



US008295946B2

(12) **United States Patent**
Inman

(10) **Patent No.:** **US 8,295,946 B2**
(45) **Date of Patent:** **Oct. 23, 2012**

(54) **ELECTRODE ASSEMBLY WITH FIBERS FOR A MEDICAL DEVICE**

(75) Inventor: **D. Michael Inman**, Gainesville, FL (US)

(73) Assignee: **Cyberonics, Inc.**, Houston, TX (US)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

(21) Appl. No.: **13/113,737**

(22) Filed: **May 23, 2011**

(65) **Prior Publication Data**

US 2011/0224767 A1 Sep. 15, 2011

Related U.S. Application Data

(62) Division of application No. 11/627,872, filed on Jan. 26, 2007, now Pat. No. 7,974,707.

(51) **Int. Cl.**
A61N 1/05 (2006.01)

(52) **U.S. Cl.** **607/118; 607/116; 607/117**

(58) **Field of Classification Search** **607/118, 607/125-128; 600/393**

See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

3,421,511 A	1/1969	Schwartz et al.
3,760,812 A	9/1973	Timm
3,796,221 A	3/1974	Hagfors
4,291,699 A	9/1981	Geddes et al.
4,305,402 A	12/1981	Katims
4,384,926 A	5/1983	Wagner
4,407,303 A	10/1983	Akerstrom
4,458,696 A	7/1984	Larimore

4,459,989 A	7/1984	Borkan
4,573,481 A	3/1986	Bullara
4,590,946 A	5/1986	Loeb
4,592,359 A	6/1986	Galbraith
4,606,349 A	8/1986	Livingston et al.
4,608,985 A	9/1986	Crish et al.
4,612,934 A	9/1986	Borkan
4,628,942 A	12/1986	Sweeney et al.
4,630,615 A	12/1986	Yomtov
4,649,936 A	3/1987	Ungar et al.

(Continued)

FOREIGN PATENT DOCUMENTS

WO 2004/069330 8/2004

OTHER PUBLICATIONS

Woodbury et al.; "Vagal Stimulation Reduces the Severity of Maximal Electroshock Seizures in Intact Rats: Use of a Cuff Electrode for Stimulating and Recording"; Department of Physiology, School of Medicine, University of Utah; Jan. 1991; pp. 94-107; vol. 14; Salt Lake City, Utah.

(Continued)

Primary Examiner — Carl H Layno

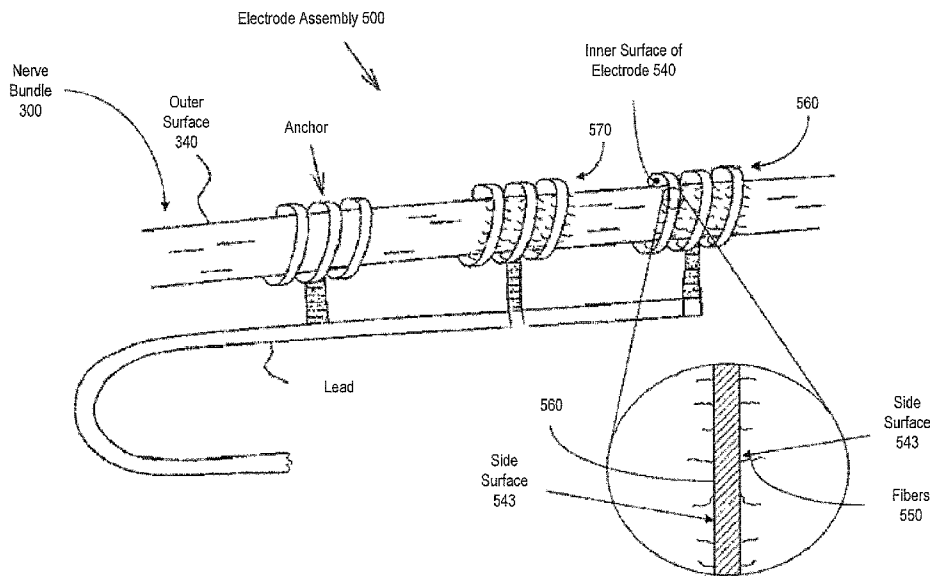
Assistant Examiner — Paula J Stice

(74) *Attorney, Agent, or Firm* — Cyberonics, Inc.

(57) **ABSTRACT**

An electrode assembly includes an electrode adapted to at least partially surround a first longitudinal portion of a target nerve or nerve bundle. The electrode includes an inner surface adapted to contact an outer surface of the target nerve or nerve bundle. The electrode also includes a plurality of fiber elements each having a proximal end and a distal end. The fiber elements are coupled at the proximal ends to the inner surface of the electrode and the distal ends of the fiber elements are operative to penetrate the outer surface of the target nerve or nerve bundle.

25 Claims, 9 Drawing Sheets



U.S. PATENT DOCUMENTS					
4,702,254 A	10/1987	Zabara	6,104,956 A	8/2000	Naritoku et al.
4,793,353 A	12/1988	Borkan	6,154,678 A	11/2000	Lauro
4,821,724 A	4/1989	Whigham et al.	6,171,239 B1	1/2001	Humphrey
4,827,932 A	5/1989	Ideker et al.	6,181,969 B1	1/2001	Gord
4,850,356 A	7/1989	Heath	6,208,902 B1	3/2001	Boveja et al.
4,860,616 A	8/1989	Smith	6,212,431 B1	4/2001	Hahn et al.
4,867,164 A	9/1989	Zabara	6,216,045 B1	4/2001	Black et al.
4,870,341 A	9/1989	Pihl et al.	6,259,951 B1	7/2001	Kuzma
4,899,750 A	2/1990	Ekwall	6,269,270 B1	7/2001	Boveja
4,903,700 A	2/1990	Whigham et al.	6,304,787 B1	10/2001	Kuzma et al.
4,920,979 A	5/1990	Bullara	6,317,633 B1	11/2001	Jorgenson et al.
4,964,407 A	10/1990	Baker, Jr. et al.	6,339,725 B1	1/2002	Naritoku et al.
4,969,468 A	11/1990	Byers et al.	6,341,236 B1	1/2002	Osorio et al.
4,979,511 A	12/1990	Terry, Jr.	6,393,325 B1	5/2002	Mann et al.
5,003,975 A	4/1991	Hafelfinger et al.	6,400,988 B1	6/2002	Gurewitsch
5,025,807 A	6/1991	Zabara	6,418,348 B1	7/2002	Witte
5,095,905 A	3/1992	Klepinski	6,445,951 B1	9/2002	Mouchawar
5,111,815 A	5/1992	Mower	6,453,198 B1	9/2002	Torgerson et al.
5,137,020 A	8/1992	Wayne et al.	6,456,481 B1	9/2002	Stevenson
5,137,021 A	8/1992	Wayne et al.	6,473,653 B1	10/2002	Schallhorn et al.
5,139,028 A	8/1992	Steinhaus et al.	6,477,417 B1	11/2002	Levine
5,146,920 A	9/1992	Yuuchi et al.	6,490,486 B1	12/2002	Bradley
5,154,172 A	10/1992	Terry, Jr. et al.	6,505,074 B2	1/2003	Boveja et al.
5,179,950 A	1/1993	Stanislaw	6,510,332 B1	1/2003	Greenstein
5,186,170 A	2/1993	Varrichio et al.	6,529,774 B1	3/2003	Greene
5,188,104 A	2/1993	Wernicke et al.	6,553,263 B1	4/2003	Meadows et al.
5,201,808 A	4/1993	Steinhaus et al.	6,556,868 B2	4/2003	Naritoku et al.
5,201,865 A	4/1993	Kuehn	6,587,719 B1	7/2003	Barrett et al.
5,205,285 A	4/1993	Baker, Jr.	6,587,727 B2	7/2003	Osorio et al.
5,215,086 A	6/1993	Terry, Jr. et al.	6,600,956 B2	7/2003	Maschino et al.
5,215,089 A	6/1993	Baker, Jr.	6,600,957 B2	7/2003	Gadsby
5,222,494 A	6/1993	Baker, Jr.	6,606,523 B1	8/2003	Jenkins
5,237,991 A	8/1993	Baker, Jr. et al.	6,609,025 B2	8/2003	Barrett et al.
5,251,634 A	10/1993	Weinberg	6,620,186 B2	9/2003	Saphon et al.
5,263,480 A	11/1993	Wernicke et al.	6,622,038 B2	9/2003	Barrett et al.
5,269,303 A	12/1993	Wernicke et al.	6,622,041 B2	9/2003	Terry, Jr. et al.
5,299,569 A	4/1994	Wernicke et al.	6,622,047 B2	9/2003	Barrett et al.
5,304,206 A	4/1994	Baker, Jr. et al.	6,648,823 B2	11/2003	Thompson
5,330,515 A	7/1994	Rutecki et al.	6,658,294 B1	12/2003	Zadeh et al.
5,335,657 A	8/1994	Terry, Jr. et al.	6,662,053 B2	12/2003	Borkan
5,351,394 A	10/1994	Weinberg	6,671,556 B2	12/2003	Osorio et al.
5,411,528 A	5/1995	Miller et al.	6,684,105 B2	1/2004	Cohen et al.
5,431,692 A	7/1995	Hansen et al.	6,687,538 B1	2/2004	Hrdlicka et al.
5,466,255 A	11/1995	Franchi	6,690,974 B2	2/2004	Archer et al.
5,501,702 A	3/1996	Plicchi et al.	6,711,440 B2	3/2004	Deal et al.
5,507,786 A	4/1996	Morgan et al.	6,718,203 B2	4/2004	Weiner et al.
5,522,865 A	6/1996	Schulman et al.	6,718,207 B2	4/2004	Connelly
5,531,778 A	7/1996	Maschino et al.	6,721,600 B2	4/2004	Jorgenson et al.
5,534,018 A	7/1996	Wahlstrand et al.	6,721,603 B2	4/2004	Zabara et al.
5,540,730 A	7/1996	Terry, Jr. et al.	6,725,092 B2	4/2004	MacDonald et al.
5,540,734 A	7/1996	Zabara	6,731,979 B2	5/2004	MacDonald
5,549,646 A	8/1996	Katz et al.	6,745,077 B1	6/2004	Griffith et al.
5,571,150 A	11/1996	Wernicke et al.	6,754,539 B1	6/2004	Erickson et al.
5,575,813 A	11/1996	Edell et al.	6,757,566 B2	6/2004	Weiner et al.
5,620,474 A	4/1997	Koopman	6,760,624 B2	7/2004	Anderson et al.
5,658,318 A	8/1997	Stroetmann et al.	6,760,625 B1	7/2004	Kroll
5,690,681 A	11/1997	Geddes et al.	6,760,628 B2	7/2004	Weiner et al.
5,700,282 A	12/1997	Zabara	6,763,268 B2	7/2004	MacDonald et al.
5,707,400 A	1/1998	Terry, Jr. et al.	6,778,856 B2	8/2004	Connelly et al.
5,713,936 A	2/1998	Staub et al.	6,792,316 B2	9/2004	Sass
5,741,311 A	4/1998	Mc Venes et al.	6,795,730 B2	9/2004	Connelly et al.
5,743,860 A	4/1998	Hively et al.	6,795,736 B2	9/2004	Connelly et al.
5,755,742 A	5/1998	Schuelke et al.	6,799,069 B2	9/2004	Weiner et al.
5,755,747 A	5/1998	Daly et al.	6,804,557 B1	10/2004	Kroll
5,759,199 A	6/1998	Snell et al.	6,819,954 B2	11/2004	Connelly
5,769,873 A	6/1998	Zadeh	6,819,958 B2	11/2004	Weiner et al.
5,796,044 A	8/1998	Cobian et al.	6,829,509 B1	12/2004	MacDonald et al.
5,814,088 A	9/1998	Paul et al.	6,843,870 B1	1/2005	Bluger
5,876,425 A	3/1999	Gord et al.	6,845,266 B2	1/2005	Weiner et al.
5,891,179 A	4/1999	Er et al.	6,850,805 B2	2/2005	Connelly et al.
5,897,577 A	4/1999	Cinbis et al.	6,875,180 B2	4/2005	Weiner et al.
5,916,239 A	6/1999	Geddes et al.	6,901,290 B2	5/2005	Foster et al.
5,919,220 A	7/1999	Stieglitz et al.	6,906,256 B1	6/2005	Wang
5,928,272 A	7/1999	Adkins et al.	6,907,295 B2	6/2005	Gross et al.
5,995,868 A	11/1999	Dorfmeister et al.	6,920,357 B2	7/2005	Osorio et al.
6,035,237 A	3/2000	Schulman et al.	6,925,328 B2	8/2005	Foster et al.
6,052,624 A	4/2000	Mann	6,944,489 B2	9/2005	Zeijlemaker et al.
6,073,050 A	6/2000	Griffith	6,949,929 B2	9/2005	Gray et al.
			6,954,674 B2	10/2005	Connelly

6,961,618 B2	11/2005	Osorio et al.	2006/0167497 A1	7/2006	Armstrong et al.
6,985,775 B2	1/2006	Reinke et al.	2006/0173493 A1	8/2006	Armstrong et al.
6,993,387 B2	1/2006	Connelly et al.	2006/0184211 A1	8/2006	Gaunt et al.
7,006,859 B1	2/2006	Osorio et al.	2006/0224199 A1	10/2006	Zeijlemaker et al.
7,010,357 B2	3/2006	Helfer et al.	2006/0253164 A1	11/2006	Zhang et al.
7,013,174 B2	3/2006	Connelly et al.	2006/0265025 A1	11/2006	Goetz et al.
7,015,393 B2	3/2006	Weiner et al.	2007/0027497 A1	2/2007	Parnis et al.
7,047,074 B2	5/2006	Connelly et al.	2007/0027498 A1	2/2007	Maschino et al.
7,054,686 B2	5/2006	MacDonald	2007/0027500 A1	2/2007	Maschino et al.
7,107,097 B2	9/2006	Stern et al.	2007/0032834 A1	2/2007	Gliner et al.
7,123,013 B2	10/2006	Gray	2007/0060991 A1	3/2007	North et al.
7,171,166 B2	1/2007	Ng et al.	2007/0073150 A1	3/2007	Gopalsami et al.
7,174,219 B2	2/2007	Wahlstrand et al.	2007/0100392 A1	5/2007	Maschino et al.
7,212,869 B2	5/2007	Wahlstrom et al.	2007/0142889 A1	6/2007	Whitehurst et al.
7,221,981 B2	5/2007	Gliner	2007/0173902 A1	7/2007	Maschino et al.
7,239,924 B2	7/2007	Kolberg	2007/0179557 A1	8/2007	Maschino et al.
7,289,856 B1	10/2007	Karicherla	2007/0179579 A1	8/2007	Feler et al.
7,584,004 B2 *	9/2009	Caparso et al. 607/118	2007/0179584 A1	8/2007	Gliner
8,024,022 B2 *	9/2011	Schulman et al. 600/372	2008/0033503 A1	2/2008	Fowler et al.
2002/0072782 A1	6/2002	Osorio et al.	2008/0046035 A1	2/2008	Fowler et al.
2003/0083726 A1	5/2003	Zeijlemaker et al.	2008/0071323 A1	3/2008	Lowry et al.
2003/0195601 A1	10/2003	Hung et al.	2008/0200925 A1	8/2008	Johnson
2004/0015205 A1	1/2004	Whitehurst et al.	2008/0215110 A1	9/2008	Gunderson et al.
2004/0147992 A1	7/2004	Bluger et al.	2008/0255582 A1	10/2008	Harris
2004/0167583 A1	8/2004	Knudson et al.	2009/0076567 A1	3/2009	Fowler et al.
2004/0172088 A1	9/2004	Knudson et al.			
2004/0210291 A1	10/2004	Erickson			
2005/0015128 A1	1/2005	Rezai et al.			
2005/0016657 A1	1/2005	Bluger			
2005/0107858 A1	5/2005	Bluger			
2005/0154426 A1	7/2005	Boveja et al.			
2005/0154435 A1	7/2005	Stern et al.			
2005/0222642 A1	10/2005	Przybyszewski et al.			
2005/0272280 A1	12/2005	Osyпка			
2006/0058597 A1	3/2006	Machado et al.			
2006/0106430 A1	5/2006	Fowler et al.			

OTHER PUBLICATIONS

Sahin; "Improved Nerve Cuff Electrode Recordings With Subthreshold Anodic Currents"; IEEE Transactions on Biomedical Engineering, Aug. 1998; pp. 1044-1050; vol. 45; No. 8.
 Bassar et al.; "New Currents in Electrical Stimulation of Excitable Tissues"; Annu. Rev. Biomed. Eng. 2000; vol. 2; pp. 377-397.

* cited by examiner

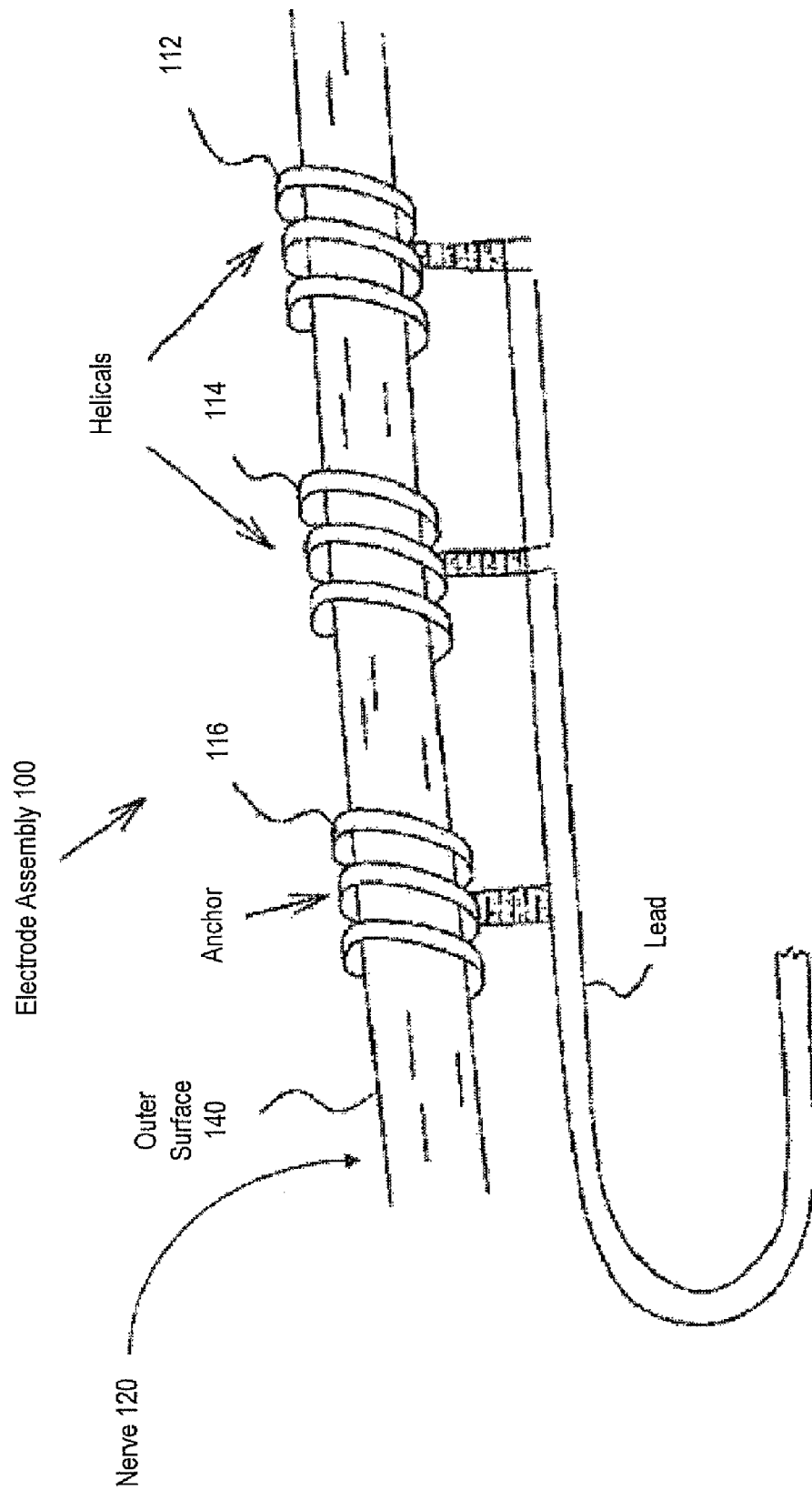


FIGURE 1
(Prior Art)

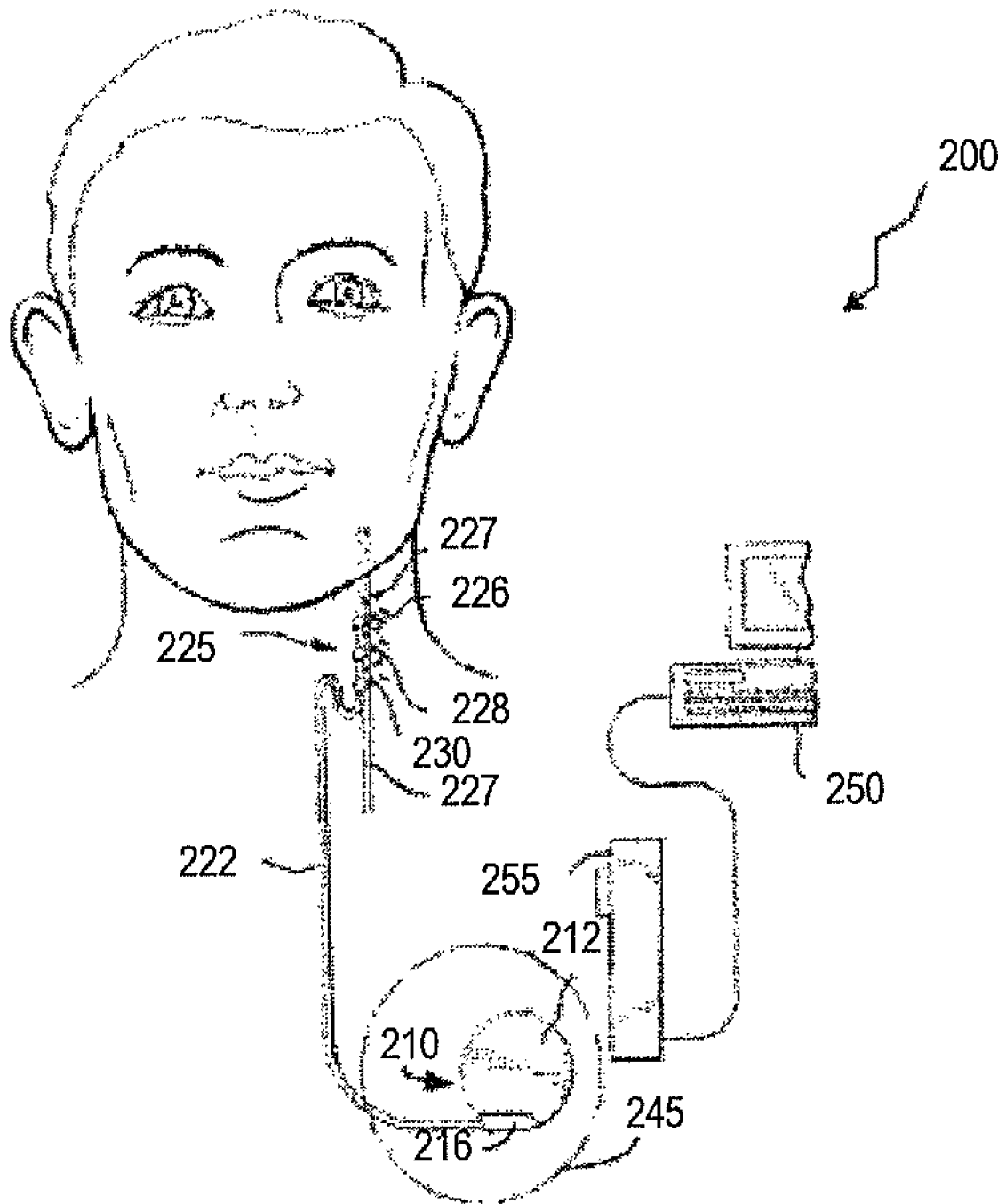


FIGURE 2

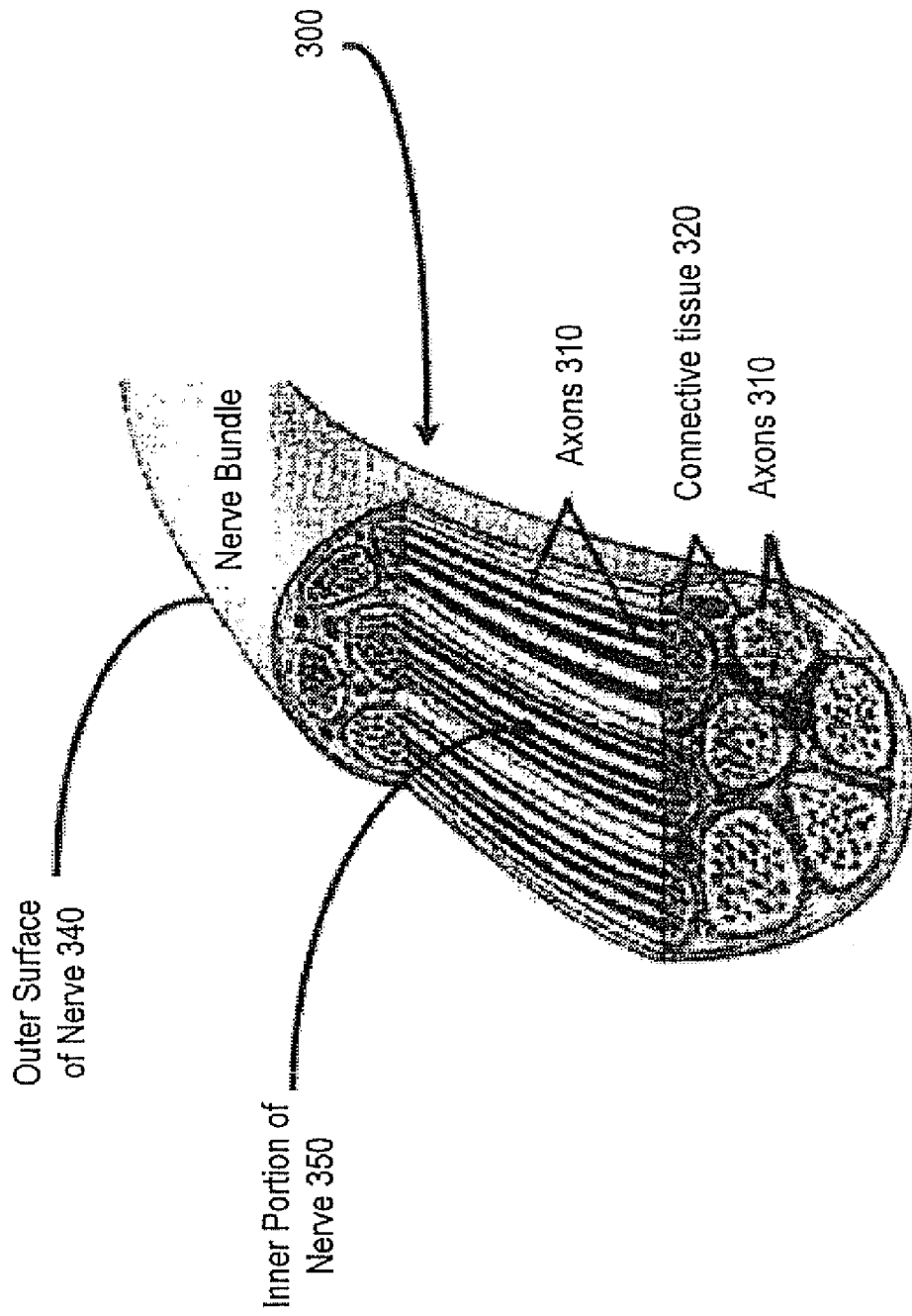


FIGURE 3

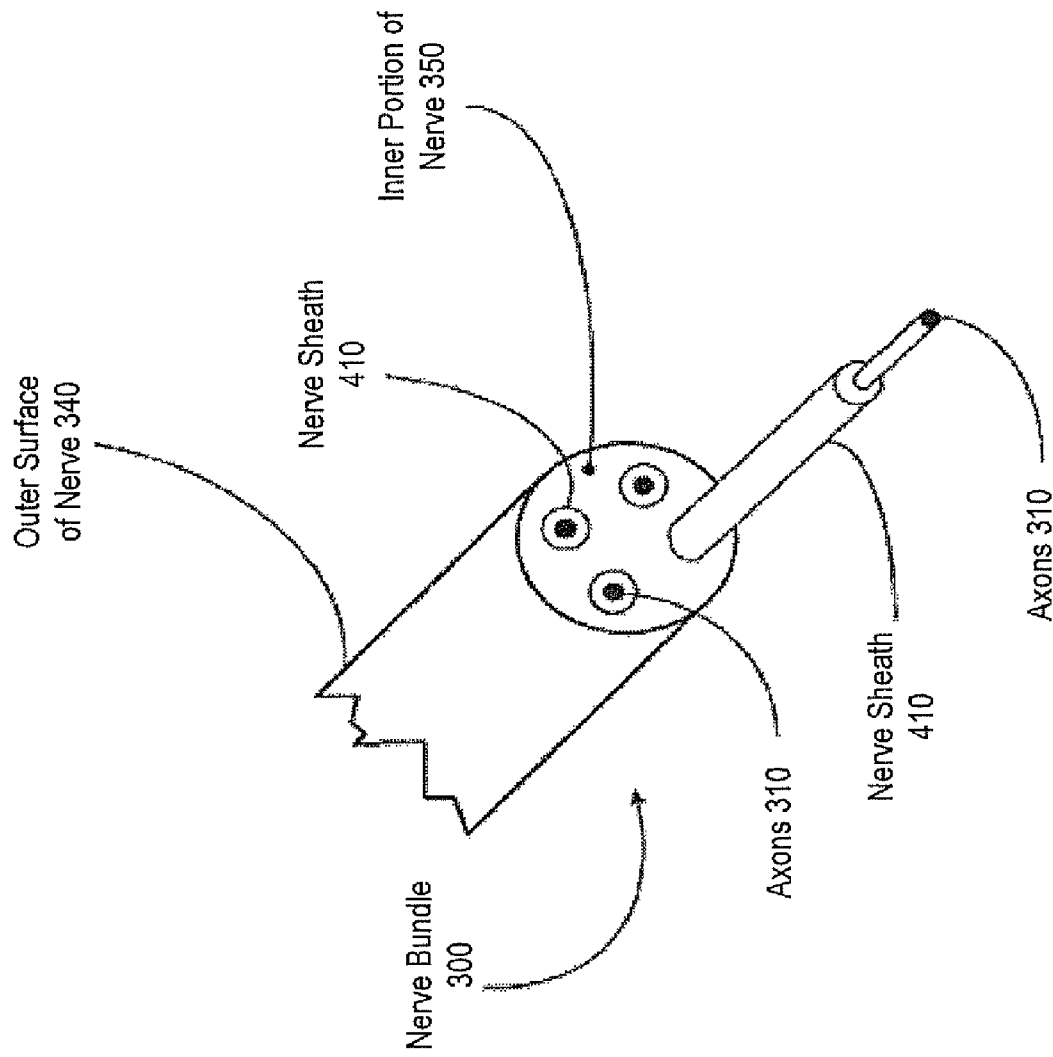


FIGURE 4

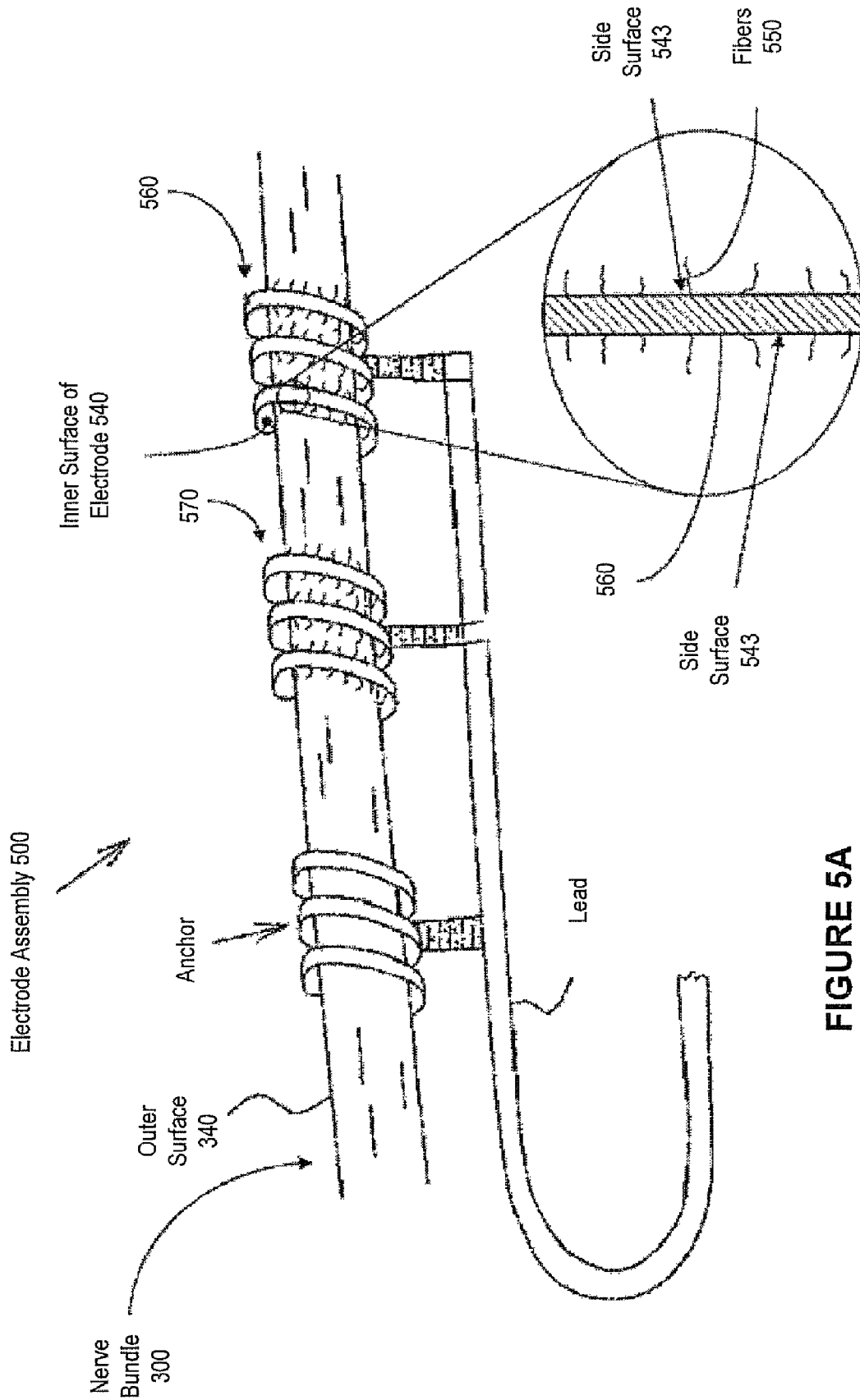


FIGURE 5A

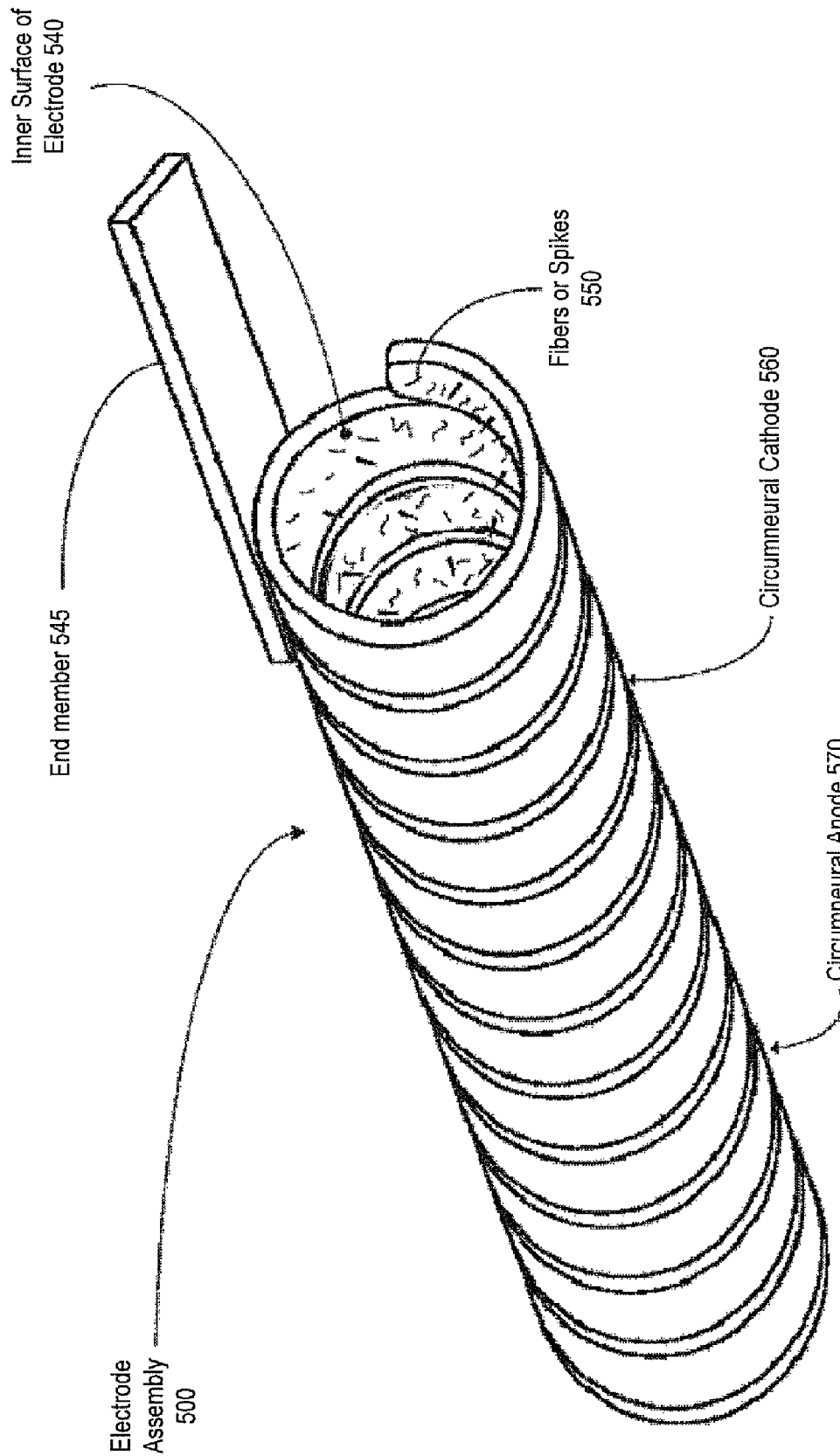


FIGURE 5B

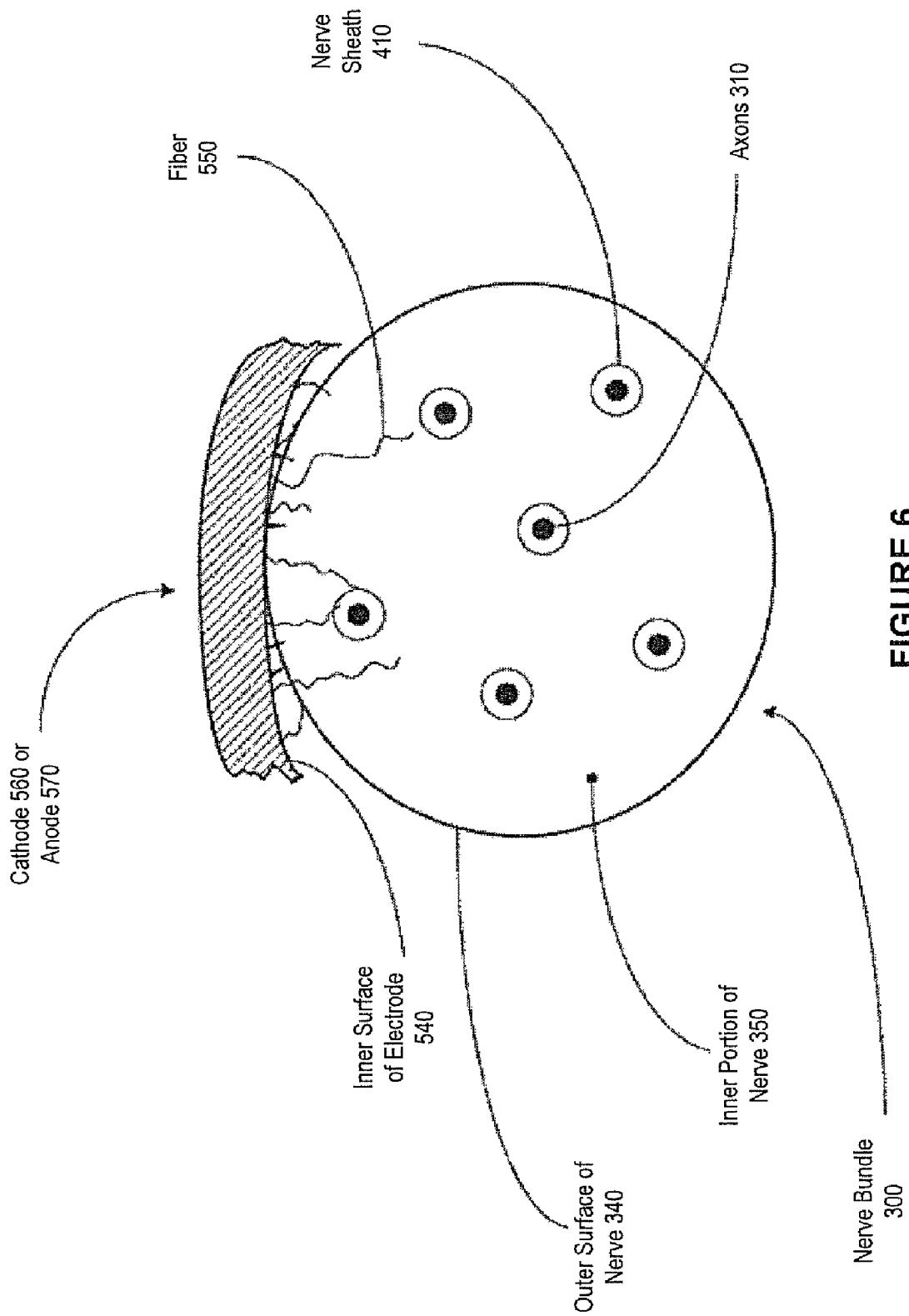


FIGURE 6

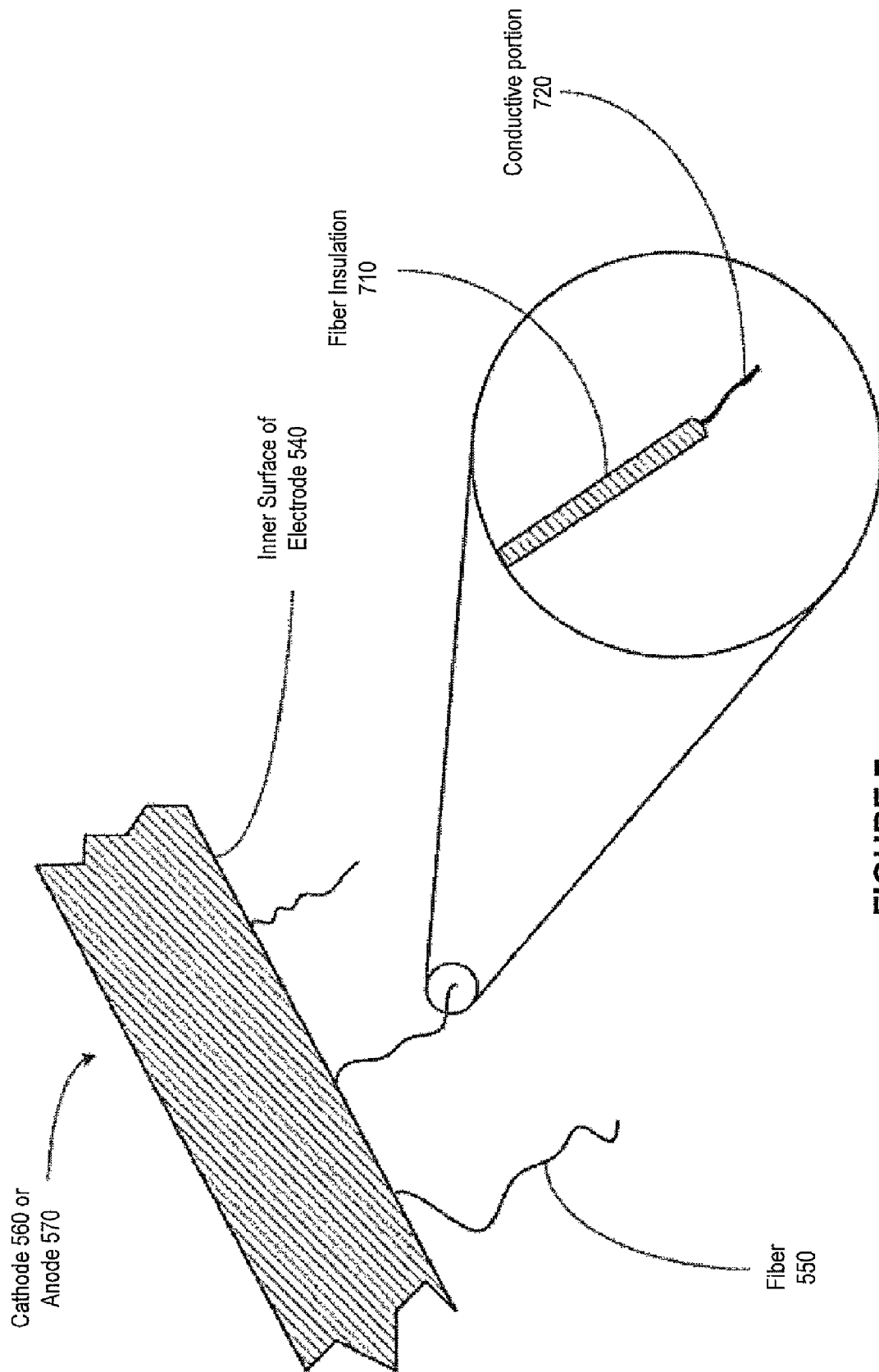


FIGURE 7

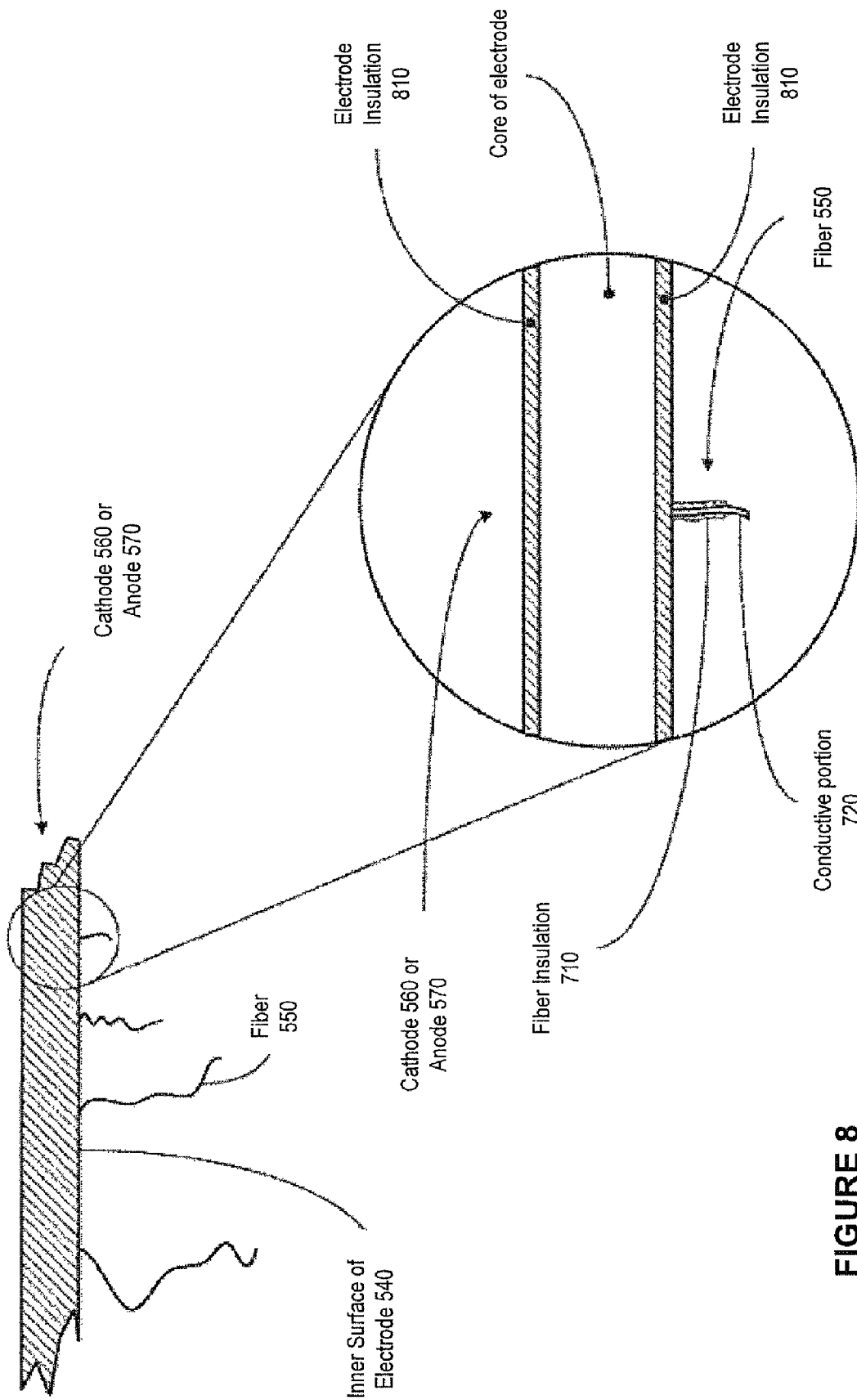


FIGURE 8

ELECTRODE ASSEMBLY WITH FIBERS FOR A MEDICAL DEVICE

CLAIM OF PRIORITY

This application claims priority as a divisional application from U.S. patent application Ser. No. 11/627,872, now issued as U.S. Pat. No. 7,974,707, filed Jan. 26, 2007, the entire contents of which are incorporated herein by reference.

FIELD OF THE DISCLOSURE

This disclosure relates generally to an apparatus for delivering an electrical signal to a patient's body using an implantable medical device (IMD) system and, more particularly, an electrode including fibrous components for improved electrical contact with a targeted portion of the patient's body for delivering a stimulation signal from an IMD.

BACKGROUND

Many advancements have been made in treating diseases such as epilepsy. Therapies using electrical signals for treating these diseases have been found to be effective. IMDs have been effectively used to deliver therapeutic stimulation to various portions of the human body (e.g., the vagus nerve) for treating these diseases. As used herein, "stimulation" or "stimulation signal" refers to the application of an electrical, mechanical, magnetic, electro-magnetic, photonic, audio and/or chemical signal to a target tissue in the patient's body. The signal is an exogenous signal that is distinct from the endogenous electrical, mechanical, and chemical activity (e.g., afferent and/or efferent electrical action potentials) generated by the patient's body and environment. In other words, the stimulation signal (whether electrical, mechanical, magnetic, electro-magnetic, photonic, audio, or chemical in nature) applied to the tissue is a signal applied from an artificial source, e.g., a neurostimulator.

A "therapeutic signal" refers to a stimulation signal delivered to a patient's body with the intent of treating a disorder by providing a modulating effect to the target tissue, e.g., a neural tissue. The effect of a stimulation signal on electrical, chemical and/or mechanical activity in the target tissue is termed "modulation"; however, for simplicity, the terms "stimulating" and "modulating", and variants thereof, are sometimes used interchangeably herein. In general, however, the delivery of an exogenous signal itself refers to "stimulation" of the target tissue, while the effects of that signal, if any, on the electrical, chemical and/or mechanical activity of the target tissue are properly referred to as "modulation." The modulating effect of the stimulation signal upon the target tissue may be excitatory or inhibitory, and may potentiate acute and/or long-term changes in electrical, chemical and/or mechanical activity. For example, the "modulating" effect of the stimulation signal to a target neural tissue may have one or more of the following effects: (a) initiation of an action potential (afferent and/or efferent action potentials); (b) inhibition or blocking of the conduction of action potentials, whether endogenously or exogenously induced, including hyperpolarizing and/or collision blocking; (c) affecting changes in neurotransmitter/neuromodulator release or uptake; and (d) changes in neuro-plasticity or neurogenesis of brain tissue.

Electrical neurostimulation may be provided by implanting an electrical device underneath the patient's skin and delivering an electrical signal to a nerve, such as a cranial nerve. In one embodiment, the electrical neurostimulation involves sensing or detecting a body parameter, with the

electrical signal being delivered in response to the sensed body parameter. This type of stimulation is generally referred to as "active," "feedback," or "triggered" stimulation. In another embodiment, the system may operate without sensing or detecting a body parameter once the patient has been diagnosed with a medical condition that may be treated by neurostimulation. In this case, the system may apply a series of electrical pulses to the nerve (e.g., a cranial nerve such as a vagus nerve) periodically, intermittently, or continuously throughout the day, or over another predetermined time interval. This type of stimulation is generally referred to as "passive," "non-feedback," or "prophylactic," stimulation. The electrical signal may be applied by an IMD that is implanted within the patient's body. In another alternative embodiment, the signal may be generated by an external pulse generator outside the patient's body, coupled by an RF or wireless link to an implanted electrode.

Generally, neurostimulation signals that perform neuromodulation are delivered by the IMD via one or more leads. The leads generally terminate at their distal ends in one or more electrodes, and the electrodes, in turn, are electrically coupled to tissue in the patient's body. For example, a number of electrodes may be attached to various points of a nerve or other tissue inside a human body for delivery of a neurostimulation signal.

Turning now to FIG. 1, a prior art electrode assembly **100** operatively coupled to a nerve bundle **120** having a plurality of individual nerve fibers or axons is illustrated. The electrode assembly **100** comes into contact with the external periphery of the nerve **120** to deliver an electrical signal to the nerve. The electrode assembly **100** includes a first helical portion **112**, a second helical portion **114** and an anchor **116** that couples the electrode to the nerve bundle **120**. The first helical portion **112** may be a cathode portion, and the second helical portion **114** may be an anode portion of the electrode assembly **100**. The electrode assembly **100** is coupled to a lead that carries an electrical signal from the IMD. Typically, state-of-the-art neurostimulation electrodes deliver electrical signals to the outer surface **140** of nerve bundle **120**. Generally, this disposition of the stimulation electrode assembly **100** only provides penetration of electrical charge into areas near the outer surface **140** of the nerve bundle **120**. Accordingly, the state-of-the-art electrode assembly **100** may only achieve an activation of a small percentage of the nerve axons in the nerve bundle **120**. Some estimates have suggested that as little as 5% of the total population of nerve axons within a nerve bundle may be activated using the state-of-the-art electrode assembly **100**.

The state-of-the-art electrode assembly **100** may only provide adequate stimulation (i.e., may only modulate electrical activity) of individual nerve fibers (axons) that are in close proximity to the outside surface of the nerve bundle **120**. Some patients may not respond to neurostimulation therapy due to the failure of electrical signals delivered to the outer portions of the nerve bundle **120** to penetrate to a sufficient depth within the nerve bundle **120** to recruit nerve axons that are relevant to the patient's condition. This factor may result in a reduced efficacy of the therapy or in some cases a complete failure of the patient to respond to the therapy.

Another problem associated with the state-of-the-art electrode assembly **100** is that, as a result of the attenuation described above, a signal with larger power than otherwise would have been required, is needed to achieve desired efficacy. Physicians may be compelled to increase the dosage, i.e., frequency, power, pulse width, etc., of stimulation signals to achieve desired efficacy. This excessive usage of power may result in reduced battery life because of the portion of the

electrical signal that is non-therapeutic or sub-optimal in achieving therapeutic efficacy.

The present disclosure is directed to overcoming, or at least reducing, the effects of one or more of the problems set forth above.

SUMMARY

In one aspect, an apparatus is provided for employing an electrode for delivering an electrical signal to a target nerve of a tissue of a patient's body, wherein the nerve has an outer surface and an inner portion. The electrode includes an inner surface to contact to the outer surface of the target nerve. The electrode also includes a plurality of fiber elements having a proximal end and a distal end. The fiber elements are coupled at the proximal end to the inner surface of the electrode.

In another aspect, an apparatus is provided for employing an electrode for delivering an electrical signal to a cranial nerve of a tissue of a patient's body, wherein the nerve includes an outer surface and an inner portion. The electrode includes a first surface to electrically couple to the cranial nerve. The electrode also includes a plurality of fibers having a proximal end and a distal end. Each of the fibers is coupled to the first surface at the proximal end. The fibers are conductive and adapted to migrate beneath the outer surface of the cranial nerve to deliver an electrical signal to the inner portion of the cranial nerve.

In yet another aspect, an implantable medical device system is provided for delivering an electrical signal to a portion of a target tissue of a patient's body. The tissue has an outer surface and an interior portion. The IMD system includes an IMD for generating an electrical signal. The system also includes an electrode that is operatively coupled to the IMD. The electrode is provided for delivering the electrical signal to the target tissue of a patient's body. The electrode includes a first surface to electrically couple to an outer surface of the target tissue. The electrode also includes a plurality of longitudinal elements coupled to the first surface. The plurality of longitudinal elements are adapted to electrically couple to at least one of the outer surface and the interior portion of the target tissue.

BRIEF DESCRIPTION OF THE DRAWINGS

The disclosure may be understood by reference to the following description taken in conjunction with the accompanying drawings, in which like reference numerals identify like elements, and in which:

FIG. 1 illustrates a prior art electrode assembly used with implantable medical devices, the electrode assembly being coupled to a nerve trunk;

FIG. 2 provides a stylized diagram of a system that includes an IMD and an electrode assembly implanted into a patient's body for providing a therapeutic electrical signal to a neural structure of the patient's body, in accordance with one illustrative embodiment;

FIG. 3 illustrates a stylized cross-sectional depiction of a target nerve for a therapeutic electrical signal;

FIG. 4 illustrates a cross-sectional view of a nerve, including a stylized isometric depiction of myelinated axon and an unmyelinated axon;

FIG. 5A illustrates an electrode assembly coupled to a nerve, in accordance with one illustrative embodiment;

FIG. 5B illustrates a helical configuration of the electrode assembly, in accordance with one illustrative embodiment;

FIG. 6 illustrates a stylized depiction of a portion of an electrode in contact with a nerve, along with stylized, cross-sectional view of the nerve in accordance with one illustrative embodiment;

FIG. 7 illustrates a stylized depiction of a fibrous material coupled to an electrode, along with a stylized, magnified depiction of the fibrous material, in accordance with one illustrative embodiment; and

FIG. 8 illustrates a stylized, magnified, cross-sectional depiction of an electrode with an insulating material, in accordance with one illustrative embodiment.

While the disclosed embodiments are susceptible to various modifications and alternative forms, specific embodiments have been shown by way of example in the drawings and are herein described in detail. It should be understood, however, that the description herein of specific embodiments is not intended to limit the disclosure to the particular forms disclosed, but on the contrary, the intention is to cover all modifications, equivalents, and alternatives falling within the scope of the disclosure as defined by the appended claims.

DETAILED DESCRIPTION

Illustrative embodiments are described herein. In the interest of clarity, not all features of an actual implementation are described in this specification. In the development of any such actual embodiment, numerous implementation-specific decisions must be made to achieve the design-specific goals, which will vary from one implementation to another. It will be appreciated that such a development effort, while possibly complex and time-consuming, would nevertheless be a routine undertaking for persons of ordinary skill in the art having the benefit of this disclosure.

This document does not intend to distinguish between components that differ in name but not function. In the following discussion and in the claims, the terms "including" and "includes" are used in an open-ended fashion, and thus should be interpreted to mean "including, but not limited to." Also, the term "couple" or "couples" is intended to mean either a direct or an indirect electrical connection. "Direct contact," "direct attachment," or providing a "direct coupling" indicates that a surface of a first element contacts a surface of a second element with no substantial attenuating medium there between. The presence of substances, such as bodily fluids, that do not substantially attenuate electrical connections does not vitiate direct contact. The word "or" is used in the inclusive sense (i.e., "and/or") unless a specific use to the contrary is explicitly stated.

The term "electrode" or "electrodes" described herein may refer to one or more stimulation electrodes (i.e., electrodes for delivering an electrical signal generated by an IMD to a tissue), sensing electrodes (i.e., electrodes for sensing a physiological indication of a patient's body), and/or electrodes that are capable of delivering a stimulation signal, as well as performing a sensing function.

Cranial nerve stimulation has been proposed to treat a number of disorders pertaining to or mediated by one or more structures of the nervous system of the body, including epilepsy and other movement disorders, depression, anxiety disorders and other neuropsychiatric disorders, dementia, traumatic brain injury, head trauma, coma, migraine headache, obesity, eating disorders, sleep disorders, cardiac disorders (such as congestive heart failure and atrial fibrillation), hypertension, endocrine disorders (such as diabetes and hypoglycemia) and pain, among others. See, e.g., U.S. Pat. Nos. 4,867,164; 5,299,569; 5,269,303; 5,571,150; 5,215,086; 5,188,104; 5,263,480; 6,587,719; 6,609,025; 5,335,657;

6,622,041; 5,916,239; 5,707,400; 5,231,988; and 5,330,515. Despite the numerous disorders for which cranial nerve stimulation has been proposed or suggested as a treatment option, the fact that detailed neural pathways for many (if not all) cranial nerves remain relatively unknown, makes predictions of efficacy for any given disorder difficult or impossible. Moreover, even if such pathways were known, the precise stimulation parameters that would modulate particular pathways relevant to a particular disorder generally cannot be predicted.

Despite the difficulties of predicting efficacy for particular disorders, the use of vagus nerve stimulation as a therapy for treating epilepsy and/or depression is an established therapy option. Electrodes may be used in a system to deliver therapeutic electrical signals from an IMD to a target portion of a patient's body (e.g., a vagus nerve) for treating these and other diseases. Embodiments disclosed herein provide for a "fibrous electrode," which refers to an electrode upon which one or more "fibers" may be coupled. Some embodiments provide for a "longitudinal element" coupled to a surface of an electrode. As used herein, a longitudinal element refers to an element whose longest dimension substantially exceeds other dimensions, e.g., length, width, cross-section, etc. Thus, a longitudinal element may include a "fiber" as previously disclosed. An example of a fiber may include, but is not limited to, a flexible material that is in mechanical and electrical communication with the electrode. These flexible materials may be formed from carbon nanotubes or interwoven fibers including carbon nanotubes, a variety of conductive materials, a variety of semi-conductive materials, and/or other materials that are relatively thin, strong and electrically conductive, or combinations of the foregoing. Embodiments disclosed herein provide for an electrode that includes one or more fibers that may be capable of penetrating an outer surface of a target tissue (e.g., a nerve bundle or an individual nerve) upon which the electrode is operatively coupled. Where the target tissue is a nerve bundle, the fibers of the electrode may penetrate the outer surface of a portion of the nerve to reach an interior portion of the nerve bundle to allow an electrical signal to be applied within the nerve bundle. Such an electrode will advantageously allow for greater electrical flux into the target nerve, and may permit recruitment and/or modulation of nerve fibers not capable of modulation with prior art electrodes coupled only to an outer surface of the nerve. Embodiments disclosed herein provide for a fibrous neurostimulation electrode that is capable of delivering electrical signals to an interior portion of a cranial nerve.

Utilizing embodiments disclosed herein, the penetration of the fibrous material operatively coupled to the electrode into the interior portion of the nerve may be used to cause the electrical signal to penetrate into the interior portions of the tissue to a greater depth than electrodes lacking said fibrous material, e.g., to various nerve fibers (axons) within the nerve bundle. Therefore, utilizing the electrodes disclosed, an increased population of nerve fibers may be modulated by the electrical signal. The "fibrous" or "fiber" electrodes provides for conductive communication with an interior portion of the nerve. The fiber or fibrous material may be of one or more of a plurality of materials, such as a stainless steel fiber, a carbon nanotube fiber, a conductive graphite fiber, a titanium fiber, a gold fiber, a copper fiber, silicon oxide, and/or one or more of any of a plurality of conductive materials capable of being formed into fibers of relatively small dimensions, e.g., below 1.0 mm.

The fibrous electrodes disclosed may also be used for sensing operations. Therefore, the fibers, e.g., microfibers or nanofibers, that are coupled to a first electrode may provide

for an increased population of nerve fibers being included and observed in sensing operations. Further, utilizing embodiments disclosed herein, a decreased amount of current density may be required to modulate a larger number of nerve fibers.

This may provide for usage of a lower power stimulation signal, while achieving equal or better delivery of therapeutic signals, and/or may allow therapeutic efficacy to be achieved for patients who otherwise would not respond to the electrical signal therapy.

Embodiments provide for applying a predetermined amount of force upon the fibrous electrode, which may prompt the fibers coupled to the electrode to migrate into the nerve bundle in a relatively slow manner. In this manner, penetration of the nerve bundles may be achieved over time without substantially causing excessive trauma to the nerve or surrounding tissue. Further, a multiplexing scheme may be used to deliver current or electrical signals to various portions of a nerve in a predetermined sequence. For example, during a first time period, the electrical signal may be applied to an exterior surface of the nerve using a first surface of the electrode, while during a second time period, the electrical signal may be applied to an interior portion of the nerve using a second, fibrous portion of the electrode. In this manner, a multiplexing scheme may be used to prompt increased diversity of nerve fibers recruited by the electrical signal. Similar benefits may be obtained when the electrode is used to sense electrical activity in the nerve bundle.

Although not so limited, a system capable of implementing particular embodiments is described below. FIG. 2 depicts a stylized implantable medical system 200 for implementing one or more embodiments. An electrical pulse generator 210 is provided, having a main body 212 including a case or shell with a header 216 for connecting to an insulated, electrically conductive lead assembly 222. The generator 210 is implanted in the patient's chest in a pocket or cavity formed by the implanting surgeon just below the skin (indicated by a dotted line 245), similar to the implantation procedure for a pacemaker pulse generator.

A fibrous electrode assembly 225, preferably including a plurality of electrodes having at least an electrode pair, is conductively connected to the distal end of the lead assembly 222, which preferably includes a plurality of lead wires (one wire for each electrode). Each electrode in the electrode assembly 225 may operate independently or alternatively, may operate in conjunction with the other electrodes. Each electrode may include one or more fibrous electrodes for applying electrical signals to a nerve bundle. In some embodiments, the fibrous portions of the electrode penetrate an outer surface of the nerve bundle to deliver electrical charge to an interior of the nerve bundle. In other embodiments, the fibers do not penetrate into the interior of the nerve, but provide for a higher charge flux into the target portion of the nerve compared to prior art electrodes. Some prior art electrodes for stimulation of neural tissues have extremely small surface areas, resulting in relatively high electrical flux across that area. When the electrical flux exceeds a threshold, the molecules of the metal electrode can be dissolved into the surrounding body fluids, which is usually toxic to the neural tissue. Because the fibers coupled to the electrode significantly increase the surface area across which the electrical charge is transferred, it provides a significantly reduced risk of electrode dissolution, thereby providing increased safety where a patient is treated with relatively strong electrical signals.

Referring again to FIG. 2, lead assembly 222 is attached at its proximal end to connectors on the header 216 of generator 210. The electrode assembly 225 may be surgically coupled

to a vagus nerve **227** in the patient's neck or at another location, e.g., near the patient's diaphragm or at the esophagus/stomach junction. Other (or additional) cranial nerves, such as the trigeminal and/or glossopharyngeal nerves may also be used to deliver the electrical signal in particular alternative embodiments. In one embodiment, the electrode assembly **225** includes a bipolar stimulating electrode pair **226, 228**. Suitable electrode assemblies which could be modified to provide embodiments are available from Cyberonics, Inc., Houston, Tex., USA as the Model 302 electrode assembly. However, persons of skill in the art will appreciate that many prior art electrode designs could be modified to provide particular embodiments. Moreover, other electrodes, such as spinal cord electrodes, deep brain stimulation (DBS) electrodes, electrodes for muscle stimulation, and electrodes for stimulation of organs or even bones could also be modified to provide particular embodiments. In one embodiment, the two electrodes are wrapped about the vagus nerve, and the electrode assembly **225** may be secured to the nerve **227** by a spiral anchoring tether **230**, such as that disclosed in U.S. Pat. No. 4,979,511 issued Dec. 25, 1990 to Reese S. Terry, Jr., and assigned to the same assignee as the instant application. Lead assembly **222** is secured, while retaining the ability to flex with movement of the chest and neck, by a suture connection to nearby tissue (not shown). While the electrode assembly **225** in FIG. 2 is described in terms of a stimulating electrode, it will be appreciated that alternative embodiments, the electrode assembly **225** may include a sensing electrode for sensing, e.g., heart rate, electrical activity in the target nerve, temperature, or other body parameters.

The electrical pulse generator **210** may be programmed with an external device, such as computer **250** using programming software known in the art of implantable medical devices. A programming wand **255** may be coupled to the computer **250** as part of the external device to facilitate radio frequency (RF) communication between the computer **250** and the pulse generator **210**. The programming wand **255** and computer **250** permit non-invasive communication with the generator **210** after the latter is implanted. In systems where the computer **250** uses one or more channels in the Medical Implant Communications Service (MICS) bandwidths, the programming wand **255** may be omitted to permit more convenient communication directly between the computer **250** and the pulse generator **210**.

Turning now to FIG. 3, a cross-sectional stylized view of a nerve or a nerve bundle **300** is illustrated. The nerve or nerve bundle **300** may have an outer surface **340** and an inner portion **350** including a plurality of axons **310** and connective tissue **320**. The axons **310** transport electrical action potentials along the axis of the nerve bundle **300**. Typically, one or more axons **310** affecting the patient's medical condition may not be sufficiently stimulated using state-of-the-art electrodes that deliver electrical signals to the exterior surface of the nerve bundle **300**. Embodiments disclosed herein provide for more robust stimulation since internal portions of the nerve bundle **300** may be more directly stimulated, and/or lower electrical flux values across the electrode providing increased safety.

Referring to FIG. 4, a cross-sectional view of the nerve bundle **300** with a stylized, isometric depiction of a myelin nerve sheath **410** surrounding an axon **310** is illustrated. It is known in the art that large nerve bundles, such as the vagus nerve, include nerves of multiple nerve types, such as A and B fibers, which are large-diameter fibers having a myelin sheath, such as nerve sheath **410**, and C fibers, which are small-diameter fibers lacking a myelin coating. These major fiber types also have numerous sub-types. The A and B fibers

typically conduct action potentials at much faster speeds along the nerve than C fibers, and have a lower threshold for the induction of action potentials with an applied electric signal. Typically, the electric signal applied to the exterior of the nerve bundle **300** may at least partially attenuate as it travels radially from the outer surface **340** of the nerve bundle **300** to the inner portion **350** and towards the central axis. Accordingly, axons of a given type near the outer surface **340** are more likely to receive sufficient electrical charge to induce an action potential than are axons in the inner portion **350** of the nerve bundle **300**, with the likelihood of a given electrical charge inducing an action potential in an individual axon decreasing radially from the outer surface **340** to the central axis of the nerve bundle **300**. Embodiments disclosed herein provide for fibrous electrodes that may penetrate the outer surface **340** of the nerve bundle **300** and/or the nerve sheath **410** to enhance delivery of electrical charge to axons near the center of the nerve bundle **300**. In this manner, a greater percentage of various nerve fibers within the nerve bundle **300**, such as the A fibers, the B fibers and/or the C fibers may be targeted and stimulated sufficiently to induce action potentials, as compared to prior art electrodes.

Referring simultaneously to FIGS. 5A and 5B, an electrode assembly including fibers and/or spikes on its inner surface, capable of being engaged to a tissue (e.g., a nerve bundle **300**) of a human body, is provided. FIG. 5A illustrates an electrode assembly **500** in contact with a nerve bundle **300**, in accordance with one illustrative embodiment. FIG. 5B illustrates a helical electrode assembly **500**, wherein an inner surface **540** of a circumneural cathode **560** or a circumneural anode **570** includes a plurality of fibers and/or spikes **550** coupled thereto. The nerve bundle **300** is generally cylindrical and has a central axis. The electrode assembly **500** of FIG. 5A may include a plurality of fiber elements **550** that are coupled to the circumneural cathode **560** or the circumneural anode **570**. The fibers **550** may refer to a plurality of materials that are conductive and suitable for joining to an inner surface **540** of the circumneural cathode **560** or the circumneural anode **570**. The inner surface **540** is suitable for engaging the outer surface **340** of the nerve bundle **300**, while the fibers **550** may engage either the outer surface **340** or the inner portion **350** of the nerve bundle **300**. A fiber **550** may deliver the electrical signals directly to any portion of the nerve bundle **300** with which it comes into contact. In one embodiment, the electrode assembly **500** is a helical shaped apparatus (as depicted in FIG. 5B) that may be wrapped about the nerve bundle **300**. FIG. 5B also illustrates an end member **545** that provides an interface to a lead wire in electrical communication with the IMD. In one embodiment, the electrode assembly **500** includes at least a first circumneural cathode portion **560** and a second circumneural anode portion **570**. The first circumneural portion **560** and/or the second circumneural portion **570** include a plurality of fibers **550** described herein for contacting a portion of the target nerve bundle **300**.

FIG. 5A also illustrates a stylized magnification of a portion of the electrode assembly **500**. In the circumneural electrode assembly **500**, each element **560, 570** may include a number of fibers **550** that protrude outward from the inner surface **540** of the elements **560, 570** and/or from side surfaces **543** of the elements **560, 570** at one or more angles relative to the inner surface **540** or the side surfaces **543**. In one embodiment, the fibers **550** in the inner surface **540** of the electrode may protrude radially inwardly from the inner surface **540** of the element **560, 570** toward the axis of the nerve bundle **300** (as exemplified in FIGS. 5A and 5B). The fibers **550** may be coupled to the electrode assembly **500** in a number of ways, including soldering, micro-welding, using adhe-

sives, photolithography process, and/or various manufacturing techniques, etc. The fibers 550 may be of a flexible configuration, a medium rigid configuration, and/or of a rigid configuration (e.g., a spike). They may also be, in some embodiments, of non-uniform cross-section, e.g., thicker at the proximal end and narrowing at the distal end. The fiber 550 may be a longitudinal element, which may refer to an element whose longest dimension substantially exceeds other dimensions, e.g., length, width, cross-section, etc. Thus, a longitudinal element may include a "fiber" as previously disclosed.

The fibers 550 provide for an electrical path from the IMD 200, through the lead assembly 222, through the elements 560, 570, and onto an inner portion of a nerve bundle 300. More specifically, the electrode assembly 500 provides a path from the fibers 550 and inner surface 540 of the cathode element 560, through the outer surface 340 of the nerve bundle 300 and into the inner portion 350 thereof, through the nerve tissue and into the fibers 550 and inner surface 540 of the anode element 570.

Turning now to FIG. 6, a stylized depiction is provided of a portion of an element 560, 570 of the electrode assembly 500 in contact with a nerve bundle 300. FIG. 6 also depicts a stylized, cross-sectional view of the nerve bundle 300, in accordance with one embodiment. The elements 560, 570 may include an inner surface 540 and a number of fibers 550. For clarity of illustration, the inner surface 540 is shown in only partial contact with outer surface 340 of nerve bundle 300. However, in an actual embodiment, substantially all of the inner surface 540 would engage the outer surface 340 of nerve bundle 300. The fibers 550 may engage either the outer surface 340 or the inner portion 350 of nerve bundle 300. The fibers 550 may penetrate, through migration, the outer surface 340 of the nerve bundle 300 over a period of time (e.g., many days, weeks, etc.). In one embodiment, external force may be applied to prompt the migration of the fibers 550 into the nerve bundle 300. In an alternative embodiment, the electrode assembly 500 may be positioned around the nerve bundle 300 in a manner, such that without applying external force, the fibers 550 may penetrate the outer surface 340 of the nerve bundle 300. In one such embodiment, the electrode elements 560, 570 may include a resilient material, such as a silicone polymer or other known biocompatible materials. The electrode elements 560, 570 may be formed to provide a slight constrictive resilient force on nerve bundle 300 to maintain contact between the electrode element (560, 570) and the nerve bundle 300, and to assist the fibers 550 to penetrate into the inner portion 350 of nerve bundle 300.

In one embodiment, the penetration of the fibers 550 into the nerve bundle 300 may take place at such a rate that trauma to the nerve bundle 300 is eliminated. In yet another alternative embodiment, migration of the fibers 550 may be controlled by electrical means (e.g., by providing predetermined electrical pulses to prompt migration of the fibers 550) such that the fibers 550 may penetrate the outer surface 340 of the nerve bundle 300 substantially without causing excessive damage to the nerve bundle 300. Other means, such as external force, small movement, etc., may be used to cause the penetration of the fibers 550 into the neurons. In still another embodiment, the fibers 550 may be formed of a shape-memory metal, such as Nitinol, and coupled by known means substantially perpendicular to inner surfaces 540 of an electrode element 560, 570. The fibers 550 may then be substantially flattened against inner surface 540 by mechanical means, thereby rendering the electrode element 560, 570 easier and safer to couple to the nerve bundle 300. The shape-memory metal may be fabricated to return to its fabrication

state (i.e., substantially perpendicular to inner surface 540) at a predetermined temperature, e.g., a temperature at or slightly above or below body temperature. Thus, after the electrode assembly 500 is wrapped around the nerve bundle 300, the temperature of the patient's body causes the fibers 550 to return to a substantially perpendicular orientation relative to inner surface 540 to facilitate penetration of the fibers 550 into the inner portion 350 of the nerve bundle 300.

FIG. 6 further illustrates that, in some cases, some of the fibers 550 of the electrode assembly 500 may penetrate various portions of the nerve bundle 300. By providing fibers 550 of differing lengths, nerve fibers at various radial distances from the outer surface 340 may be selectively targeted for stimulation.

FIG. 7 illustrates a stylized, magnified depiction of one embodiment of a fiber 550 of a circumneural cathode 560 or a circumneural anode 570, in accordance with one illustrative embodiment. In some embodiments, the fiber 550 may include a fiber insulation 710 and a conductive portion 720. A segment of the conductive portion 720 may be encapsulated by the fiber insulation 710 such that only the exposed portion of the fiber 550 (i.e., the conductive portion 720) is capable of delivering a stimulation signal. In this manner, penetration to particular radial depths within the nerve bundle 300 may be achieved. For example, referring simultaneously to FIGS. 6 and 7, a fiber 550 that penetrates the outer surface 340 of the nerve bundle 300 and moves into significant proximity of the axons 310 may have an exposed conductive portion 720 that comes into contact with the axons 310. In other words, the remaining portion of the fiber 550 (i.e., the portion from the inner surface 540 of the electrode element 560, 570 through the nerve bundle 300, and to a desired depth within the inner portion 350 of the nerve bundle 300) is insulated and only the tip of the fiber 550 is exposed. Thus, only the axons 310 in the immediate vicinity of the conduction portion 720 of the fiber 550 will be stimulated. Therefore, a specific targeting and/or more effective stimulation, of A-fibers, B-fibers, C-fibers and/or the axons 310 in the inner portion 350 of the nerve bundle 300 may be achieved by insulating portions of the fiber 550 and exposing only the conductive portion 720 to target more specific regions of the nerve bundle 300.

In alternative embodiments substantially the entire length of the fibers 550 may be conductive, and penetration of charge into specific areas of the inner portion 350 of the nerve bundle 300 may be controlled by the distribution and length of the fibers 550.

FIG. 8 illustrates a stylized, magnified, cross-sectional depiction of a portion of the circumneural cathode 560 or the circumneural anode 570 and associated fibers 550, in accordance with an illustrative embodiment. In this embodiment, the inner surface 540 of the circumneural cathode 560 or the circumneural anode 570 may be coated with an insulating material (electrode insulation 810), similar to the insulation 710 on portions of the fibers 550, discussed above with respect to FIG. 7. In this configuration, neither the inner surface 540 of the circumneural cathode 560 or the circumneural anode 570 nor the insulated portions of the fibers 550 provide electrical stimulation to the nerve. Instead, only the conductive portions 720 (i.e., the exposed tips) of the fibers 550 deliver the electrical signal to the nerve bundle 300. Therefore, a more focused delivery of the stimulation signal may be provided to the inner portion 350 of the nerve bundle 300, as opposed to the outer surface 340 of the nerve bundle 300. Thus, portions of the nerve bundle 300 may be specifically targeted without providing stimulation to other portions of a nerve bundle 300. In this manner, focused delivery of stimulation to specific portions of the nerve bundle 300 may

be achieved. Utilizing multiplexing of delivery of the electrical signal, a sequence of targeted electrical signals throughout the nerve bundle **300** may be achieved for increased efficacy and targeted delivery of stimulation signals.

Utilizing embodiments disclosed herein, a more robust delivery of electrical signal/stimulation may be achieved. This may increase efficacy and provide various advantages, such as increased population of nerve fibers being activated by stimulation. Further advantages provided by particular embodiments may include increased population of nerve fibers being accessed for observation during sensing operations. These advantages may lead to a reduction of the power used by the IMD since more direct current electrical signals may be provided.

All of the methods and apparatuses disclosed and claimed herein may be made and executed without undue experimentation in light of the present disclosure. While the methods and apparatus have been described in terms of particular embodiments, it will be apparent to those skilled in the art that variations may be applied to the methods and apparatus and in the steps, or in the sequence of steps, of the methods described herein without departing from the concept and scope of the disclosure, as defined by the appended claims. It should be especially apparent that the principles disclosed may be applied to selected cranial nerves other than, or in addition to, the vagus nerve to achieve particular results in treating patients having epilepsy. More generally, the techniques and apparatus may be applied to any neural structure with regard to which a more controlled delivery of an electrical signal throughout the structure (as opposed to its periphery only) is desired or needed.

The particular embodiments disclosed above are illustrative only and may be modified and practiced in different but equivalent manners apparent to those skilled in the art having the benefit of the teachings herein. Furthermore, no limitations are intended to the details of construction or design herein shown other than as described in the claims below. It is, therefore, evident that the particular embodiments disclosed above may be altered or modified and all such variations are considered within the scope of the disclosure. Accordingly, the protection sought herein is as set forth in the claims below.

What is claimed is:

1. An electrode assembly comprising:
 - an electrode adapted to fully encircle a first longitudinal portion of a target nerve or nerve bundle, said electrode comprising:
 - an inner surface adapted to contact an outer surface of said target nerve or nerve bundle, and
 - a plurality of fiber elements each comprising a proximal end and a distal end, wherein said plurality of fiber elements are coupled at said proximal ends to said inner surface of said electrode and said distal ends of said plurality of fiber elements are operative to penetrate said outer surface of said target nerve or nerve bundle.
2. The electrode assembly of claim 1, wherein said distal ends of said plurality of fiber elements are operative to penetrate said outer surface of said target nerve or nerve bundle by migrating into an inner portion of said target nerve or nerve bundle.
3. The electrode assembly of claim 2, wherein said distal ends of said plurality of fiber elements migrate into said inner portions of said target nerve or bundle in response to one or more electrical pulses provided to the electrode.
4. The electrode assembly of claim 1, wherein said plurality of fiber elements are comprised of a conductive material

including at least one of copper, titanium, an alloy metal, iron, steel, and a carbon-based structure.

5. The electrode assembly of claim 1, wherein each of said plurality of fiber elements comprises an electrically insulated portion proximate to said proximal end and a conductive portion proximate to said distal end, and wherein said electrically insulated portion of each of said plurality of fiber elements is encapsulated with an electrically insulating material and the conductive portion is electrically exposed.

6. The electrode assembly of claim 5, further comprising:

- a second electrode having a second conductive portion disposed on a second inner surface of the second electrode, the second conductive portion operative to contact said outer surface of said target nerve or nerve bundle; and

wherein the plurality of fiber elements of the conductive portion of the electrode are operative to contact an inner portion of said target nerve or nerve bundle.

7. The electrode assembly of claim 6, wherein the conductive portion is operative to provide a first electrical signal to said inner portion of said target nerve or nerve bundle at a first time and the second conductive portion is operative to provide a second electrical signal to said outer surface of said target nerve or nerve bundle at a second time.

8. The electrode assembly of claim 6, wherein the conductive portion is operative to sense a first electrical activity at said inner portion of said target nerve or nerve bundle at a first time and the second conductive portion is operative to sense a second electrical activity at said outer surface of said target nerve or nerve bundle at a second time.

9. The electrode assembly of claim 1, wherein at least a portion of said inner surface of said electrode is substantially nonconductive.

10. The electrode assembly of claim 1, wherein said target nerve or nerve bundle is a cranial nerve including at least one of a vagus nerve, a glossopharyngeal nerve, and a trigeminal nerve.

11. The electrode assembly of claim 1, wherein said plurality of fiber elements comprise a variety of lengths adapted to penetrate a plurality of distances into said target nerve or nerve bundle.

12. The electrode assembly of claim 1, wherein said electrode is operative to apply an electrical signal to said target nerve or nerve bundle to treat at least one of a depression disorder and an epilepsy disorder.

13. The electrode assembly of claim 1, further comprising:

- a second electrode adapted to at least partially surround a second longitudinal portion of said target nerve or nerve bundle, said second electrode comprising:

- an inner surface adapted to contact said outer surface of said target nerve or nerve bundle, and

- a second plurality of fiber elements each comprising a proximal end and a distal end, wherein said second plurality of fiber elements are coupled at said proximal ends to said inner surface of said second electrode and said distal ends of said second plurality of fiber elements are operative to penetrate said outer surface of said target nerve or nerve bundle.

14. The electrode assembly of claim 13, wherein the electrode is a circumneural cathode and the second electrode is a circumneural anode.

15. The electrode assembly of claim 1, wherein the electrode is operative to sense an electrical activity in said target nerve or nerve bundle.

16. The electrode assembly of claim 1, further comprising:

- a non-conductive support member configured to substantially

13

surround the first longitudinal portion of said target nerve or nerve bundle, the electrode disposed on said non-conductive support member.

17. An electrode assembly comprising:
 a circumneural cathode adapted to substantially surround a first longitudinal portion of a cranial nerve; 5
 a circumneural anode adapted to substantially surround a second longitudinal portion of said cranial nerve;
 wherein said circumneural cathode and circumneural anode each comprise: 10
 a first surface adapted to contact said cranial nerve; and
 a plurality of fibers, each of said fibers having a proximal end and a distal end, wherein each of said fibers is coupled to said first surface at said proximal end, said fibers being conductive and adapted to penetrate an outer surface of the cranial nerve. 15

18. The electrode assembly of claim 17, wherein said first surface is a surface of a helical structure adapted to be wrapped around said cranial nerve, wherein at least a portion of said first surface is configured to electrically couple to said cranial nerve. 20

19. The electrode assembly of claim 17, wherein said plurality of fibers are oriented generally perpendicular to said first surface.

20. The electrode assembly of claim 17, wherein said plurality of fibers are comprised of a shape-memory metal configured to return to a desired orientation upon reaching a threshold temperature. 25

21. The electrode assembly of claim 17, wherein said plurality of fibers are comprised of a carbon nanotube structure.

14

22. An implantable medical device system for providing an electrical signal therapy to a patient, the implantable medical device system comprising:

an implantable medical device configured to generate an electrical signal; and

an electrode assembly that, when operatively coupled to said implantable medical device, is operable to provide said electrical signal generated by the implantable medical device to a target tissue, said electrode assembly comprising an electrode adapted to fully encircle a portion of the target tissue, said electrode comprising:

a first surface adapted to electrically couple to an outer surface of said target tissue; and

a plurality of fibers coupled to said first surface, said plurality of fibers being adapted to electrically couple to at least one of said outer surface and an interior portion of said target tissue.

23. The implantable medical device system of claim 22, further comprising a lead assembly, said lead assembly comprising a proximal portion adapted to be connected to the implantable medical device and a distal portion being adapted to be coupled to said electrode.

24. The implantable medical device system of claim 22, wherein said plurality of fibers are configured to migrate into said interior portion of said target tissue.

25. The implantable medical device system of claim 22, wherein said electrode is a circumneural cathode or a circumneural anode.

* * * * *