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(54) **SURGICAL DEVICE WITH ARTICULATION AND WRIST ROTATION**

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(58) **Field of Classification Search**

None

See application file for complete search history.

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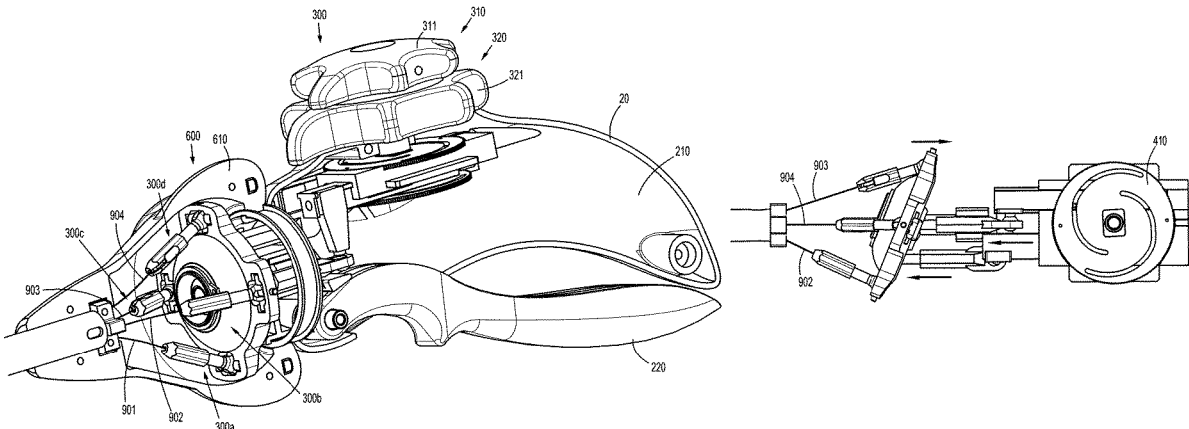
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(57) **ABSTRACT**

A surgical instrument comprising a handle assembly, an elongated shaft, an end effector, a rotation mechanism, and an articulation mechanism is disclosed. The rotation mechanism is disposed in mechanical cooperation with the handle assembly and effects rotation of the end effector about the second longitudinal axis. The articulation mechanism is disposed in mechanical cooperation with the handle assembly and effects movement of the end effector from a first position where the first longitudinal axis is substantially aligned with the second longitudinal axis to a second position where the second longitudinal axis is displaced from the first longitudinal axis. The articulation mechanism comprises a first articulation control disposed in mechanical cooperation with the handle assembly, a first cable and a second cable. Actuation of the first articulation control in a first direction causes the first cable to move distally and causes the second cable to move proximally.

**17 Claims, 20 Drawing Sheets**



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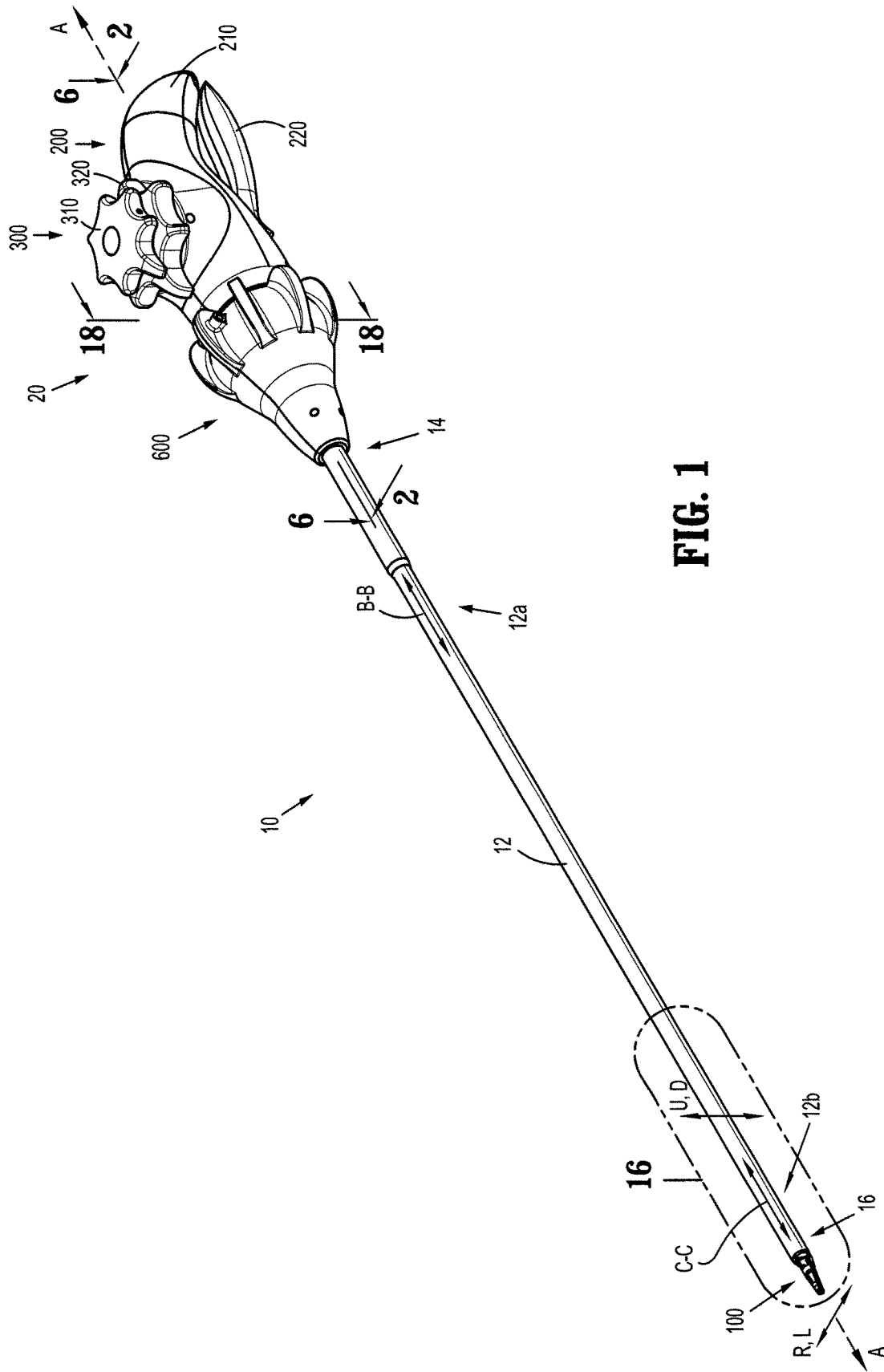


FIG. 1

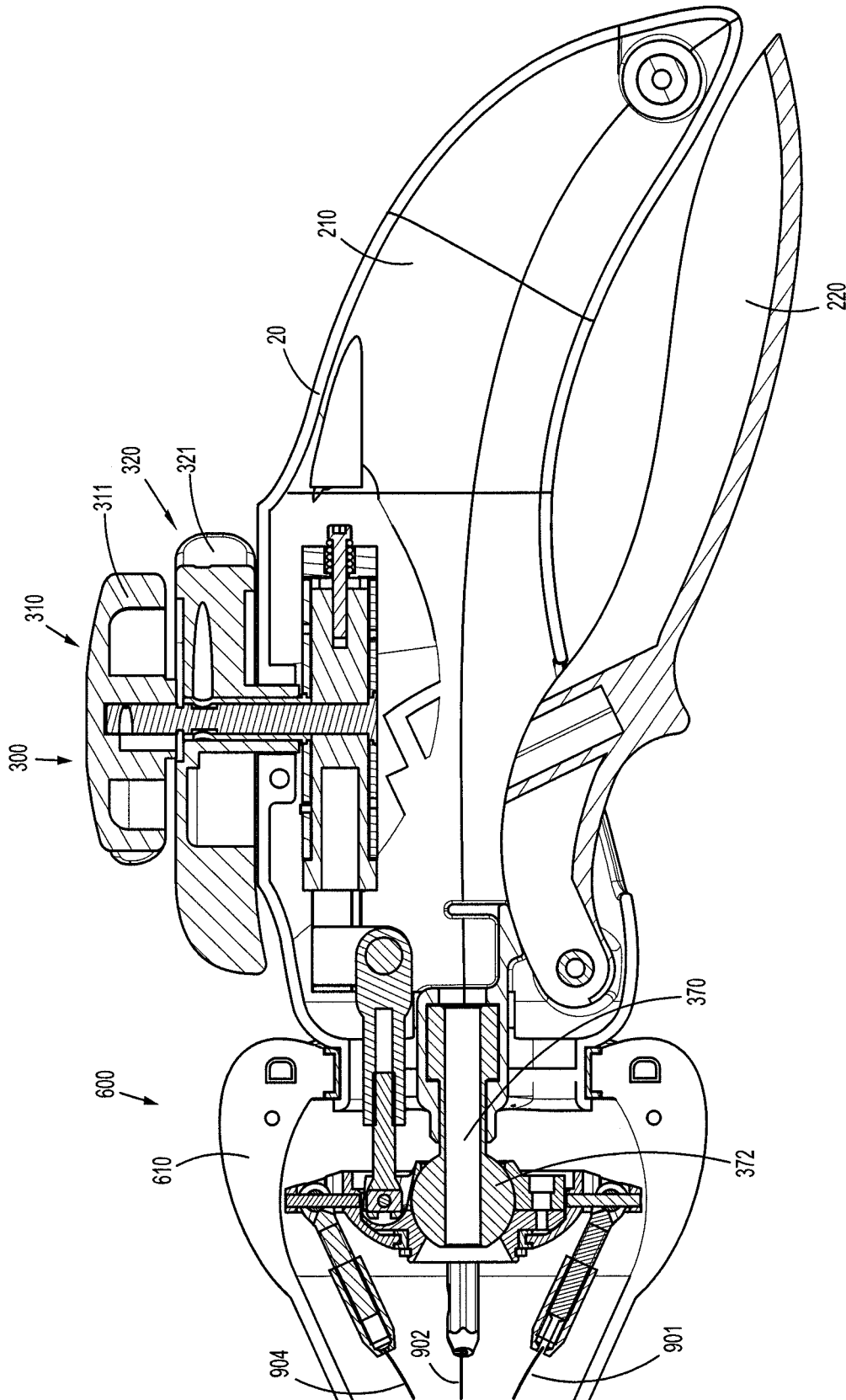


FIG. 2

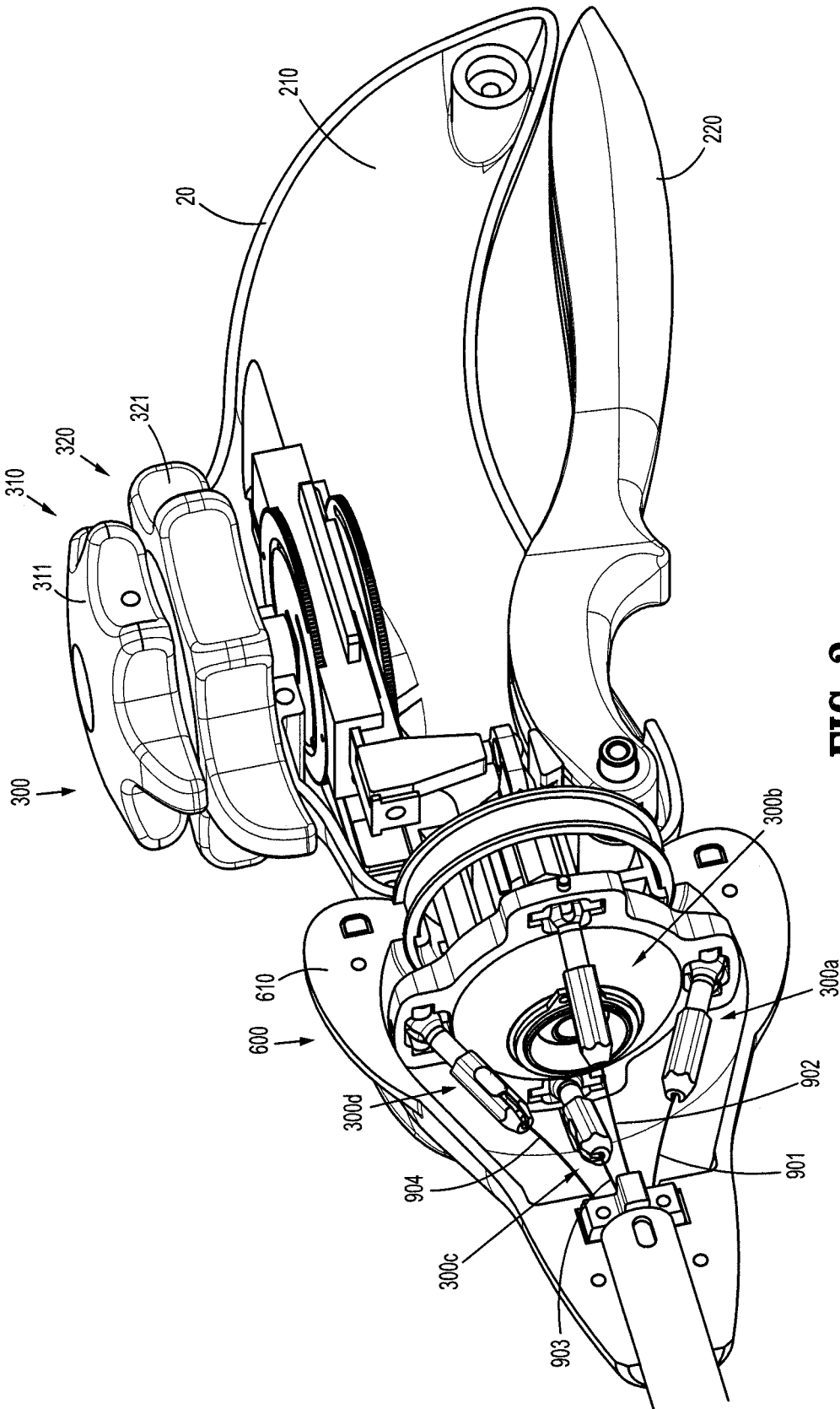
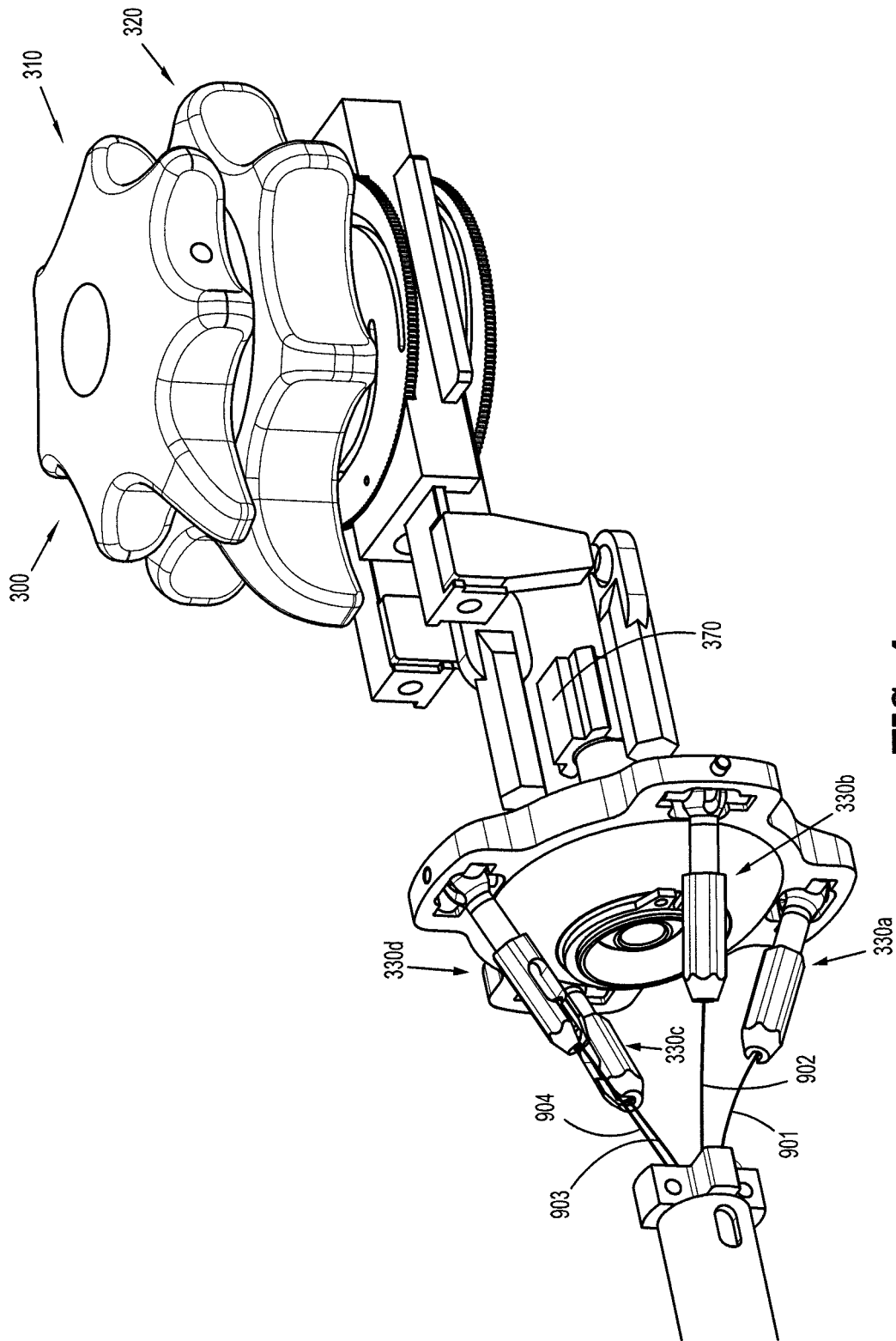


FIG. 3



**FIG. 4**

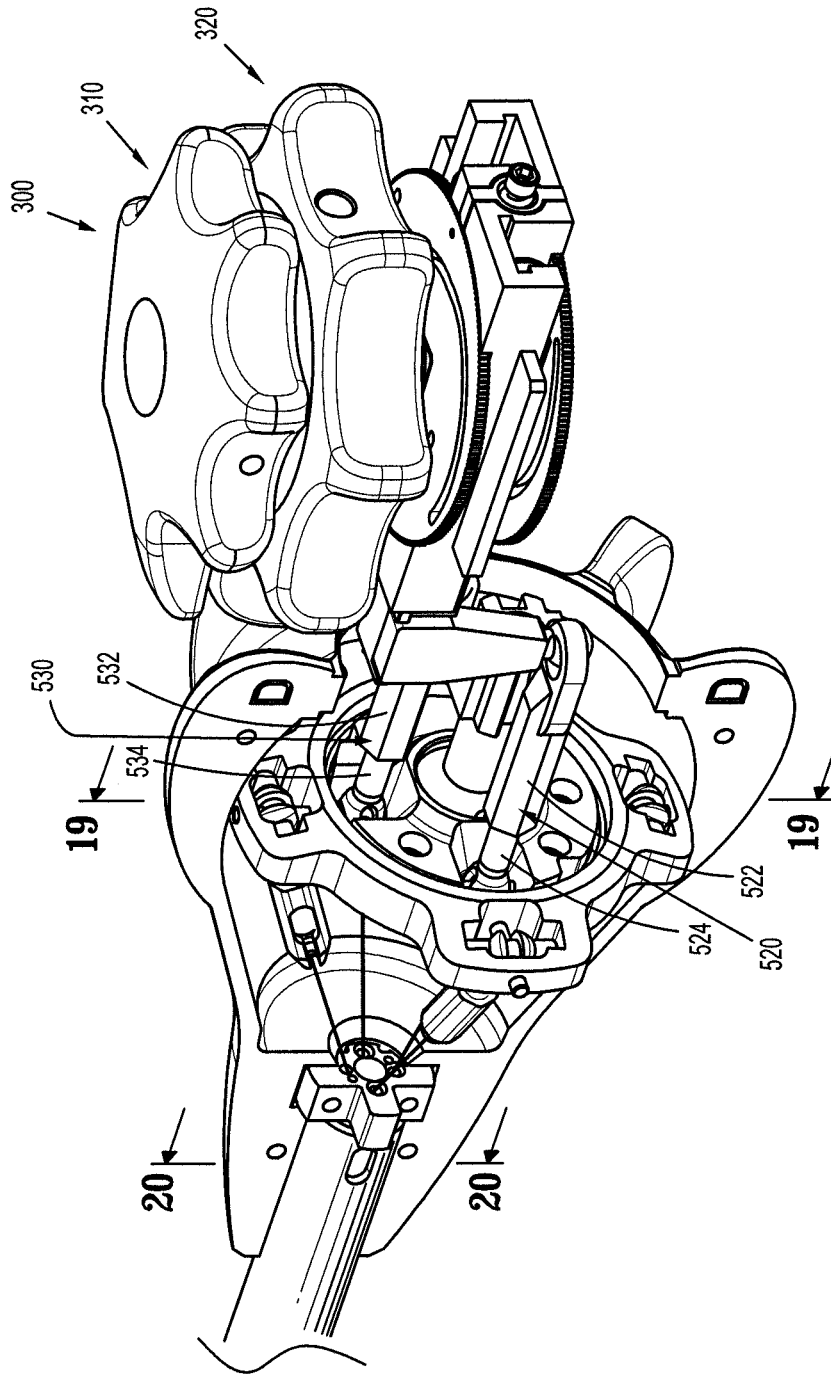
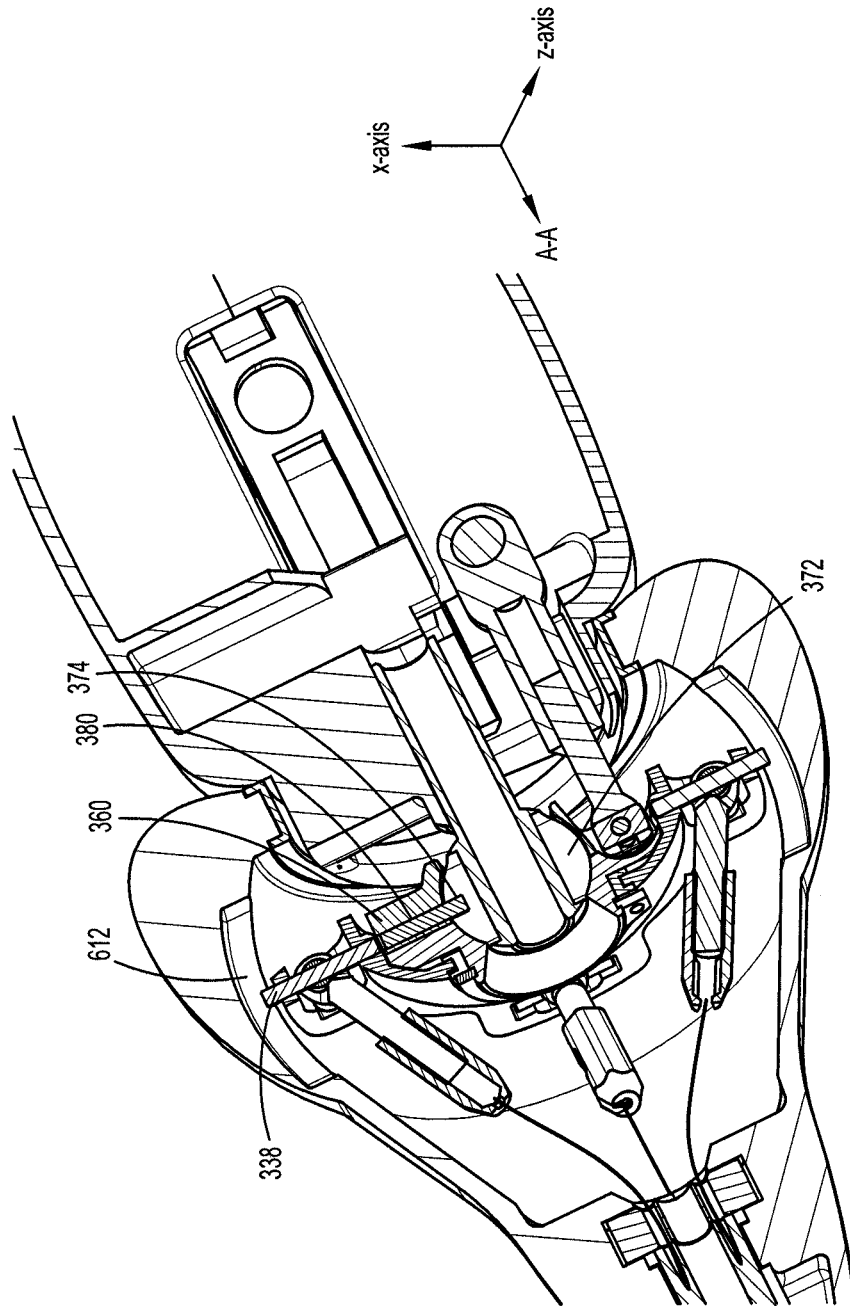


FIG. 5



**FIG. 6**



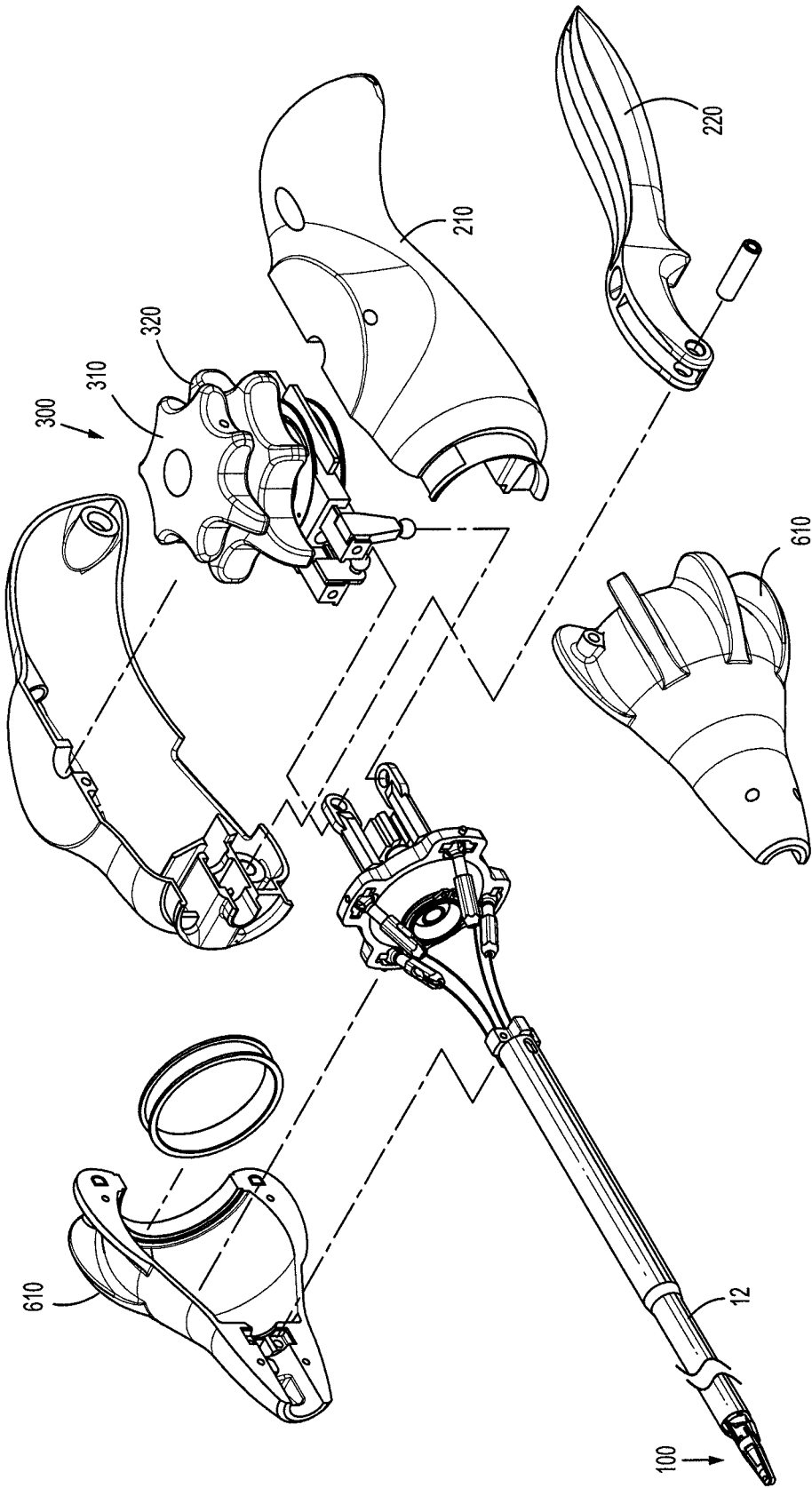


FIG. 7

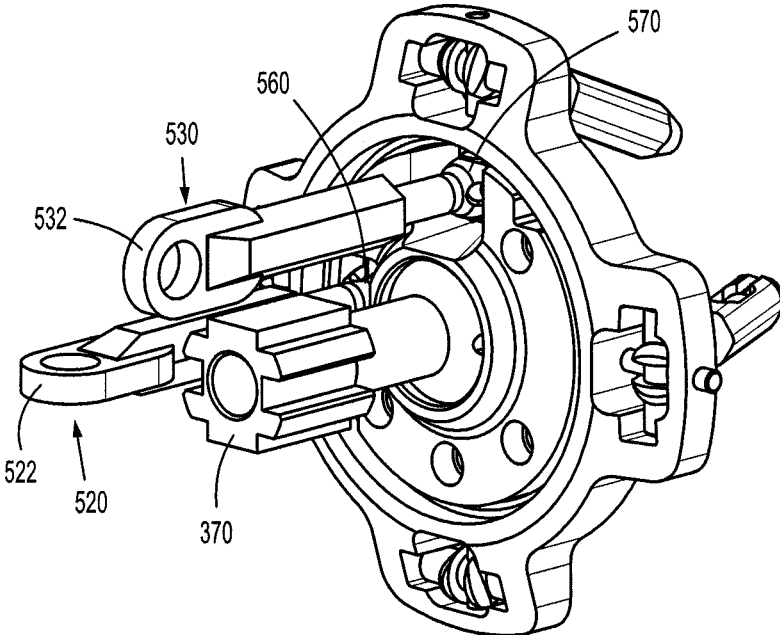


FIG. 8

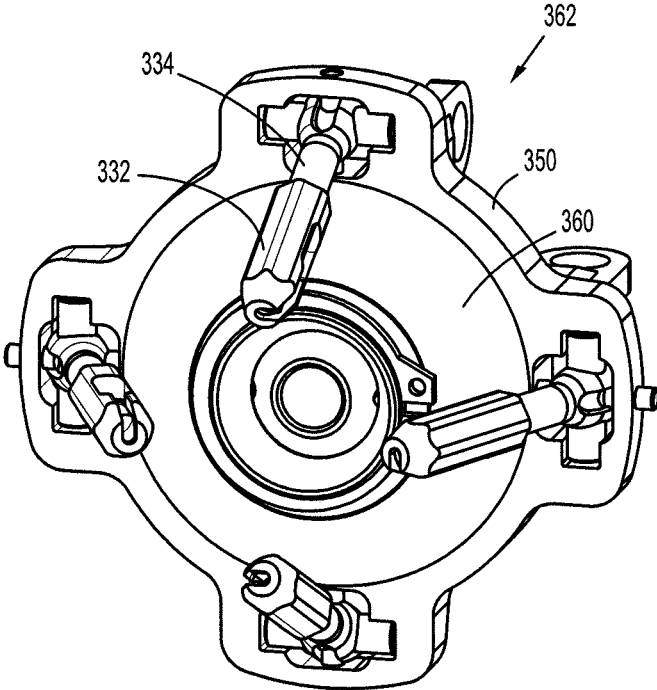


FIG. 9

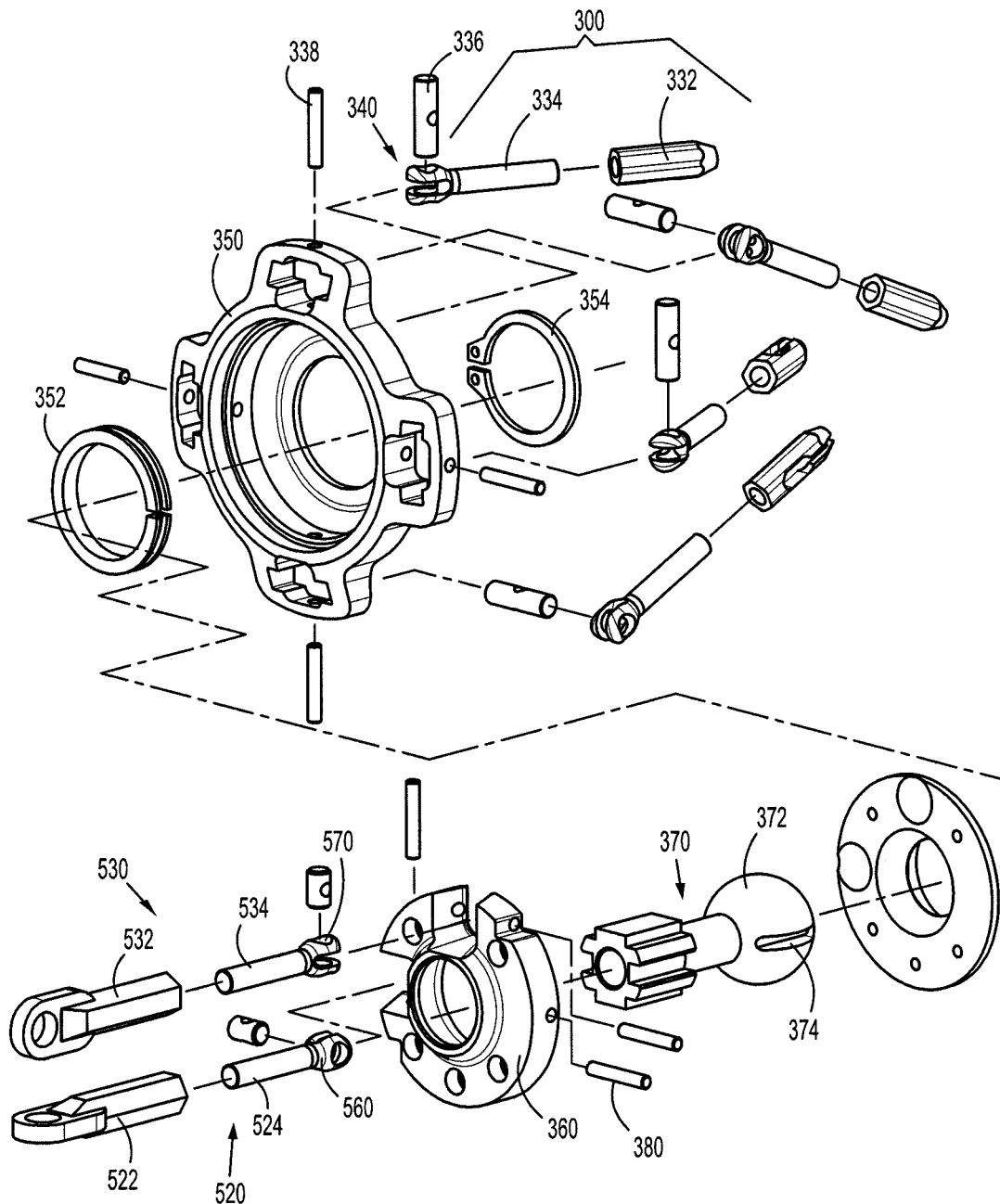


FIG. 10

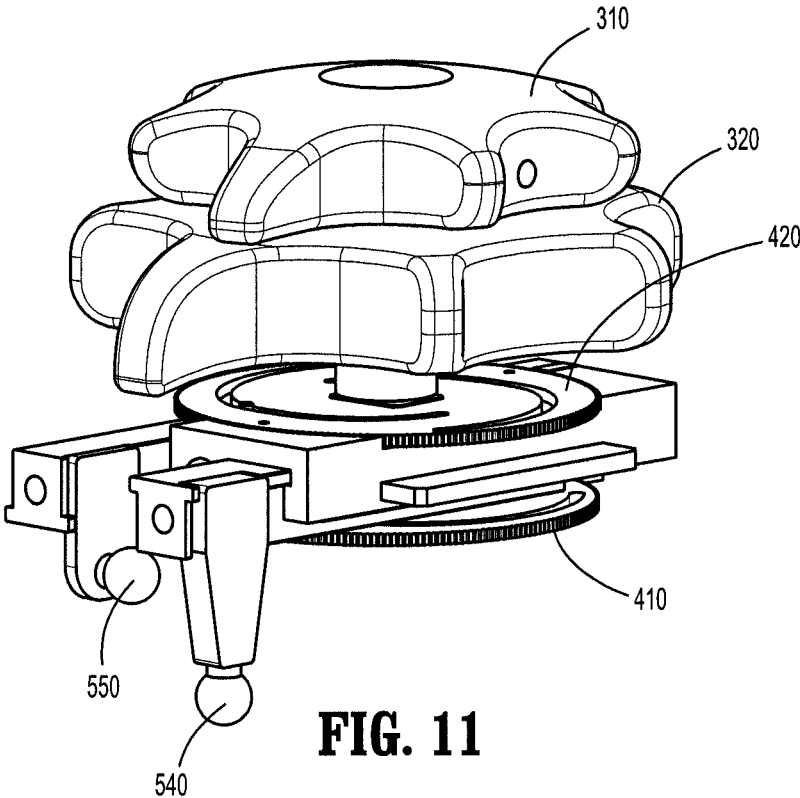


FIG. 11

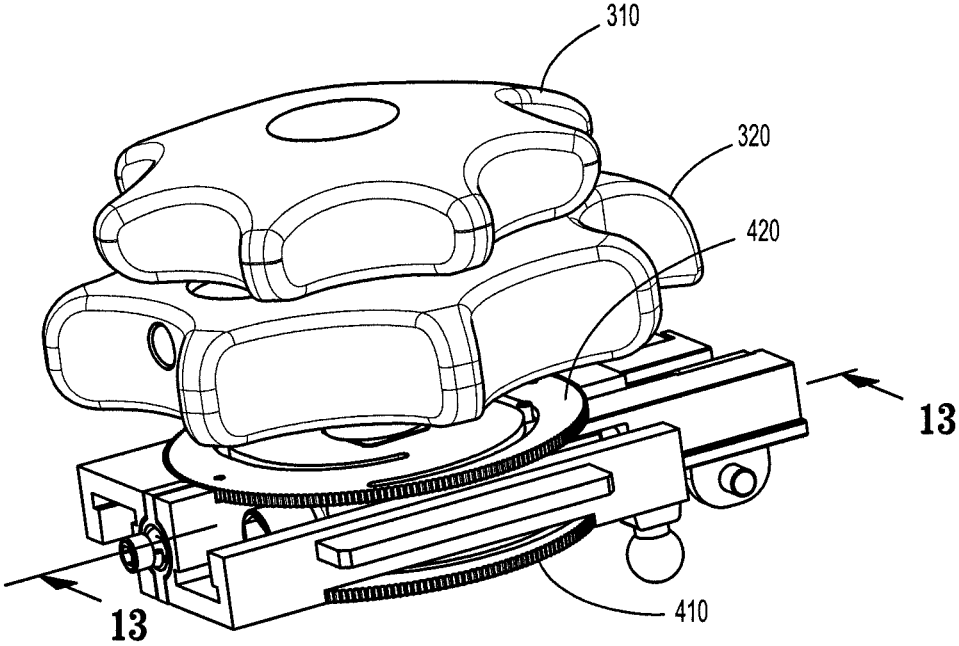


FIG. 12

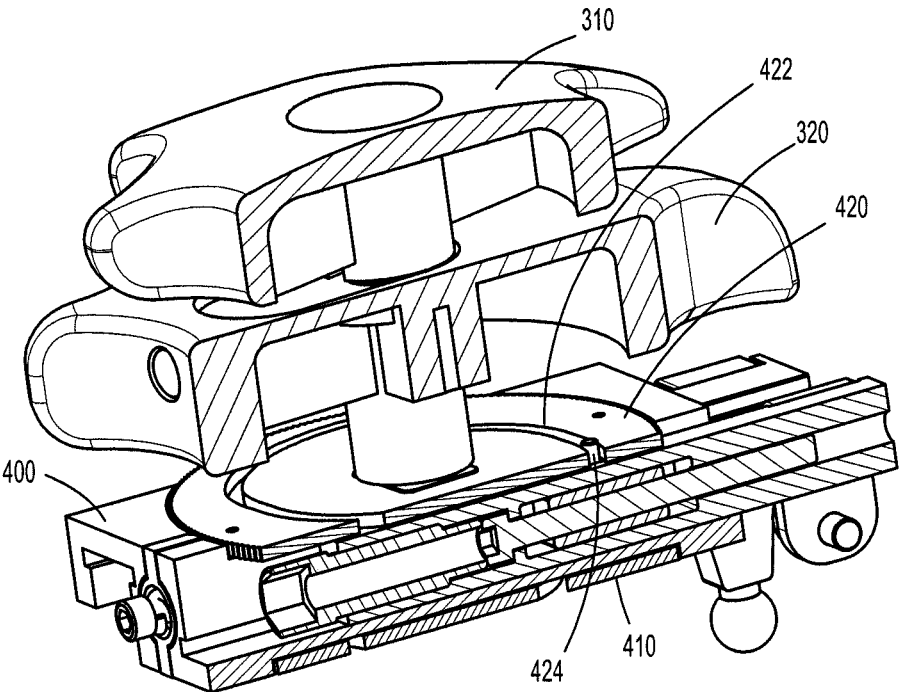


FIG. 13

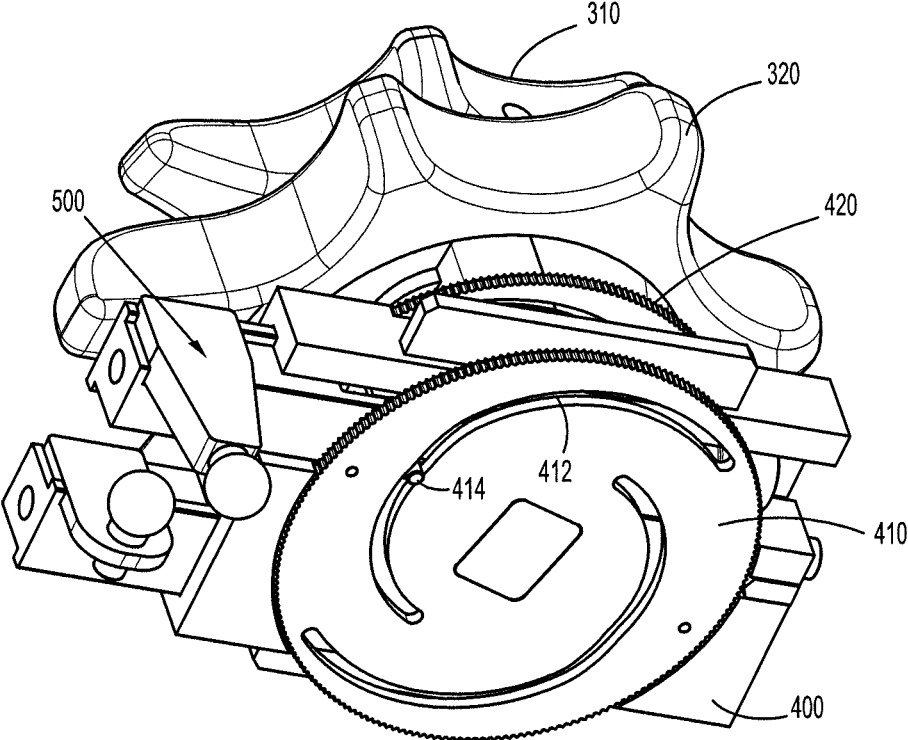
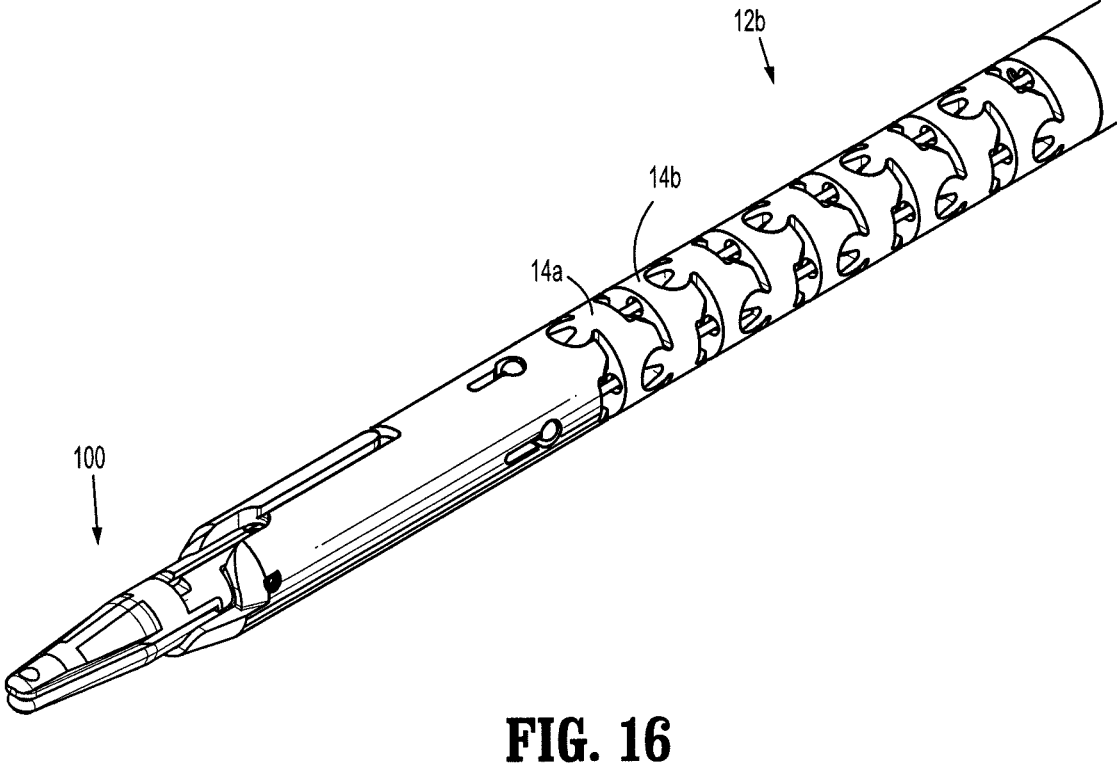
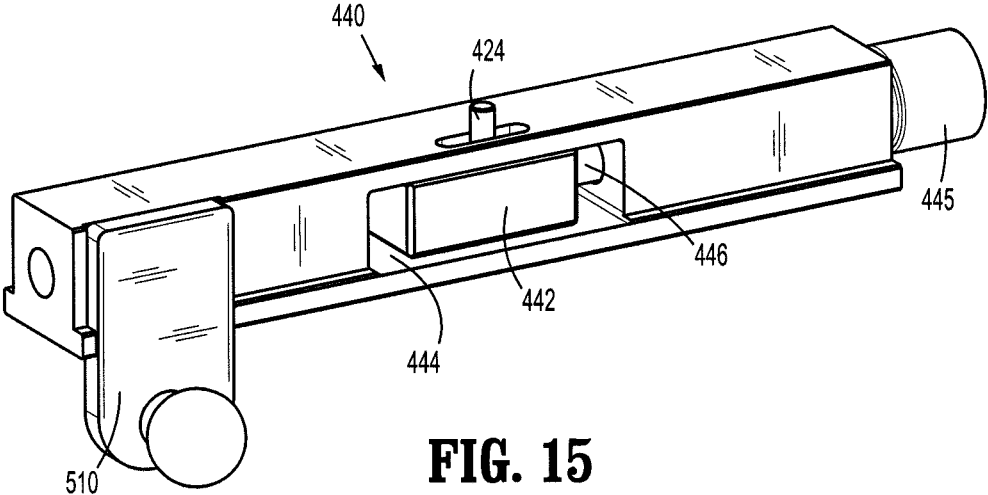
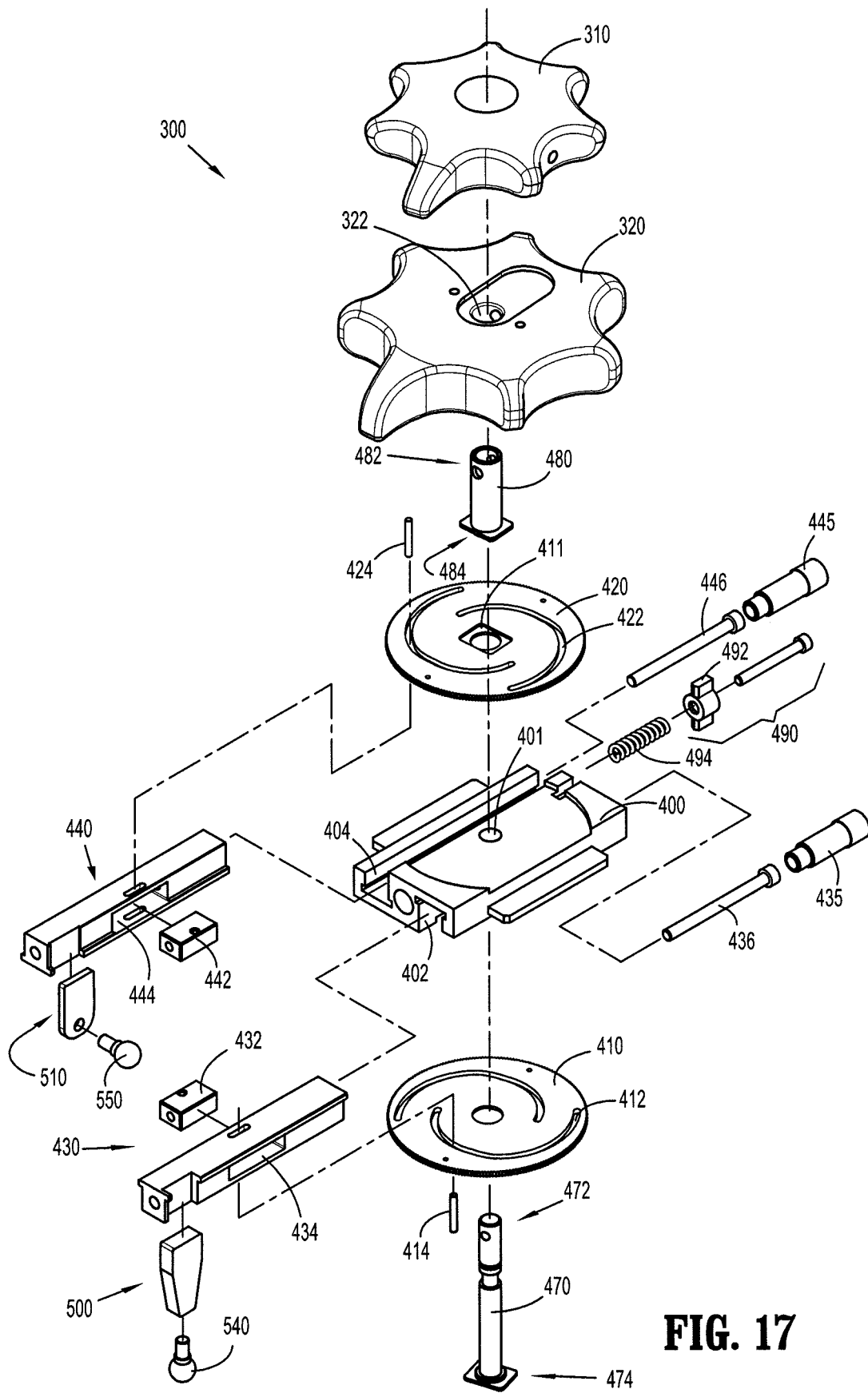


FIG. 14





**FIG. 17**

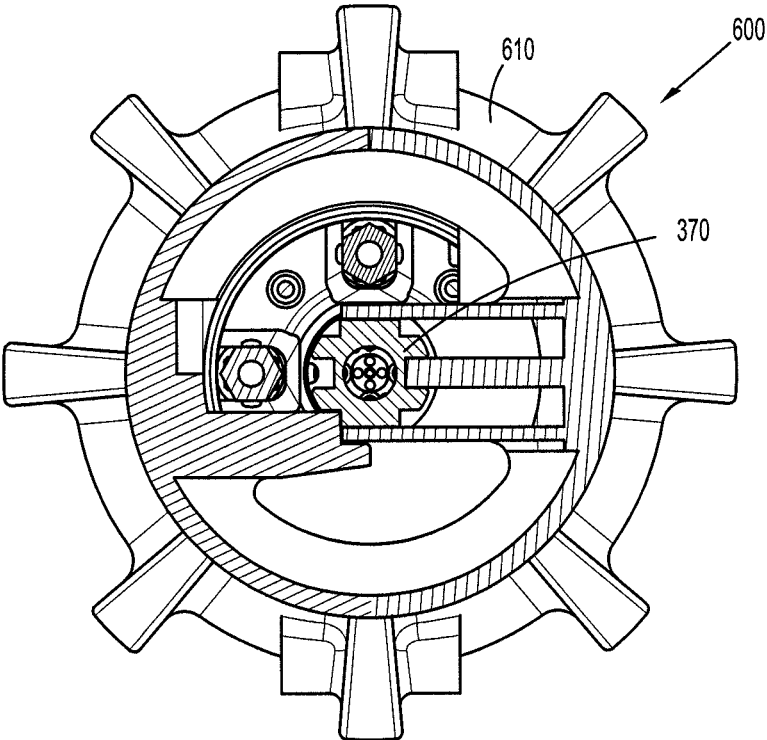


FIG. 18

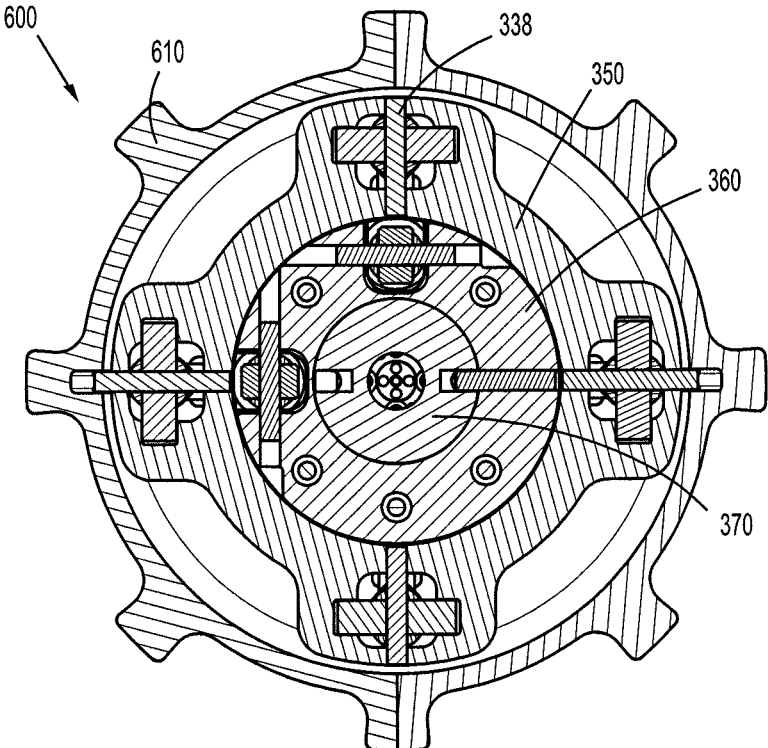


FIG. 19



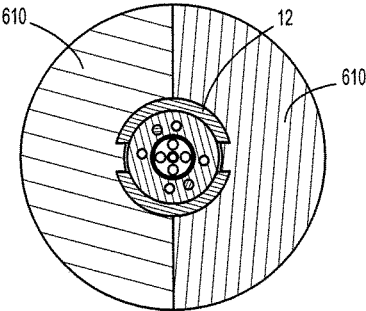


FIG. 20

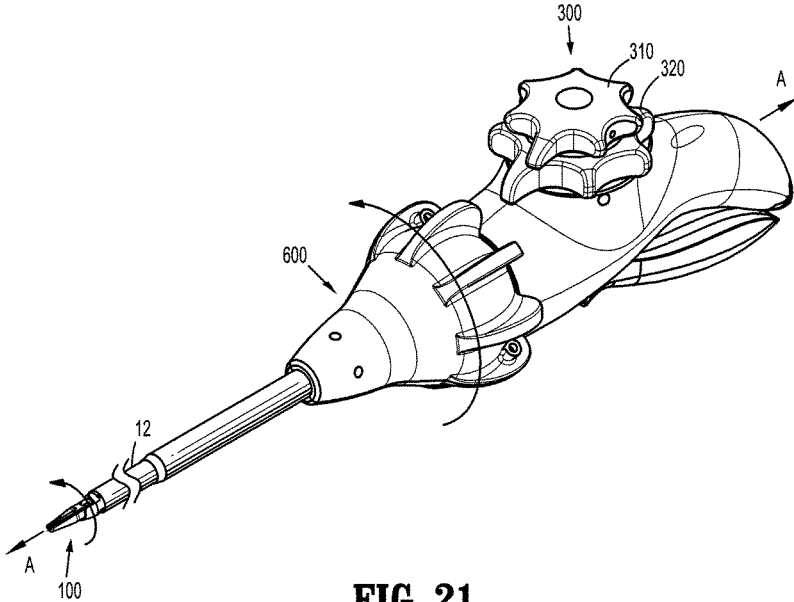


FIG. 21

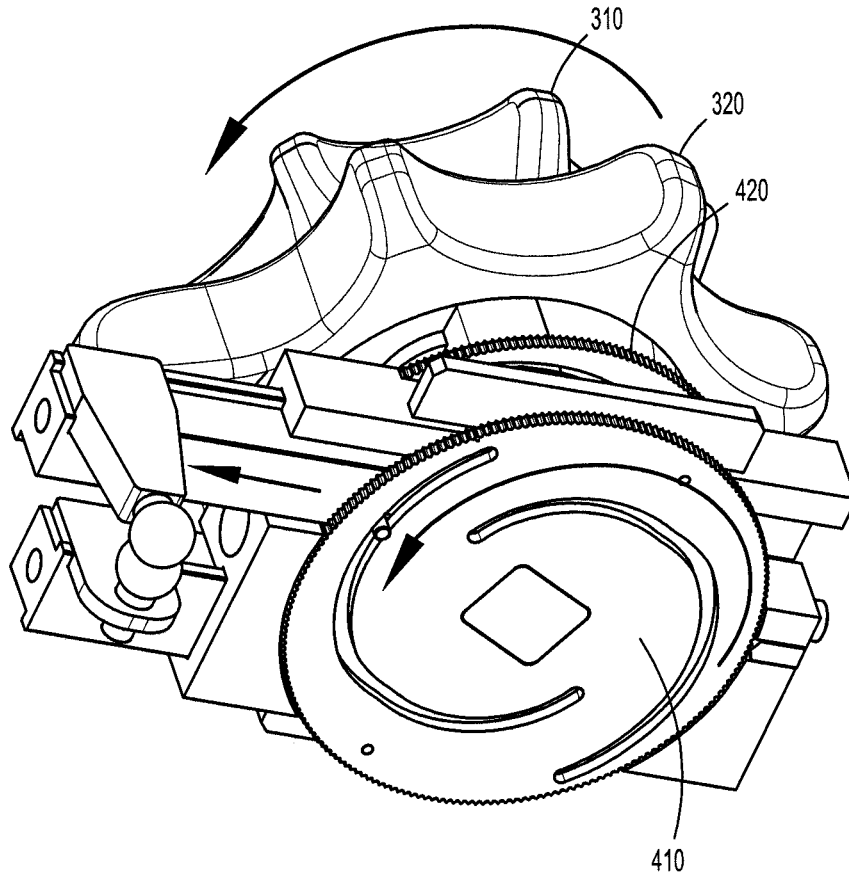


FIG. 22

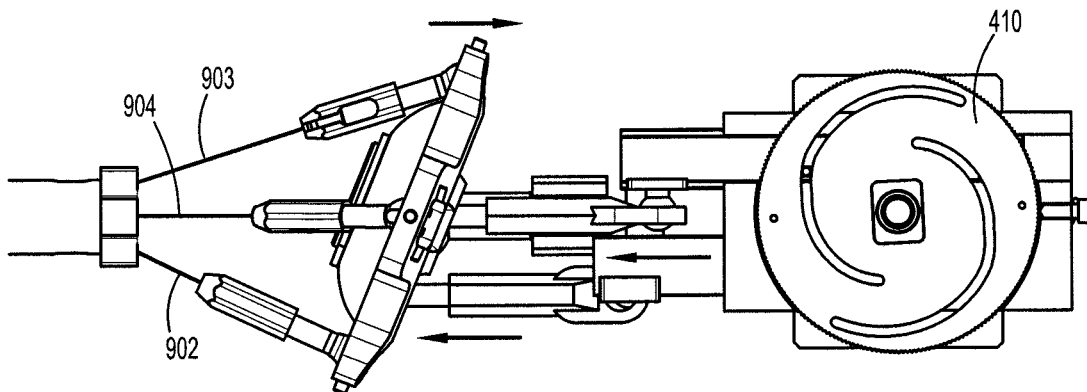


FIG. 23

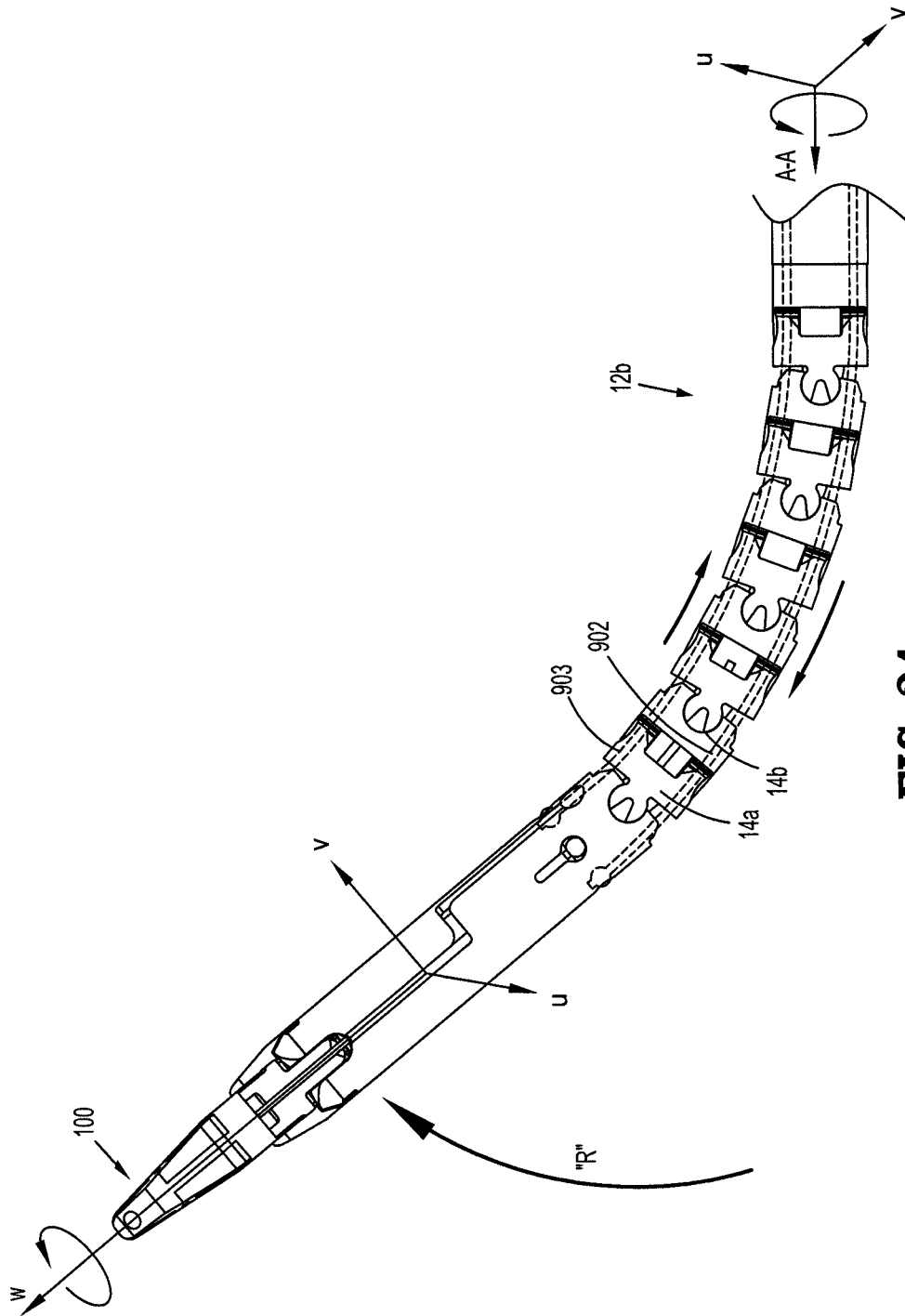


FIG. 24

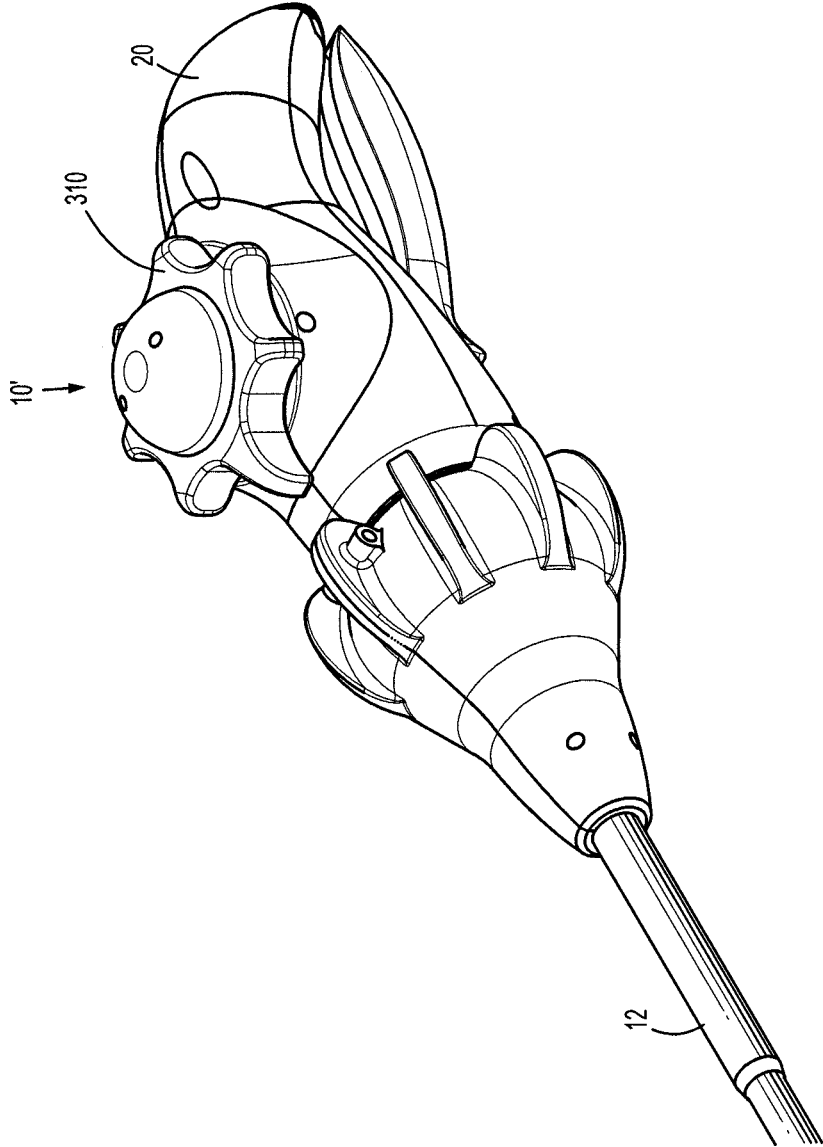


FIG. 25

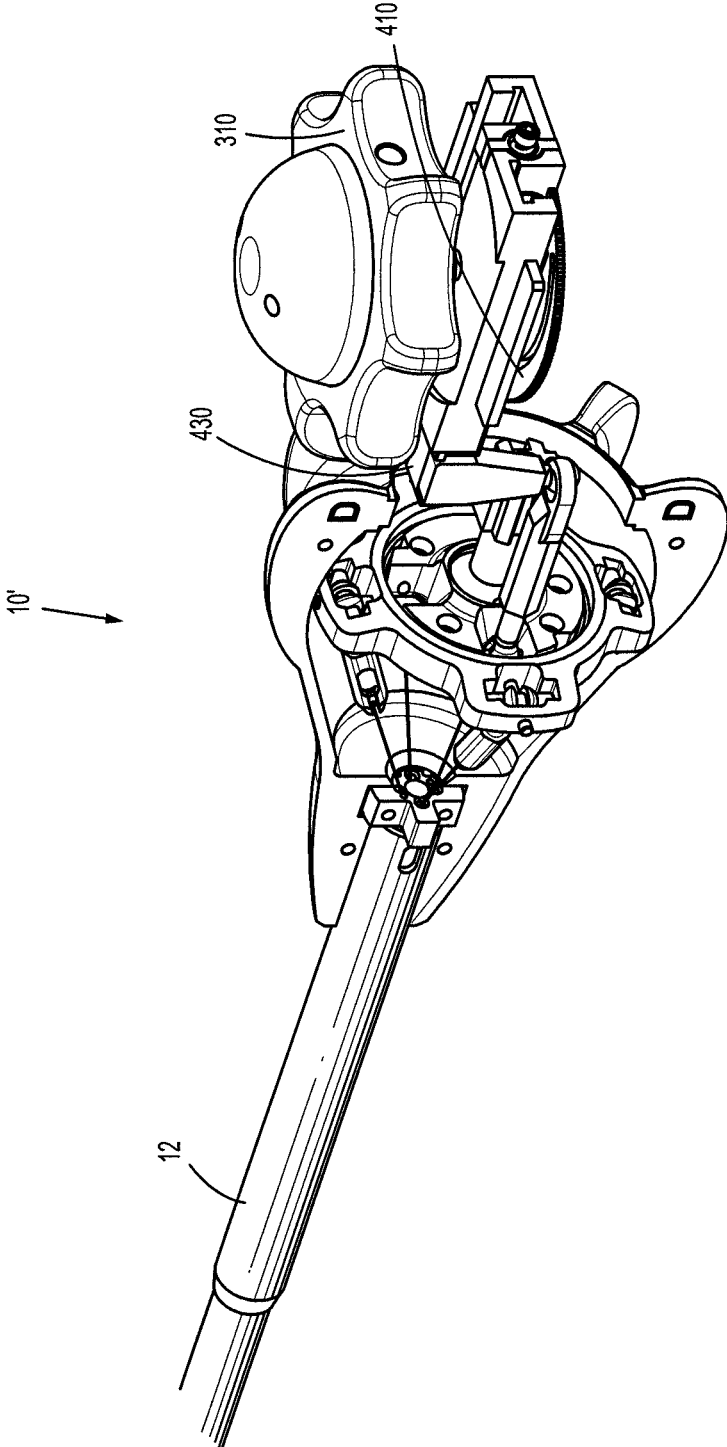


FIG. 26

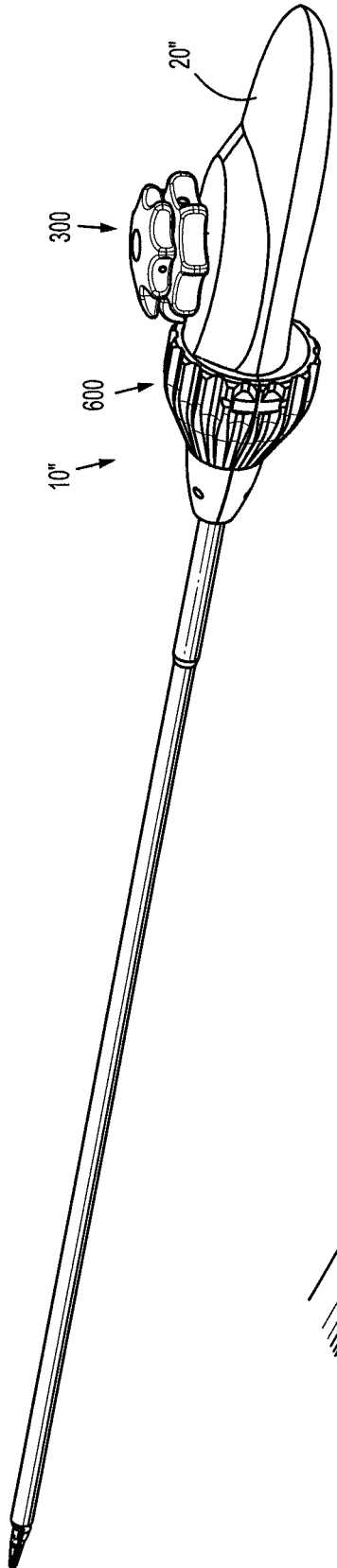


FIG. 27

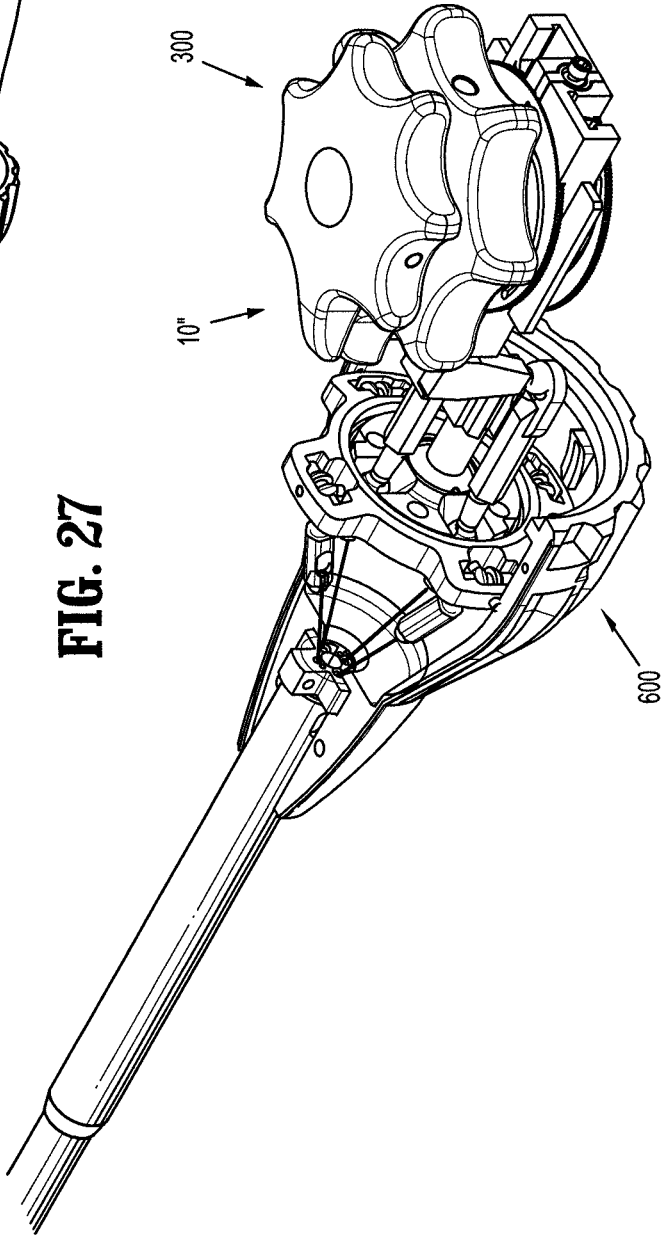


FIG. 28

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## SURGICAL DEVICE WITH ARTICULATION AND WRIST ROTATION

### CROSS-REFERENCE TO RELATED APPLICATIONS

This present application is a divisional of U.S. patent application Ser. No. 15/422,636 filed Feb. 2, 2017, which issued as U.S. Pat. No. 10,448,964, which is a continuation of U.S. patent application Ser. No. 13/543,931 filed on Jul. 9, 2012, now abandoned, which claims benefit of and priority to U.S. Provisional Application No. 61/505,604, filed Jul. 8, 2011, and the disclosures of each of the above-identified applications are hereby incorporated by reference in their entirety.

### BACKGROUND

The present disclosure relates to a device for surgically manipulating tissue. More particularly, the present disclosure relates to a device for surgically joining and/or cutting tissue utilizing an elongated, generally flexible and articulating shaft.

### TECHNICAL FIELD

Various types of surgical instruments used to surgically join tissue are known in the art, and are commonly used, for example, for closure of tissue or organs in transection, resection, anastomoses, for occlusion of organs in thoracic and abdominal procedures, and for electrosurgically fusing or sealing tissue.

One example of such a surgical instrument is a surgical stapling instrument, which may include an anvil assembly, a cartridge assembly for supporting an array of surgical staples, an approximation mechanism for approximating the cartridge and anvil assemblies, and a firing mechanism for ejecting the surgical staples from the cartridge assembly.

Using a surgical stapling instrument, it is common for a surgeon to approximate the anvil and cartridge members. Next, the surgeon can fire the instrument to emplace staples in tissue. Additionally, the surgeon may use the same instrument or a separate instrument to cut the tissue adjacent or between the row(s) of staples.

Another example of a surgical instrument used to surgically join tissue is an electrosurgical forceps, which utilize both mechanical clamping action and electrical energy to effect hemostasis by heating the tissue and blood vessels to coagulate, cauterize and/or seal tissue. As an alternative to open forceps for use with open surgical procedures, many modern surgeons use endoscopes and endoscopic instruments for remotely accessing organs through smaller, puncture-like incisions. As a direct result thereof, patients tend to benefit from less scarring and reduced healing time.

### SUMMARY

The present disclosure relates to a surgical instrument comprising a handle assembly, an elongated shaft, an end effector, a rotation mechanism, and an articulation mechanism. The rotation mechanism is disposed in mechanical cooperation with the handle assembly and effects rotation of the end effector about the second longitudinal axis. The articulation mechanism is disposed in mechanical cooperation with the handle assembly and effects movement of the end effector from a first position where the first longitudinal axis is substantially aligned with the second longitudinal

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axis to a second position where the second longitudinal axis is displaced from the first longitudinal axis. The articulation mechanism comprises a first articulation control disposed in mechanical cooperation with the handle assembly, a first cable and a second cable. Actuation of the first articulation control in a first direction causes the first cable to move distally and causes the second cable to move proximally.

### BRIEF DESCRIPTION OF THE DRAWINGS

Various embodiments of the presently disclosed surgical instrument are described herein with reference to the drawings wherein:

FIG. 1 is a perspective view of an endoscopic forceps depicting a handle assembly, a flexible shaft, an articulation assembly, a rotation assembly, and an end effector assembly according to the present disclosure;

FIG. 2 is a cross-sectional view of the handle assembly, the articulation assembly and a portion of the rotation assembly taken along line 2-2 of FIG. 1;

FIG. 3 is a partial perspective, partial cross-sectional view of the features shown in FIG. 2;

FIGS. 4 and 5 are perspective views of the articulation assembly of FIGS. 1-3;

FIG. 6 is a perspective view of a portion of the articulation assembly and a portion of the rotation assembly taken along line 6-6 of FIG. 1;

FIG. 7 is an assembly view of the forceps of FIG. 1;

FIGS. 8 and 9 are perspective views of a portion of the articulation assembly of the present disclosure;

FIG. 10 is an assembly view of the portion of the articulation assembly of FIGS. 8 and 9;

FIGS. 11-14 are perspective views of another portion of the articulation assembly;

FIG. 15 is a perspective view of a slider of the articulation mechanism of the present disclosure;

FIG. 16 is a perspective view of the area of detail illustrated in FIG. 1;

FIG. 17 is an assembly view of a portion of the articulation assembly of the present disclosure;

FIGS. 18-20 are cross-sectional views of portions of the articulation assembly and the rotation assembly of the present disclosure;

FIG. 21 is a perspective view of the forceps of the present disclosure;

FIGS. 22 and 23 are views of a portion of the articulation assembly of the present disclosure;

FIG. 24 illustrates an articulated distal end of the forceps of the present disclosure;

FIG. 25 is a perspective view of a handle portion of a second embodiment of the disclosed forceps;

FIG. 26 is a perspective view of the handle portion of FIG. 25 with portions of the handle assembly removed;

FIG. 27 is a perspective view of forceps according to a third embodiment of the present disclosure; and

FIG. 28 is a perspective view of the handle portion of FIG. 27 with portions of the handle assembly removed.

### DETAILED DESCRIPTION

Referring initially to FIG. 1, one embodiment of an endoscopic vessel sealing forceps is depicted generally as 10. In the drawings and in the descriptions which follow, the term "proximal," as is traditional, will refer to the end of the forceps 10 which is closer to the user, while the term "distal" will refer to the end which is farther from the user. The forceps 10 comprises a housing 20, an end effector assembly

100 and an elongated shaft 12 extending therebetween to define a longitudinal axis A-A. A handle assembly 200, an articulation assembly 300 including two articulation controls 310 and 320, and a rotation assembly 600 are operable to control the end effector assembly 100 to grasp, seal and divide tubular vessels and vascular tissue. Although the forceps 10 is configured for use in connection with bipolar surgical procedures, various aspects of the present disclosure may also be employed for monopolar surgical procedures. Additionally, while the figures depict a certain type of a forceps, other types of forceps and other endoscopic surgical instruments are encompassed by the present disclosure. Further details of endoscopic forceps are described in commonly-owned U.S. Patent Publication No. 2010/0179540 to Marczyk et al., and U.S. patent application Ser. No. 12/718,143 to Marczyk et al., the entire contents of each of which are hereby incorporated by reference herein

Further details of an endoscopic surgical stapling instrument including surgical fasteners are described in commonly-owned U.S. Pat. No. 6,953,139 to Milliman et al., the entire contents of which are hereby incorporated by reference herein.

Generally, handle assembly 200 includes a fixed handle 210 and a movable handle 220. The fixed handle 210 is integrally associated with the housing 20, and the movable handle 220 is movable relative to fixed handle 210 to induce relative movement between a pair of jaw members of the end effector assembly 100. The movable handle 220 is operatively coupled to the end effector assembly 100 via a drive rod or a flexible drive rod (not explicitly shown in the accompanying figures), which extends through the elongated shaft 12, and reciprocates to induce movement in the jaw members. The movable handle 220 may be approximated with fixed handle 210 to move the jaw members from an open position wherein the jaw members are disposed in spaced relation relative to one another, to a clamping or approximated position wherein the jaw members cooperate to grasp tissue therebetween. Electrosurgical energy may be transmitted through tissue grasped between jaw members to effect a tissue seal. Further details of these components and various other components of the disclosed forceps are disclosed in the references that have incorporated in detail above.

Elongated shaft 12 of forceps 10 includes a distal end 16 dimensioned to mechanically engage the end effector assembly 100 and a proximal end 14, which mechanically engages the housing 20. The elongated shaft 12 includes two portions: a proximal portion 12a defining a proximal shaft axis B-B and a distal portion 12b defining a distal shaft axis C-C.

The proximal portion 12a of the shaft 12 may exhibit various constructions. For example, the proximal portion 12a may be formed from a substantially rigid tube, from flexible tubing (e.g., plastic), or the proximal portion 12a may be formed as a composite of a flexible tube and a rigidizing element, such as a tube of braided steel, to provide axial (e.g., compressional) and rotational strength. In other embodiments, the proximal portion 12a may be constructed from a plastically deformable material.

The distal portion 12b of shaft 12 includes an exterior casing or insulating material disposed over a plurality of links 14a, 14b, etc. (see FIGS. 16 and 24; hereinafter "links 14"). The links 14 are configured to pivot relative to one another to permit the distal portion 12b of the shaft 12 to articulate relative to the proximal shaft axis B-B. In one embodiment, the links 14 are nestingly engaged with one another to permit pivotal motion of the distal portion 12b in two orthogonal planes in response to movement of articu-

lation controls 310 and 320. The links 14 may be shaped to permit the distal portion 12b of the shaft 12 to be self-centering, or to have a tendency to return to an unarticulated configuration.

Articulation assembly 300 sits atop housing 20 and is operable via articulation controls 310 and 320 to move the end effector assembly 100 (and the articulating distal portion 12b of the shaft 12) in the direction of arrows "U, D" and "R, L" relative to axis proximal shaft axis B-B as explained in more detail below.

The links 14 each include a central lumen extending longitudinally therethrough. The central lumen permits passage of various actuators, including a drive rod, a knife rod and four steering cables 901, 902, 903 and 904 (e.g., FIG. 4) through the elongated shaft 12.

The four steering cables 901-904 may be substantially elastic and slideably extend through elongated shaft 12. A distal end of the each of the steering cables 901-904 is mechanically engaged with the end effector 100. Proximal ends of the steering cables 901-904 are operatively coupled to the articulation controls 310, 320 as described below.

Referring now to FIGS. 2-6 the articulation assembly 300 permits selective articulation of the end effector assembly 100 to facilitate the manipulation and grasping of tissue. More particularly, the two controls 310 and 320 include selectively rotatable wheels, 311 and 321, respectively, that sit atop the housing 20. Each wheel, e.g., wheel 311, is independently moveable relative to the other wheel, e.g., 321, and allows a user to selectively articulate the end effector assembly 100 in a given plane of articulation relative to the longitudinal axis A-A. For example, rotation of wheel 311 articulates the end effector assembly 100 along arrows R, L (or right-to-left articulation) by inducing a differential tension and a corresponding motion in steering cables 902 and 903. Similarly, rotation of wheel 321 articulates the end effector assembly along arrows U, D (or up-and-down articulation) by inducing a differential tension and a corresponding motion in steering cables 901 and 904.

The articulation assembly 300 and the rotation assembly 600, comprise the articulating-rotating mechanism and include wheels 311 and 321, and a rotation knob 610 to effect articulation and/or rotation of the end effector 100. Details regarding the various components of the articulating-rotating mechanism are described in detail below.

Distal ends of cables 901-904 are disposed in mechanical engagement with end effector 100, and travel proximally through shaft 12, as described above. Proximal ends of cables 901-904 are disposed in mechanical cooperation with post assemblies 330a-330d, respectively. Each post assembly 330 includes a sleeve 332, which is disposed at least partially around a post 334 (see FIGS. 9 and 10). It is envisioned that the sleeves 332 and the posts 334 are threadably engaged with each other to allow the tension of the cables to be adjusted.

With particular reference to FIGS. 9 and 10, an outer disc 350 and an inner disc 360 comprise a disc assembly 362. Each post 334 is connected to outer disc 350 via pins 336, 338 and a ball joint 340. The interaction between the posts 334 and the outer disc 350 allow the posts 334 to swivel about pins 336, 338 with respect to outer disc 350. Outer disc 350 radially surrounds inner disc 360 and is rotatable around inner disc 360. That is, a series of bearings 352 and clips 354 are disposed between inner disc 360 and outer disc 350 to enable outer disc 350 to rotate with respect to inner disc 360. Additionally, as shown in FIG. 6, an outer portion of pins 338 engages a groove 612 in rotation knob 610. Thus, as rotation knob 610 rotates, outer disc 350, post



assemblies **330**, and cables **901-904** also rotate, which causes end effector **100** to rotate around longitudinal axis A-A (or around the w-axis as discussed below with reference to FIG. 24).

The inner disc **360** is connected to housing **20** via a connector **370**. More particularly, inner disc **360** is connected to a distal portion of connector **370** via a ball-joint connection **372**, and connector **370** is stationary with respect to housing **20**. Additionally, connector **370** is hollow, such that portions of elongated mechanisms (e.g., firing rod, knife rod, etc.) can be advanced between housing **20** and shaft **12**. Such elongated mechanisms are not illustrated in the accompanying figures in the interest of visual clarity.

A pin **380** engages both ball-joint connection **372** and inner disc **360**. An outer portion of pin **380** engages inner disc **360**, and an inner portion of pin **380** engages a slot **374** within ball-joint connection **372** (see FIG. 6). This connection results in inner disc **360** being able to rotate with respect to the X- and Z-axes, but unable to rotate with respect to the longitudinal axis A-A. The orientation of inner disc **360** and outer disc **350** results in outer disc **350** rotating with inner disc **360** around the X- and Z-axes. Additionally, as discussed above, outer disc **350** is also able to rotate around the longitudinal axis A-A when driven by rotation knob **610**.

Referring now to FIG. 17, for example, articulation assembly **300** also includes a block **400**, a first disc **410**, a second disc **420**, a first slider **430**, and a second slider **440**. First articulation control **310** is connected to first disc **410** via a first post **470**; second articulation control **320** is connected to second disc **420** via a second post **480**. More particularly, an upper portion **472** of first post **470** is mechanically coupled to first articulation control **310** (e.g., via a pin), and a lower portion **474** of first post **470** is mechanically coupled to first disc **410**. An upper portion **482** of second post **480** is mechanically coupled to second articulation control **320** (e.g., via a pin), and a lower portion **484** of second post **480** is mechanically coupled to second disc **420**. As shown in FIG. 17, lower portions **474**, **484** of posts **470**, **480** may include a polygonal-shape (e.g. a square) that is dimensioned to fit within a corresponding recess **411** in the corresponding disc **410**, **420** (the lower portion of first disc **410** is not shown). Additionally, an outer diameter of first post **470** is smaller than an inner diameter of second post **480**, thus enabling first post **470** to extend through second post **480**. First post **470** also extends through an opening **401** in block **400** and an opening **322** in first disc **320**. As such, rotation of first articulation control **310** causes rotation of first disc **410**, and rotation of second articulation control **320** causes rotation of second disc **420**.

Each disc **410**, **420** has at least one arcuate slot **412**, **422** therein. In the illustrated embodiments, discs **410**, **420** each include two slots. In this embodiment, discs **410**, **420** are identical to each other (and flipped about the Z-axis (FIG. 6) with respect to each other), e.g., to facilitate manufacturing. Following pins **414**, **424** extend through respective slots **412**, **422**, and are coupled to respective sliders **430**, **440**. The location of following pins **414**, **424** can be adjusted within respective sliders **430**, **440** by the mechanisms illustrated in FIGS. 15 and 17. More particularly, sliders **430**, **440** each include a slidable block **432**, **442** connected to respective pins **414**, **424**, and which are slidable within a cavity **434**, **444**. Proximal screws **435**, **445** threadably engage sliders **430**, **440**, and each about a respective distal screw **436**, **446**. Distal screws **436**, **446** extend through and threadably engage respective slidable blocks **432**, **442**, such that rotation of proximal screws **435**, **445** causes translation of respective slidable blocks **432**, **442**, and thus pins **414**, **424**.

Additionally, sliders **430**, **440** slidably engage longitudinal slots **402**, **404**, respectively, in block **400**. As such, rotation of articulation control **310** causes rotation of first disc **410**, which causes following pin **414** to move along arcuate slot **412**, which causes slider **430** to move longitudinally through longitudinal slot **402** in block **400**. Likewise, rotation of articulation control **320** causes longitudinal translation of slider **440** with respect to block **400**.

Sliders **430**, **440** are connected to inner disc **360** via a first connecting arms **500**, **510** and second connecting arms **520**, **530**. First connecting arms **500**, **510** downwardly depend from respective sliders **430**, **440** and are connected to second connecting arms **520**, **530**, respectively, via ball joints **540**, **550**. Second connecting arms **520**, **530** include proximal portions **522**, **532** and distal portions **524**, **534**, which are longitudinally translatable (e.g., threaded) with respect to one another to allow the length of second connecting arms **520**, **530** to be adjusted. Second connecting arms **520**, **530** are connected to inner disc **360** via ball joints **560**, **570**. The ball joint **560**, **570** connections allow three-dimensional movement (i.e., about the longitudinal axis A-A and the Y- and Z-axes) of disc assembly **362**. Additionally, as shown in FIG. 5, for example, first connecting arm **520** is radially offset 90° from second connecting arm **530**. That is, in the illustrated embodiment, first connecting arm **520** engages inner disc **360** at a top portion thereof (i.e., in a 12:00 position in FIG. 5), and second connecting arm **530** engages inner disc **360** at a lateral portion thereof (i.e., in a 9:00 position in FIG. 5).

In use, rotation of first articulation control **310** causes first slider **430** to longitudinally translate, which causes a top portion of disc assembly **362** to move distally/proximally. Such movement by the top portion of disc assembly **362** causes upper cable **904** and lower cable **901** to in opposite directions from one another (i.e., one cable moves distally, the other cable moves proximally). When upper cable **904** is moved distally (i.e., produces slack) and lower cable **901** is moved proximally (i.e., produces tension), end effector **100** articulates downwardly, in the substantial direction of arrow "D" in FIG. 1. When upper cable **904** is moved proximally and lower cable **901** is moved distally, end effector **100** articulates upwardly, in the substantial direction of arrow "U" in FIG. 1. As can be appreciated, rotation of second articulation control **302** causes translation of cables **902**, **903** (see FIG. 23), which causes end effector **100** to articulate in the directions of arrows "R" and "L" in FIG. 1.

Further, with particular reference to FIG. 24, when the end effector **100** is articulated in a particular direction and amount (e.g., "R" in FIG. 24), and when coordinate system {u, v, w} is associated with the end effector **100**. FIG. 24 illustrates that rotation of rotation knob **610** about longitudinal axis A-A, causes the end effector **100** to rotate about axis "w"; end effector **100** does not rotate around longitudinal axis A-A. Thus, the end effector **100** maintains its articulation (i.e., its "R" position in FIG. 24) while being able to rotate about the w-axis.

Additionally, in the illustrated embodiments, first disc **410** and second disc **420** include serrations along perimeters thereof. A member **490**, as shown in FIG. 17, includes a distal end **492** that is biased into each disc **410**, **420** via a spring **494**, such that rotation of articulation control **310** and/or **320** causes distal end **492** of member **490** to contact successive serrations, which produces an audible sound to facilitate use.

Another forceps **10'** according to an embodiment of the present disclosure is illustrated in FIGS. 25 and 26. This embodiment includes a single articulation control **310**, a

single disc **410**, and a single slider **430**. In this embodiment, a user can rotate articulation control **310** in addition to the housing **20** for full articulation control of end effector **100**.

FIGS. **27** and **28** illustrate another embodiment of a forceps **10"** having housing **20'**, which is usable with the articulation assembly **300** and rotation assembly **600** of the present disclosure. As illustrated, housing **20'** lacks a movable handle. Here, it is envisioned that any type of actuation mechanism, including powered actuation, is usable with forceps **10"**.

While several embodiments of the disclosure have been depicted in the drawings, it is not intended that the disclosure be limited thereto, as it is intended that the disclosure be as broad in scope as the art will allow and that the specification be read likewise. Therefore, the above description should not be construed as limiting, but merely as exemplifications of particular embodiments. Those skilled in the art will envision other modifications within the scope and spirit of the claims appended hereto.

What is claimed is:

**1.** A surgical instrument comprising:

a handle assembly;

an elongated shaft extending distally from the handle assembly and defining a first longitudinal axis;

an end effector disposed in mechanical cooperation with a distal portion of the elongated shaft, the end effector defining a second longitudinal axis and including a pair of jaw members;

a rotation mechanism disposed in mechanical cooperation with the handle assembly and configured to rotate the pair of jaw members of the end effector about the second longitudinal axis by a rotation of at least a portion of the rotation mechanism about the first longitudinal axis relative to the handle assembly;

an articulation mechanism disposed in mechanical cooperation with the handle assembly and configured to move the end effector from a first position where the first longitudinal axis is aligned with the second longitudinal axis to a second position where the second longitudinal axis is displaced from the first longitudinal axis, the articulation mechanism including:

a first articulation control disposed in mechanical cooperation with the handle assembly;

a second articulation control disposed in mechanical cooperation with the handle assembly, the first articulation control and the second articulation control are independently actuatable with respect to each other;

a first cable, a distal portion of the first cable disposed in mechanical cooperation with the end effector;

a second cable, a distal portion of the second cable disposed in mechanical cooperation with the end effector;

a third cable, a distal portion of the third cable disposed in mechanical cooperation with the end effector; and

a fourth cable, a distal portion of the fourth cable disposed in mechanical cooperation with the end effector;

wherein the first articulation control is actuatable in a first direction to cause the first cable to move distally with respect to the handle assembly and to cause the second cable to move proximally with respect to the handle assembly, and wherein the second articulation control is actuatable in a second direction to cause the third cable to move distally with respect to the

handle assembly and to cause the fourth cable to move proximally with respect to the handle assembly;

a first disc;

a second disc; and

a link mechanism,

wherein proximal portions of the first cable, the second cable, the third cable and the fourth cable are coupled to the first disc, the first disc is rotatable about the first longitudinal axis relative to the handle assembly, and the link mechanism connects the first articulation control and the second articulation control to the second disc.

**2.** The surgical instrument according to claim **1**, wherein the rotation mechanism is configured to rotate the elongated shaft about the first longitudinal axis and relative to the handle assembly.

**3.** The surgical instrument according to claim **1**, wherein the rotation mechanism is configured to rotate the first cable and the second cable about the first longitudinal axis.

**4.** The surgical instrument according to claim **1**, wherein the articulation mechanism further includes a first slider, the second disc disposed in mechanical cooperation with the first articulation control and the first slider disposed in mechanical cooperation with the second disc such that actuation of the first articulation control causes longitudinal translation of the first slider, which causes longitudinal translation of the first cable and the second cable.

**5.** The surgical instrument according to claim **1**, wherein the second position of the end effector remains unchanged in response to actuation of the rotation mechanism.

**6.** The surgical instrument according to claim **1**, wherein the first articulation control includes a first wheel, the second articulation control includes a second wheel, and each of the first and second wheels is selectively and independently rotatable about a rotation axis which is disposed perpendicularly to the first longitudinal axis.

**7.** A surgical instrument comprising:

a handle assembly;

an elongated shaft extending distally from the handle assembly and defining a first longitudinal axis;

an end effector disposed in mechanical cooperation with a distal portion of the elongated shaft, the end effector defining a second longitudinal axis;

a rotation mechanism disposed in mechanical cooperation with the handle assembly and configured to rotate the end effector about the second longitudinal axis by a rotation of at least a portion of the rotation mechanism about the first longitudinal axis relative to the handle assembly; and

an articulation mechanism disposed in mechanical cooperation with the handle assembly and configured to move the end effector from a first position where the first longitudinal axis is aligned with the second longitudinal axis to a second position where the second longitudinal axis is displaced from the first longitudinal axis, the articulation mechanism having:

a first articulation control disposed in mechanical cooperation with the handle assembly;

a second articulation control disposed in mechanical cooperation with the handle assembly, the first articulation control and the second articulation control are independently actuatable with respect to each other;

a first cable, a distal portion of the first cable disposed in mechanical cooperation with the end effector, wherein a proximal portion of the first cable is

coupled to a first disc, the first disc is rotatable about the first longitudinal axis relative to the handle assembly;

a second cable, a distal portion of the second cable disposed in mechanical cooperation with the end effector,

wherein the first articulation control is actuatable in a first direction to cause the first cable to move distally with respect to the handle assembly, and wherein the second articulation control is actuatable in a second direction to cause the second cable to move distally with respect to the handle assembly.

8. The surgical instrument according to claim 7, wherein the first disc is rotatable about a second disc.

9. The surgical instrument according to claim 7, wherein the first disc is rotatable with respect to a second disc and at least a portion of the first disc is disposed at the same longitudinal position along the first longitudinal axis as at least a portion of the second disc.

10. The surgical instrument according to claim 9, wherein the second disc is rotationally fixed about the first longitudinal axis with respect to the handle assembly.

11. The surgical instrument according to claim 9, wherein the second disc defines a passageway between the handle assembly and the elongated shaft.

12. The surgical instrument according to claim 9, further including a link mechanism connecting the first articulation control to the second disc.

13. An articulation mechanism for use with a surgical instrument, the articulation mechanism comprising:

- a first articulation control;
- a second articulation control independently actuatable with respect to the first articulation control;
- a first cable disposed in mechanical cooperation with the first articulation control;
- a second cable disposed in mechanical cooperation with the first articulation control;

- a third cable disposed in mechanical cooperation with the second articulation control;
- a fourth cable disposed in mechanical cooperation with the second articulation control;
- a disc defining a disc axis and disposed in mechanical cooperation with the first articulation control; and
- a slider defining a slider axis and disposed in mechanical cooperation with the disc, the slider axis is parallel to the disc axis, and the disc is rotatable about the disc axis relative to the slider,

wherein the first articulation control is actuatable in a first direction to cause the first cable to move distally with respect to a portion of the first articulation control and to cause the second cable to move proximally with respect to the portion of the first articulation control, and wherein the second articulation control is actuatable in a second direction to cause the third cable to move distally with respect to a portion of the second articulation control and to cause the fourth cable to move proximally with respect to the portion of the second articulation control.

14. The articulation mechanism according to claim 13, wherein the first articulation control is actuatable to cause longitudinal translation of the slider.

15. The articulation mechanism according to claim 14, wherein the slider is longitudinally translatable to cause longitudinal translation of the first cable and the second cable.

16. The articulation mechanism according to claim 13, wherein the first articulation control includes a first wheel, the second articulation control includes a second wheel, and each of the first and second wheels is selectively and independently rotatable about a rotation axis.

17. The articulation mechanism according to claim 16, wherein the rotation axis is perpendicular to an axis defined by the first cable.

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