminator 272, an alignment controller 273, a detector 274, and/or an aligner 275.

The beamsplitter 258, such as a dichroic beamsplitter in one embodiment, can be positioned in the optical path of the source beam 224A between the light source 224 and the guide proximal end 222P of the light guide 222A. In certain embodiments, the beam splitter 258 is configured to pass light for wavelengths longer than those visible to the other optical elements of the optical alignment system 257 so that the individual guide beam 224B that is directed toward the guide proximal end 222P of the light guide 222A. Such threshold wavelength can be referred to as the cutoff wavelength. The beamsplitter 258 can be further configured to reflect all light having a wavelength that is shorter than the cutoff wavelength. In some embodiments, the cutoff wavelength can be 950 nm. The dichroic beamsplitter 258 can reflect a small percentage of light energy depending on the ratio of dichroic coating on the beamsplitter 258.

In some embodiments, other optical elements (e.g., the coupling lens 262) can be positioned between one or more of the beamsplitters 258 and the light guide 222A. The beam splitter 258 can be configured to focus the individual guide beam 224B down onto the guide proximal end 222P of the light guide 222A, thereby coupling the individual guide beam 224B into the light guide 222A. One or more of the beamsplitters 258 can be used in combination with other optical elements, such as the imaging lens 263 and the filter 264, in order to focus the imaging beam 224C into the camera 265.

In other embodiments, one or more of the beamsplitters 258 can be positioned in the path of the imaging beam 224C to allow a percentage of the imaging beam 224C to be directed to the detector 274 for analysis of light energy returning through the light guide 222A or the face of the guide proximal end 222P. This photo-analysis can be used for diagnostics and for failure detection methods.

The beamsplitter(s) 258 can vary depending on the design requirements of the catheter system 200, the light guides 222A, and/or the optical alignment system 257. It is understood that the beamsplitter 258 can include additional sys-

tems, subsystems, components, and elements than those specifically shown and/or described herein.

The reflector(s) **260** can reflect the light energy emitted by the light source **224** to one or more optical elements of the optical alignment system **257**. In one embodiment, the reflector(s) **260** can include a mirror. In certain embodiments, one or more of the reflectors **260** can fold the source beam **224A** from the light source **224** at an angle of approximately 90 degrees. Alternatively, one or more of the reflectors **260** can fold the source beam **224A** from the light source **224** at an angle that is greater or less than 90 degrees. The reflector(s) **260** can direct the source beam **224A** through the coupling lens **262** toward one or more light guides **222A**. In one embodiment, one or more of the reflectors **260** can be fixed. Alternatively, one or more of the reflectors **260** can be movable, either manually or by one or more optics movers **270**, such as by one or more piezoelectric actuators in one non-exclusive embodiment.

The reflector **260** can vary depending on the design requirements of the catheter system **200**, the light guides **222A**, and/or the optical alignment system **257**. It is understood that the reflector **260** can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The coupling lens **262** can couple the individual guide beam **224B** onto the guide proximal end **222P** of one or more light guides **222A**. The coupling lens **262** can focus and/or collimate the source beam **224A** into the individual guide beam **224B**. The coupling lens **262** can be used to focus the guide beam **224B** down to form a spot that will couple into at least one of the light guides **222A**. The coupling lens **262** can also collimate light sources (e.g., the light source **224**) near the focusing location (see, e.g., the source beam **524B**, FIG. 5B), which is set to be near the guide proximal end **222P** of the light guide **222A**. The light energy from the guide beam **224B** is scattered off of the focused spot on the guide proximal end **222P**.

In some embodiments, since the source beam **224B** and/or the imaging beam **224C** can be collimated, a separate set of optics can focus the source beam **224B** and/or the imaging beam **224C** to form an image. In various embodiments, since the source beam **224B** and/or the imaging beam **224C** between the coupling lens **262** and the imaging lens **262** is collimated, the separation between the optical elements is not critical to imaging performance. The various light beams disclosed herein can be separated by a distance convenient for arranging optical elements on any given platen. The focal length of the optics controls the magnification of the light guide **222A** on the sensor (such as the camera **265**). The separation between optics and image sensor allows for focusing of the image generated at the desired plane at the object independent of the location where the energy source is focused.

The coupling lens **262** can vary depending on the design requirements of the catheter system **200**, the light guides **222A**, and/or the optical alignment system **257**. It is understood that the coupling lens **262** can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein. Additionally, or alternatively, the coupling lens **262** can omit one or more of the systems, subsystems, and elements that are specifically shown and/or described herein.

The imaging lens **263** can couple the imaging beam **224C** onto the camera **265** or any suitable imaging system of the optical alignment system **257**. The imaging lens **263** can vary depending on the design requirements of the catheter system **200**, the light guides **222A**, and/or the optical align-

ment system **257**. It is understood that the imaging lens **263** can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The filter **264** can filter the light energy from the source beam **224A**, the guide beam **224B** and/or the imaging beam **224C**. The filter **264** can vary depending on the design requirements of the catheter system **200**, the light guides **222A**, the optical alignment system **257**, and/or the camera **265**. It is understood that the filter **264** can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The optical elements disclosed in the various embodiments herein can be configured in any position or order. In some embodiments, such as the embodiment illustrated in FIG. 2, can create optical paths for 1) coupling primary IR energy and 2) imaging the end face of the ferrule (e.g., the guide proximal end **222P**), and imaging some of the primary energy scattered or reflected at the end face of the ferrule or conveniently collocated target.

The camera **265** can capture images of the light energy in the form of the imaging beam **224C**. In the first alignment configuration (as shown in the embodiment displayed in FIG. 2) of the optical alignment system **257**, the camera receives the imaging beam **224C** that is reflected and/or scattered back from the guide proximal end **222P**. This scattered light is captured by the coupling lens **262** and focused by the imaging lens **263** to form an image of the focused spot.

In various embodiments, the image of the focused spot will be superimposed on the image of the guide proximal end **222P** in the same image space. An additional filter **264** can be added to reduce the amount of IR signal arriving from the scattered source and to balance the intensity of the focused spot in the image relative to the guide proximal end **222P** and light guide **222A**.

In certain embodiments, as the multiplexer **223** scans laterally across the guide proximal end **222P** of one or more light guides **222A**, the camera **265** creates an image of the guide proximal end **222P** in the visible spectrum. This could rely on ambient visible light as an illumination source. Alternatively, a separate source such as the illuminator **272** could illuminate the guide proximal end **222P** to improve image quality and brightness.

The camera **265** can vary depending on the design requirements of the catheter system **200** and/or the optical alignment system **257**. It is understood that the camera **265** can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The camera controller **266** can control the camera **265**. The camera controller **266** can also send signals to the signal processor **269**. The camera controller **266** can control the illuminator **272** as necessary to adjust image brightness and contrast. The camera controller **266** can vary depending on the design requirements of the catheter system **200**, the light guides **222A**, the optical alignment system **257**, the camera **265**, and/or the signal processor **269**. It is understood that the camera controller **266** can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The amplifier **267** can amplify various signals sent from components of the optical alignment system **257**. As shown in FIG. 2, the signal from the detector **274** can be directed to the amplifier, where the detection of and intensity evaluation of the imaging beam **224C** are determined. In particu-

lar, in certain embodiments, the signal from the detector 274 is directed toward the amplifier 267, where the signal from the detector 274 is amplified.

The amplifier 267 can vary depending on the design requirements of the catheter system 200, the light guides 222A, the optical alignment system 257, the camera 265, and/or the signal processor 269. It is understood that the amplifier 267 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The system controller 268 can control any and/or all of the components of the catheter system 200, the multiplexer 223, and/or the optical alignment system 257. In some embodiments, the system controller 268 controls the emission of light energy from the light source 224. In other embodiments, the system controller 268 controls the optics mover 270.

The system controller 268 can vary depending on the design requirements of the catheter system 200, the multiplexer 223, and/or the optical alignment system 257. It is understood that the system controller 268 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The signal processor 269 can process various signals sent from components of the optical alignment system 257. The signal processor 269 can monitor and record data of the image information and/or other received signals. The signal processor 269 can segment the image to obtain the light guide 222A core/center location and direct the optical alignment system 257 to align the guide beam 224B to the focused spot location in the image space.

In other embodiments, the signal processor 269 can use the scaling of the image and separate calibrations to determine the exact displacement of the actual focal spot relative to the location of the center/core of the light guide 222A for improved coupling. These calibrations can account for all offsets and drifts in the guide beam 224B and the physical location of the aligned light guide 222A due to the mechanical tolerances and stack-ups. The system controller 268 can then use the data to adjust the location of the light guide bundle 222 using the aligner 275. This brings the focused location into perfect alignment with the core/center of the aligned light guide 222A.

The signal processor 269 can vary depending on the design requirements of the catheter system 200, the light guides 222A, the optical alignment system 257, the camera 265, and/or the amplifier 267. It is understood that the signal processor 269 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The optics mover 270 moves and/or controls moving components of the optical alignment system 257, such as the light source mover 271. The optics mover 270 can vary depending on the design requirements of the catheter system 200, the optical alignment system 257, and/or the light source mover 271. It is understood that the optics mover 270 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The light source mover 271 can move the light energy, the light source 224, and/or the multiplexer 223 so that the light energy is properly aligned within at least one of the light guides 222A. In some embodiments, the system controller 268 controls the optics mover 270 that is connected to the light source mover that positions the multiplexer 223 and aligns a beam axis (not shown) of the guide beam 224B within one or more of the light guides 222A. Using the

embodiments disclosed herein, the optical alignment system 257 can utilize the light source mover 271 to align the energy source 224 with any desired channel within the light guide bundle 222, trigger the energy source 224, and move to the next desired channel within the light guide bundle 222.

The light source mover 271 can vary depending on the design requirements of the catheter system 200, the light guides 222A, the optical alignment system 257, and/or the optics mover 270. It is understood that light source mover 271 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

In some embodiments, the light source mover 271 can include a linear translation stage. The multiplexer 223 can be configured to move across the linear translation stage about the multiplexer axis 223X.

The illuminator 272 can illuminate the guide proximal end 222P so that the alignment of the light energy and the guide proximal end 222P is easier to detect and analyze by the optical alignment system 257. The illuminator 272 can vary depending on the design requirements of the catheter system 200, the light guides 222A, and/or the optical alignment system 257. It is understood that the illuminator 272 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein. In some embodiments, the illuminator 272 can include a visible light source such as a visible LED.

The alignment controller 273 controls the alignment components of the optical alignment system 257, such as the aligner 275. The alignment controller 273 can vary depending on the design requirements of the catheter system 200, the light guides 222A, the optical alignment system 257, and/or the aligner 275. It is understood that the alignment controller 273 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The detector 274 can receive the light energy from the imaging beam 224C when the optical alignment system 257 is in a second alignment configuration (shown in FIG. 3). The detector 274 can detect the light energy from the imaging beam 224C and converts the detected light energy to signals. The detector 274 can send the signals to the amplifier 267 to be amplified and sent to the signal processor 269.

The detector 274 can vary depending on the design requirements of the catheter system 200, the optical alignment system 257, the amplifier 267, and/or the signal processor 269. It is understood that the detector 274 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

The aligner 275 can align various components of the alignment system 257, such as the light guide bundle 222 and the light source mover 271. The aligner 275 can vary depending on the design requirements of the catheter system 200, the light guides 222A, the optical alignment system 257, and/or the alignment controller 273. It is understood that the aligner 275 can include additional systems, subsystems, components, and elements than those specifically shown and/or described herein.

In other embodiments, the aligner 275 can include stepper motors, and/or piezo actuators to adjust the height and tilt of the light guide bundle 222. In one alignment process, the optical alignment system 257 would align the light source mover 271 near a first channel in the light guide bundle 222 (corresponding with one light guide 222A) and capture an

image of the guide proximal end 222P and the corresponding light guide 222A with the guide beam 224B focused location.

In certain embodiments, the magnification of the light guide 222A in the image can be controlled so that the image is small relative to the light guide bundle 222 size in the image. The system controller 268 can calculate the offset and adjust movement parameters in at least two directions to align the focused location with the center/core of the light guide 222A. The system controller 268 can align the source beam 224B with the final light guide 222A in the linear array of the light guide bundle 222 and capture an image of the guide proximal end 222P and the light guide 222A along with the focused location. The positional offset can be used to set the tilt of the light guide bundle 222 by rotating it around the center of one of the light guides 222A. This process could continue iteratively to adjust position and tilt parameters for the light guide 222A as a whole. The process can continue to return to each light guide 222A location and adjust the linear position along the multiplexer axis 223X. This process can be executed as an initial alignment of light source 224 and the optical alignment system 257 to a new guide bundle 222. Once the configuration described herein is completed, the optical alignment system 257 can operate over a time interval during which the alignment would remain stable.

In various embodiments, the optical alignment system 257 would utilize optical compensation devices (e.g., multiple reflectors 260, steering wedges) to adjust the focused location relative to the light guide bundle 222. Steering wedges (not shown) can be placed in the path of the source beam 224A, the guide beam 224B, and/or the imaging beam 224C in order to account for deviations in linear directions within a plane. The optical alignment system 257 can adjust the guide beam 224B location to a pre-aligned light guide bundle 222.

In some embodiments, the image of the focused location could also be obtained from other surfaces or targets than the guide proximal end 222P and/or the light guide 222A. For example, a flat ceramic target could be located near the light guide 222A along a bundle axis of the guide bundle 222. The light source mover 222 could offset the multiplexer 223 a set distance to track the location of the focused location on the new target. The signal processor 269 can subtract the offset when determining the location of the focused location relative to the light guide 222A image space.

In various embodiments, the first alignment configuration can be an initial setup and alignment configuration. In the first alignment configuration, the light guide bundle 222, including the individual light guides 222A, is coupled to the multiplexer 223. The system controller 268 can position the light source mover 271 at the first light guide 222A position. The camera controller 266 can engage the illuminator 272 and begin to capture images of the light guide 222A and the guide proximal end 222P. The system controller 268 can engage pulses of the light source 224 at low energy, and the camera 265 can capture a suitable image. The signal processor 269 can analyze this image and computes the offset to line up linear positional parameters to improve coupling for the first optical channel (e.g., the first light guide 222A in the light guide bundle 222). The optical alignment system 257 can then reiterate the process for each channel in the light guide bundle 222.

FIG. 3 is a simplified schematic view of a portion of an embodiment of the catheter system 300, including an

embodiment of the optical alignment system 357, the optical alignment system 357 being utilized in a second alignment configuration.

The design of the catheter system 300 is substantially similar to the embodiments illustrated and described herein. It is appreciated that various components of the catheter system 300, such as are shown in FIG. 1, are not illustrated in FIG. 3 for purposes of clarity and ease of illustration. However, it is appreciated that the catheter system 300 can include most, if not all, of such components.

As shown in FIG. 3, the catheter system 300 again includes a light source 324 that is configured to generate light energy in the form of a source beam 324A, e.g., a pulsed source beam, that can be selectively and/or alternatively directed to and received by each light guide 322A (within the light guide bundle 322) as an individual guide beam 324B. In one non-exclusive embodiment, the light source 324 is an infrared laser source, and the light guide 322A is a small diameter, multimode optical fiber.

In certain embodiments, as shown in FIG. 3, the source beam 324A from the light source 324 passes through at least one optical element, such as one or more beamsplitters 358, one or more reflectors 360, one or more coupling lenses 362, one or more imaging lenses 363, and/or one or more filters 364. Some or all of the optical elements can be configured to focus, reflect, and/or filter the source beam 324A as the individual guide beam 324B down onto a guide proximal end 322P of the light guide 322A, thereby coupling the individual guide beam 324B in the form of the pulse of infrared energy into the light guide 322A. The individual guide beam 324B, when aligned with the light guide 322A, travels toward the plasma generator 333. In some embodiments, each optical element can be configured to focus, reflect, and/or filter an imaging beam 324C toward the camera 365.

As illustrated in the embodiment of FIG. 3, the catheter system 300 can again include the multiplexer 323 having the multiplexer axis 323X, the camera controller 366, the amplifier 367, the system control 368, the signal processor 369, the optics mover 370, the light source mover 371, the illuminator 372, the alignment controller 373, the detector 374, and/or the aligner 375. Each of the components can have the same and/or substantially similar functionality and/or components as described in the embodiments disclosed herein.

In the second alignment configuration (shown in FIG. 3), the detector 374 can receive the light energy from the imaging beam 324C. The detector 374 can detect the light energy from the imaging beam 324C and converts the detected light energy to signals. The detector 374 can send the signals to the amplifier 367 to be amplified and sent to the signal processor 369.

In other embodiments, the second alignment configuration can be a high-energy mode. In the second alignment configuration, the optical alignment system 357 would have already completed the initial setup and alignment process described in the first alignment configuration. In the second alignment configuration, the optical alignment system 357 can the light source mover 371 at a predetermined position along the multiplexer axis 323X for a given optical channel and fire the light source 324. The optical alignment system 357 collects light that is reflected as the imaging beam 324C and directs the imaging beam 324 to the detector 374. The detector 374 can be used in the second alignment configuration to analyze for optical failures at the proximal and distal end of the light guides 322A as well as monitor the plasma generated by the plasma generator 333. The optical

alignment system 357 can capture and analyze this data and determine whether to move the guide beam 324B to the next optical channel. If the optical alignment system 357 is nominal, then it aligns the guide beam 324B to the next channel and triggers the light source 324, repeating the process down the full array of the light guide bundle 322.

FIG. 4 is a simplified schematic view of a portion of an embodiment of the catheter system 400, including an embodiment of the optical alignment system 457, the optical alignment system 457 being utilized in a third alignment configuration.

The design of the catheter system 400 is substantially similar to the embodiments illustrated and described herein. It is appreciated that various components of the catheter system 400, such as are shown in FIG. 1, are not illustrated in FIG. 4 for purposes of clarity and ease of illustration. However, it is appreciated that the catheter system 400 can include most, if not all, of such components.

As shown in FIG. 4, the catheter system 400 again includes a light source 424 that is configured to generate light energy in the form of a source beam 424A, e.g., a pulsed source beam, that can be selectively and/or alternatively directed to and received by each light guide 422A (within the light guide bundle 422) as an individual guide beam 424B. Some or all of the optical elements can be configured to focus, reflect, and/or filter the source beam 424A as the individual guide beam 424B down onto a guide proximal end 422P of the light guide 422A, thereby coupling the individual guide beam 424B in the form of the pulse of infrared energy into the light guide 422A. The individual guide beam 424B, when aligned with the light guide 422A, travels toward the plasma generator 433.

In certain embodiments, as shown in FIG. 4, the source beam 424A from the light source 424 passes through, reflects off of, or otherwise interacts with, at least one optical element, such as one or more reflectors 460. Each reflector 460 can include one or more adjustable mirrors and/or mounted mirrors. In some embodiments, the reflector 460 can include one or more adjustment fasteners (not shown) that enable the positioning and/or adjustment of the reflector 460. It is appreciated that, in certain embodiments, one or more of the reflectors 460 can be fixed and immovable. In some embodiments, the optical alignment system 457 can further include one or more reflector movers 461.

Each reflector mover 461 can move one of the reflectors 460 to more accurately guide the source beam 424A and/or the individual guide beams 424B throughout the catheter system 400 and into the guide proximal end 422P of the light guide 422A. The reflector mover 461 can be controlled by the alignment controller 473 and/or the system controller 463.

Each reflector mover 461 can include one or more suitable actuators, such as a stepper motor, a piezoelectric actuator, or any other suitable type of actuator. The reflector mover 461 can move a corresponding reflector 460 with at least one, and up to six, degrees of freedom along and/or about the X, Y, and Z axes (not shown) of the reflector 460.

As illustrated in the embodiment of FIG. 4, the catheter system 400 can include the optics mover 470. The optics mover 470 can have the same and/or substantially similar functionality and/or components as described in the embodiments disclosed herein. For example, the optics mover 470 can include a stepper motor, a piezoelectric actuator, or any other suitable type of actuator.

FIG. 5A is a simplified view of a guide proximal end 522P, and a portion of the guide beam 524B reflected off the light guide 522A, the portion of the guide beam 524B being

shown in an unaligned state. As shown in the embodiment illustrated in FIG. 5A, the unaligned state is when the portion of the guide beam 524 is not substantially within a guide center 522C of the light guide 522A. FIG. 5A shows the focused location of the guide beam 324B (illustrated in FIG. 3) that has been scattered off of the guide proximal end 322P (illustrated in FIG. 3). By adjusting the position of the light guide bundle and/or the guide beam 324, the scattered light can be captured by the camera 365 (illustrated in FIG. 3).

FIGS. 5A and 5B can illustrate a dual-imaging approach to optical alignment. FIGS. 5A and 5B can demonstrate some of the images captured by the camera 365 of the optical alignment system 357 (illustrated in FIG. 3).

FIG. 5B is a simplified view of a guide proximal end 522P, and a portion of the guide beam 524B reflected off the light guide 522A, the portion of the guide beam 524B being shown in an aligned state. In the embodiment shown in FIG. 5B, the portion of the guide beam 524B is shown in the aligned state, with the portion of the guide beam substantially within the guide center 522C of the light guide 522A. FIG. 5B demonstrates Fresnel reflection from fused silica surfaces within the light guide 522A, rather than the scattering depicted in FIG. 5A.

FIG. 6 is a flow chart of one embodiment of a method for treating a treatment site within or adjacent to a vessel wall or a heart valve using a catheter system having features and/or steps of the present invention. It is understood that the method pursuant to the disclosure herein can include greater or fewer steps than those shown and described relative to FIG. 6. Stated another way, the method according to the present invention can omit one or more steps illustrated in FIG. 6 or add additional steps not shown and described in FIG. 6 and still fall within the purview of the present invention. Further, the sequence of the steps can be varied from those shown and described relative to FIG. 6. The sequence of steps illustrated in FIG. 6 is not intended to limit the sequencing of steps in any manner.

In the embodiment illustrated in FIG. 6, at step 676, a system controller is configured to control an optics mover.

At step 678, the system controller can be configured to control an optical alignment system and/or any component of the optical alignment system, such as a light source, a camera, an aligner, an amplifier, an illuminator, a detector, a filter, a beamsplitter, a camera controller, a signal processor, a multiplexer and/or a light guide bundle.

At step 680, a light mover is coupled to the multiplexer so the light mover can move the multiplexer. In some embodiments, the light mover is a linear translational stage.

At step 682, the light source generates light energy.

At step 684, the multiplexer receives the light energy generated by the light source.

At step 686, the multiplexer directs the light energy within a light guide.

At step 688, the light guide reflects a portion of the light energy back towards a detector.

At step 690, the detector or another component of the optical alignment system detects the alignment of the light energy and the light guide.

At step 692, the optical alignment system aligns the light energy with the light guide, so they are substantially coupled.

It is appreciated that the active detection and alignment of the coupling of the light energy with the light guide, through the use of the present invention, provides multiple advantages with respect to the performance, reliability, and proper usage of an IVL catheter, in particular one that utilizes an

energy source to create a localized plasma which in turn produces a high energy bubble inside a balloon catheter. Specific advantages this invention provides include: 1) providing active compensation for connector and ferrule mechanical tolerances, thereby reducing system performance dependence on light carrier's mechanical tolerances and tolerances of their location in a multi-channel array, and 2) providing active compensation for drift in energy beam pointing that occurs in the source itself or through changes or motion of internal or coupling optics due to thermal drift or other factors. The active compensation ultimately reduces performance dependence on the accuracy of connecting and aligning the multi-channel array to the multiplexer and improves the speed and performance of the multiplexer and multi-channel ferrule system.

In particular, in various embodiments, the present invention comprises a multiplexer as a precision linear mechanism that translates coupling optics along a linear path. This approach can include a single degree of freedom. A ferrule can organize the individual optical fibers into a liner pattern with precise interval spacing. An example of a ferrule that can be used by the system is a V-groove ferrule block, as used in multi-channel fiber optics communication systems. The linear translation mechanism can be electronically controlled by the optical alignment system to line the beam path up sequentially with each individual fiber organized in the ferrule. The translating mechanism carries necessary beam directing optics and focusing optics to focus the laser energy onto each fiber to improve the optical coupling. By utilizing the systems and methods disclosed herein, the low divergence of the laser beam over the short distance of motion of the translated coupling mechanism has a minimum impact on coupling efficiency to the fiber. The optical alignment system can drive the mechanism to align the beam path with a selected fiber optic channel and then fires the laser in pulsed or semi-CW mode.

In other embodiments, the optical alignment system can incorporate secondary optics and an image sensor to directly image the ferrule block and the optical fibers. This subsystem simultaneously images the focused spot of the energy beam scattered off the ferrule or a strategically located nearby target. The image of the energy spot is in the same image reference frame allowing direct computation of offset from the core of the optical fiber. This data can be computed using image processing methods and algorithms to determine offset and compute compensation adjustment. A positioning mechanism can then adjust the positioning of the ferrule array to provide improved coupling of the focused spot to the fiber core.

The systems and methods disclosed in the various embodiments provided herein can be implemented on any multiplexer configuration, including linear, circular, patterned, or scanned configurations, provided that the wavelength separating beamsplitter can be inserted in the beam path between the coupling optics and the energy source. The systems and methods disclosed herein can enable the coupling lens to function in dual-use mode, both coupling energy into a light guide and part of the imaging lens to image the light guide.

It is appreciated that the systems and methods of optical alignment provided herein address multiple potential issues with the performance, reliability, and proper usage of an IVL catheter, in particular one that utilizes an energy source to create a localized plasma which in turn produces a high energy bubble inside a balloon catheter. Specific problems solved by the systems and methods disclosed herein include:

- 1) Complex laser systems with moving components suffer from beam pointing errors. These pointing errors can be induced by vibration, the thermal drift of optical components and mirrors, and long-term mechanical changes in mounting the source and optics. This drift in beam pointing can be angular or lateral and would create offsets in the focused spot location. Without compensation for these drifts, the error in spot location relative to the optical fiber core leads to a loss in coupling efficiency and damage to the fiber at high energies. The systems and methods disclosed herein provide active compensation for actual beam drift as it occurs at the point of coupling.
- 2) The systems and methods disclosed herein provide compensation for mechanical tolerance stack-ups of assemblies and true alignment for optical fibers, ferrule, connector, and receptacle, thereby making it possible to use low-cost, low-precision components on the SUD and improve COGS.
- 3) The systems and methods disclosed herein reduce the multiplexer performance dependence on the accuracy of static or fixed positioning mechanism in multiplexer and associated quality and precision of its optical and mechanical components, thereby improving the speed and performance of the multiplexer and multi-channel ferrule system.

It should be noted that, as used in this specification and the appended claims, the singular forms "a," "an," and "the" include plural referents unless the content and/or context clearly dictates otherwise. It should also be noted that the term "or" is generally employed in its sense including "and/or" unless the content or context clearly dictates otherwise.

It should also be noted that, as used in this specification and the appended claims, the phrase "configured" describes a system, apparatus, or other structure that is constructed or configured to perform a particular task or adopt a particular configuration. The phrase "configured" can be used interchangeably with other similar phrases such as arranged and configured, constructed and arranged, constructed, manufactured and arranged, and the like.

The headings used herein are provided for consistency with suggestions under 37 CFR 1.77 or otherwise to provide organizational cues. These headings shall not be viewed to limit or characterize the invention(s) set out in any claims that may issue from this disclosure. As an example, a description of a technology in the "Background" is not an admission that technology is prior art to any invention(s) in this disclosure. Neither is the "Summary" or "Abstract" to be considered as a characterization of the invention(s) set forth in issued claims.

The embodiments described herein are not intended to be exhaustive or to limit the invention to the precise forms disclosed in the detailed description provided herein. Rather, the embodiments are chosen and described so that others skilled in the art can appreciate and understand the principles and practices. As such, aspects have been described with reference to various specific and preferred embodiments and techniques. However, it should be understood that many variations and modifications may be made while remaining within the spirit and scope herein.

It is understood that although a number of different embodiments of the catheter systems have been illustrated and described herein, one or more features of any one embodiment can be combined with one or more features of one or more of the other embodiments, provided that such combination satisfies the intent of the present invention.

While a number of exemplary aspects and embodiments of the catheter systems have been discussed above, those of skill in the art will recognize certain modifications, permutations, additions, and sub-combinations thereof. It is therefore intended that the following appended claims and claims hereafter introduced are interpreted to include all such modifications, permutations, additions, and sub-combinations as are within their true spirit and scope, and no limitations are intended to the details of construction or design herein shown.

What is claimed is:

1. A catheter system for treating a treatment site within or adjacent to a vessel wall or a heart valve, the catheter system comprising:

- a light source that generates light energy;
- a first light guide that receives the light energy from the light source, the first light guide having a guide proximal end;
- a second light guide that receives the light energy from the light source, the second light guide having a guide proximal end;
- a multiplexer that directs the light energy toward the guide proximal end of the first light guide and the guide proximal end of the second light guide; and
- an optical alignment system that determines an alignment of the light energy relative to at least one of the guide proximal ends, the optical alignment system adjusting a positioning of the light energy relative to the at least one of the guide proximal ends based at least partially on the alignment of the light energy relative to the at least one of the guide proximal ends, the optical alignment system including an imaging system including an imaging sensor that is configured to capture images of a focal point of the light source and the at least one of the guide proximal ends.

2. The catheter system of claim 1 wherein the imaging system is configured to simultaneously capture images of the focal point of the light source and a scattered energy beam scattered off the at least one of the guide proximal ends.

3. The catheter system of claim 1 wherein the imaging system is configured to utilize an image reference frame that allows direct computation of a distance offset from a center of the at least one of the guide proximal ends.

4. The catheter system of claim 3 wherein the imaging system is configured to determine the distance offset and compute a compensation adjustment of the alignment of the light energy relative to the at least one of the guide proximal ends.

5. The catheter system of claim 4 wherein the optical alignment system further includes an alignment positioner that positions the alignment of the light energy relative to the at least one of the guide proximal ends based on the computed compensation adjustment to substantially couple the light source and the at least one of the guide proximal ends.

6. The catheter system of claim 1 wherein the optical alignment system further includes a reflector and a reflector mover that moves the reflector.

7. The catheter system of claim 1 wherein the light source is a pulsed IR laser.

8. The catheter system of claim 1 wherein the optical alignment system further includes an illuminator that illuminates the at least one of the guide proximal ends to provide improved image quality and brightness.

9. The catheter system of claim 8, wherein the system controller controls the illuminator and adjusts an image brightness and contrast.

10. A catheter system for treating a treatment site within or adjacent to a vessel wall or a heart valve, the catheter system comprising:

- a light source that generates light energy;
 - a first light guide that receives the light energy from the light source, the first light guide having a guide proximal end;
 - a second light guide that receives the light energy from the light source, the second light guide having a guide proximal end;
 - a multiplexer that directs the light energy toward the guide proximal end of the first light guide and the guide proximal end of the second light guide; and
 - an optical alignment system that determines an alignment of the light energy relative to at least one of the guide proximal ends, the optical alignment system adjusting a positioning of the light energy relative to the at least one of the guide proximal ends based at least partially on the alignment of the light energy relative to the at least one of the guide proximal ends, the optical alignment system including an imaging system including an imaging sensor that is configured to capture images of a focal point of the light source and the at least one of the guide proximal ends;
- wherein the optical alignment system further includes one of a stepper motor and a piezo actuator that is configured to adjust a yaw, pitch, and roll of at least one of the light guides.

11. The catheter system of claim 10 further comprising a system controller that is configured to control the optical alignment system so that the light energy is substantially coupled to the at least one of the guide proximal ends.

12. The catheter system of claim 10 wherein at least one of the light guides is an optical fiber and the light source is a laser.

13. The catheter system of claim 10 wherein the optical alignment system further includes an optical aligner that is configured to align the light energy with the at least one of the guide proximal ends.

14. The catheter system of claim 13 wherein the optical aligner is controlled by the system controller.

15. The catheter system of claim 10 further comprising a system controller that is configured to control an actuator that positions the multiplexer and aligns the light energy relative to the at least one of the guide proximal ends.

16. The catheter system of claim 10 wherein the light source is a pulsed IR laser.

17. The catheter system of claim 10 wherein the optical alignment system further includes optical compensators that are configured to adjust the positioning of the light source relative to the at least one of the guide proximal ends, the optical compensators including a plurality of optical steering wedges positioned in a path of the light source, the plurality of optical steering wedges being configured to improve a coupling of the light source and the at least one of the guide proximal ends.

18. The catheter system of claim 10 wherein the optical alignment system further includes a reflector and a reflector mover that moves the reflector.

19. The catheter system of claim 10 wherein the optical alignment system further includes an illuminator that illuminates the at least one of the guide proximal ends to provide improved image quality and brightness.

20. The catheter system of claim 19 wherein the system controller controls the illuminator and adjusts an image brightness and contrast.