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(54) **OPENING AND CLOSING DEVICE AND
RESPIRATORY ASSISTANCE DEVICE**

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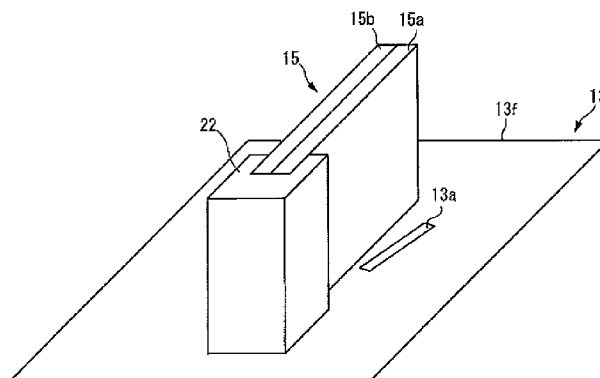
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(57) **ABSTRACT**

A respiratory assistance device **10** includes: a mask **13**
having an expiratory hole **13a**; an expiratory valve **15**
provided in the mask **13**, for opening and closing the
expiratory hole **13a**; and a control unit **17** for performing
overall control on the entire device. The mask **13** and the
expiratory valve **15** together form an opening and closing
device. The expiratory valve **15** is deformable by deforma-
tion of a piezo element **15a**. The expiratory valve **15** is
disposed on an inner surface **13f** so that a deformation
direction thereof, i.e., a thickness direction thereof, extends
(Continued)



along the inner surface 13f of the mask 13 and a side surface 15m slides along the inner surface 13f by the deformation thereof.

11 Claims, 16 Drawing Sheets

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- (52) **U.S. Cl.**
 CPC *A61M 16/20* (2013.01); *A61M 16/202* (2014.02); *F04D 33/00* (2013.01); *F16K 31/006* (2013.01); *A61M 16/0012* (2014.02); *A61M 16/0051* (2013.01); *A61M 2016/0027* (2013.01); *A61M 2016/0039* (2013.01); *A61M 2205/0266* (2013.01); *A61M 2205/0294* (2013.01); *A61M 2205/502* (2013.01); *A61M 2205/52* (2013.01); *F04C 2270/041* (2013.01)

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Fig. 1

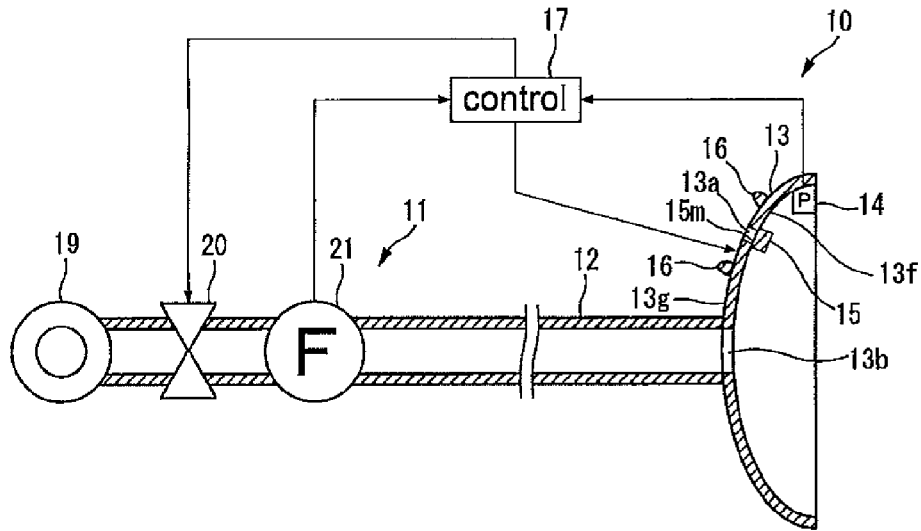


Fig. 2A

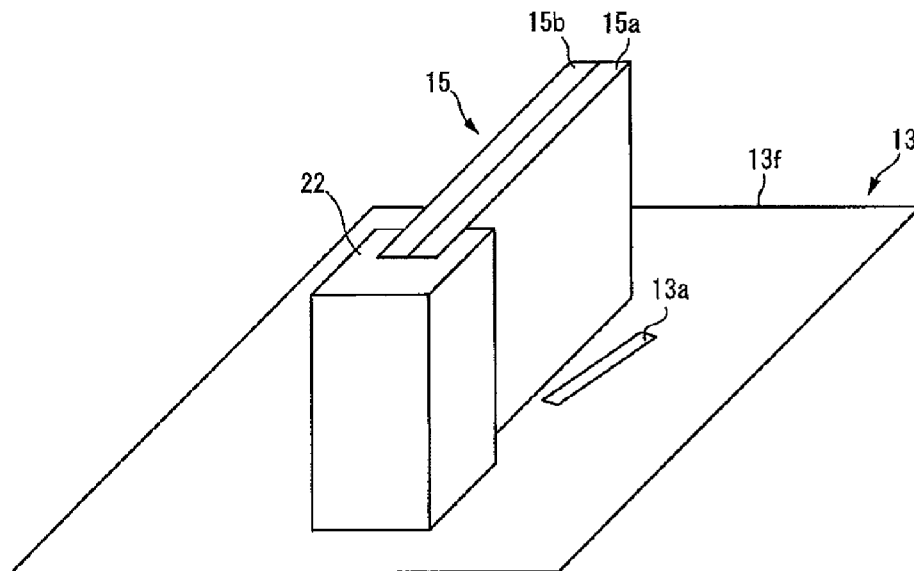


Fig. 2B

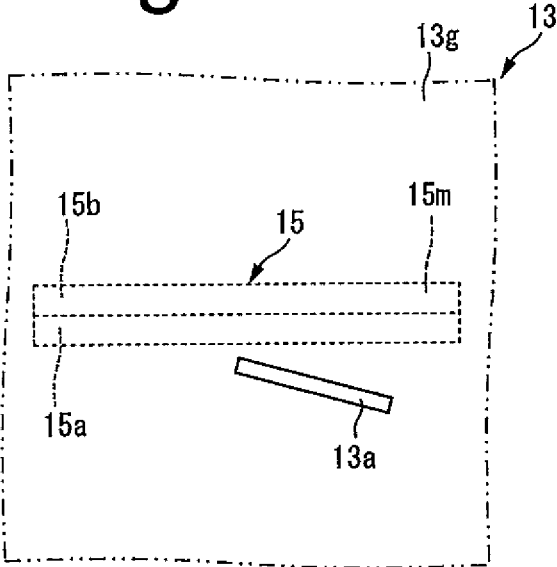


Fig. 2C

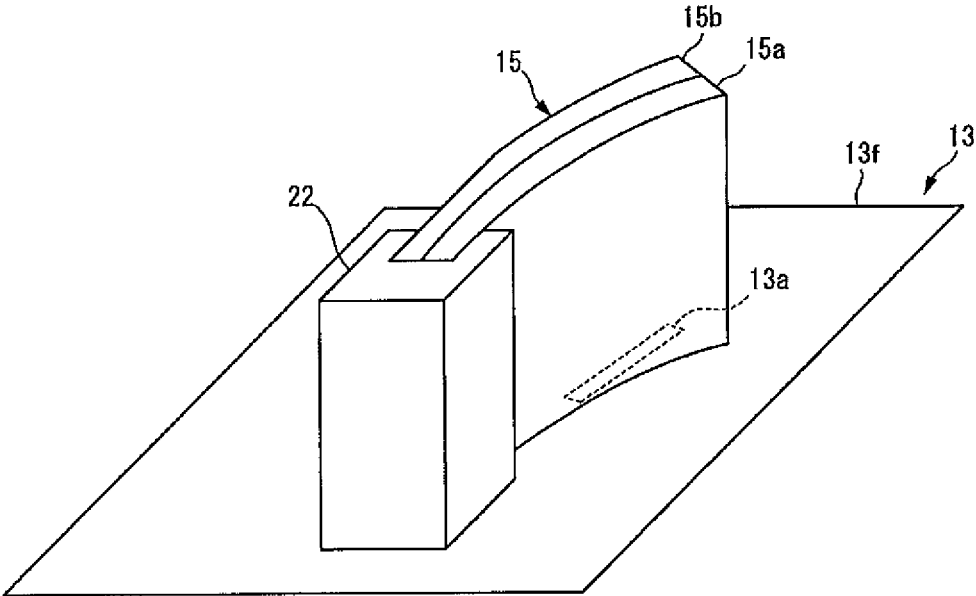


Fig. 2D

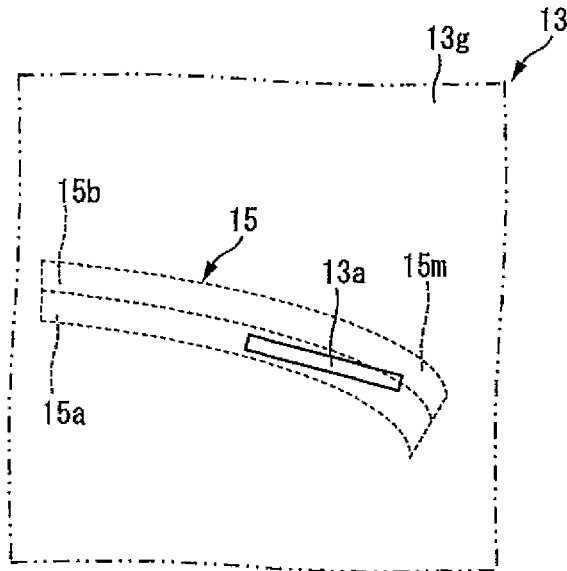


Fig. 3

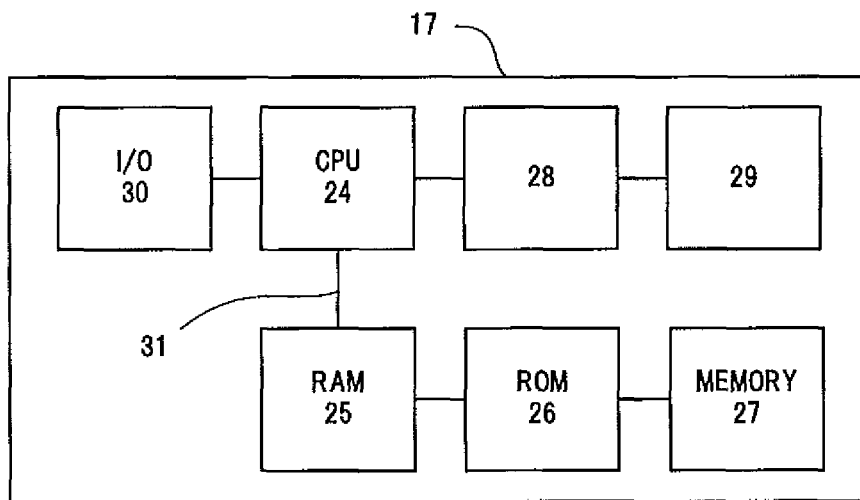


Fig. 4

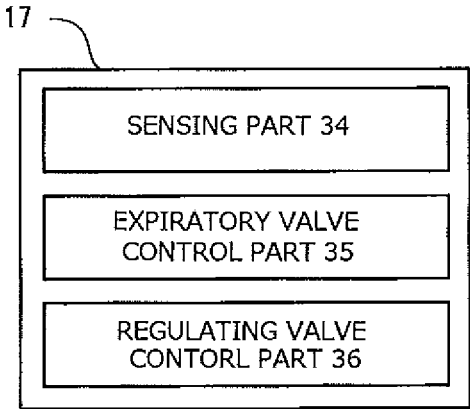
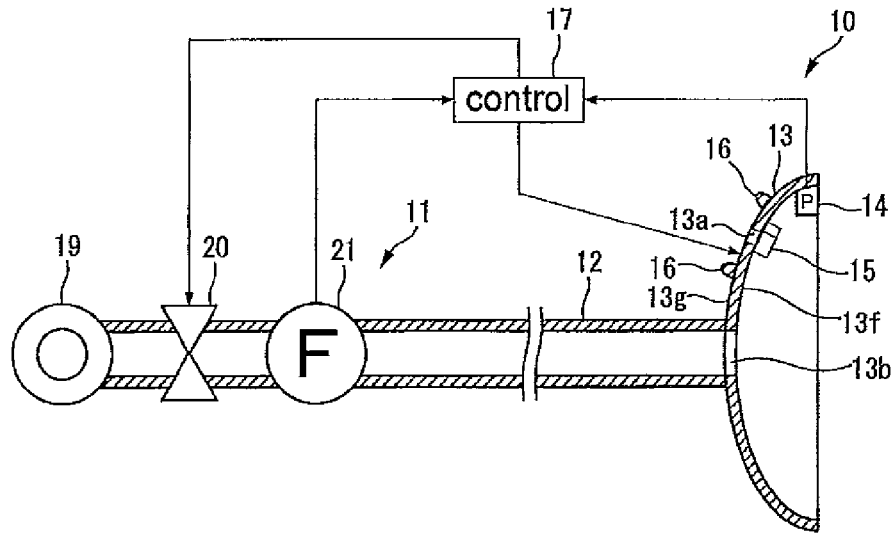


Fig. 5

(A)



(B)

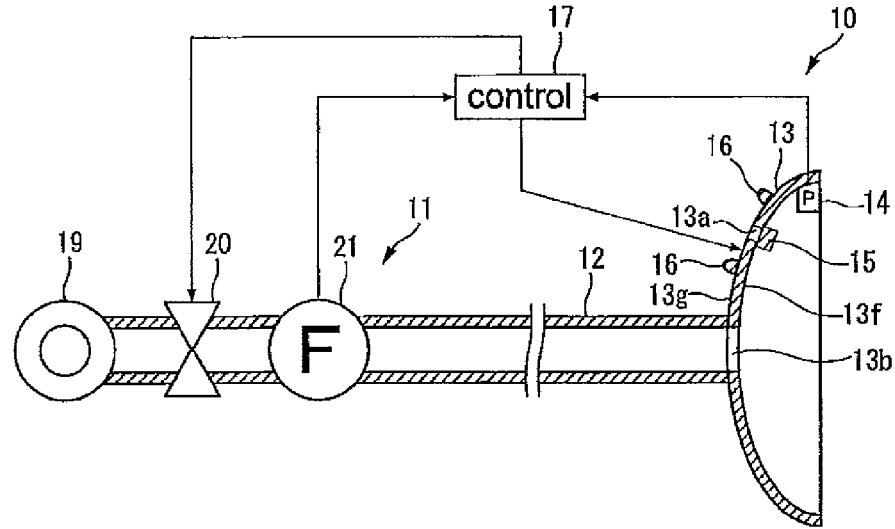


Fig. 6

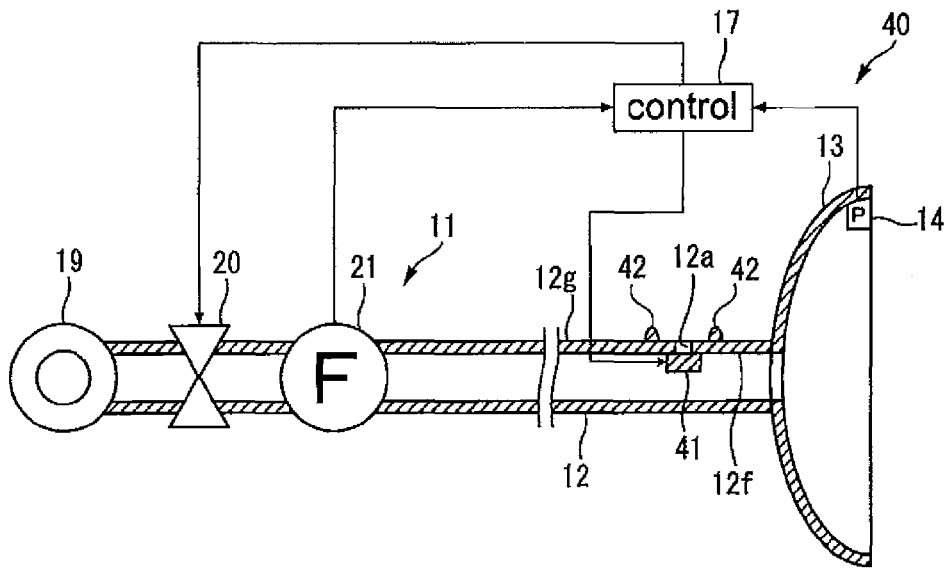


Fig. 7

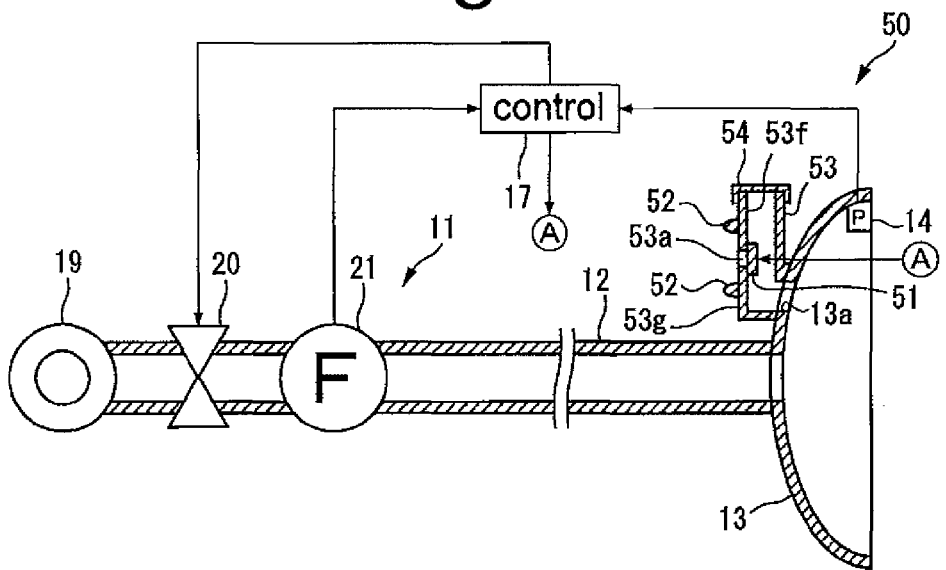


Fig. 8

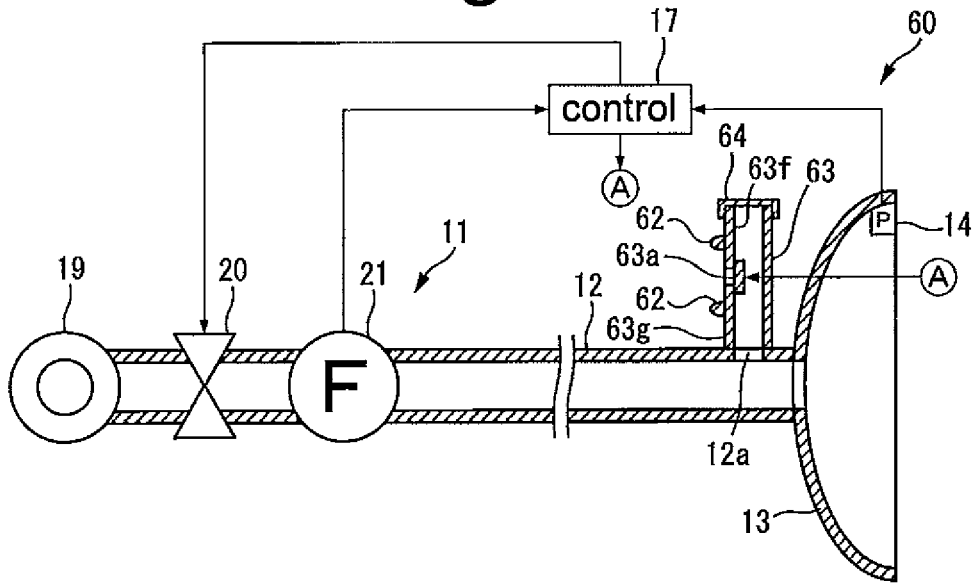


Fig. 9

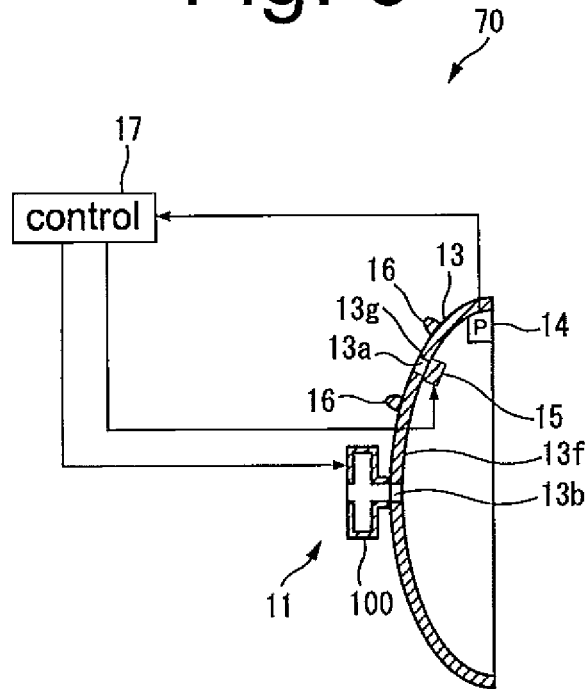


Fig. 10

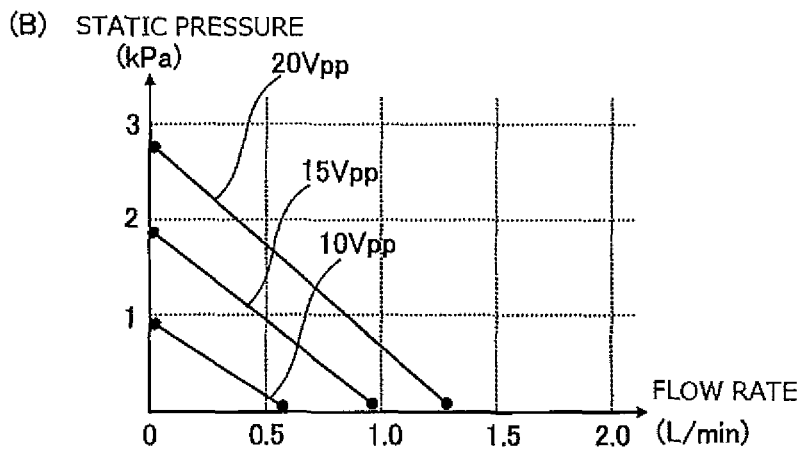
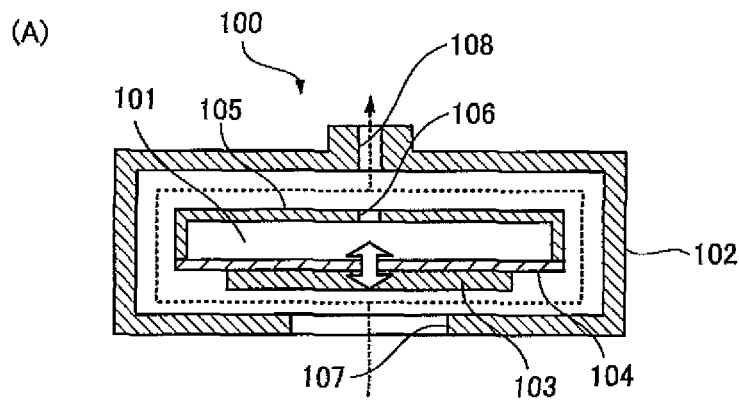


Fig. 11

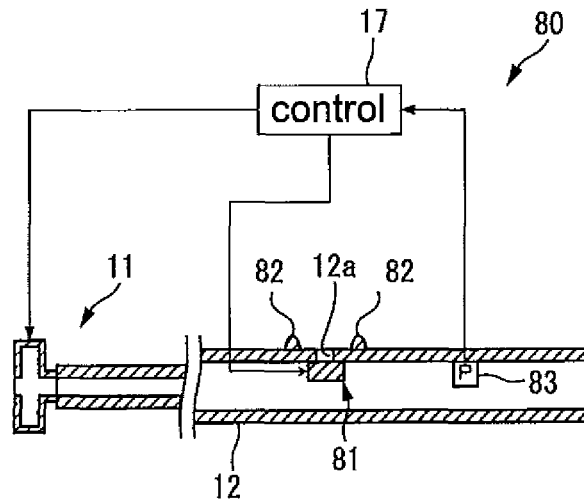


Fig. 12

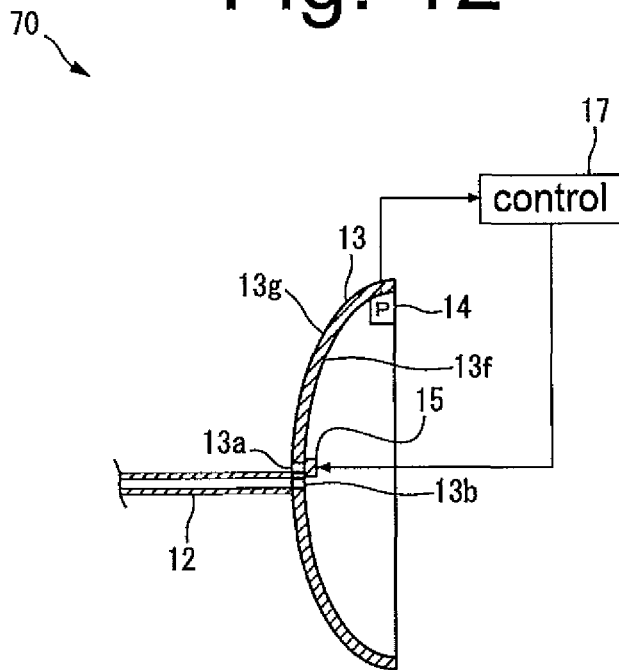


Fig. 13

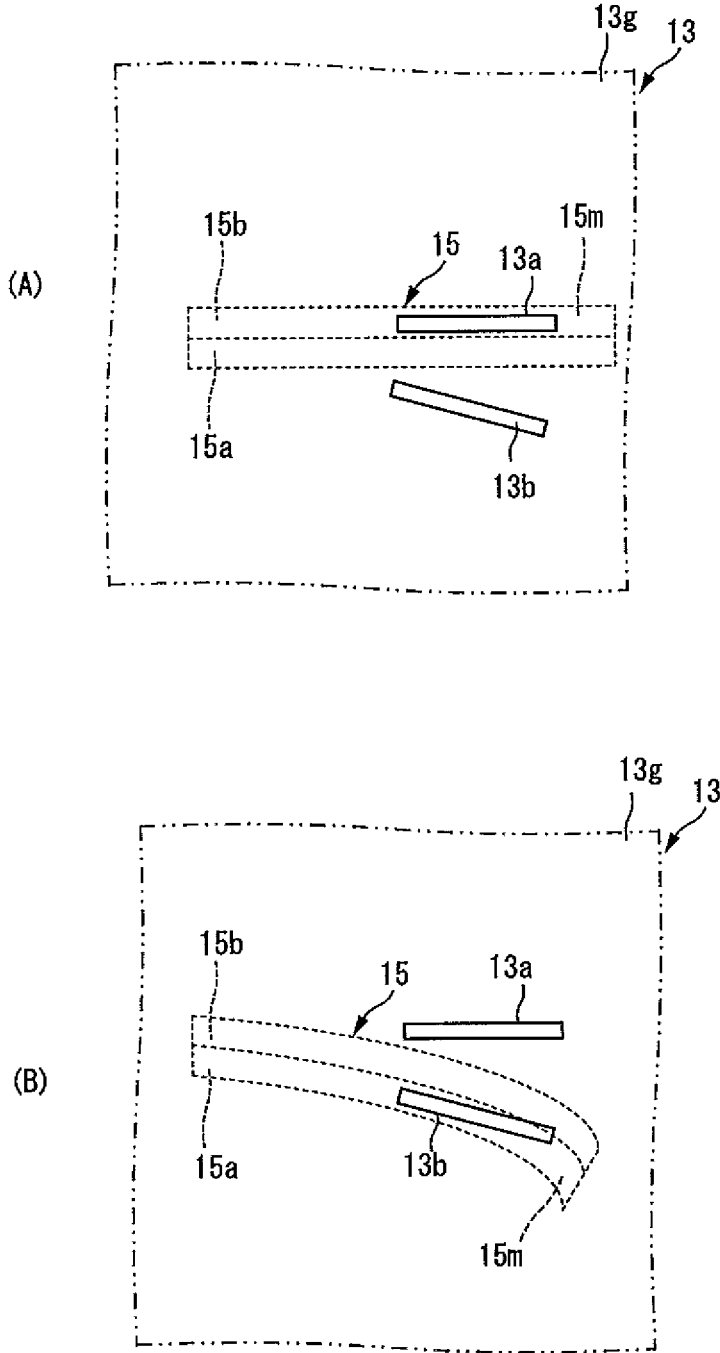


Fig. 14

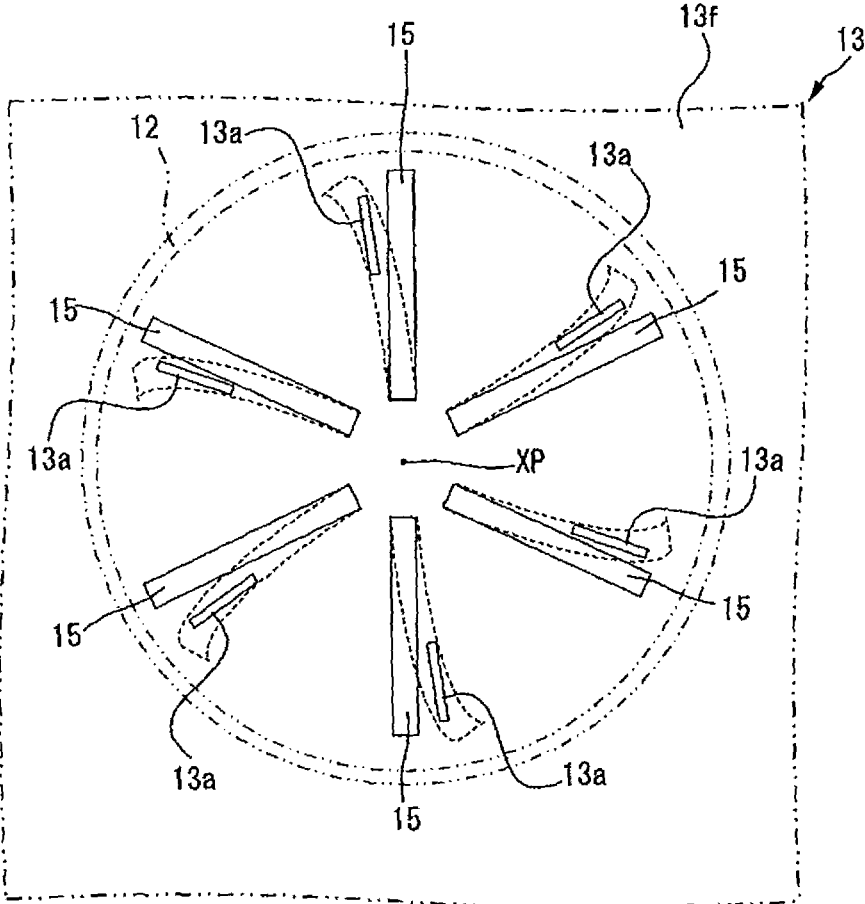


Fig. 15

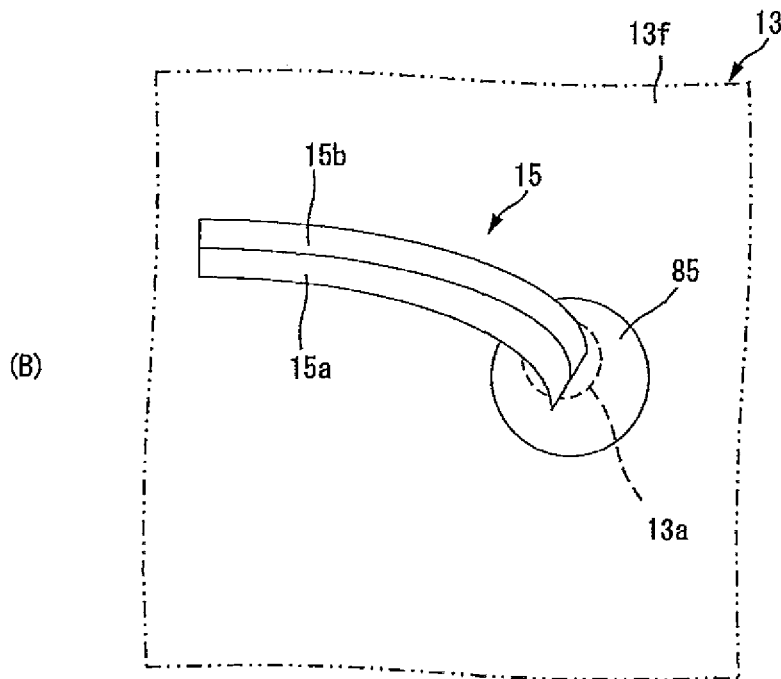
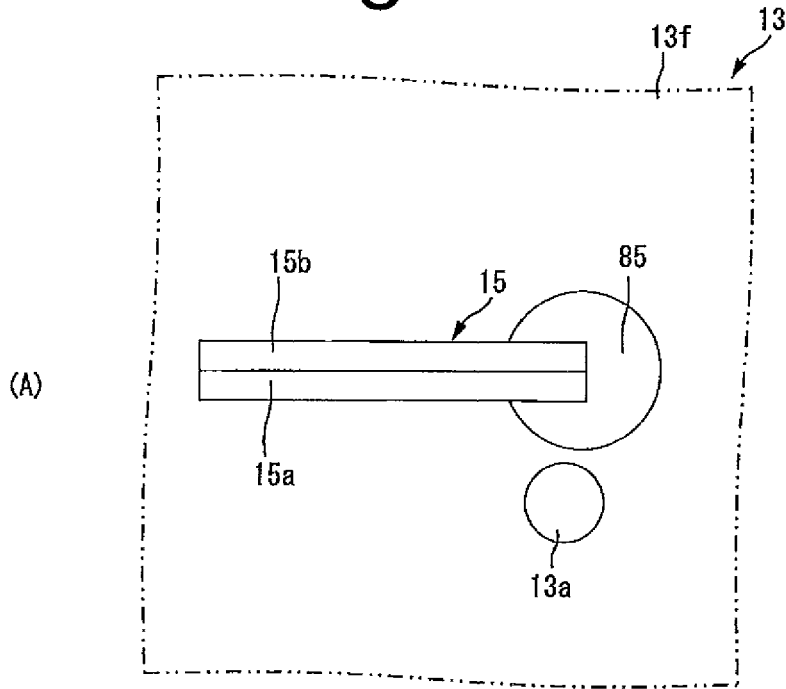


Fig. 16

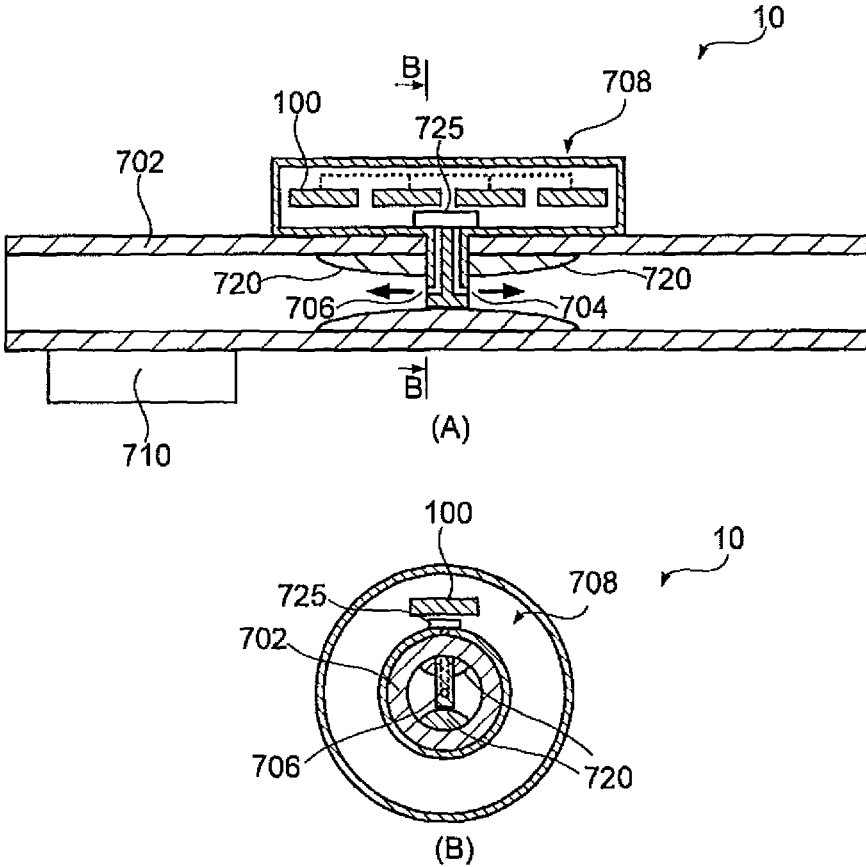


Fig. 17

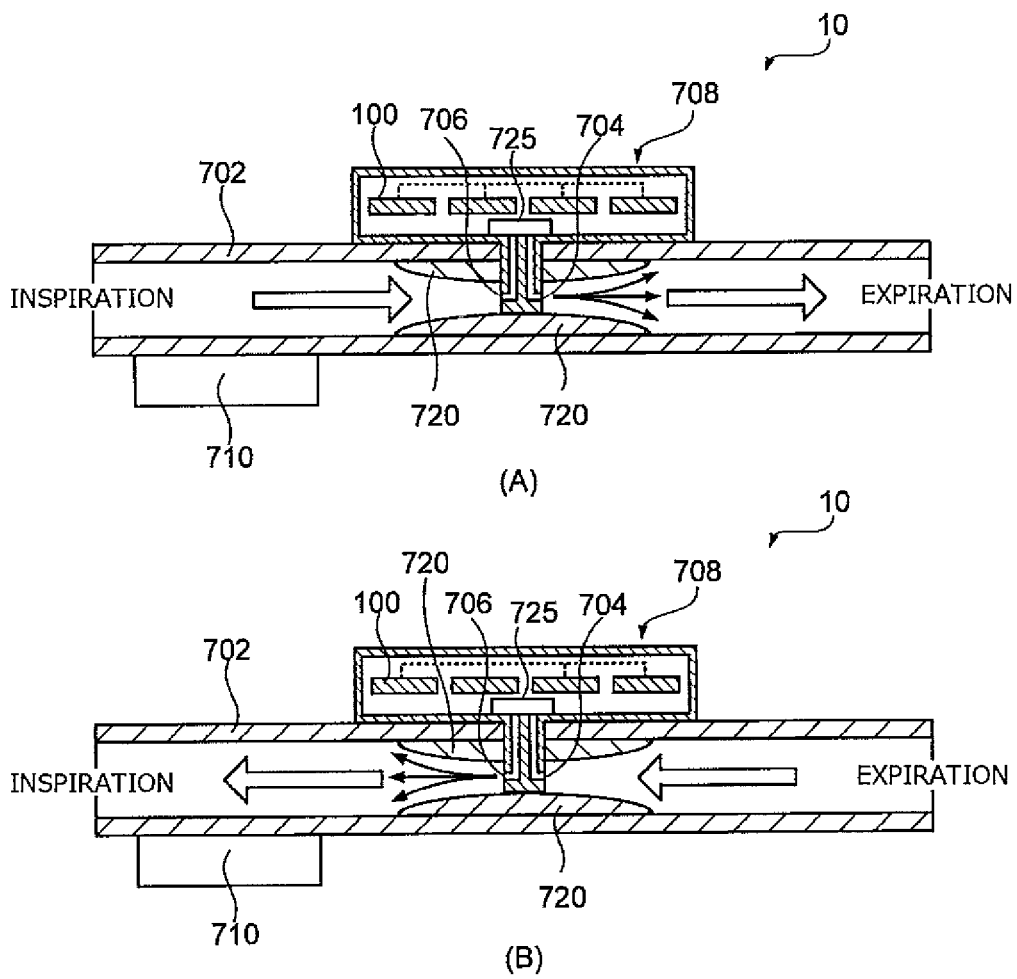


Fig. 18

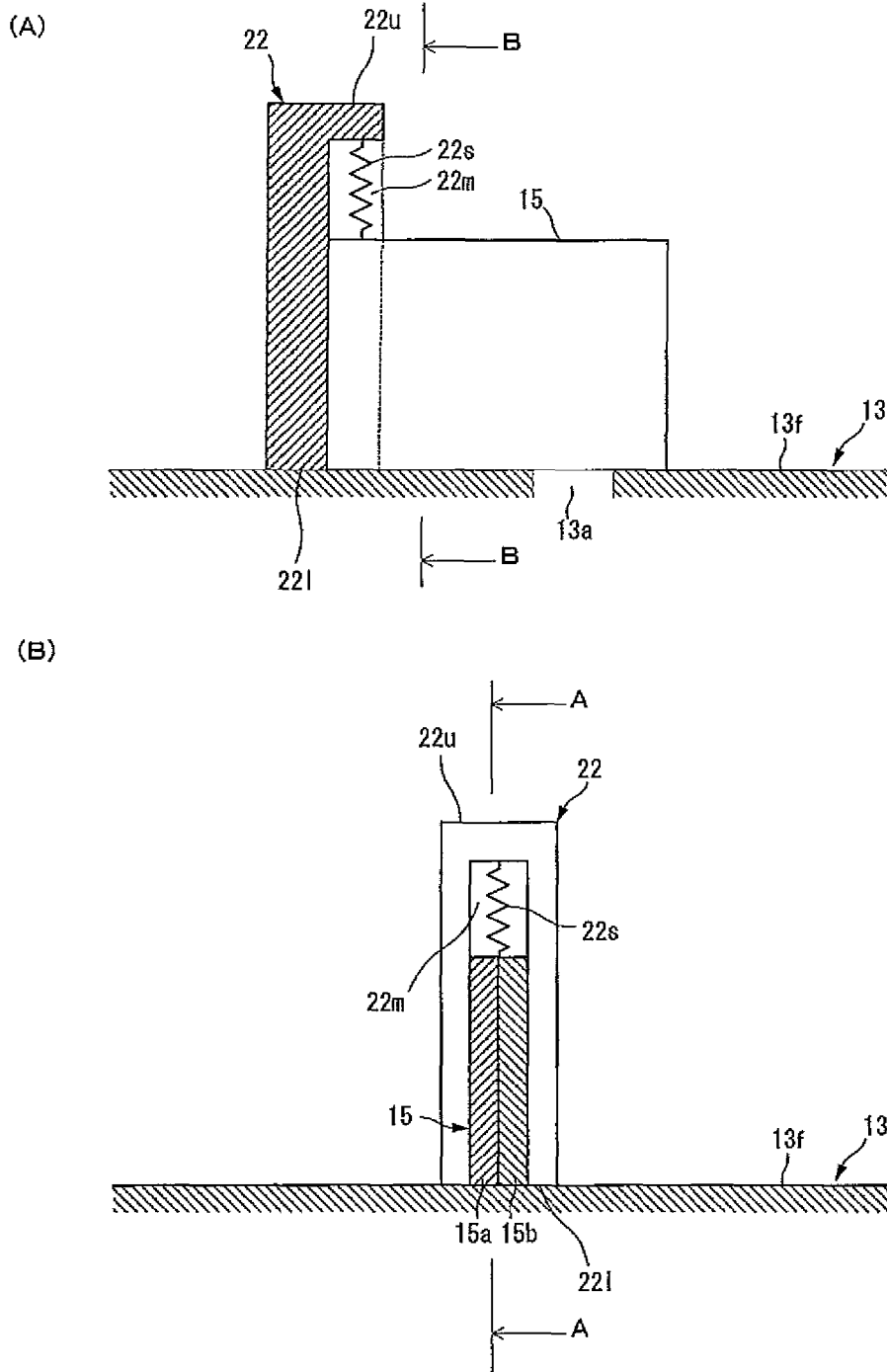
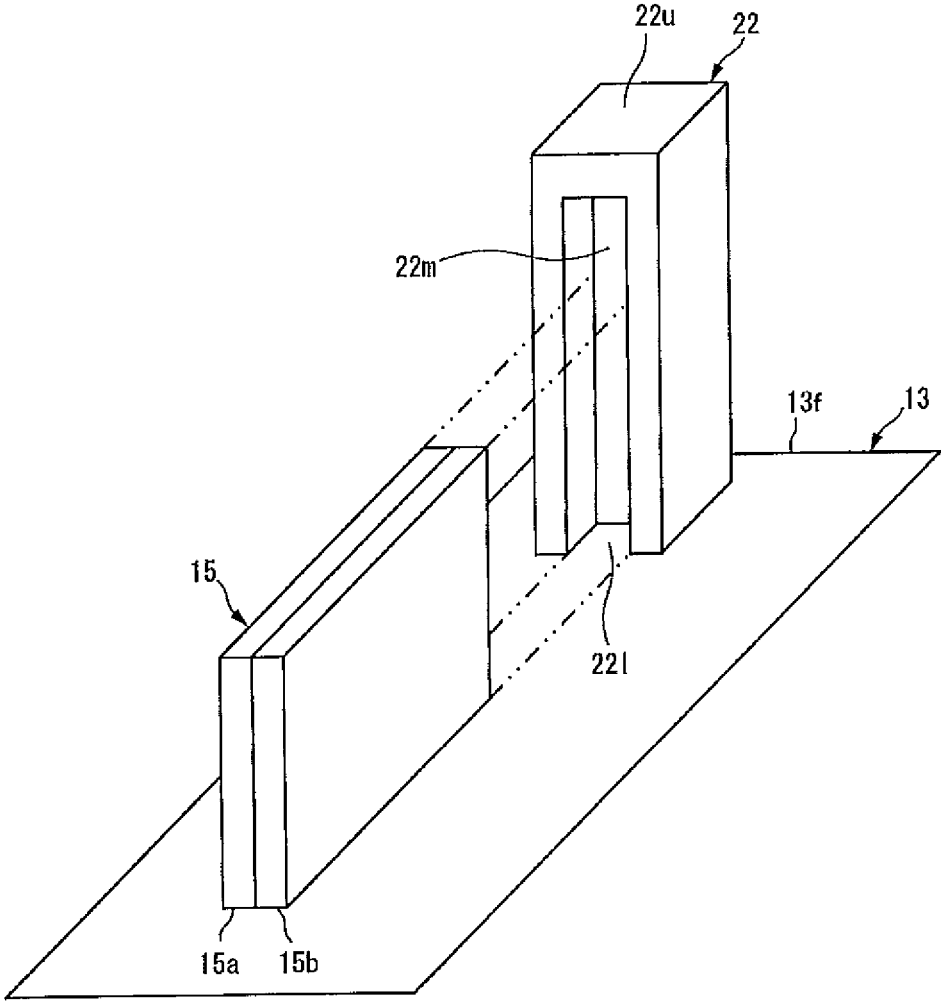


Fig. 19



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**OPENING AND CLOSING DEVICE AND
RESPIRATORY ASSISTANCE DEVICE**

TECHNICAL FIELD

The present invention relates to an opening and closing device and a respiratory assistance device.

BACKGROUND ART

Respiratory assistance devices such as artificial respirators are used in medical practice. A typical respiratory assistance device includes an oxygen supply source such as an oxygen tank, an inspiratory pipe connected to the supply source, a mask attached to a tip of the inspiratory pipe, an expiratory pipe branched from the inspiratory pipe, an expiratory valve fixed to a tip of the expiratory pipe, etc. (for example, Japanese Patent Application Laid-Open Nos. Hei. 02-131765, Hei. 02-131773, Hei. 02-131774, and Hei. 05-245204).

Various methods such as a controlled ventilation (Controlled Ventilation) method used for a patient in the absence of spontaneous breathing (a patient under general anesthesia, during cardiopulmonary resuscitation, or in a critical condition) and an assisted ventilation (Assisted Ventilation) method in which a positive pressure (Positive Pressure) is created in an air passage in synchronization with the spontaneous breathing of a patient are employed for such respiratory assistance devices.

In a respiratory assistance device employing any of these methods, oxygen sent out from the oxygen tank is supplied to lungs as inspiratory air via the inspiratory pipe. The oxygen supplied to the lungs is then exhaled by the lungs as expiratory air. If the expiratory air is discharged into the expiratory pipe, a pressure in the expiratory pipe is increased. A control unit then receives a sensing signal from a pressure sensor having detected the pressure increase in the expiratory pipe and opens the expiratory valve. In this manner, the expiratory air is emitted to the outside from the expiratory pipe.

SUMMARY OF INVENTION

Technical Problem

A diaphragm valve has been known as an expiratory valve employed in such a respiratory assistance device. The diaphragm valve includes: a valve seat formed along a circumference of an opening of a hole through which the expiratory air passes (hereinafter referred to as an expiratory hole); and a valve element movable between a position supported by the valve seat and blocking the expiratory hole (blocking position) and a position away from the valve seat and opening the expiratory hole (opening position).

The valve element of this diaphragm valve is required to have a rigidity just enough to resist a pressure from the expiratory hole in order to maintain the blocking position. As means for enhancing the rigidity of the valve element, changing the forming material thereof, reviewing the shape thereof, increasing the size of the valve element itself, and the like, can be considered.

However, if the forming material or shape of the valve element is changed, the procurement cost or processing cost thereof is thereby increased. Moreover, if the size of the valve element itself is increased, the downsizing of the diaphragm valve becomes difficult to achieve. These prob-

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lems are not limited to the expiratory valve employed in the respiratory assistance device but common to the diaphragm valve.

The present invention has been made in view of the aforementioned problems. It is an object of the present invention to provide an opening and closing device having a rigidity enough to resist a pressure from the hole and capable of being manufactured inexpensively and downsized easily, and a respiratory assistance device including the opening and closing device.

Solution to Problem

As a result of intensive research made by the present inventor, the aforementioned object is achieved by the following means.

An opening and closing device includes: a separating member having a separating surface with a hole through which a fluid passes when opened; and an opening and closing mechanism having a deformable member deformable in a plane direction of the separating surface, wherein the opening and closing mechanism can be transitioned by deformation of the deformable member between a first state and a second state in which opening amounts of the hole are different from each other.

Preferably, the deformable member is formed in a shape of a plate deformable in a thickness direction thereof, and the deformable member extends from the separating surface so that a direction of the deformation coincides with the plane direction of the separating surface. Moreover, the hole is preferably formed in a slit shape and the deformable member preferably covers the hole with a side surface thereof.

Preferably, the opening and closing mechanism includes a cover provided at a free end side of the deformable member and covers the hole by moving the cover. Moreover, said hole includes a first hole and a second hole and the first hole and the second hole are preferably opened in the separating surface, and the opening and closing mechanism preferably can be transitioned by deforming the common deformable member between a state in which the first hole is blocked and the second hole is opened and a state in which the second hole is blocked and the first hole is opened.

Preferably, the deformable member is a piezoelectric element, and the opening and closing device includes a controller for controlling deformation of the piezoelectric element. Moreover, a biasing mechanism for biasing the opening and closing mechanism toward the separating surface is preferably provided.

A respiratory assistance device includes the above-described opening and closing device, and the separating member is formed by: a mask for covering a nose or a mouth; and a communicating pipe which communicates with a space formed inside the mask in a worn state.

The hole is preferably formed in the mask or the communicating pipe. Moreover, the hole preferably forms an expiratory pathway through which expiratory air is exhaled from the nose or the mouth passes.

A respiratory assistance device includes: the above-described opening and closing device; a flow passage through which an expiratory or inspiratory gas passes; an inspiratory nozzle disposed in the flow passage, for jetting an acceleration gas in an inspiratory direction; an expiratory nozzle disposed in the flow passage closer to an expiratory direction side than the inspiratory nozzle, for jetting an acceleration gas in the expiratory direction; a pump unit for supplying the acceleration gas to the inspiratory nozzle and the expiratory

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nozzle; an inspiratory Venturi wall extending from the inspiratory nozzle toward the inspiratory direction in the flow passage so as to spread out the acceleration gas emitted from the inspiratory nozzle in order to set the inspiratory direction side from the inspiratory nozzle at a negative pressure; and an expiratory Venturi wall extending from the expiratory nozzle toward the expiratory direction in the flow passage so as to spread out the acceleration gas emitted from the expiratory nozzle in order to set the expiratory direction side from the expiratory nozzle at a negative pressure, wherein the opening and closing device can be transitioned between a state in which one of the inspiratory nozzle and the expiratory nozzle is blocked and a state in which the other one of them is blocked.

Advantageous Effects of Invention

The above-described opening and closing device has a rigidity sufficient to resist a pressure from the hole and can be manufactured inexpensively and downsized easily. Such an opening and closing device is suitable for use also as an opening and closing device (for example, an expiratory valve) in a respiratory assistance device.

BRIEF DESCRIPTION OF DRAWINGS

FIG. 1 is a schematic view illustrating a configuration of a respiratory assistance device according to a first embodiment of the present invention.

FIG. 2A is a schematic view of an expiratory valve provided in a mask, illustrating a state in which the expiratory valve opens an expiratory hole.

FIG. 2B is a schematic view of the expiratory valve provided in the mask, illustrating the state in which the expiratory valve opens the expiratory hole.

FIG. 2C is a schematic view of the expiratory valve provided in the mask, illustrating a state in which the expiratory valve blocks the expiratory hole.

FIG. 2D is a schematic view of the expiratory valve provided in the mask, illustrating the state in which the expiratory valve blocks the expiratory hole.

FIG. 3 is a block diagram illustrating a hardware configuration of a control unit.

FIG. 4 is a block diagram illustrating a functional configuration of the control unit.

FIG. 5 shows schematic views illustrating a control example of the respiratory assistance device wherein (A) shows a case when a user performs expiration and (B) shows a case when the user performs inspiration.

FIG. 6 is a schematic view illustrating a configuration of a respiratory assistance device according to a second embodiment of the present invention.

FIG. 7 is a schematic view illustrating a configuration of a respiratory assistance device according to a third embodiment of the present invention.

FIG. 8 is a schematic view illustrating a configuration of a respiratory assistance device according to a fourth embodiment of the present invention.

FIG. 9 is a schematic view illustrating a configuration of a respiratory assistance device according to a fifth embodiment of the present invention.

FIG. 10(A) is a cross-sectional view illustrating a configuration example of a micro pump and FIG. 10(B) is a graph showing pressure-flow rate lines of the micro pump.

FIG. 11 is a schematic view illustrating a configuration of a respiratory assistance device according to a sixth embodiment of the present invention.

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FIG. 12 is a schematic view illustrating an expiratory valve capable of selectively blocking an expiratory hole and an inspiratory hole provided in a mask.

FIG. 13 shows schematic views illustrating the expiratory valve capable of selectively blocking the expiratory hole and the inspiratory hole provided in the mask wherein (A) shows a state in which the expiratory valve blocks only the expiratory hole and (B) shows a state in which the expiratory valve blocks only the inspiratory hole.

FIG. 14 is a schematic view of a mask having a plurality of expiratory holes.

FIG. 15 shows schematic views of an expiratory valve including a piezo element and a cover provided in the piezo element and capable of opening and closing an expiratory hole by deformation of the piezo element.

FIG. 16 shows schematic views illustrating a respiratory assistance device including an expiration and inspiration switching valve capable of selectively blocking an expiratory nozzle and an inspiratory nozzle.

FIG. 17(A) is a schematic view of the respiratory assistance device when air is emitted from the expiratory nozzle and FIG. 17(B) is a schematic view of the respiratory assistance device when air is emitted from the inspiratory nozzle.

FIG. 18(A) is a cross-sectional view taken along the line A-A, illustrating an outline of an expiratory valve provided in a mask and components disposed therearound, and FIG. 18(B) is a cross-sectional view taken along the line B-B, illustrating an outline of the expiratory valve provided in the mask and the components disposed therearound.

FIG. 19 is an exploded perspective view illustrating an outline of the expiratory valve provided in the mask and the respective components disposed around the expiratory valve.

DESCRIPTION OF EMBODIMENTS

Embodiments of the present invention will now be described below with reference to the accompanying drawings.

FIG. 1 illustrates, as an example, a configuration of a respiratory assistance device 10 for medical use according to the first embodiment of the present invention. The respiratory assistance device 10 includes: a supply source 11 for sending out an inspiratory gas; an inspiratory pipe 12 with its base end being connected to the supply source 11; a mask 13 attached to a tip of the inspiratory pipe 12 and having an expiratory hole 13a; an air gauge 14 for measuring a gas pressure inside the mask 13; an expiratory valve 15 provided in the mask 13 and serving as an opening and closing mechanism for the expiratory hole 13a; a plurality of safety members 16 provided around the expiratory hole 13a so as to protrude toward the outer side of an expiratory pathway; and a control unit 17 for performing overall control on the entire device. The mask 13 and the expiratory valve 15 together form an opening and closing device.

The mask 13 is a wearing device that covers a mouth and a nose. The mask 13 serves to separate the mouth and the nose from the ambient air (separating member). The mask 13 is provided with an inspiratory hole 13b. The inspiratory pipe 12 and the mask 13 communicate with each other via the inspiratory hole 13b. An inspiratory pathway is formed by the inspiratory pipe 12, the inspiratory hole 13b, and the mask 13. The expiratory pathway is formed by the mask 13 and the expiratory hole 13a. Note that the mask 13 may be a wearing device that covers either the mouth or the nose.

The supply source **11** includes: a gas tank **19** that retains a gas such as air or oxygen in a compressed state; a regulating valve **20** for regulating a flow rate of the gas sent out from the gas tank **19**; and a flowmeter **21** for measuring the flow rate of the gas regulated by the regulating valve **20**. The regulating valve **20** is controlled on the basis of sensing data (measured results, sensing signals) from the air gauge **14** and from the flowmeter **21**. While the regulating valve **20** is not limited to a particular type, an electric valve, an electromagnetic valve with a high response speed, or the like, can be employed. The flowmeter **21** outputs the sensing data to the control unit **17**.

The inspiratory pipe **12** is formed by a bellows tube made of a resin. The inspiratory pipe **12** and the mask **13** worn by a patient together form a space and serve as a pathway for the gas sent out from the supply source **11**. A gas pressure inside the inspiratory pipe **12** coincides with a gas pressure inside the mask **13** worn by the patient in a steady state. The air gauge **14** outputs the sensing data to the control unit **17**.

As shown in FIGS. **2A** to **2D**, the expiratory valve **15** emits the gas inside the mask **13** to the outside of the mask **13** by opening and closing the expiratory hole **13a** formed in a slit shape and functions as a check valve for preventing a back-flow thereof. The plate-shaped expiratory valve **15** is a valve having a monomorph (unimorph) structure in which a piezo element (piezoelectric element) **15a** to be displaced according to an amount of voltage applied is layered on a metal plate **15b** and having a cantilever structure. The respiratory assistance device **10** further includes a fixing member **22** for fixing one end of the expiratory valve **15** to the mask **13**. The fixing member **22** is provided so as to extend from an inner surface **13f** of the mask **13**. The one end of the expiratory valve **15** is fixed to the mask **13** by the fixing member **22** with a position erecting from the inner surface **13f**. Note that the fixing member **22** is preferably provided with a fixing groove into which the one end of the expiratory valve **15** can be fitted. A cantilever length of the expiratory valve **15** is preferably about 30 mm or more and about 40 mm or less. A displacement stroke of the expiratory valve **15** is preferably 2 mm or more and 3 mm or less. Note that the piezo element may have a both-end supported structure.

The piezo element **15a** is deformable between an extended state (see FIGS. **2A** and **2B**) and a bent state (see FIGS. **2C** and **2D**) by turning ON and OFF the voltage application thereto. When the piezo element **15a** is in the extended state, a side surface **15m** of the expiratory valve **15** is in a state in which the expiratory hole **13a** is opened. When the piezo element **15a** is in the bent state, on the other hand, the side surface **15m** of the expiratory valve **15** is in a state in which the expiratory hole **13a** is blocked. In this manner, the expiratory valve **15** becomes deformable as a result of the deformation of the piezo element **15a**. Moreover, the expiratory valve **15** is provided on the inner surface **13f** so that a deformation direction thereof, i.e., a thickness direction thereof, coincides with the plane direction of the inner surface **13f** of the mask **13**. Moreover, it is preferable that the expiratory valve **15** be provided on the inner surface **13f** so that the side surface **15m** slides along the inner surface **13f** by the deformation of the expiratory valve **15**. The inner surface **13f** may be a flat surface or a curved surface. Thus, the expiratory valve **15** can be transitioned by the deformation of the piezo element **15a** between the state in which the expiratory hole **13a** formed in the mask **13** is opened (see FIGS. **2A** and **2B**) and the state in which by the side surface **15m** of the expiratory valve **15**, the expiratory hole **13a** is blocked by the side surface **15m** (see FIGS. **2C** and **2D**).

The piezo element **15a** may be in the bent state when a voltage is being applied thereto and in the extended state when no voltage is being applied thereto as shown in FIGS. **2A** to **2D**. Or alternatively, the piezo element **15a** may be in the extended state when a voltage is being applied thereto and in the bent state when no voltage is being applied thereto.

Although the expiratory valve **15** with the monomorph structure is introduced here, it is apparent that a bimorph structure in which two piezo elements are attached together can be employed instead.

Referring back to FIG. **1**, if the expiratory hole **13a** is covered by an object outside the mask **13**, the expiratory pathway cannot be secured by the actuation of the expiratory valve **15**. It is therefore preferable that the safety members **16** be provided in the mask **13**. The safety members **16** are formed so as to protrude from an outer surface **13g** of the mask **13** and arranged so as to be dotted near the expiratory hole **13a**. Consequently, a gap can be formed between an aperture plane of the expiratory hole **13a** on the outer surface **13g** side and the object covering the expiratory hole **13a**. Thus, the expiratory pathway can be secured by the actuation of the expiratory valve **15**.

As shown in FIG. **3**, the control unit **17** includes a CPU **24**, a first storage medium **25**, a second storage medium **26**, a third storage medium **27**, an input device **28**, a display device **29**, an input and output interface **30**, and a bus **31**.

The CPU **24** is what is called a central processing unit and executes various programs to realize various functions of the control unit **17**. The first storage medium **25** is what is called a RAM (Random Access Memory) and used as a work area for the CPU **24**. The second storage medium **26** is what is called a ROM (Read Only Memory) and stores a basic operating system executed by the CPU **24**. The third storage medium **27** is configured by a hard disk device incorporating a magnetic disk, a disk device accommodating a CD, a DVD, or a BD, a non-volatile semiconductor flash memory device, and the like. The third storage medium **27** saves various programs executed by the CPU **24**.

The input device **28** is an input key, a keyboard, or a mouse and inputs a variety of information. The display device **29** is a display and displays various operating states. A power supply for operating the expiratory valve **15** and control signals are inputted to and outputted from the input and output interface **30**. Furthermore, the input and output interface **30** also obtains data such as a program from an external personal computer. The bus **31** serves as a line for integrally connecting the CPU **24**, the first storage medium **25**, the second storage medium **26**, the third storage medium **27**, the input device **28**, the display device **29**, the input and output interface **30**, and the like to achieve communication among them.

FIG. **4** shows a functional configuration obtained when a control program stored in the control unit **17** is executed by the CPU **24**. The control unit **17** includes: a sensing part **34**; an expiratory valve control part **35**; and a regulating valve control part **36**, as the functional configuration. The sensing part **34** constantly obtains the sensing data from the air gauge and transmits such data to the expiratory valve control part **35**. Furthermore, the sensing part **34** constantly obtains the sensing data from the air gauge **14** and the flowmeter **21** and transmits such data to the regulating valve control part **36**. The expiratory valve control part **35** refers to the sensing data from the sensing part **34** and controls a control signal to the expiratory valve **15** so as to approximate a target opening amount. The regulating valve control part **36** refers

to the sensing data from the sensing part **34** and controls a control signal to the regulating valve **20** so as to approximate a target flow rate value.

Control examples for the respiratory assistance device **10** will be described next with reference to FIG. **5(A)** and FIG. **5(B)**.

First of all, if expiratory air is exhaled from a mouth or nose wearing the mask **13**, the pressure inside the mask **13** is increased. If the pressure inside the mask **13** is increased, the increased value is sensed by the air gauge **14**. The sensing data is outputted to the control unit **17**. The control unit **17** controls the expiratory valve **15** on the basis of the sensing data. More specifically, the control unit **17** operates the expiratory valve **15** so as to open the expiratory hole **13a** as shown in FIG. **5(A)**. The expiratory air is emitted to the outside of the mask **13** through the expiratory hole **13a**.

Emitting the expiratory air to the outside of the mask **13** causes the pressure inside the mask **13** to decrease. If the pressure inside the mask **13** is decreased, the decreased value is sensed by the air gauge **14**. The sensing data is outputted to the control unit **17**. The control unit **17** controls the expiratory valve **15** on the basis of the sensing data. More specifically, the control unit **17** operates the expiratory valve **15** so as to block the expiratory hole **13a**. Consequently, a closed space is formed inside the mask **13**, thereby allowing for an inspiratory operation.

Subsequently, when inspiration is performed by the mouth or nose wearing the mask **13**, the pressure inside the mask **13** is decreased. If the pressure inside the mask **13** is decreased, the decreased value is sensed by the air gauge **14**. The sensing data is outputted to the control unit **17**. The control unit **17** controls the supply source **11** on the basis of the sensing data. More specifically, the control unit **17** opens the regulating valve **20** so as to send out the gas from the gas tank **19** as the inspiratory air as shown in FIG. **5(B)**. Thereafter, the pressure inside the mask **13** is increased. If the pressure inside the mask **13** is increased, the increased value is sensed by the air gauge **14**. The sensing data is outputted to the control unit **17**. The control unit **17** controls the supply source **11** on the basis of the sensing data. More specifically, the control unit **17** closes the regulating valve **20** so as to stop the sending out of the gas from the gas tank **19** as the inspiratory air. Thereafter, the expiratory operation and the inspiratory operation are repeated in the same manner.

Here, if the deformation direction of the piezo element **15a** coincides with a direction away from the inner surface **13f** or closer to the inner surface **13f**, the deformation direction of the piezo element **15a** is substantially parallel to the direction of a force generated by a pressure difference between the inside and outside of the mask **13**. Thus, the piezo element **15a** is easily deformed by the force generated by the pressure difference between the inside and outside of the mask **13**. In the above-described respiratory assistance device **10**, on the other hand, the expiratory valve **15** is disposed so that the deformation direction of the piezo element **15a** coincides with a direction along the inner surface **13f**. Therefore, the deformation direction of the piezo element **15a** is substantially perpendicular to the direction of the force generated by the pressure difference between the inside and outside of the mask **13**. Consequently, the piezo element **15a** is hardly deformed by the force generated by the pressure difference between the inside and outside of the mask **13**. In this manner, the expiratory valve **15** is rigid enough to resist the pressure from the expiratory hole **13a**. Moreover, since the piezo

element can be used as the expiratory valve **15** itself, an increase in procurement cost or processing cost can be avoided.

As described above, the opening and closing device formed by the mask **13** and the expiratory valve **15** is rigid enough to resist the pressure from the hole and can be manufactured inexpensively and downsized easily. Furthermore, due to its simple configuration, the opening and closing device can easily obtain a high reliability.

Moreover, the expiratory valve **15** is disposed so that the deformation direction of the piezo element **15a** coincides with the direction along the inner surface **13f**. Therefore, as compared with the case where the deformation direction of the piezo element **15a** coincides with the direction away from the inner surface **13f** or closer to the inner surface **13f**, a fully-opened state of the expiratory hole **13a** can be easily obtained with a smaller deformation amount of the piezo element **15a**.

Moreover, since the piezo element **15a**, capable of easily adjusting the deformation amount thereof by an applied voltage value, is used, the opening percentage of the expiratory hole **13a** can be easily adjusted. Consequently, the discharge amount of the expiratory air can be adjusted. Therefore, the flow rate of the expiratory air emitted from the expiratory valve **15** can be prevented from changing abruptly. In other words, the gas pressure inside the mask **13** can be prevented from changing abruptly, thereby easing a load on the patient.

Furthermore, the expiratory valve **15** is configured to include the piezo element **15a**. Thus, as compared with a case where an electromagnetic valve is employed as the expiratory valve, the expiratory valve **15** has a longer lifetime and is more durable.

Thus, the application of the present invention allows for use as a home artificial respirator by a patient suffering from sleep apnea syndrome or the like.

Moreover, the expiratory valve **15** is in the state in which the expiratory hole **13a** is opened when no voltage is being applied to the piezo element **15a**. Therefore, even when the expiratory valve **15** stops its operation due to a failure or the like, the expiratory valve **15** is forced to be in the state in which the expiratory hole **13a** is opened. Thus, the expiratory pathway can be secured.

Also, since the expiratory valve **15** is provided in the mask **13**, the responsiveness of the expiratory valve **15** to the expiratory operation is high. Thus, a load on the patient is small.

Furthermore, since the expiratory valve **15** is provided inside the mask **13**, the expiratory valve **15** can be prevented from interfering with an object outside the mask **13**. Note that the expiratory valve **15** may be provided on the outer surface of the mask **13**.

FIG. **6** illustrates, as an example, a configuration of a respiratory assistance device **40** according to the second embodiment. The first embodiment and the second embodiment have many identical or similar portions. The description of such portions will be therefore omitted when appropriate and points different from those in the first embodiment will be described mainly. Also, with regard to the third and following embodiments to be described later, descriptions common to the other embodiments will be omitted when appropriate and points different from those in the other embodiments will be described mainly.

In the respiratory assistance device **40**, a vent hole **12a** is formed in the inspiratory pipe **12** instead of forming the expiratory hole **13a** (see FIG. **1**) in the mask **13**. Also, instead of providing the expiratory valve **15** and the plurality

of safety members 16 in the mask 13, an expiratory valve 41 and a plurality of safety members 42 are provided in the inspiratory pipe 12 according to the respiratory assistance device 40. Thus, the inspiratory pipe 12 functions also as the expiratory pathway.

The expiratory valve 41, having a configuration similar to the expiratory valve 15 shown in FIGS. 2A to 2D, is provided on an inner surface 12f such that a deformation direction thereof, i.e., a thickness direction thereof, extends along the inner surface 12f of the inspiratory pipe 12 and a side surface thereof slides along the inner surface 12f by the deformation thereof. Thus, the expiratory valve 15 can be transitioned by the deformation of the piezo element between a state in which the vent hole 12a is opened and a state in which the vent hole 12a is closed. Moreover, the safety members 42 are formed so as to protrude from an outer surface 12g of the inspiratory pipe 12 and arranged so as to be dotted near the vent hole 12a.

It is preferable that the expiratory valve 41 be provided at a position as close as possible to the mask 13 within a range not causing a slow responsiveness to the expiratory operation. Specifically, the expiratory valve 41 is provided preferably at a position where a length from the mask 13 in the inspiratory pipe 12 is within 300 mm, and more preferably at a position within 100 mm. In other words, the expiratory valve 41 is provided preferably at a position where a distance of the expiratory pathway from an entrance into a body such as a mouth is within 310 mm, and more preferably at a position within 110 mm.

FIG. 7 illustrates, as an example, a configuration of a respiratory assistance device 50 according to the third embodiment. In the respiratory assistance device 50, an expiratory valve 51 and a plurality of safety members 52 are provided in the mask 13 via an exhaust pipe 53 instead of providing the expiratory valve 15 and the plurality of safety members 16 directly on the mask 13. More specifically, the exhaust pipe 53 is provided on the mask 13 so that a base end thereof covers the expiratory hole 13a. A tip of the exhaust pipe 53 is closed by a cap 54. A vent hole 53a is formed in a middle portion of the exhaust pipe 53. Thus, the exhaust pipe 53 functions also as the expiratory pathway.

The expiratory valve 51, having a configuration similar to the expiratory valve 15 shown in FIGS. 2A to 2D, is provided on an inner surface 53f such that a deformation direction thereof, i.e., a thickness direction thereof, extends along the inner surface 53f of the exhaust pipe 53 and a side surface thereof slides along the inner surface 53f by the deformation thereof. Thus, the expiratory valve 51 can be transitioned by the deformation of the piezo element between a state in which the vent hole 53a is opened and a state in which the vent hole 53a is blocked. Moreover, the safety members 52 are formed so as to protrude from an outer surface 53g of the exhaust pipe 53 and arranged so as to be dotted near the vent hole 53a. It is preferable that the exhaust pipe 53 be set as short as possible within a range not causing a slow responsiveness of the expiratory valve 51 to the expiratory operation. Specifically, a length of the exhaust pipe 53 is preferably within 500 mm, and more preferably within 300 mm.

FIG. 8 illustrates, as an example, a configuration of a respiratory assistance device 60 according to the fourth embodiment. In the respiratory assistance device 60, an expiratory valve 61 and a plurality of safety members 62 are provided in the inspiratory pipe 12 via an exhaust pipe 63 instead of providing the expiratory valve 15 and the plurality of safety members 16 directly on the mask 13. More specifically, the exhaust pipe 63 is provided on the inspira-

tory pipe 12 so that a base end thereof covers the vent hole 12a. A tip of the exhaust pipe 63 is closed by a cap 64. Also, a vent hole 63a is formed in a middle portion of the exhaust pipe 63. Thus, the inspiratory pipe 12 functions also as the expiratory pathway.

The expiratory valve 61, having a configuration similar to the expiratory valve 15 shown in FIGS. 2A to 2D, is provided on an inner surface 63f so that a deformation direction thereof, i.e., a thickness direction thereof, extends along the inner surface 63f of the exhaust pipe 63 and a side surface thereof slides along the inner surface 63f by the deformation thereof. Thus, the expiratory valve 61 can be transitioned by the deformation of the piezo element between a state in which the vent hole 63a is opened and a state in which the vent hole 63a is blocked. Moreover, the safety members 62 are formed so as to protrude from an outer surface 63g of the exhaust pipe 63 and arranged so as to be dotted near the vent hole 63a.

It is preferable that the exhaust pipe 63 be set as short as possible within a range not causing a slow responsiveness of the expiratory valve 61 to the expiratory operation. Specifically, a length of the exhaust pipe 63 is preferably within 500 mm, and more preferably within 300 mm. Moreover, it is preferable that the exhaust pipe 63 be provided at a position as close as possible to the mask 13. Specifically, the exhaust pipe 63 is provided preferably at a position where a length from the mask 13 in the inspiratory pipe 12 is within 150 mm, and more preferably at a position within 50 mm. In other words, the exhaust pipe 63 is provided preferably at a position where a distance of the expiratory pathway from an entrance into a body such as a mouth is within 160 mm, and more preferably at a position within 60 mm.

FIG. 9 illustrates, as an example, a configuration of a respiratory assistance device 70 according to the fifth embodiment. The respiratory assistance device 70 includes a micro pump 100 as the supply source 11 and includes only the mask 13 as the inspiratory pathway. In other words, the micro pump 100 is directly connected to the mask 13. This micro pump 100 is the micro pump proposed in Patent Literature WO 2008/069266. As shown in FIG. 10(A), the micro pump 100 includes: a primary blower chamber 101; and a secondary blower chamber 102 formed outside the primary blower chamber 101.

The primary blower chamber 101 includes: a piezoelectric element 103 serving as an oscillation source; a diaphragm 104 to which the piezoelectric element 103 is fixed; and an oscillation frame 105 to form a space together with the diaphragm 104. The oscillation frame 105 has an opening 106 through which a fluid is moved between the inside and outside of the primary blower chamber 101. The secondary blower chamber 102 includes: a suction port 107 on the diaphragm 104 side; and a discharge port 108 provided so as to face the opening 106.

According to the thus described micro pump 100, when the diaphragm 104 resonates by the piezoelectric element 103, the fluid is moved between the primary blower chamber 101 and the secondary blower chamber 102. A fluid resistance due to such a fluid movement causes the oscillation frame 105 to resonate. The resonance of the diaphragm 104 and the oscillation frame 105 causes the fluid to be sucked in from the suction port 107 and to be discharged from the discharge port 108.

The micro pump 100 is suitable for use as a blower for transporting a gas. The micro pump 100 can perform such transportation without employing a check valve. While the micro pump 100 is extremely small, having a box shape with an outer diameter of about 20 mm×20 mm×2 mm, the micro

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pump **100** can transport air of about 1 L/min at a maximum (when the static pressure is 0 Pa) and can obtain a static pressure of about 2 kPa at a maximum (flow rate of 0 L/min) when the input sine wave is set at 26 kHz under 15 V_{pp} (Volt peak to peak).

On the other hand, the micro pump **100** transports a fluid by means of the oscillation of the diaphragm **104** caused by the piezoelectric element **103**. Thus, there is naturally a limit in its transportable fluid volume. This static pressure-flow rate characteristic also exhibits a straight line as shown in FIG. **10(B)**. More specifically, in order to obtain a static pressure of about 1 kPa, for example, the flow rate is 0.5 L/min.

If the V_{pp} of the input sine wave is changed to 10 or 20, the amplitude of the piezoelectric element **103** is thereby changed. Thus, the flow rate and the pressure can be changed. More specifically, if the V_{pp} of the input sine wave is smoothly changed, the flow rate and the pressure can be smoothly changed. Alternatively, if the frequency of the input sine wave is changed, the flow rate and the pressure can be changed. More specifically, if the frequency of the input sine wave is smoothly changed, the flow rate and the pressure can be smoothly changed. Note however that the flow rate and the pressure each have an upper limit depending on the capacity of the piezoelectric element **103** and the strength or durability of the components. The micro pump **100** is generally used at a rated V_{pp} and a rated frequency.

Although a monomorph (unimorph) structure in which the single piezoelectric element **103** is attached to the diaphragm **104** is introduced here, it is apparent that a bimorph structure in which two piezoelectric elements are attached together in order to increase the amount of oscillation can be employed instead.

FIG. **11** illustrates, as an example, a configuration of a respiratory assistance device **80** according to the sixth embodiment. The respiratory assistance device **80** includes the micro pump **100** as the supply source **11** and includes only the inspiratory pipe **12** as the inspiratory pathway. In the respiratory assistance device **80**, an expiratory valve **81** and a plurality of safety members **82** are provided in the inspiratory pipe **12** instead of providing the expiratory valve **15** and the plurality of safety members **16** in the mask **13**. Thus, the inspiratory pipe **12** functions also as the expiratory pathway. It is preferable that the expiratory valve **81** be provided at a position as close as possible to the tip of the inspiratory pipe **12** within a range not causing a slow responsiveness to the expiratory operation and within a range not resulting in an insertion thereof into the mouth of a patient. Furthermore, in the respiratory assistance device **80**, an air gauge **83** is provided inside the inspiratory pipe **12** instead of providing the air gauge **14** inside the mask **13**.

It is apparent that the respiratory assistance device according to the present invention is not limited to the above-described embodiments and various modifications can be made thereto without departing from the scope of the present invention. Also, the constituent elements of the above-described embodiments may be applied to other embodiments to the extent possible.

In other words, in the above-described embodiments, the positions, sizes, shapes, and quantities in the respective configurations can be changed appropriately. Modifications of the first embodiment will be described below as examples.

Modifications of the first embodiment will be described specifically as examples. As shown in FIGS. **12** and **13**, it is preferable that the expiratory hole **13a** and the inspiratory hole **13b** formed in the mask **13** be provided so as to be close

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to each other. "Being close" herein refers to a range smaller than the deformation amount of the piezo element **15a**. Thus, the expiratory valve **15** can be transitioned by the deformation of the piezo element **15a** between a state in which only the expiratory hole **13a** formed in the mask **13** is blocked (see FIG. **13(A)**) and a state in which only the inspiratory hole **13b** is blocked (see FIG. **13(B)**). This reliably allows for switching between a state in which the expiratory air inside the mask **13** is emitted to the outside of the mask **13** and a state in which the inspiratory gas from the inspiratory pipe **12** is sent into the mask **13**. Furthermore, since the inspiratory pipe **12** is formed in a protruding manner near the expiratory hole **13a** on the outer surface of the mask **13**, the inspiratory pipe **12** functions also as a safety member.

Alternatively, as shown in FIG. **14**, a plurality of expiratory holes **13a** may be provided in the mask **13**. These expiratory holes **13a** are provided at portions of the mask **13** facing the aperture plane of the tip portion of the inspiratory pipe **12**. Alternatively, any reference position XP may be set at a portion of the mask **13** facing the aperture plane of the tip portion of the inspiratory pipe **12** and the expiratory holes **13a** may be arranged around the reference position XP. It is preferable that an expiratory valve **15** be provided for each of the expiratory holes **13a** formed in the mask **13** to open and close the corresponding expiratory hole **13a**. The plurality of expiratory valves **15** are controlled independently of one another to open and close the expiratory holes **13a**, respectively. Thus, by changing the number of the expiratory valves **15** to be opened, the flow rate of the expiratory air can be adjusted. In this manner, without controlling the applied amount of a voltage to the piezo element **15a**, the flow rate of the expiratory air can be adjusted stepwisely only by controlling ON and OFF of the voltage to the piezo elements **15a** in order to change the number of the expiratory valves **15** to be opened. In other words, the flow rate of the expiratory air can be adjusted with such a simple control. Moreover, the flow rate of the expiratory air can be adjusted more smoothly by controlling the applied amount of the voltage to the piezo element **15a**.

In the above-described embodiment, the expiratory valve **15** having the piezo element **15a**, which is a deformable member, is used as the opening and closing mechanism. Also, the expiratory valve **15** is configured so as to be transitioned by the deformation of the piezo element **15a** between the state in which the expiratory hole **13a** is blocked by the side surface **15m** (see FIG. **1**) of the expiratory valve **15** (see FIGS. **2C** and **2D**) and the state in which the expiratory hole **13a** is opened (see FIGS. **2A** and **2B**). However, the present invention is not limited thereto. The expiratory hole **13a** may be opened and closed by using a cover **85** provided at a free end side of the expiratory valve **15**. In this case, the expiratory valve **15** and the cover **85** together form the opening and closing mechanism (see FIG. **15**). The cover **85** has a sliding surface to slide along the inner surface **13f**. The cover **85** is disposed so that the deformation direction of the expiratory valve **15**, i.e., the thickness direction of the expiratory valve **15**, extends along the inner surface **13f** of the mask **13** and the sliding surface slides along the inner surface **13f** by the deformation of the expiratory valve **15**.

Alternatively, in the above-described first to fourth embodiments, the micro pump **100** may be provided as the supply source **11** in place of the gas tank **19** or the like. In each of the above-described embodiments including the cases of the above-described fifth and sixth embodiments, a plurality of micro pumps **100** may be provided and disposed in series or in parallel or disposed in a matrix.

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Alternatively, while a mask **13** covering a mouth and a nose is provided as the inspiratory pathway and the expiratory pathway in the above-described first to fifth embodiments, a wearing device such as a nosepiece worn by a nose may be provided in place of the mask **13**.

Note that the shape of the expiratory hole **13a** or the inspiratory hole **13b** (see FIG. **14**) such as a circle (see FIG. **15**), an ellipse, a polygon, or a slit shape (see FIGS. **2A** to **2D**) may be appropriately determined depending on its usage.

When the hole is opened and closed by means of a temperature change, a bimetal may be used as the opening and closing mechanism. In this case, it is advantageous in that there is no need for a control unit controller. Coefficients of thermal expansion, shapes, and sizes of the materials of the bimetal may be determined so as to achieve transition between the opened state and the closed state.

In the above-described embodiments, the expiratory valve is deformed between the fully-opened state of the expiratory hole **13a** (see FIGS. **2A** and **2B**) and the fully-closed state of the expiratory hole **13a** (see FIGS. **2C** and **2D**). Depending on its usage, however, the expiratory valve **15** may be deformed between a state in which the opening amount of the expiratory hole **13a** is A and a state in which the opening amount of the expiratory hole **13a** is B which is greater than A. This allows the flow rate of the expiratory air to be adjusted stepwisely.

Moreover, the above-described opening and closing device can be applied not only to the opening and closing of a hole through which the expiratory air passes but also to the opening and closing of a hole through which a fluid (a gas or a liquid) passes and the opening and closing of a hole through which a solid passes.

Furthermore, another embodiment will be described. A respiratory assistance device **10** shown in FIG. **16** is configured to include: a flow passage **702** through which a gas for respiration passes; an expiratory nozzle **704** and an inspiratory nozzle **706** disposed in the flow passage **702** and capable of emitting acceleration air in an expiratory direction and in an inspiratory direction, respectively; a pump unit **708** disposed on an outer surface of the flow passage **702** in a circumferential direction thereof; and a battery **710** for driving the pump unit **708**. Venturi walls **720** are disposed near the expiratory and inspiratory nozzles **704** and **706** disposed in the flow passage **702**. The Venturi wall **720** includes a portion extending from the inspiratory nozzle **706** toward the inspiratory direction and a portion extending from the expiratory nozzle **704** toward the expiratory direction. Note that the battery **710** may be disposed at a remote location or may be omitted by connecting a power supply line.

In the pump unit **708**, a plurality of (for example, four) micro pumps **100** are arranged. The pump unit **708** is provided with an integrated discharge port (not shown) which is a place from which air transported by all the micro pumps **100** is discharged finally. An expiration and inspiration switching valve **725** is disposed at the integrated discharge port. The expiration and inspiration switching valve **725** has a configuration similar to that of the above-described expiratory valve **15**. The expiration and inspiration switching valve **725** is switchable between a state in which the inspiratory nozzle **706** is blocked and a state in which the expiratory nozzle **704** is blocked. If the expiration and inspiration switching valve **725** blocks the inspiratory nozzle **706**, the air sent out from the pump unit **708** is emitted from the expiratory nozzle **704** as shown in FIG. **17(A)**. The air emitted from the expiratory nozzle **704** is

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spread out by the Venturi walls **720**, thereby setting the expiratory side in a negative pressure state. Thus, carbon dioxide discharged from the inspiratory side (lung side) is attracted and caused to flow in the expiratory direction. Consequently, the expiratory operation can be assisted. When the expiration and inspiration switching valve **725** blocks the expiratory nozzle **704**, on the other hand, the air sent out from the pump unit **708** is emitted from the inspiratory nozzle **706** as shown in FIG. **17(B)**. The air emitted from the inspiratory nozzle **706** is spread out by the Venturi walls **720**, thereby setting the inspiratory side in a negative pressure state. Thus, oxygen supplied from the expiratory side is sucked in and is caused to flow in the inspiratory direction (lung side). Consequently, the inspiratory operation can be assisted.

Furthermore, as a result of the reduced distance between the pump unit **708** and the expiratory and inspiratory nozzles **704** and **706**, an improved responsiveness in the breathing assisting operation can be obtained.

In the above-described embodiment, as shown in FIGS. **2A** to **2D**, an expiratory valve having the monomorph (unimorph) structure formed by the piezo element (piezoelectric element) **15a** and the metal plate **15b** is employed as the expiratory valve **15** and the piezo element **15a** is switched between the extended state (see FIGS. **2A** and **2B**) and the bent state (see FIGS. **2C** and **2D**) by turning ON and OFF the voltage application to the piezo element **15a**. However, the behavior of the piezo element **15** in the ON and OFF control of the voltage application includes not only deformation in the thickness direction thereof but also deformation in the width direction thereof (the height direction from the inner surface **13f**). Therefore, if the turning ON and OFF of the voltage application to the piezo element **15a** is repeatedly performed, a gap is created between the expiratory valve **15** and the inner surface **13f** as a result of the deformation in the width direction of the piezo element **15a**. Consequently, the expiratory valve **15** can no longer close the expiratory hole **13a**.

If such is the case, it is preferable that a holding groove **22m** capable of holding one end of the expiratory valve **15** be formed in the fixing member **22** and a spring **22s** for biasing the expiratory valve **15** toward the inner surface **13f** be disposed in the holding groove **22m** as shown in FIGS. **18** to **19**.

The holding groove **22m** is formed on a side surface of the fixing member **22** with a size into which the one end of the expiratory valve **15** can be inserted. The holding groove **22m** extends in the height direction from the inner surface **13f** (the width direction of the expiratory valve **15**). Moreover, the dimension of the holding groove **22m** in the width direction of the expiratory valve **15** is longer than that of the expiratory valve **15**. Furthermore, one end side of the holding groove **22m**, i.e., an upper surface (the surface opposite to a lower surface) **22u** side of the fixing member **22**, is closed whereas the other end side thereof, i.e., a lower surface (the surface in contact with the inner surface **13f**) **221** side of the fixing member **22**, is opened at the lower surface **221**.

The spring **22s** is disposed in the holding groove **22m** over a range from the one end of the expiratory valve **15** toward the upper surface **22u**. One end of the spring **22s** abuts against the surface of the holding groove **22m** on the upper surface **22u** side. The other end of the spring **22s** abuts against the surface of the expiratory valve **15** on the upper surface **22u** side. Therefore, the spring **22s** biases the expiratory valve **15** downward, i.e., toward the inner surface **13f**.

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In this manner, the spring 22s biasing the expiratory valve 15 toward the inner surface 13f is disposed. Thus, even when the deformation of the piezo element 15a is repeatedly performed, a gap is less likely to be formed between the expiratory valve 15 and the inner surface 13f. Consequently, the closing operation of the expiratory hole 13a by the expiratory valve 15 can be reliably performed.

Alternatively, if the expiratory hole 13a is opened and closed by the cover 85 provided at the free end side of the expiratory valve 15 as shown in FIG. 15, a spring for biasing the cover 85 toward the inner surface 13f may be provided between the free end of the expiratory valve 15 and the cover 85.

The invention claimed is:

1. An opening and closing device comprising:
 - a separating member having a separating surface with a hole provided therein through which a fluid can pass when opened; and
 - an opening and closing mechanism having a plate-shaped deformable member comprising a piezoelectric element and which is oriented such that its thickness direction always extends along the separating surface and deforms in its thickness direction along a plane direction that extends along the separating surface, wherein the opening and closing mechanism is transitioned by deformation of the deformable member along the separating surface between first and second states in which opening amounts of the hole differ from each other.
2. The opening and closing device according to claim 1, wherein
 - the hole is formed in a slit shape, and
 - the deformable member covers the hole with a side surface thereof.
3. The opening and closing device according to claim 1, wherein
 - the opening and closing mechanism includes a cover provided at a free end side of the deformable member, and covers the hole by moving the cover.
4. The opening and closing device according to claim 1, wherein
 - said hole includes a first hole and a second hole and the first hole and the second hole are opened in the separating surface,
 - the opening and closing mechanism can be transitioned by deforming the common deformable member between two states, and
 - an opening amount of the first hole in one state of the two states is different from an opening amount of the first hole in the other state, and an opening amount of the second hole in the one state of the two states is different from an opening amount of the second hole in the other state.

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5. The opening and closing device according to claim 1, wherein the deformable member is a piezoelectric element, and

the opening and closing device comprises a controller for controlling deformation of the piezoelectric element.

6. The opening and closing device according to claim 1, comprising a biasing mechanism for biasing the opening and closing mechanism toward the separating surface.

7. A respiratory assistance device comprising the opening and closing device according to claim 1, wherein

the separating member is formed by: a mask for covering a nose or a mouth; and a communicating pipe communicated with a space formed inside the mask in a worn state.

8. The respiratory assistance device according to claim 7, wherein the mask includes the separating member so that the hole is formed in the mask.

9. The respiratory assistance device according to claim 7, wherein the communicating pipe includes the separating member so that the hole is formed in the communicating pipe.

10. The respiratory assistance device according to claim 7, wherein the hole forms an expiratory pathway through which expiratory air exhaled from the nose or the mouth passes.

11. A respiratory assistance device comprising:

- the opening and closing device according to claim 1;
- a flow passage through which an expiratory or inspiratory gas passes;
- an inspiratory nozzle disposed in the flow passage, for jetting an acceleration gas in an inspiratory direction;
- an expiratory nozzle disposed in the flow passage closer to an expiratory direction side than the inspiratory nozzle, for jetting an acceleration gas in the expiratory direction;
- a pump unit for supplying the acceleration gas to the inspiratory nozzle and the expiratory nozzle;
- an inspiratory Venturi wall extending from the inspiratory nozzle toward the inspiratory direction in the flow passage so as to spread out the acceleration gas emitted from the inspiratory nozzle in order to set the inspiratory direction side from the inspiratory nozzle at a negative pressure; and
- an expiratory Venturi wall extending from the expiratory nozzle toward the expiratory direction in the flow passage so as to spread out the acceleration gas emitted from the expiratory nozzle in order to set the expiratory direction side from the expiratory nozzle at a negative pressure, wherein the opening and closing device can be transitioned between a state in which one of the inspiratory nozzle and the expiratory nozzle is blocked and a state in which the other one of them is blocked.

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